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**DEVELOPMENT AND EVALUATION
OF AN IMPEDANCE CARDIOGRAPHIC SYSTEM
TO MEASURE CARDIAC OUTPUT
AND OTHER CARDIAC PARAMETERS**

July 1, 1967 to June 30, 1968

Performed under Contract No. NAS 9-4500

by

University of Minnesota

Minneapolis, Minnesota

for

NATIONAL AERONAUTICS AND SPACE ADMINISTRATION

Manned Spacecraft Center

Houston, Texas

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by

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D. A. Witsoe, M.E.E., and R.P. Patterson, M.E.E.,
Co-Investigators

University of Minnesota College of Medical Sciences
Minneapolis, Minnesota

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The main objective of the last year's work was to obtain a scientific evaluation, outside of the University of Minnesota, of the Impedance Cardiograph as a means to determine cardiac output, stroke volume and other cardiac parameters. This will then provide a wider spectrum of experience and opinion upon which to base a final decision as to the use of the system during space flight.

It is with great gratitude that the cooperative efforts of the investigators, known and unknown, who have participated in this work is acknowledged.

The need is enormous for a non-invasive means to obtain information relative to cardiac function. In clinical applications it would greatly expand the range of patients that could be studied, since in many cases the surgical insertion of catheters is not justified. The same is especially true of research applications where catheterization can only be justified in unusual situations.

The work reported here has advanced the understanding of the use and limitations of the Impedance Cardiograph. Much research is still needed to build up a body of knowledge and experience to fully appreciate the potential value of the system. Similar to the history of the electrocardiograph, it probably will take years to acquire sufficient information to combine precise scientific knowledge with empirical observations into a widely acceptable clinical and research tool. New concepts must be developed to advance from measurements of cardiac output to the more intimate mechanisms of myocardial function. The Impedance Cardiograph holds great promise in this area.

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Part I

The following portion of this report was presented by invitation at two symposia. The first was held during the annual meeting of the American Association for Medical Instrumentation in Houston, July 1968. The second time was an Aerospace Medicine Symposium held as part of The International Congress of Chest Physicians in Washington D.C., October 5, 1968. In both events Dr. Charles Berry was the moderator. In each case there was evidence of considerable interest in this area judging from the response from the audience and the requests for reprints and other information. Interest has ranged from questions concerning various clinical applications to research applications such as use in high performance aircraft and the possible use on parachute jumpers during free fall. In the latter case, use of the miniature units developed for space flight were suggested with an appropriate telemetry system. In the other applications the standard Impedance Cardiograph developed in our laboratories would meet the requirements for hospital and aircraft applications since the device can operate on 115VAC, (50-400) Hz at about 25 watts. Total volume of the unit is approximately 0.75 cubic foot and weighs 16 pounds. This should be suitable for most aircraft applications.

THE IMPEDANCE CARDIOGRAPH AS A NON-INVASIVE MEANS
TO MONITOR CARDIAC FUNCTION

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A four electrode Impedance Cardiograph has been developed to meet a need in clinical medicine and research laboratories for a simple, bloodless method of monitoring various parameters of cardiac function without penetrating the skin (Fig. 1). Previous work in this laboratory has been directed toward an effort to equate the small thoracic impedance changes observed during the cardiac cycle to ventricular stroke volume and cardiac output in human beings. The following equation was used for stroke volume:

$$\Delta V = \rho \frac{L^2 T}{Z_o^2} (dZ/dt)_{\min}$$

ΔV = ventricular stroke volume (cc)

ρ = the electrical resistivity of blood at 100 kHz
(average value 150 ohm-cm)

L = the mean distance (cm) between the two inner
electrodes
(2 and 3) (measured front and back) Fig. 3

Z_o = the impedance, in ohms, between the two inner
electrodes (2 and 3) Fig. 3

$(dZ/dt)_{\min}$ = ohms per second (Fig. 6)

T = ventricular ejection time in seconds (Fig. 6)

Cardiac Output = stroke volume x pulse rate.

Thus far this has met with limited success due to a variety of technical difficulties (1,2,3). Valvular disorders frequently make this calculation difficult due to distortions of the waveforms (Fig. 7).

The purpose of this investigation was to evaluate the Impedance Cardiograph as a non-invasive method to monitor certain parameters related to cardiac dynamics.

Methods and Procedure

Four aluminized Mylar strips attached to an adhesive tape backing are placed around the subject as shown in Fig. 1. Two strip electrodes are placed around the neck separated as far as possible. A third electrode is placed around the thorax at the level of the xiphisternal joint and a fourth electrode around the lower abdomen. A harness to support the cables connecting the electrodes to the impedance system was developed for use during various activity experiments (Fig. 2). A schematic diagram of the main elements of the Impedance Cardiograph is illustrated in Fig. 3. Electrodes 1 and 4 are attached to a constant current oscillator supplying alternating current at 100 kHz at approximately 4 ma. The impedance between electrodes 2 and 3 then produces a voltage proportional to the total impedance between impedance between electrodes 2 and 3. This total impedance has been labeled as Z_0 . This impedance is usually in the range of about 25 ohms. During the cardiac cycle this impedance changes by approximately .1 to .2 ohms (ΔZ). Two differentiators are built into the system to provide the first and second time derivatives of ΔZ . The value of Z_0 is read out automatically on a digital display on the front panel of the instrument (Fig. 4). The other outputs (ΔZ , dZ/dt , d^2Z/dt^2) are fed into any suitable strip chart recorder or a tape recorder. The solid state circuitry and output terminals are shown in Fig. 5. A typical recording taken on a normal young adult is shown in Fig. 6. Heart sounds, ΔZ , dZ/dt , and the ECG were recorded to illustrate the impedance events in their time relation to the cardiac cycle.

From such a recording, the (R-Z) interval, the ventricular ejection time (T) and the peak value of the first derivative $(dZ/dt)_{\min}$ can be determined. The heart sounds are frequently helpful in confirming the ejection time. ΔZ was recorded since it has been observed that valvular disorders such as mitral valve insufficiency produce distortions in the waveform of ΔZ and consequently (dZ/dt) , Fig. 7.

The peak negative value of the first derivative, $(dZ/dt)_{\min}$, has been observed to occur simultaneous with the peak ejection rate of the left ventricle in experiments on anesthetized dogs in our laboratories (1967 Final Report). Also, in these experiments the magnitude of $(dZ/dt)_{\min}$ varied in a linear fashion with variations in peak ejection rate. The (R-Z) interval includes the factor of cardiac contractility as described by Siegel, et al. (4,5) which involves the time from the R spike to the intraventricular $(dP/dT)_{\max}$, as well as the time for the ventricles to reach maximum ejection rate. If future work confirms these findings, the Impedance Cardiograph can then provide a simple, non-invasive means to determine overall myocardial function. In resting, young healthy adults the (R-Z) interval has been recorded from 110 to about 150 msec, with exercise this may be reduced to 60 to 90 msec. In healthy resting young adults, $(dZ/dt)_{\min}$ has been noted in the approximate range of 1.4 - 1.9 ohms per second. With exercise this value can increase to over three ohms per second. In three patients diagnosed as cardiomyopathy, $(dZ/dt)_{\min}$ was found at approximately one ohm per second (.9 - 1.2). In another case with a severe ventricular

septal defect $(dZ/dt)_{\min}$ was recorded at 4.6 ohms per second. The (R-Z) interval was 60 msec. The ventricular ejection time has also been found to vary in relation to pulse rate.

Another clinical application of the Impedance Cardiograph has been as a monitor of cardiac function without measuring the various parameters described. The visual observation and comparison of a series of impedance cardiograms following cardiac surgery has provided the surgical staff a rapid and convenient means to follow the patient's recovery. Two examples are shown in figures 7, 8 and 9. Recordings of the heart sounds and (dZ/dt) on a patient in which the suture line holding an artificial mitral valve had opened are shown in figure 7. The pre-operative waveform of both ΔZ and (dZ/dt) were greatly distorted due to the regurgitation of blood around the mitral valve. Two hours following repair of the valve the (dZ/dt) waveform approximated a normal waveform except that the value of $(dZ/dt)_{\min}$ was very small indicating a very feeble ventricular ejection. This correlated with the clinical observation of a critically ill patient very near a shock status. Twenty-four hours later it can be seen that the ventricular ejection was much stronger as indicated by the increase in the height of (dZ/dt) and with the waveform improving more toward the normal characteristics. This again correlated with the clinical observations that the patient had improved but was still considered critical.

In order to assess the value of impedance measurements in patients with severe cardiac abnormalities, post-operative records were taken on a patient who had received three artificial valves

and had an extremely enlarged heart. Figure 8 is a photograph of a post-operative chest x-ray of the patient showing the three artificial valves (mitral, tricuspid, and aortic) as well as the greatly enlarged heart. Recordings of the (dZ/dt) impedance waveform taken two hours, twenty-four hours, and seventy-two hours post-operative are shown in Fig. 9. The two hours post-operative record indicates an irregular heart rate and small amplitude but typically formed (dZ/dt) waveform. By 24 hours post-operative, the heart rate had become more regular and some increase in the (dZ/dt) amplitude is seen. For the records shown in Fig. 9, the average two hour post-operative heart rate was 150 bpm, 24 hours 77 bpm and 72 hours 81 bpm. With increased pulse rates in normal subjects we have noted a diminished amplitude of (dZ/dt) tracings for relatively constant cardiac output, thus the small amplitude signals of the two hour post-operative measurement when compared to the 24 hour post-operative measurement could be due in part to the differences in pulse rates. It is of interest to note, however, that the pulse rates at 24 hours and 72 hours post-operative were approximately the same; while the 72 hour (dZ/dt) waveform had a considerably larger amplitude indicating a more forceful ventricular ejection and an increased stroke volume. Significantly, the patient's clinical appearance had greatly improved at 72 hours as he was sitting up in bed and talking with the nurses.

Although the records shown on one patient do not provide conclusive proof for all cases, it is apparent that the metal valves and enlarged heart did not affect the origin of the ΔZ

waveform or the response of the waveform to increases in quality of cardiac functions such as contractility and cardiac output. Also, examination of the (dZ/dt) waveform only, without computation of stroke volume and cardiac output, provided the surgeons with a quick and convenient means to assess cardiac function without the additional surgical trauma associated with the dye dilution or similar techniques for measuring cardiac output.

Discussion

It appears that with additional clinical experience and basic research that the Impedance Cardiograph will become a very useful means to obtain information relating to cardiac function without penetrating the skin in both clinical and research applications. In addition, preliminary observations indicate that the system should be of value in certain pulmonary diseases. The value Z_0 is a measure of the total impedance from the base of the neck to the xiphisternal joint. In the event of pulmonary congestion or edema, the value of Z_0 will be low due to a greater conductivity through the chest. The converse is true with increasing volume of air in the chest. The ratio of L^2/Z_0^2 corrects for variations in distance between the electrodes (2 and 3), Fig. 3. It appears that this ratio will be of value in following certain chest diseases without penetrating the skin and with a reduced number of chest x-rays.

Summary

1. The Impedance Cardiograph as described here is a device capable of providing information concerning the mechanical function

of the heart without penetrating the skin. The entire procedure is comparable to that of recording the electrocardiogram. The system creates no hazard nor discomfort to the patient or experimental subject. The procedure to obtain the impedance information is simple, convenient and inexpensive, suitable for any clinical or research application.

2. The device can be used in a variety of applications.
 - a. Various parameters of cardiac function can be calculated or measured for a permanent record providing the heart valves are intact.
 - b. Serial recordings on a strip chart can provide the physician with a rapid and easy means to monitor cardiac function. These signals are also suitable for display on cathode ray tubes in a cardiac monitoring center. One such application would be the simultaneous display of (dZ/dt) and the electrocardiogram. Thus any discrepancies between ventricular ejection and the ECG would become apparent.
 - c. Valvular disorders produce changes in the waveform of both ΔZ and (dZ/dt). This shows promise of value as a diagnostic aid. Unfortunately this also makes calculation of stroke volume difficult if not impossible.
 - d. The electrodes are disposable, comfortable and have been left in place up to four days without difficulties.
3. Further investigation of the Impedance Cardiograph is needed to determine the full significance and usefulness of the system. The cardiac parameters observed in this study should also be

recorded during prolonged space flight. If this is not possible, at least pre and post flight recordings should be made.

1. Electrical impedance plethysmography. Nyboer, J., and C.C. Thomas. Springfield, Illinois.
2. Principles of applied biomedical instrumentation. Geddes, L.A. and L.E. Baker. John Wiley & Sons Inc. New York, New York.
3. Development and evaluation of an impedance cardiac output system. Kubicek, W.G., J.N. Karnegis, R.P. Patterson, D.A. Witsoe and R.H. Mattson. Aerospace Medicine, Vol. 37, No. 12, Dec. 1966.
4. The quantification of myocardial contractility in dog and man. Siegel, J.H., E.H. Sonnenblick, R.D. Judge, and W.S. Wilson. Cardiologia 45:189-220, 1964.
5. The quantification of myocardial contractility by impedance plethysmography. Siegel, J.H. and M. Fabian. Fed. Proc. March-April 1968, Vol. 27, page 445.

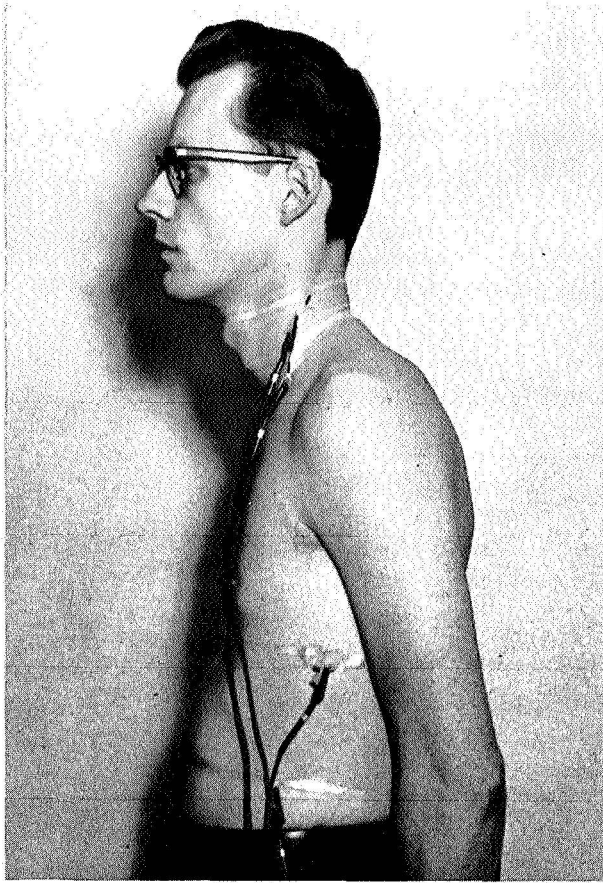


Fig. 1 The disposable electrodes made of aluminized Mylar strips on an adhesive tape backing are shown with the lead wires from the impedance system attached.

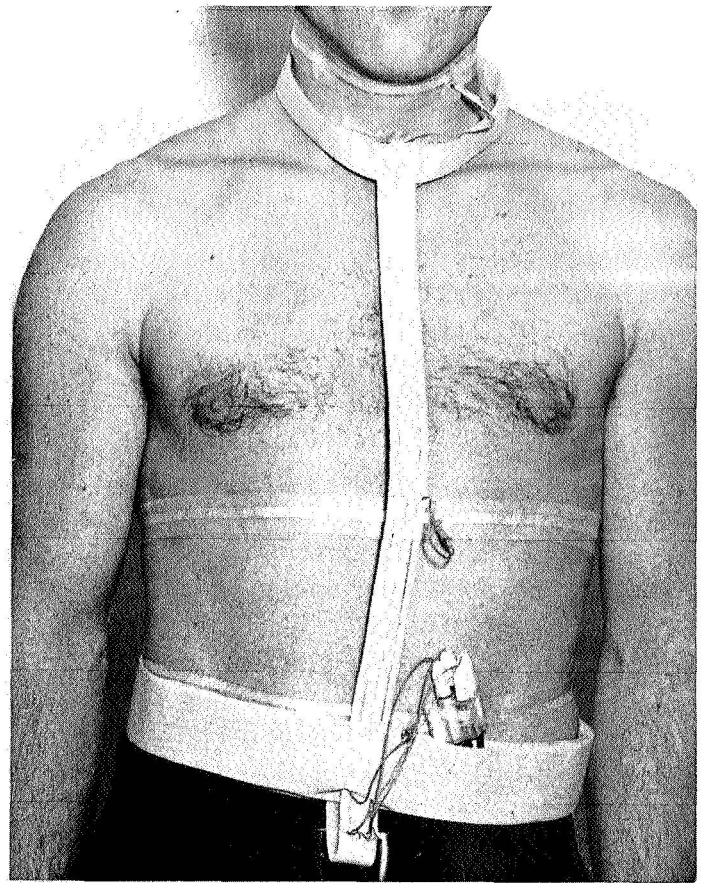


Fig. 2 A view of the Velcro harness to support the connecting cables.

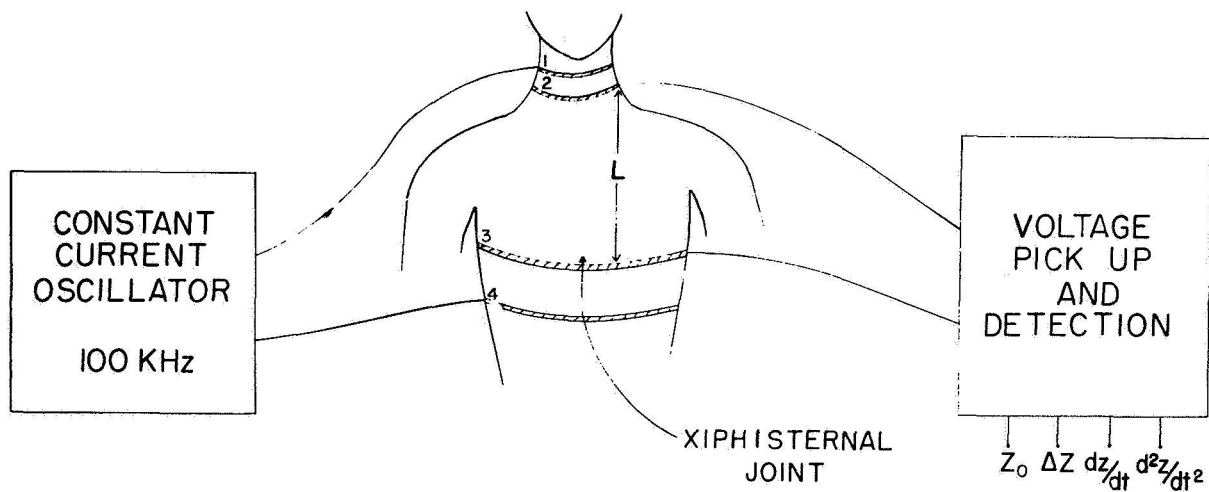


Fig. 3 A schematic diagram of the main elements of the Impedance Cardiograph connected to the electrodes shown in Fig. 1.



Fig. 4 The front panel of the Impedance Cardiograph showing the controls and the automatic digital display of Z_0 .

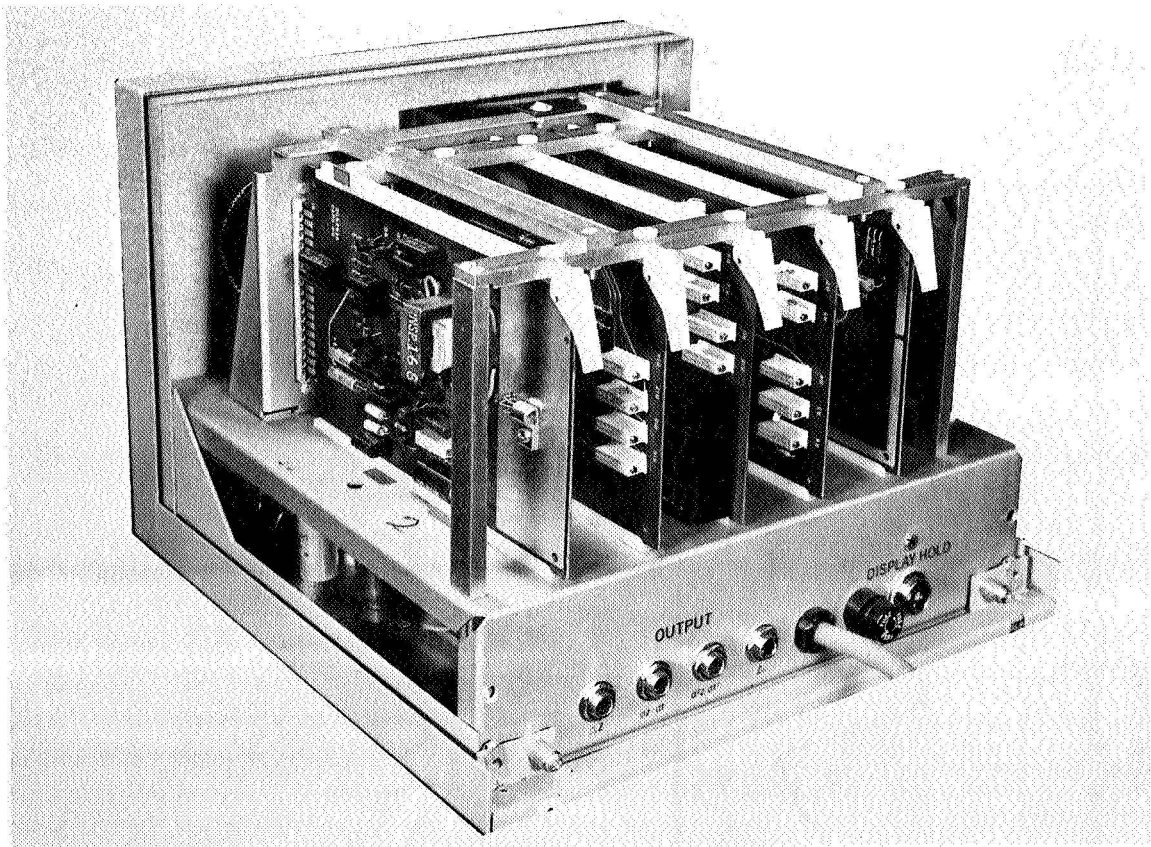


Fig. 5 A view of the solid state circuitry and output terminals.

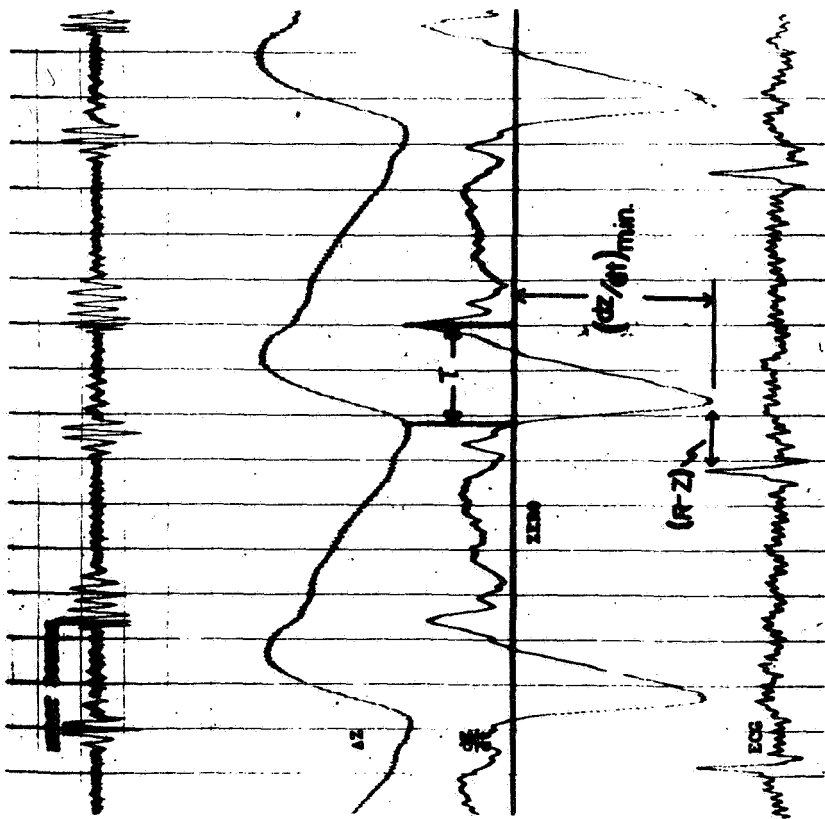


Fig. 6 A record of heart sounds, ΔZ , (dZ/dt) and the ECG taken on a normal adult. The ventricular ejection time (T), the (R-Z) interval and $(dZ/dt)_{min}$ are shown. Time marks 100 msec.

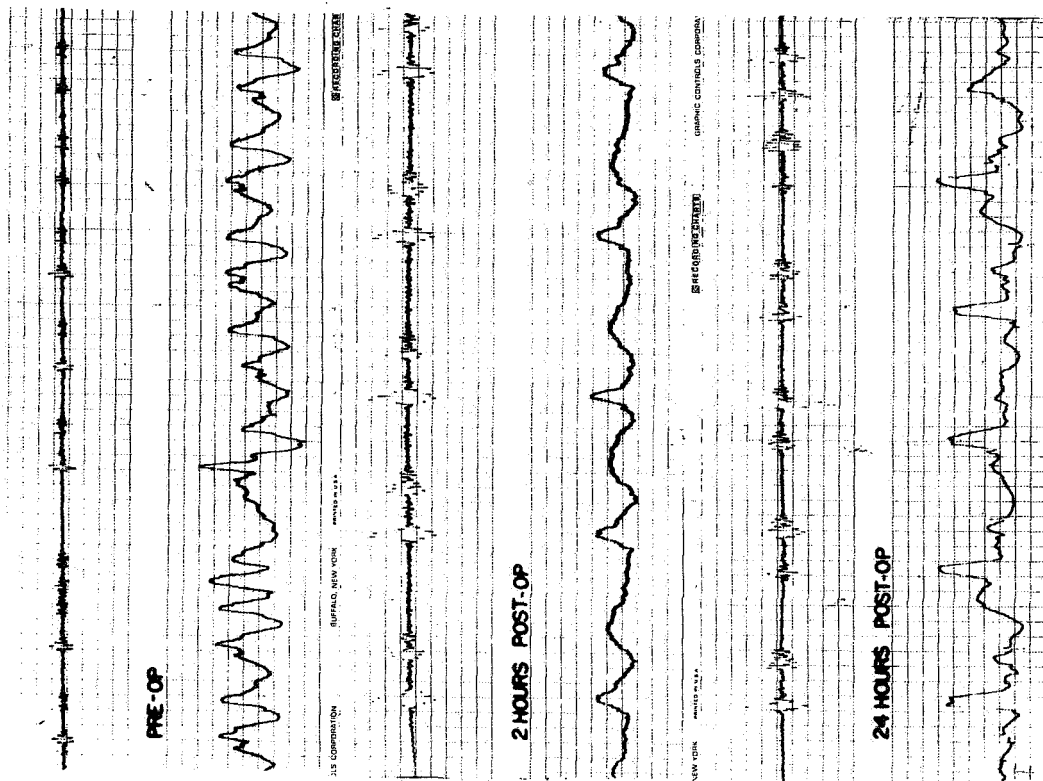


Fig. 7 Recordings of heart sounds and (dZ/dt) taken before and following surgery to repair a leak around an artificial mitral valve. Time marks 100 msec.

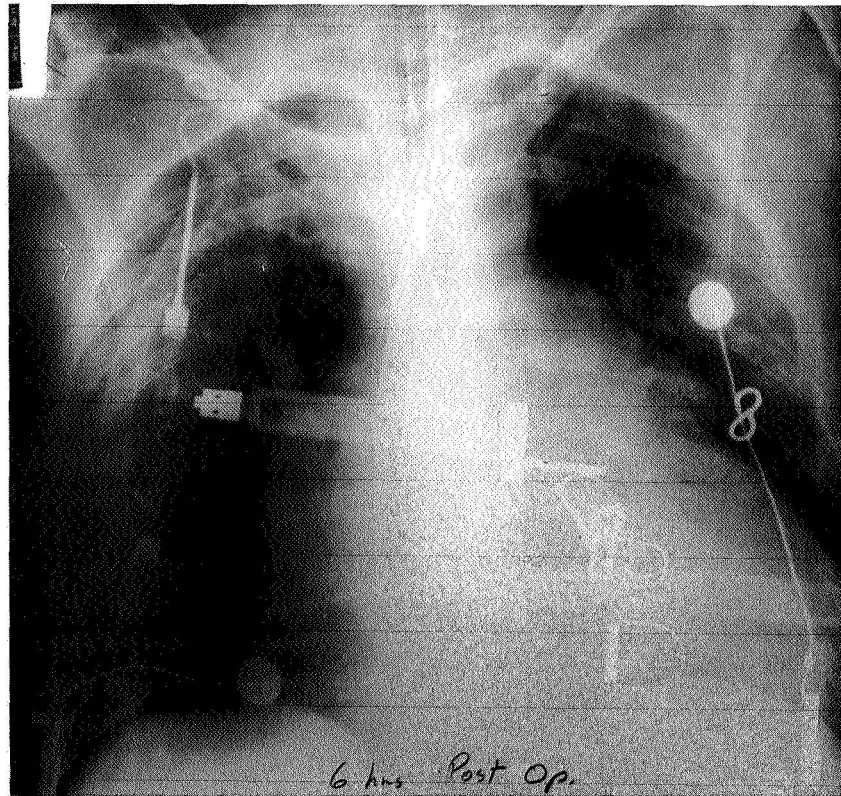


Fig. 8 A chest x-ray showing an enlarged heart with three artificial valves (mitral, tricuspid and aortic).

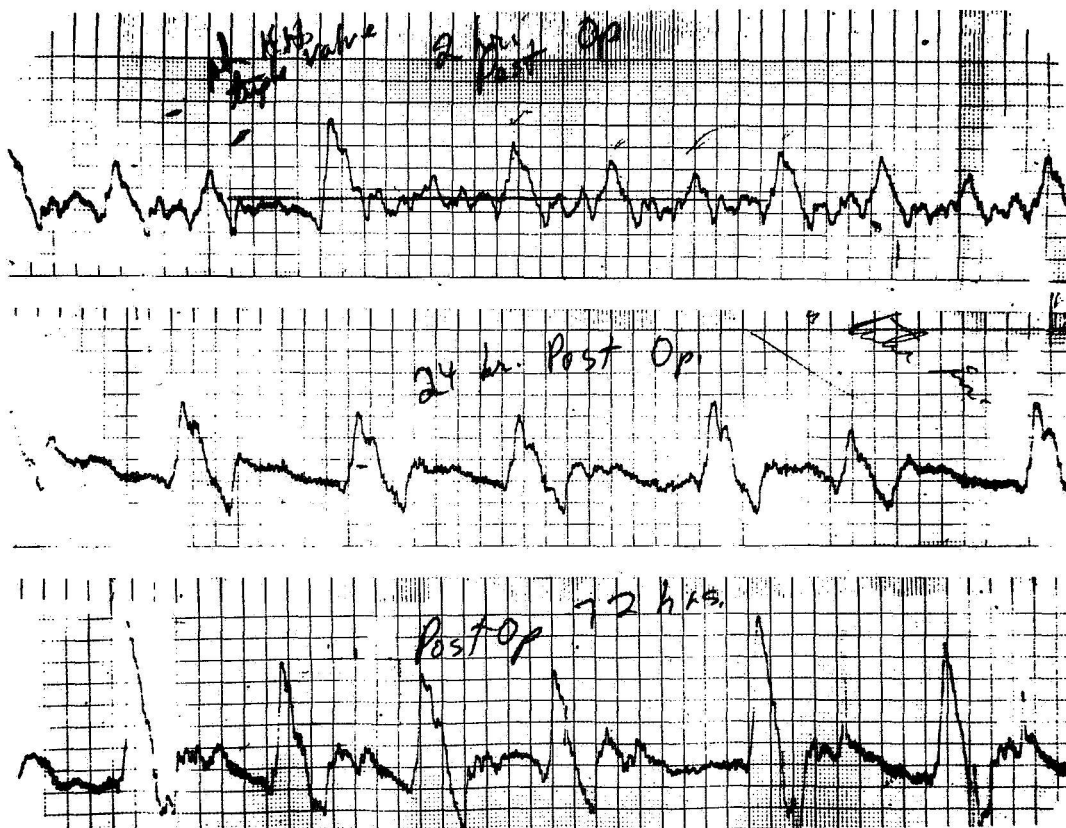


Fig. 9 Recordings of (dz/dt) , two, twenty-four and seventy-two hours following surgery to insert the valves shown in Fig. 7. Time marks 100 msec.

PART II

A COMPARISON STUDY OF SIMULTANEOUS CARDIAC OUTPUT DETERMINATIONS
BY THE IMPEDANCE METHOD AND INDICATOR DILUTION TECHNIQUE
OR THE FICK METHOD

Following pages display the name and address of the principal investigators who have conducted comparison studies between the impedance and indicator dilution techniques and have submitted data. On the opposite page is a brief description of their experimental design. In addition, Dr. Loren Heather, Orange County Medical Center, Orange, California and Dr. Homer Warner, Latter-Day Saint's Hospital, Salt Lake City, Utah have similar projects under way but have not as yet submitted data. All of these investigators are to be commended for their work in a very short time. In most cases the Impedance Cardiograph was delivered to these centers in the late fall of 1967 or winter of 1968. Dr. Smith and his colleagues at Marquette University obtained a unit on loan for four months this past summer. The listing of the principal investigators is according to the person responsible for acquisition of the Impedance Cardiograph. The listing, undoubtedly, does not do justice to the many colleagues associated with each project.

Dr. Smith submitted a detailed report along with their data. This report is intended as a first draft of a manuscript for publication. Dr. Greenfield submitted a reprint of published data along with additional data subsequent to the publication. These two reports are included in their entirety.

These data are not included in the following group.

The other investigators submitted an amazing amount of data in a very short time. Consequently only a brief description of the details of each study is available. All data are tabulated as submitted from each laboratory. In addition, we have computed impedance to standard method ratios of cardiac output. When possible we also calculated the mean of these ratios for each individual or each patient. The mean ratio was then used to correct the impedance cardiac output values. Each set of data was then plotted in two ways; a) the absolute values as submitted from each laboratory and b) the individual corrected impedance values plotted against the values by the standard method. A total of 220 simultaneous comparison values were obtained from these laboratories. These points are presented in a combined graph in figure II-1 and the combined graph with the individual corrected impedance values are presented in figure II-2. This procedure was used in order to provide a rapid picture of the comparison data. It has been suggested that the impedance method would improve in its usefulness if even one or two simultaneous determinations of cardiac output by the impedance method and by some standard method could be obtained to first, in effect, calibrate the individual. This should then improve the reliability of the impedance method for prolonged observation of cardiac output and relative changes in cardiac output in situations where catheters could not be maintained in place for long periods of time.

An extensive statistical study of these data has not been

attempted since a symposium is planned where each investigator will be invited to present his own data in more detailed form. Most investigators have indicated that more data will be available at a later time.

It has become apparent that certain valvular disorders may distort the ΔZ and consequently the (dZ/dt) waveform and thus make the calculation of stroke volume by the impedance method difficult. Consequently some of the data presented may have been altered by these difficulties.

In other cases no obvious reason could be presented for the differences between the impedance and standard method values of stroke volume or cardiac output.

Dr. Smith et al. reported a high correlation between the absolute values of cardiac output by the impedance and dye dilution methods during passive tilt experiments. Their normalized data do not show as good a correlation as the absolute values. If the mean of the Z to Dye ratios had been used rather than the first values in each experiment the effect of random variations may have been reduced.

As indicated by Dr. Greenfield and others, more research and experience is needed to improve the formula used to calculate stroke volume by the impedance method.

An enormous need still exists for a simple atraumatic technique to determine several parameters of cardiac function. Further investigation of all possible applications of the impedance system to cardiovascular physiology is justified in view of the progress that has been made during a very brief field trial.

<u>Principal Investigator</u>	<u>Center</u>
1. Dr. Robert S. Eliot Division of Cardiology	University of Florida Gainsville, Florida
2. Dr. Joseph C. Greenfield, Jr. Applied Physiology Laboratory	Durham V.A. Hospital Durham, North Carolina
3. Mr. William Judy, formerly of Department of Physiology	Baylor University Houston, Texas
4. Dr. J.N. Karnegis, Director Cardiac Catheter Laboratory	Miller Hospital St. Paul, Minnesota
5. Dr. Thomas Killip, <u>et al.</u> , Head, Section of Cardiology	Cornell Medical Center New York, New York
6. Dr. Ronald Lauer Department of Pediatrics	U. of Kansas Medical Center Kansas City, Kansas
7. Dr. Wayne Martin Dept. of Anesthesiology	U. of Washington Medical School Seattle, Washington
8. Dr. James Ronan Division of Cardiology	Georgetown U. Medical Center Washington, D.C.
9. Dr. J. H. Siegel & M. Fabian Department of Surgery	Jacobi Medical Center Bronx, New York
10. Dr. James J. Smith <u>et al.</u> Departments of Physiology & Mechanical Engineering	Marquette University Milwaukee, Wisconsin
11. Dr. J. Richard Warbasse, <u>et al.</u> Chief, Cardiovascular Service & Laboratory	U.S. Public Health Service Hospital Baltimore, Maryland

<u>Standard Method Utilized</u>	<u>Intervention</u>	<u>Material</u>
Cardiogreen indicator dilution	Isuprel infusion	patients
Pressure gradient technic for instantaneous S.V. Car- diogreen indicator dilution	Electrical pacing Isoproterenol infusion	patients
Isotope indicator dilution	Supine bicycle exercise	volunteers
Direct Fick Cardiogreen indicator dilution	Supine bicycle exercise Isuprel infusion	patients
Cardiogreen indicator dilution	Electrical pacing	patients
Direct Fick	Isuprel infusion	patients
Cardiogreen indicator dilution	Anesthetized patients- effect of nitrous-oxide on halothane anesthesia	patients
Cardiogreen indicator dilution	Shock Isuprel infusion Angiotension	patients
Cardiogreen indicator dilution	Isuprel Inhalation-100% O ₂	patients
Cardiogreen indicator dilution	70° passive tilt	volunteers
Cardiogreen indicator dilution	Supine bicycle exercise Isuprel infusion	patients

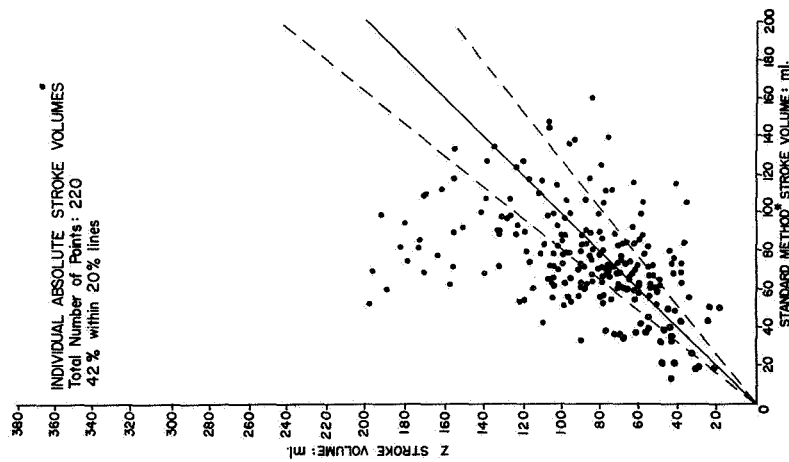


Fig. II-1 A composite graph of all of the stroke volume values obtained by the Impedance method plotted against the values of stroke volume obtained by the Dye, Fick or Isotope dilution technique

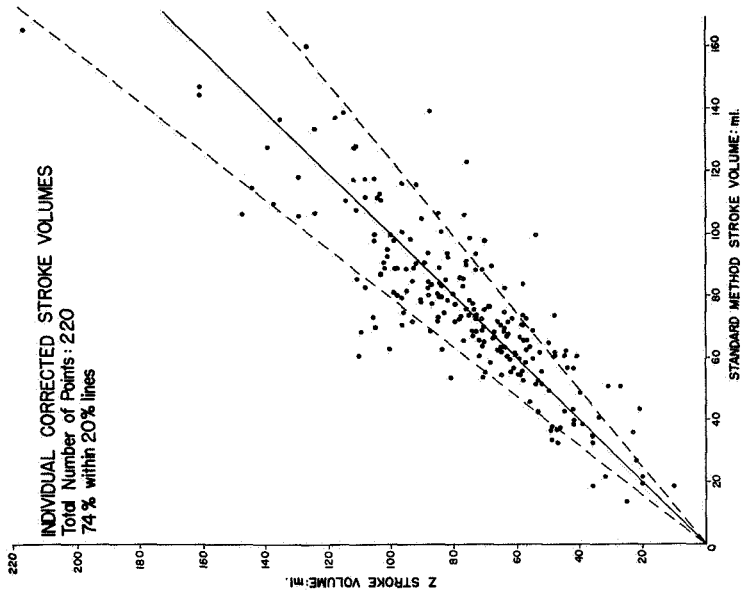


Fig. II-2 A composite graph of the corrected stroke volume values obtained by the Impedance method plotted against the original values of stroke volume obtained by one of the standard methods

The Application of Impedance Cardiography
to the Study of Postural Stress in the Human

John E. Bush, Ph.D., V. Thomas Wiedmeier, Ph.D.,
Felix E. Tristani, M.D. and James J. Smith, M.D., Ph.D.

From the Department of Physiology, Marquette School of Medicine,
Department of Mechanical Engineering, Marquette University,
and the Section on Clinical Hemodynamics,
Wood Veterans Administration Hospital
Milwaukee, Wisconsin

A TRIBUTE

Dr. John E. Bush, age 33, Associate Professor of Engineering and senior author of this paper died in a hunting accident on October 13, 1968. This project, on which he worked with infectious enthusiasm, was carried out with spirit, thoroughness and imagination and with his characteristic zeal for getting at the root of the problem.

From the give and take in the research lab, from the joint efforts to get the data and the often noisy discussions of what the data really meant, he came through to us as a person unfailingly considerate of his fellow man, with little pretense and much compassion.

Accordingly, we who knew him and worked with him are proud to dedicate our continuing efforts in this project to John Bush--scientist, colleague, friend.

It is our intent in the following to document our experience with the Minnesota Impedance Cardiograph during a study of human responses to graded circulatory stress and specifically to a standard head-up tilt test.

The two main components of any circulatory response are central or cardiac, and peripheral. The scarcity of practicable methods for the measurement of stroke volume and cardiac output is well known; even scarcer are methods which are applicable to intact, unanesthetized human subjects during the application of stress.

Although transthoracic impedance has been previously suggested for the biological measurement of volume and flow, particularly in respiration (1,2), only recently has a serious effort been made by Kubicek, Kinnen and their colleagues (3,4,5,6) to adapt electrical impedance to cardiography. These studies have indicated that upon the passage of a constant sinusoidal current across the chest there are impedance changes which are synchronous with the cardiac cycle and that the first derivative of the main impedance wave seems to be a predictable function of aortic blood flow (3). Comparison of impedance-calculated cardiac output with a standard dye-dilution method yielded good agreement in the case of the dog (4) and satisfactory correlation in the human (3).

However, recent evidence on the validity of the impedance method in cardiography has been somewhat conflicting. Harley and Greenfield (7) tested the Minnesota instrument in normal individuals and cardiac patients

and found the impedance-calculated output relatively unsatisfactory, at least in certain cardiac disorders; they added however that the method has potential value and deserved further evaluation. Hill *et al.* presented a rather gloomy picture of the usefulness of electrical impedance plethysmography, primarily on theoretical grounds (8).

On the other hand, Coleman *et al.* (9) found impedance cardiography to be a useful tool in their study of cardiodynamic responses of the human to heat and reported good agreement in the dog between the impedance-predicted cardiac output and aortic flow as determined with the electromagnetic flowmeter. Siegel and Fabian (10) believe that the first derivative of the impedance wave (dz/dt) provides valuable information on the development of ventricular pressure (maximum dp/dt) and suggested that this parameter may be a valid estimate of myocardial contractile force in the intact animal or human; this possibility was originally suggested by Kubicek (4). Recent reports by Namon and Gollan (11,12) have further indicated that, in the dog, the transthoracic impedance was an effective measure of stroke volume and that in their view the reactive impedance component is considerably more useful in this regard than the resistance fraction.

The possible utility of a non-invasive and easily adaptable method of measuring cardiac output in the intact human prompted us to conduct the present investigations with two primary objectives in mind: 1) To determine the validity of the transthoracic impedance method for the measurement of cardiac output in the intact human and 2) to determine its usefulness in studying the response of the cardiovascular system to a standardized postural stress.

Methods and Procedure

The present study was carried out in three phases:

Series I: *The Determination of the Validity of the Impedance Method for Cardiac Output*--Eight normal male subjects, 20-26 years of age, were used in these experiments. Simultaneous cardiac output determinations were made with dye-dilution and the impedance method in the supine position, at various stages of a 20-minute, 70° head-up tilt, and during the subsequent supine recovery period. In this series, the subject when tilted stood on a footboard, i.e., the body weight was transmitted to the feet.

These experiments were performed in the Catheterization Laboratory of the Research Service of the Veterans Administration Hospital under the direction of Dr. Tristani. After infiltration of local anesthetic, a disposable polyethylene needle was inserted into the right brachial artery and a venous catheter into a right antecubital vein. Indicator-dilution curves were obtained following bolus injection of 5 mg of Indocyanine green into the antecubital vein while continuously withdrawing blood from the arterial needle through a Gilford pump and a Gilford densitometer. The curves were inscribed on an Electronics-for-Medicine DC amplifier and recorder. Cardiac output was calculated using the standard Stewart-Hamilton method. The transthoracic impedance wave and the first derivative of the impedance wave were simultaneously recorded on the same instrument.

Series II: *A Study of Cardiorespiratory Responses to Postural Stress with Hip Suspension*--In these experiments, normal males, 20-26 years of age, were subjected to a 20-minute vertical tilt involving

pelvic suspension on a bicycle seat; the legs of the subject were unsupported. The seat was fixed to the tilt table so the subject could be passively shifted from the supine to the suspended position. Twelve experiments were done on eight subjects; in four cases, the test was repeated in the same subject at an interval of about one week in order to study the repeatability of the responses. In this series, precordial ECG and tachograph (Model SP4, Grass Instrument Co., Quincy, Mass.) recordings were made in addition to impedance. Systolic and diastolic blood pressures were automatically recorded through a microphone pickup of the Korotkoff sounds as previously described (13). Pulmonary alveolar CO_2 tension was monitored with a Beckman gas analyzer (Spinco Model LB-1), ventilatory volume with a wide bore, low resistance, differential pressure gas flowmeter and respiratory rate by fluctuations of this flowmeter record. All of these variables were recorded simultaneously on two Grass Polygraphs (Model 5, Grass Instrument Co., Quincy, Mass.).

Series III: A Study of Impedance Cardiographic Responses to Postural Stress in the Passively Tilted, Standing Subject--In this series, normal males, 20-26 years of age, were placed in a 70° head-up position with body weight transmitted to the feet. The procedure for this series was similar to that in Series I except that no arterial or venous punctures were made.

In all experiments, the general procedure was similar to that previously described (13), i.e., the room was darkened and kept quiet, the subject was instructed to keep his eyes closed and relax and the room temperature was held at $75 \pm 3^\circ\text{F}$. The signal from the cardiograph

was recorded at several minute intervals throughout the test; during recording of the impedance signal, the subject was instructed to "exhale in the ordinary way and hold the breath without bearing down". This was done to minimize the effect of respiration on the impedance signal as recommended by Kubicek (4) and to reduce the tendency of the subject to a Valsalva maneuver.

Impedance Recordings

The Minnesota Impedance Cardiograph, Model 202, used in this study is a four-electrode, impedance plethysmographic system developed to monitor left ventricular output (4). Two band electrodes (3M tape) were placed around the subject's neck and separated by 2 cm; a third was placed around the thorax 1 cm below the xiphisternal joint, and the fourth around the lower abdomen. The electrode placements are illustrated in Figure 1. The upper neck and abdominal electrodes were excited by a 100 KHZ constant sinusoidal current and the resulting voltage (proportional to the magnitude of impedance changes) was monitored from the inner two electrodes. Previous work has indicated that the first derivative of the impedance signal is functionally related to the stroke volume of the heart. Kubicek states that the relationship appears to be more consistent for relative changes than for absolute determinations (4); hence, in most of our studies relative (normalized) impedance values are presented as well as the absolute values.

The form of the impedance signal as recorded from the cardiograph is shown in Figure 2. The right half of the recording contains the calibration signals and the left half contains the actual impedance signal. The upper channel shows the change in thoracic impedance (ΔZ)

while the middle channel indicates the time derivative of the impedance wave, i.e., dz/dt . On the lower channel is the ECG from modified bipolar chest leads. The method recommended for calculating stroke volume in milliliters involves the following equation (4):

$$\Delta V = \rho \frac{L^2}{Z_0^2} T \left| \frac{dz}{dt} \right|_{\max} \quad [1]$$

where ρ = blood resistivity (= 150 Ω -cm)
 L = mean distance between inner electrodes (cm)
 Z_0 = basic impedance between the two inner electrodes
 T = ventricular ejection time as described in Figure 2
 $\left| \frac{dz}{dt} \right|_{\max}$ = magnitude of peak value of impedance signal (see Fig. 2)

The above equation is based on a model which assumes that the change in the impedance signal is due to a change in volume of a cylinder of blood of length, L (pure resistance), which conducts current in parallel with the other thoracic elements. For calculating relative changes in stroke volume, Eq. 1 is normalized with respect to a reference value, $[\Delta V]_r$ so that

$$NSV = \frac{\Delta V}{[\Delta V]_r} \quad [2]$$

Similarly, the normalized cardiac output (NCO) is calculated as:

$$NCO = \frac{\Delta V \times HR}{[\Delta V \times HR]_r} \quad [3]$$

where HR is the heart rate.

The values for T , $\left| \frac{dz}{dt} \right|_{\max}$ and HR used in the above equations were taken from the impedance signals and averaged for five heart beats whenever possible. The impedance signals were recorded at 2-3 minute intervals at a paper speed of 50 mm/sec. In most cases, the reference values, $[]_r$, are averages of the last readings prior to tilting.

Results

Series I: Validity of the Impedance Method

Values obtained during simultaneous determinations of stroke volume (SV) and cardiac output (CO) are plotted in Figures 3 and 4 and the respective normalized values, i.e., ratios, in Figures 5 and 6. In the latter instances, the first resting supine value for each individual was used as a reference for the determination of the proportional stroke volume (or cardiac output) for the remaining determinations with that method in that subject. There was good correlation between the absolute values for SV and CO but lesser correlation between the relative ones. In order to determine if there was a systematic tendency for one method to read higher or lower than the other, ratios of impedance (Z) CO/dye-dilution CO were calculated for each set of determinations and the results are shown in Table 1. Certain subjects had relatively higher impedance values and others lower ones but the mean ratio of 1.09 indicated a small tendency toward overestimation of the CO with the impedance method. The supine or vertical position did not seem to appreciably affect the ratio.

Series II: Study of Cardiovascular Responses to Vertical Hip Suspension

In Figure 7 are shown mean values for heart rate, normalized stroke volume and cardiac output, systolic and diastolic blood pressure and total peripheral resistance (TPR) before, during and after the 20-minute suspended tilt. The data show that incident to tilt there is a rise in heart rate, a fall in stroke volume and cardiac output, and a rise in diastolic pressure with a slight decline in pulse pressure. These results are similar to those previously reported in passive head-up tilt (13).

The TPR was calculated as the quotient of the mean arterial blood pressure ($DP + 1/3PP$) and the cardiac output. By having the pretilt value for each individual serve as his own control, the relative total peripheral resistance ratios were calculated during the different parts of the experiment for each of the subjects. The mean values indicate a rise in TPR during tilt which is the expected response. The usual small rise in mean arterial blood pressure during the tilt, and the almost universal fall in cardiac output result in a significant rise in the calculated resistance quotient.

There was a great deal of individual variation in the pattern of the circulatory response to the tilt. For example, the blood pressure records of subjects M.Bo. (Fig. 8) and J.Ki. (Fig. 9) were quite similar but the central and peripheral mechanisms to maintain the pressures were evidently very different in the two cases. Subject M.Bo. (Fig. 8) had very little decrease in cardiac output and only a modest rise in heart rate so that there was relatively little change in total peripheral resistance. Subject J.Ki. (Fig. 9) had not only a more marked response in heart rate but also a sharp persistent fall in cardiac output. A marked vasoconstriction to a sizable tissue mass was obviously required in this case to maintain the blood pressure. The availability of impedance cardiographic data is most advantageous for analysis of such mechanisms.

The impedance cardiographic data which was available also permitted the calculation of additional auxiliary data useful in analyzing circulatory function. In Figure 10 are shown mean values for the amplitude of the derivative of the impedance wave (dz/dt) (in absolute

and relative units) and the ejection time index (ETI) which was calculated according to the method of Weissler *et al.* (14) using the formula:

$ETI = T + 0.0016 \text{ HR.}$ Since neither the phonocardiogram nor the carotid pulse was recorded during this study, the ejection time (T) from the impedance signal was used.

The height of the impedance derivative may provide information comparable to dp/dt in the aorta and as such, furnish an approximate measure of cardiac contractile power (4); the prevailing tendency during tilt was toward a decline in dz/dt . The mean values for ETI decreased during passive tilt (Fig. 10) but the absolute values--both during the control and tilt periods--were less than those previously reported (14). It is not certain at this time whether this disparity is associated with the use of the impedance^{time}_(T) in our study or to other factors.

Variations in the R-ΔZ interval (period from the R wave of the ECG to the ejection of blood into the aorta) includes the time of ventricular electromechanical delay but in the main represents alterations in the time of isometric contraction period (4). Mean values for these determinations during suspended tilt are also shown in Figure 10 and indicate a distinct prolongation during postural stress.

Series III: Study of Impedance Cardiographic Responses to Head-up Tilt
with Feet Supported

In the final series, eleven normal males were subjected to 20 minutes of 70° head-up tilt which involved quiet standing with feet resting on a footboard so that the body weight was directly transmitted to the lower extremities. The mean values for heart rate, stroke volume and cardiac

output (absolute and normalized) are plotted in Figure 11. The comparison of the cardiovascular responses to footboard tilt (Fig. 11) and to hip suspension tilt (Fig. 9) indicate that the responses were very similar; comparison of records in individuals who underwent both types of stress indicated a tendency for more marked response in the case of the footboard tilt as evidenced by a greater increase in heart rate and a more marked fall in cardiac output. This finding was rather unexpected since the suspension of the body without support to the lower extremities is almost universally considered to be a more severe stress. This question however requires further investigation with additional subjects.

Discussion

The rather high correlation of absolute values for stroke volume (SV) and cardiac output (CO) derived from the two methods was somewhat surprising since previous reports had emphasized that impedance is useful primarily for determining relative changes in cardiac output (4,7). Kubicek, in his dog experiments, found good agreement between cardiac output (Z values) and aortic flows as determined with the electromagnetic flowmeter. However, the regression slopes were different for different animals which would indicate that absolute values for impedance changes are not likely to be comparable from one individual to the other (4).

Nevertheless, the correlation coefficients obtained in our study were high, suggesting that further exploration of impedance as a measure of cardiac output would certainly be warranted. Two factors might be taken into consideration in evaluating our results. Firstly, our study

was done in resting and posturally stressed subjects in which the cardiac outputs were almost invariably normal or subnormal and only rarely increased. It is possible that the impedance method is more reliable when used within the normal and low range of cardiac output rather than at the higher levels. Visual inspection of our scattergrams (Figs. 3,4, 5 and 6) suggests that the correlation of absolute values was about the same at low outputs as at high outputs. However, the correlation of normalized stroke volumes seemed to be less in the lower output range although our "n" was relatively small for such an analysis. Previous efforts at validation have indicated a greater dispersion of values when cardiac output was increased with exercise or isoproterenol injection (3,7); a second possible factor in our study was the apparent improvement in the instrument since the report of Harley and Greenfield (7). In addition to the direct readout of the derivative (dz/dt), we have been favorably impressed with the applicability of the instrument for laboratory use. The output signals are in the neighborhood of 0.5 volts and can be easily recorded. The 3M electrode tape is easy to apply and produces little discomfort to the subject if it is not applied too tightly. Contact resistances were not checked but no problems were encountered with the electrode tape. The electrode locations did not interfere with other instruments typically used. Electrocardiogram electrodes can be applied between the impedance electrodes without affecting either signal as long as the ground for the ECG is below the fourth impedance electrode.

The study of the circulatory responses of normal male subjects to postural stress in the form of a 20-minute hip suspension indicated considerable individual variation--which has been the experience of most

investigators in this area. Additional cardiac data--such as may be obtained with the impedance cardiograph--could be very helpful in exploring the factors underlying these differences as it was in this study.

Impedance cardiographic information also yields the possibility of additional derived data for the assessment of physiological performance as exemplified in Figure 10. Obviously the validity of such derived data will depend upon further substantiation of the impedance data itself; nonetheless, the assessment of characteristics such as ventricular contractility represents a very interesting potential.

Because of its relative practicability, the instrument may be used to study repeatability of response in the same subject. When we compared the records of repetitive tilt-saddle experiments, there appeared to be repeatable patterns of response in stroke volume, cardiac output, heart rate, blood pressure and TPR characteristic of the individual. This very important problem needs to be studied with considerable care and with greater precision. The main point however is that the cardiograph provides a means of obtaining more detailed useful cardiovascular data on individual response to repeated stress--which represents a very important need in human stress physiology.

The atraumatic nature of the procedure is a significant advantage. Although the availability of well-trained subjects and skillful techniques will permit laboratory use of indwelling catheters, a non-invasive and convenient method such as impedance cardiography represents a very real potential advance in experimental and clinical physiology.

It is well known that intravascular manipulation often causes a significant hypotensive stress (15,16,17). It is evident however that before impedance cardiography can achieve full usefulness in human research, a good deal of additional work will be required, not only to determine the validity of absolute and relative impedance measurements but to discover the limitations and reservations within which the method can yield useful information both in the normal subject and the cardiac patient.

From a technical standpoint, it would seem profitable to explore further the possibility suggested by Namon and Gellan (11,12) that reactive impedance may have greater utility for blood flow measurements than resistive impedance. Another aspect for further research is the apparent necessity for respiratory apnea during the recording. This is a distinct disadvantage.

Finally, it might be well to explore further the role of heart rate and its practical role in the use of the cardiograph. Tachograph recordings in human experiments illustrate the rapid fluctuations in rate, especially during stress. While stroke output can be a useful physiological parameter, perhaps automatic averaging over a longer period than 5 to 10 beats would be advantageous. The question also arises as to whether longer periods of determination might increase the usefulness of the instrument during respiration.

Summary

The Minnesota Impedance Cardiograph, Model 202 was used to investigate 1) the validity of impedance plethysmography as a measure of cardiac output and 2) its practicability and value for the study of circulatory stress in the intact human. A comparison of thirty-five simultaneous determinations of cardiac output with the impedance method and with ordinary dye-dilution techniques was made in eight normal male subjects. The correlation coefficients (r) for the absolute values were +0.91 for cardiac output and +0.82 for stroke volume. For relative changes--with each method serving as its own control--the correlation coefficients were +0.57 for normalized cardiac output and +0.63 for normalized stroke volume. Twenty-minute hip suspension of normal subjects caused an increase in mean values for heart rate, decrease in cardiac output, slight elevation of diastolic blood pressure and distinct elevation of the total peripheral resistance. These changes were all quite comparable to those previously observed by other investigators. The recording of central cardiovascular events gives useful insight into the mechanism of circulatory response in the intact human under stress. Impedance recording also provides the opportunity to derive auxiliary data such as the amplitude of the impedance time derivative, the left ventricular ejection time index and the R-ΔZ interval--all of which may be useful in determining cardiac dynamics.

It is our opinion that the potential value of the impedance cardiograph for research and clinical use is considerable. It would seem as if such a potential would warrant further intensive efforts, not only to determine the basic validity of the procedure, but to further improve its applicability and utility.

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TABLE 1
 RATIOS OF $\frac{\text{Z-CALCULATED CARDIAC OUTPUT}}{\text{DYE-CALCULATED CARDIAC OUTPUT}}$

(N = 35)

Subject No.	Supine (pretilt)		Tilt		Supine (post-tilt)	Mean
	+5 min	+10 min	T + 5 min	T + 15 min	+5 min	
1	1.12	1.43	1.19	0.86 0	1.33	1.27
2	0.96	0.99	0.88	1.14 5	0.84	0.81
3	0.93		0.74	1.03	1.16	0.99
4	1.08		1.11	0.96 1	1.01	1.06
5	0.83	1.08	1.04		0.99	0.98
6	0.80		0.99	1.28 2	0.72	0.84
7	1.42	1.26	1.13	1.75 2	1.51	1.32
8	1.17	1.38	1.20	1.17	1.16	1.33
Mean Ratio	1.04	1.23	1.03	1.17	1.09	1.09 ± 0.19

TABLE 2
VALUES FOR Z-CALCULATED AND DYE-CALCULATED STROKE VOLUMES

Subject	Time	Z Method			Dye Method			Normalized Data			
		SV (ml)	HR	CO (L/min)	SV (ml)	HR	CO (L/min)	NSV- Z	NSV Dye	NCO Z	NCO Dye
1. D.Jo.	CH + 5'	91.0	67	6.10	79.2	69	5.46				
	CH + 10'	108.0	68	7.34	74.8	68	5.09	1.19	0.94	1.20	0.93
	T + 5'	51.8	83	4.30	40.7	88	3.58	0.57	0.51	0.70	0.66
	RH + 1'	110.0	56	6.16	81.5	56	4.56	1.21	1.03	1.00	0.84
2. T.Ba.	CH + 5'	70.4	63	4.44	74.6	62	4.62				
	CH + 10'	68.5	62	4.25	76.3	56	4.27	0.97	1.02	0.96	0.92
	T + 11'	45.4	72	3.27	52.7	70	3.69	0.64	0.71	0.74	0.80
	T + 17'	44.8	71	3.18	53.6	69	3.70	0.64	0.72	0.72	0.80
	RH + 5'	71.4	54	3.86	84.0	55	4.62	1.01	1.13	0.87	1.00
3. W.Ma.	CH + 5'	111.6	63	7.03	111.4	68	7.58				
	T + 5'	70.3	65	4.57	86.1	72	6.20	0.63	0.77	0.65	0.82
	T + 15'	70.7	76	5.37	65.1	72	4.69	0.63	0.58	0.76	0.62
	RH + 15'	117.5	66	7.76	101.0	66	6.67	1.05	0.91	1.10	0.88
4. F.Mi.	CH + 5'	166.4	62	10.32	158.7	60	9.52				
	T + 5'	109.5	69	7.56	103.0	66	6.80	0.66	0.65	0.73	0.71
	T + 10'	100.8	72	7.26	97.5	72	7.02	0.60	0.61	0.70	0.74
	RH + 5'	164.3	64	10.52	152.6	68	10.38	0.99	0.96	1.02	1.09
5. S.Mo.	CH + 5'	111.5	67	7.47	124.6	72	8.97				
	CH + 15'	141.0	61	8.60	113.4	70	7.94	1.26	0.91	1.15	0.88
	T + 5'	63.8	82	5.23	60.3	84	5.06	0.57	0.48	0.70	0.56
	T + 15'	60.7	85	5.16	63.9	84	5.37	0.54	0.51	0.69	0.59
	RH + 5'	130.2	59	7.68	110.6	70	7.74	1.17	0.89	1.03	0.86
6. W.Wa.	CH + 5'	109.9	78	8.57	127.5	84	10.71				
	T + 5'	78.6	95	7.46	83.3	90	7.50	0.72	0.65	0.87	0.70
	RH + 5'	70.2	97	6.81	105.4	90	9.49	0.64	0.83	0.79	0.89
7. A.Sp.	CH + 5'	81.2	78	6.34	67.9	66	4.48				
	CH + 10'	92.9	70	6.51	74.0	70	5.18	1.14	1.09	1.03	1.16
	T + 5'	56.5	87	4.92	48.4	90	4.36	0.70	0.71	0.78	0.97
	T + 15'	48.9	93	4.55	39.4	90	3.55	0.60	0.58	0.72	0.79
	RH + 5'	94.5	69	6.52	65.6	66	4.33	1.16	0.97	1.03	0.97
8. J.Ho.	CH + 5'	90.6	63	5.71	68.0	72	4.90				
	CH + 10'	86.9	70	6.09	64.6	68	4.39	0.96	0.95	1.07	0.89
	T + 5'	43.2	93	4.02	37.4	90	3.36	0.48	0.55	0.70	0.69
	T + 10'	61.9	88	5.45	34.5	90	3.11	0.68	0.51	0.95	0.63
	RH + 5'	90.4	62	5.60	64.3	75	4.83	1.00	0.94	0.98	0.98

Footnotes for Table 2

CH + 5' = control horizontal + 5 min (determination made 5 min after subject assumed control supine position)

T + 5' = tilt + 5 min (determination made 5 min after subject was passively tilted to 70° upright position; ordinarily subject was tilted after 15 min in the control horizontal position)

RH + 5' = recovery horizontal + 5 min

SV = stroke volume (ml)

HR = heart rate (for dye method, average rate during curve; for Z method, average rate of five beats)

CO = cardiac output (L/Min)

Basic data for cardiac output determinations were taken simultaneously for dye dilution by Dr. Tristani and his assistants and for impedance method by Dr. Wiedmeier and his team; respective calculations were made and submitted independently by the two groups. These data are shown in Figures 3 and 4.

Normalized values indicate that the first resting supine value for each subject was used as a reference for the determination of the ratio of stroke volume or cardiac output for the remaining determinations with that method in that subject. Data graphed in Figures 5 and 6.

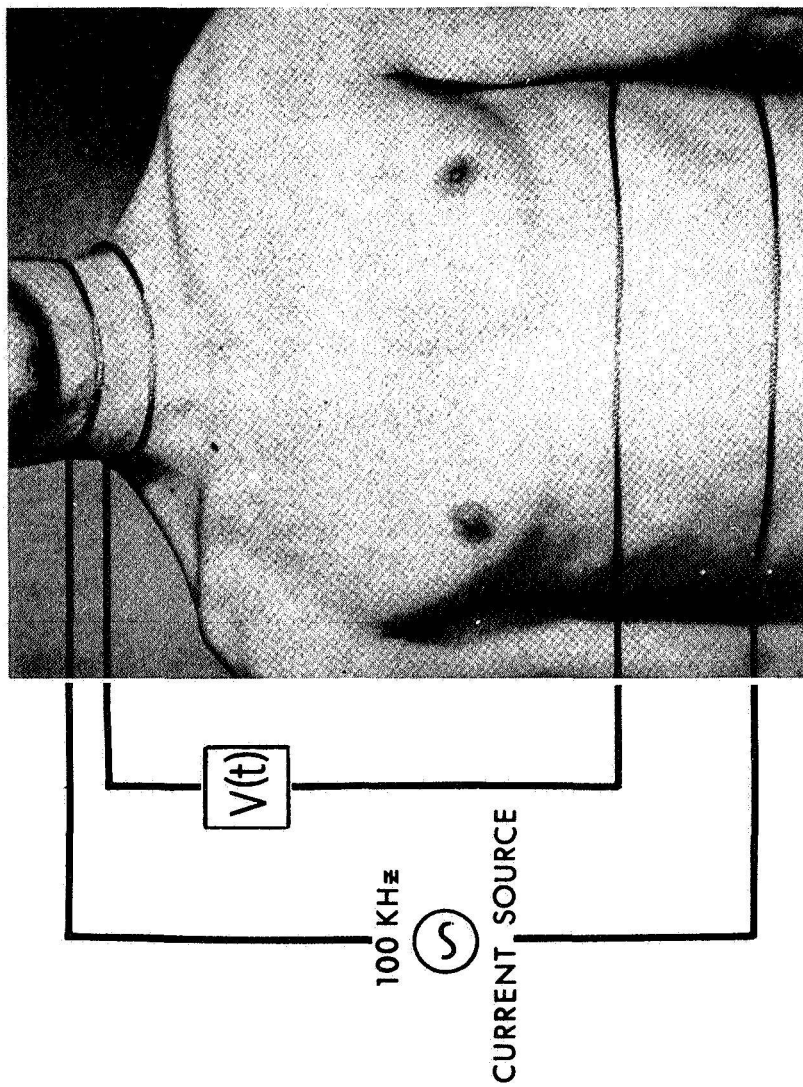


Fig. 1. Subject with four band electrodes.

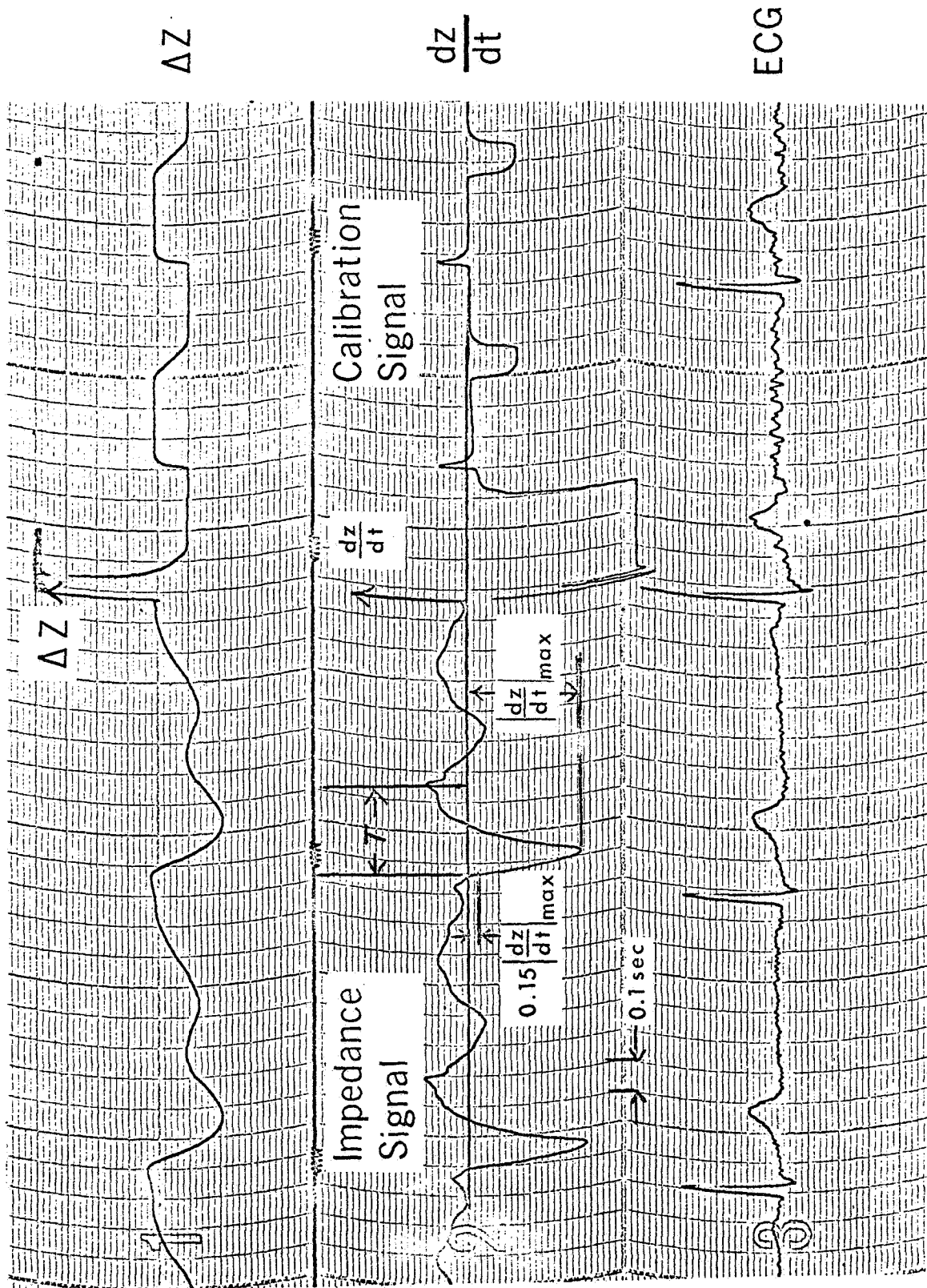


Fig. 2. Impedance wave (ΔZ), the first derivative of the impedance wave ($\frac{dz}{dt}$) and ECG tracing. (Paper speed: 50 mm/sec)

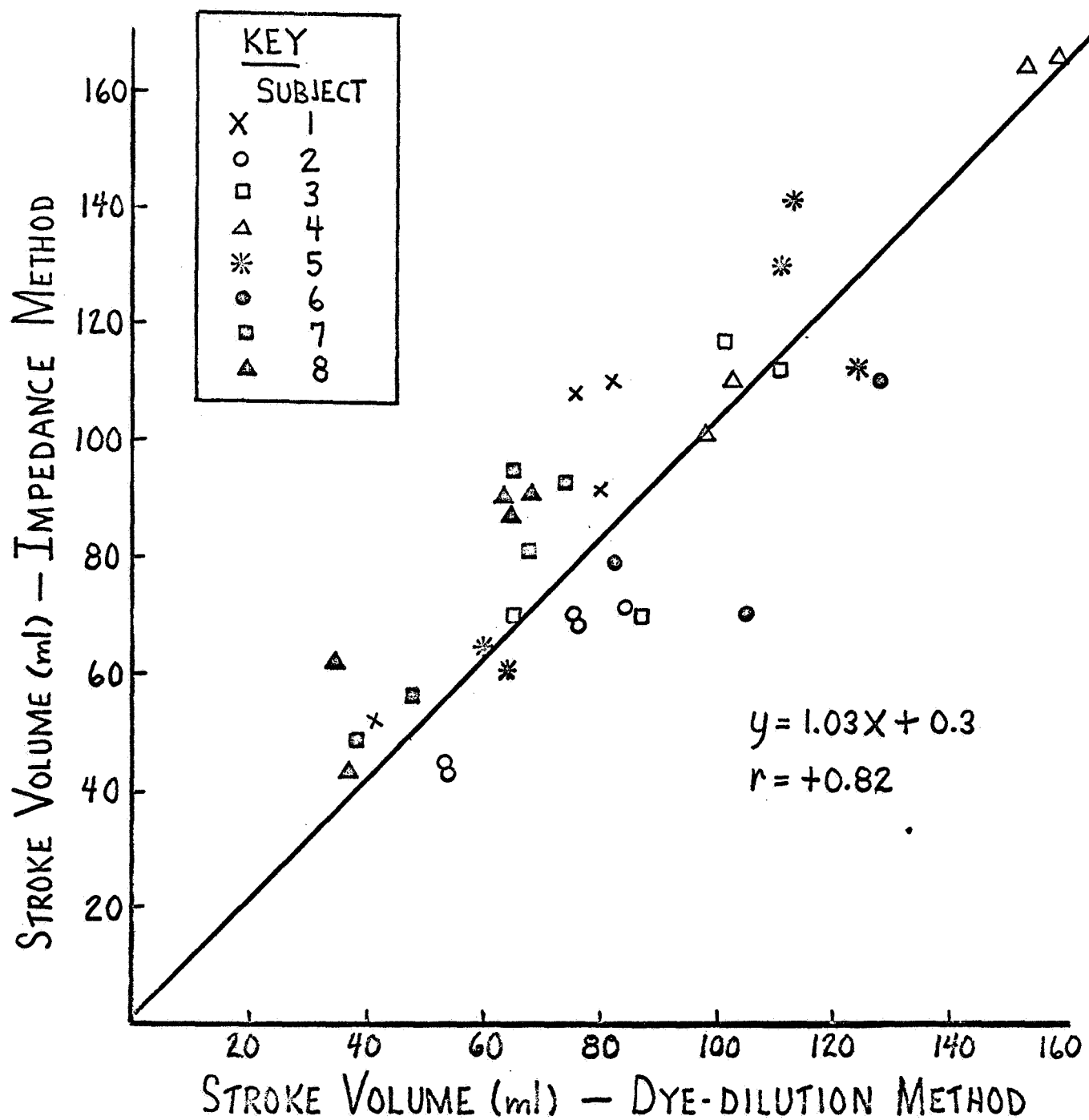


Fig. 3. Stroke Volume in Head-up Tilt--Dye-dilution vs Impedance Values
 (35 determinations in 8 normal males)

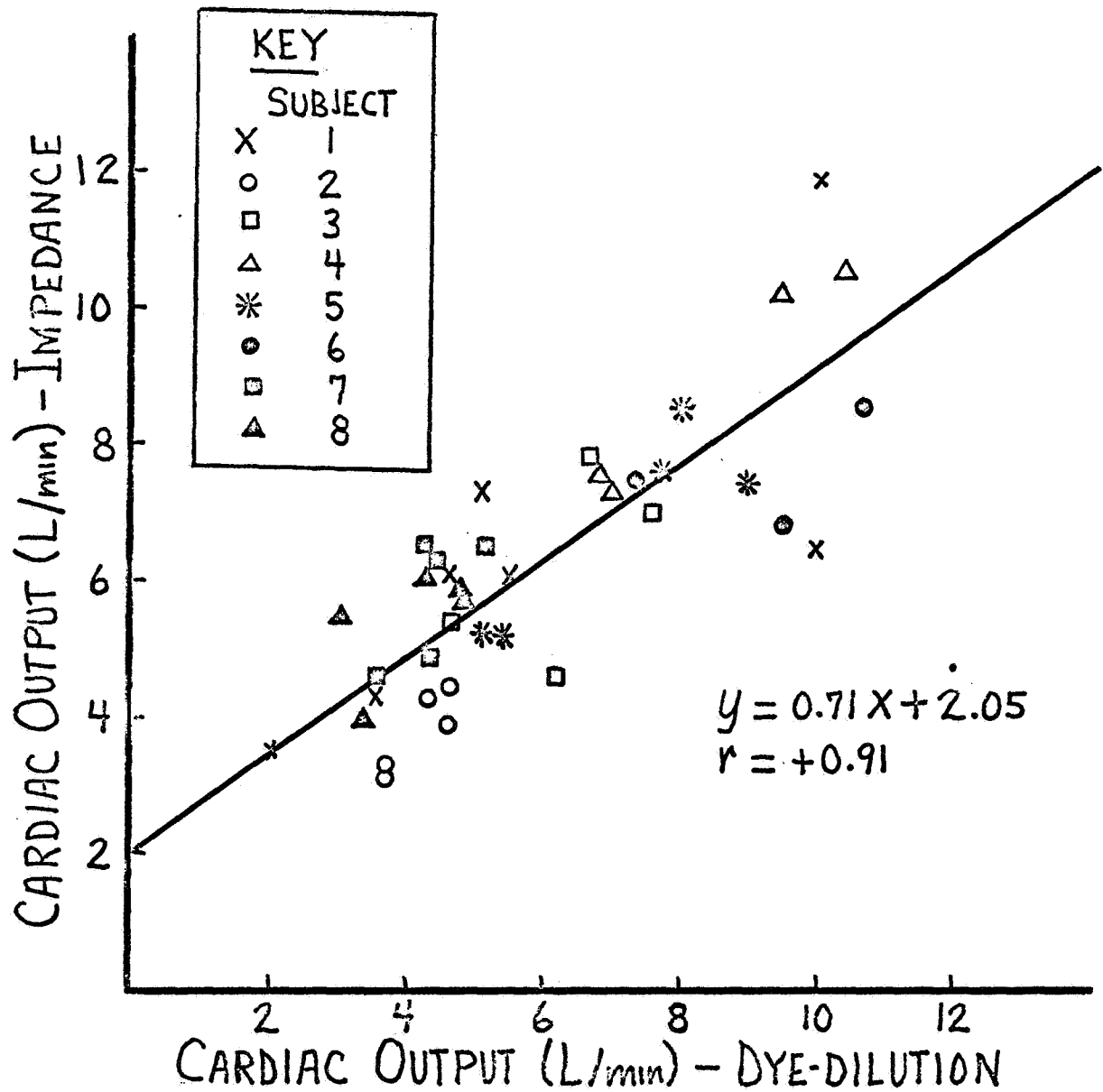


Fig. 4. Cardiac Output in Head-up Tilt--Dye-dilution vs Impedance Values (35 determinations in 8 normal males)

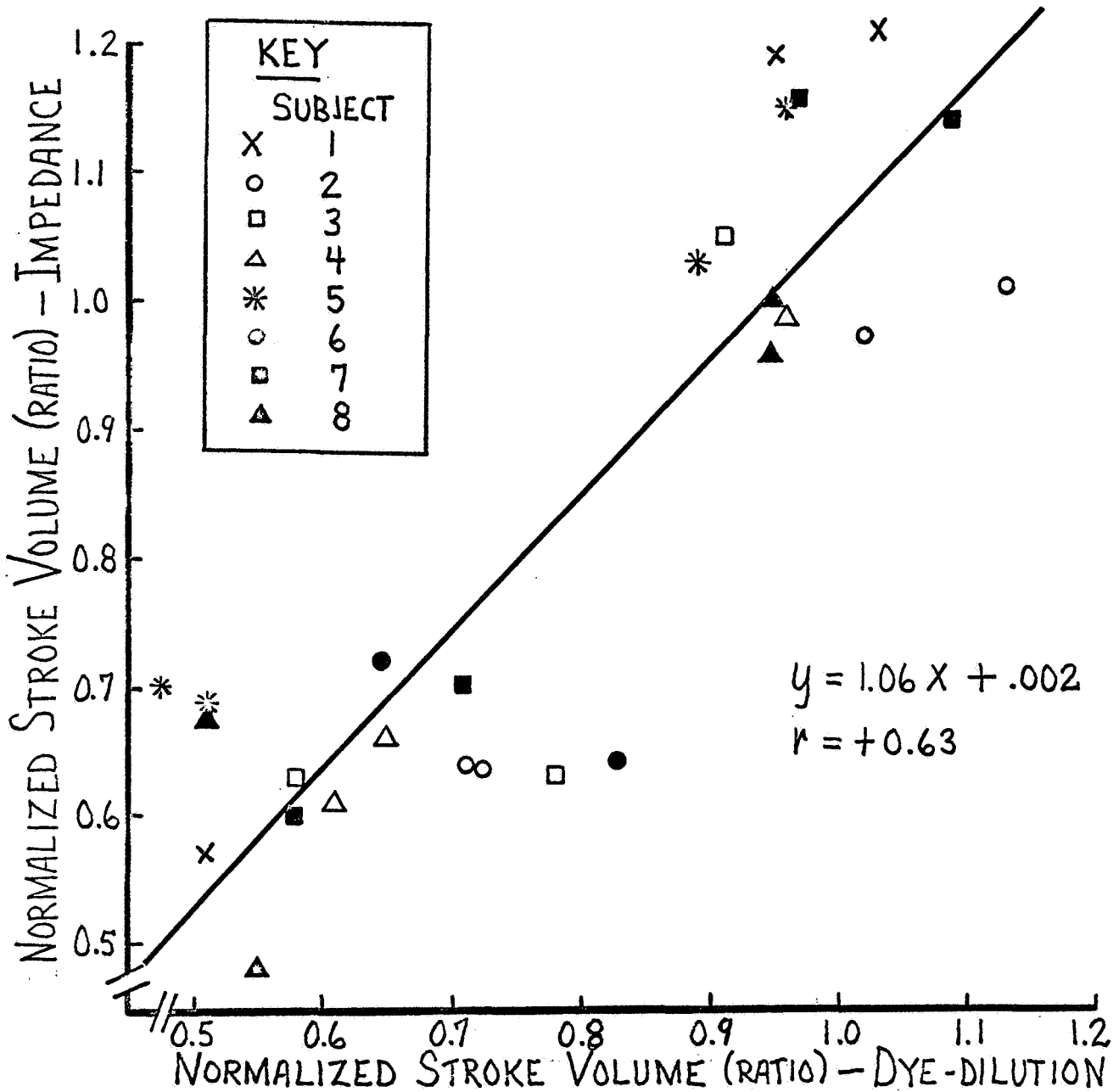


Fig. 5. Stroke Volume in Head-up Tilt--Ratios of Change with Dye-dilution and Impedance Methods Based on Respective Individual Control Values

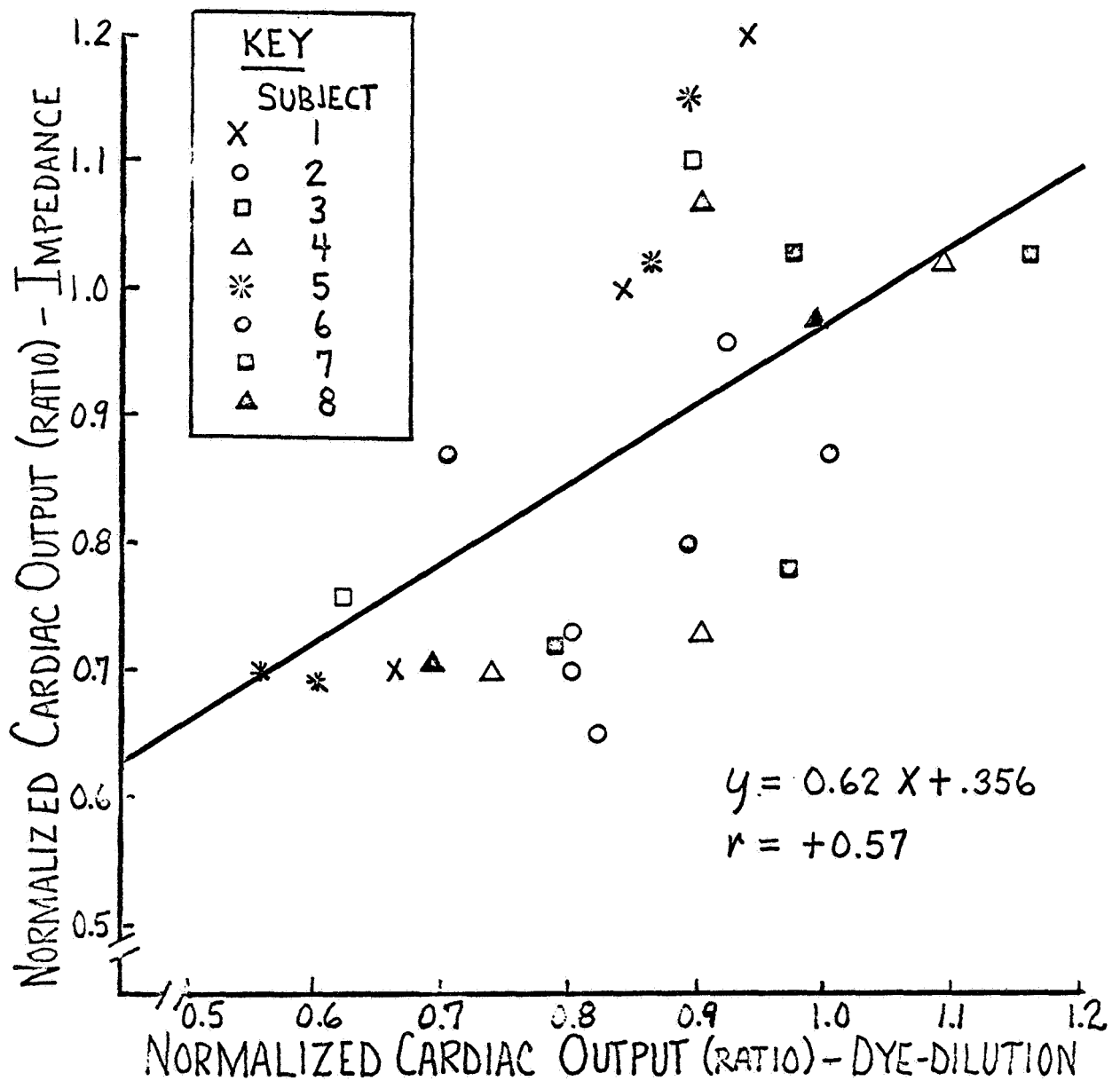


Fig. 6. Cardiac Output in Head-up Tilt--Ratios of Change with Dye-dilution and Impedance Methods Based on Respective Individual Control Values

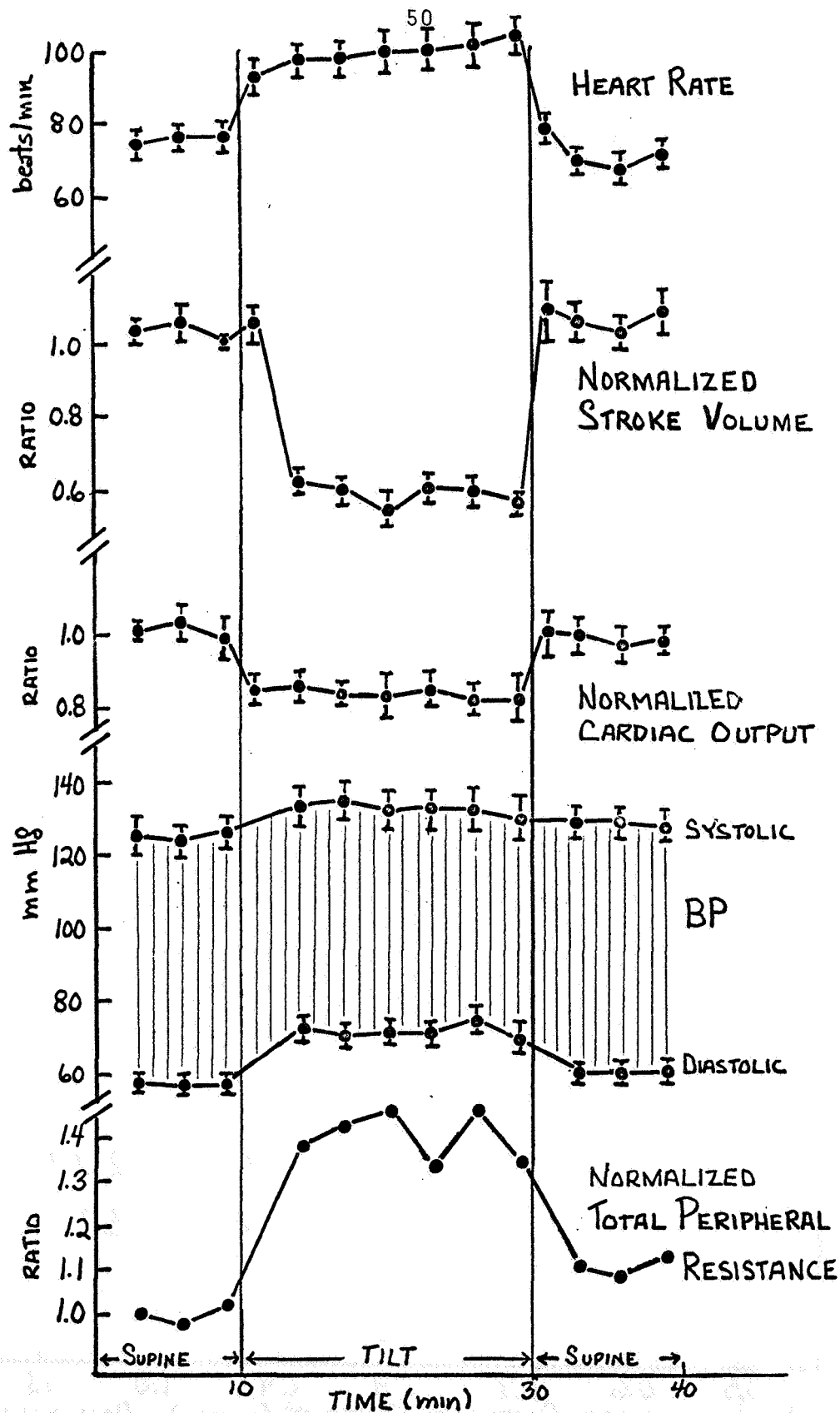


Fig. 7. Cardiovascular Responses to Vertical Tilt with Hip Suspension (Mean values with S.E. for 12 experiments in 8 males)

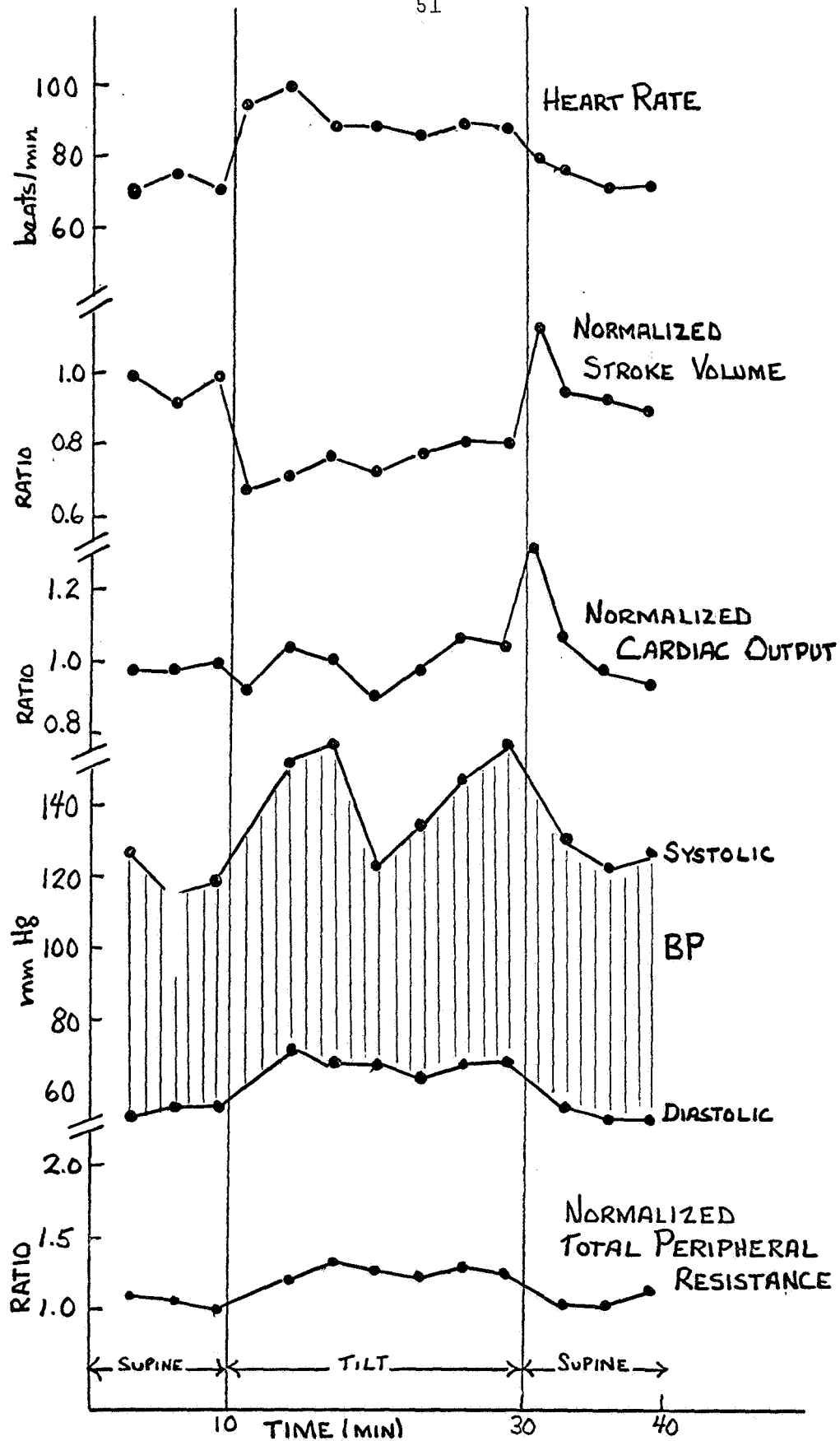


Fig. 8. Cardiovascular Responses to Vertical Tilt with Hip Suspension (Subject: M.Bo.)

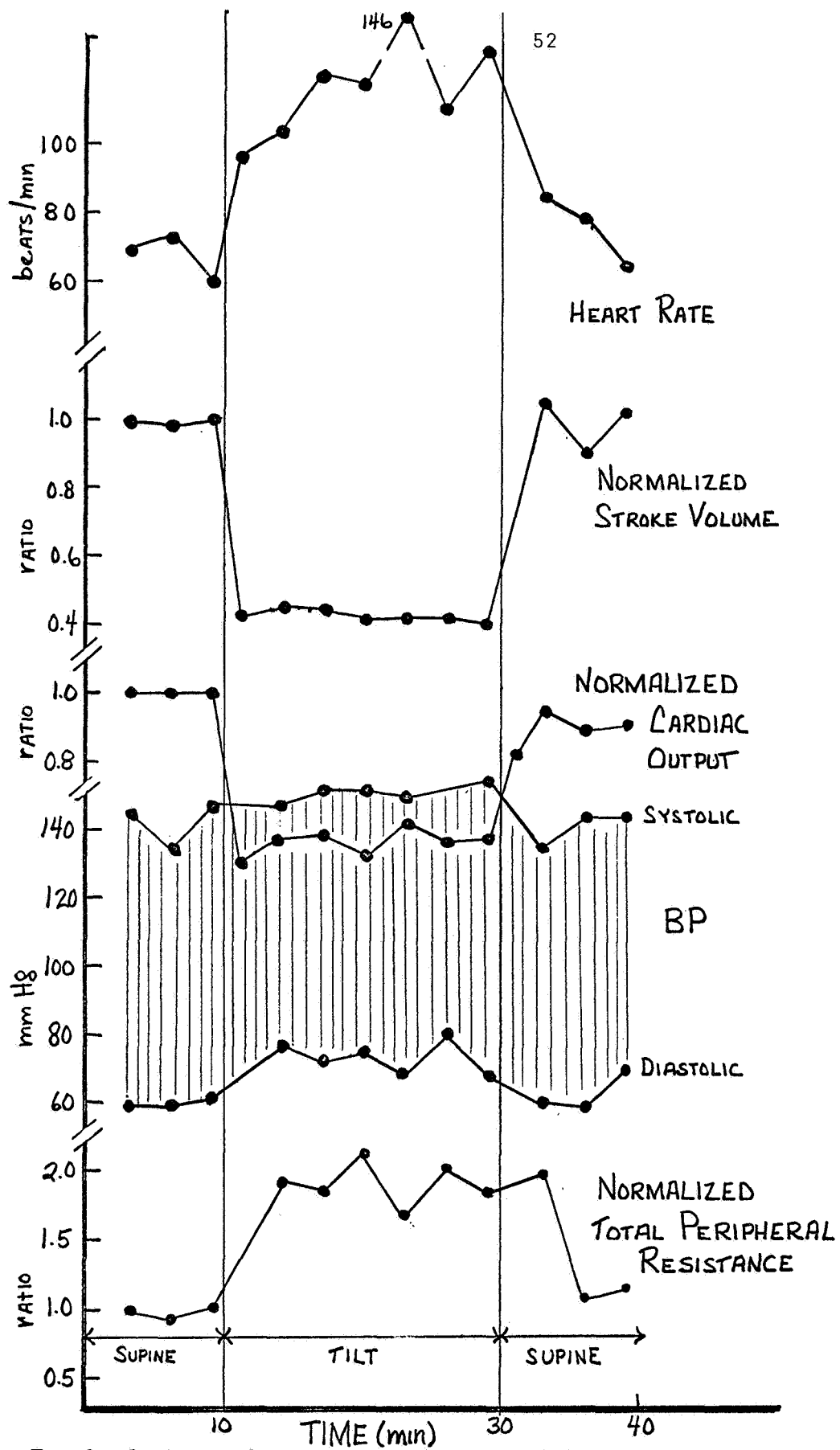


Fig. 9. Cardiovascular Responses to Vertical Tilt with Hip Suspension (Subject: J.Ki.)

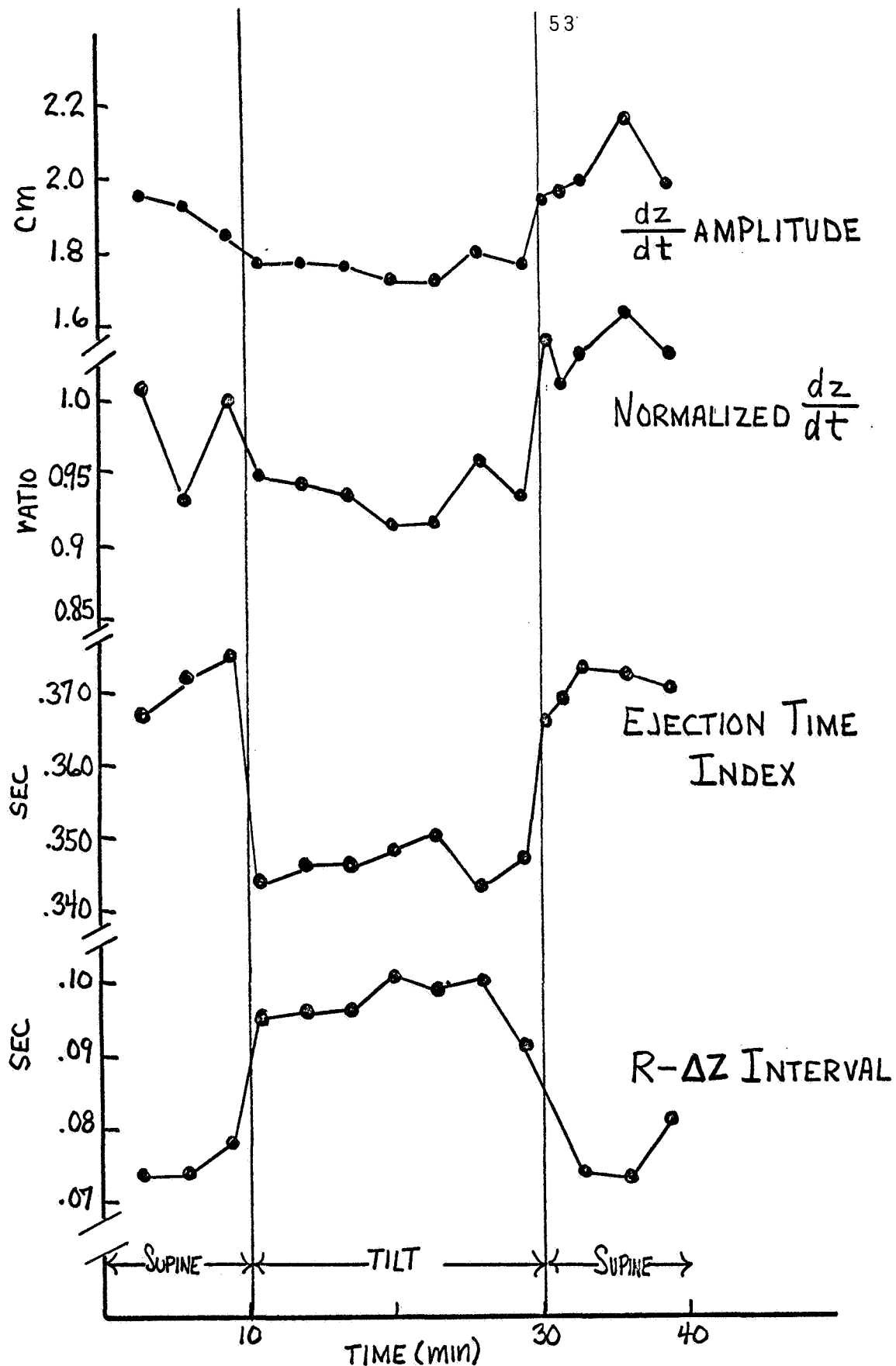


Fig. 10. Auxiliary Cardiovascular Values Derived from Impedance Data
(Mean values of 12 experiments in 8 normal male subjects)

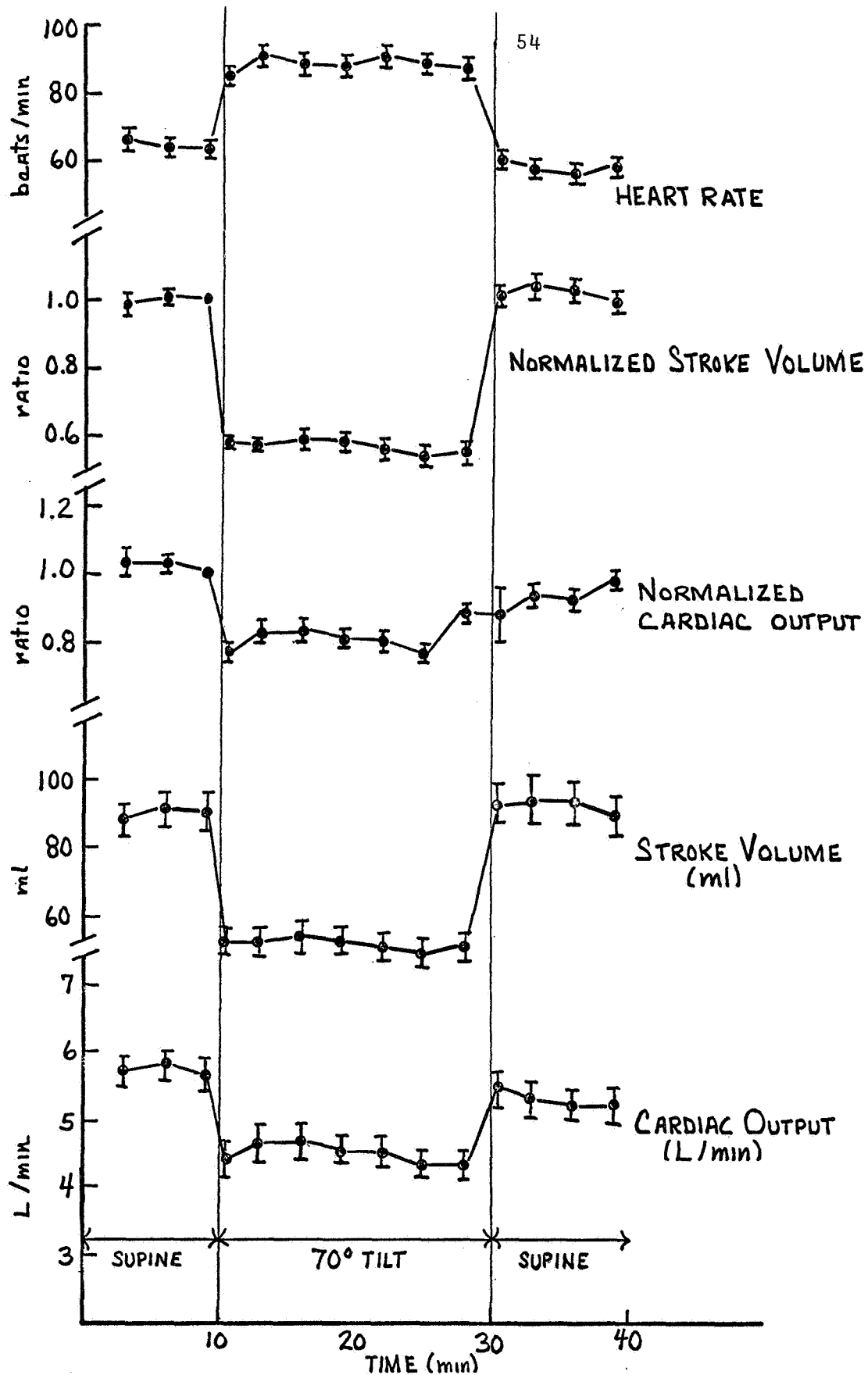


Fig. 11. Stroke Volume and Cardiac Output Responses to Head-up Tilt. Body Weight Supported by Footboard (Mean Values with S.E. for 11 Normal Male Subjects)

TABLE II-A (Greenfield)

Correlation coefficients computed by linear regression of DZ/DT, ZSV and DE on SV, in six patients with idiopathic myocardial hypertrophy. Alterations of stroke volume were produced by atrial pacing at indicated heart rates.

PATIENT	HEART RATES PER MINUTE	NUMBER OF BEATS	DZ/DT-SV _{Dye} r =	ZSV-SV _{Dye} r =	DE-SV _{Dye} r =
1	86, 92, 102, 115	60	0.598	0.648	0.506
2	78, 102, 115, 128	40	0.849	0.943	0.942
3	94, 103, 126, 137, 158	63	0.433	0.623	0.914
4	97, 126, 141, 165	60	0.690	0.688	0.417
5*	71, 85, 107, 118, 140, 154	73	0.461	0.792	0.943
	71, 85, 107, 118, 140	58	0.884	0.913	0.929
	154	15	0.776	0.894	0.961
6	94, 106, 114, 125, 158	73	0.930	0.955	0.923

DZ/DT = maximum first time derivative of transthoracic impedance change;

ZSV = impedance stroke volume

DE = duration of ejection

SV_{Dye} = stroke volume by dye dilution method

*In this patient the regression equation was markedly different at a heart rate of 154/min. than at other heart rates; the results of separate regressions are therefore presented.

Determination of Cardiac Output in Man by Means of Impedance Plethysmography

A. HARLEY, M.B., M.R.C.P., and JOSEPH C. GREENFIELD, JR., M.D.

An electrical impedance plethysmographic method employing cervical and lower thoracic electrodes and an indicator dilution technique were used to record cardiac output simultaneously in 13 normal subjects during a control period and following an infusion of isoproterenol. A correlation coefficient of $r = 0.68$ was found for these 26 paired values. In addition cardiac output was measured simultaneously in 24 patients with various types of heart disease by an indicator dilution technique and by impedance plethysmography. The correlation coefficient between these determinations was $r = 0.26$. In six patients with atrial fibrillation impedance stroke volume was found to be directly proportional to the preceding cycle length. Satisfactory correlation was found between stroke volumes estimated by impedance plethysmography and by direct measurement using the pressure gradient technique in two patients with mitral stenosis and atrial fibrillation. Although the later results are somewhat encouraging, from these preliminary findings it is felt that the current impedance plethysmographic methods as employed in this study are not refined to the point that clinical application is warranted. However, since this method has potential value as an atraumatic method for determining cardiac output and stroke volume, it deserves further evaluation.

IT HAS LONG BEEN KNOWN that the electrical impedance of the thorax of both man and animals varies regularly during the cardiac and respiratory cycles. As the movement of blood into, out of, and within the thorax is the most obvious result of cardiac contraction, attempts have been made to relate these observed changes in impedance with stroke output. Kubicek and co-workers postulated that the maximum rate of decrease in electrical impedance which occurs during the initial part of cardiac systole is related to ventricular stroke volume.^{2,5} Comparison of impedance

plethysmographic estimates of ventricular stroke volume with values obtained from the more conventional Fick and indicator dilution methods by these investigators have indicated at least a reasonable relationship between cardiac output and electrical impedance changes.⁴ This report is a further evaluation of impedance plethysmography as an atraumatic method of estimating cardiac output in man, both by direct comparison with an indicator dilution technique and by following the variation in stroke volume in patients having atrial fibrillation.

METHODS

Simultaneous indicator dilution curves and impedance records were obtained in 13 healthy male subjects before and after an intravenous infusion of isoproterenol. Cardiac output was also measured simultaneously by indicator dilution and impedance plethysmography in 24 hospitalized patients with heart disease who were undergoing diagnostic studies or treatment at the Durham Veterans Administration Hospital. The clinical diagnosis of these patients are shown in Table I. Six of the patients had atrial fibrillation and in two of these stroke volume was compared to simultaneous direct measurement of stroke volume by the pressure gradient technique.^{1*}

A Model 2110 Medtronic impedance bridge** was used with a four-electrode system to obtain the im-

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Dr. Greenfield is the recipient of a Career Development Award (1-K3-HE-28, 112) from the U.S.P.H.S.

*The pressure gradient technique is so far the only reported method for obtaining instantaneous aortic blood flow in man under physiological conditions. Briefly, it involves the extremely accurate measurement of the instantaneous lateral pressures at two points in the ascending aorta with a double lumen catheter. The difference between these pressures is an approximate measure of instantaneous pressure gradient from which the blood flow may be computed by simple analog computer methods.

**Medtronics, Inc., 3055 Old Highway 8, Minneapolis, Minn. 55418.

pedance measurements. The electrodes were of the type described by Kubicek and co-workers.⁴ A cervical collar contained the upper pair of electrodes. The third electrode was placed around the thorax two finger breadths below the tip of the xiphos-sternum and the fourth electrode 5 cm caudally. The electrodes were applied some ten or more minutes before use. Care was taken to insure that contact to the chest and neck was even but not tight. The distance, L , between the two inner electrodes was measured as accurately as possible in centimeters in the mid-coronal plane. The impedance between the inner two electrodes was measured while a 100 kc. excitation frequency was applied to the outer pair of electrodes. All measurements were made during relaxed mid-expiratory apnea. In many over cooperative subjects some practice was required before relaxation could be consistently achieved rather than the subject performing a Valsalva or a Muller maneuver. Heart sounds were recorded with a Shure Model SP-5S crystal microphone⁵ applied either to the second or third left interspace at the left sternal edge, wherever best definition of the second heart sound was obtained. The impedance change signal from the inner two electrodes was displayed on an oscilloscope and recorded by a Honeywell Visicorder together with the electrocardiogram and the phonocardiogram. In some patients the carotid pressure pulse was also measured with an externally applied transducer.

The value of the maximum impedance change for each beat was determined graphically as shown in Figure 1. The stroke volume was calculated from this value by the formula given by Kubicek and co-workers.⁴

TABLE I. COMPARISON OF INDICATOR DILUTION AND IMPEDANCE DETERMINATIONS OF CARDIAC OUTPUT IN 24 PATIENTS WITH ACQUIRED HEART DISEASE

Patient No.	Age Yrs.	Diagnosis	Indicator Dilution Cardiac Output L/min	Impedance Cardiac Output L/min
1	53	Mitral Stenosis	2.16	3.52
2	45	Mitral Stenosis	2.65	4.12
3	63	Mitral Stenosis	2.61	4.41
4	36	Mitral Stenosis and Insufficiency	4.95	7.94
5	46	Mitral Insufficiency and Stenosis	3.37	4.29
6	40	Mitral Insufficiency and Stenosis	4.47	4.31
7	52	Mitral Insufficiency	2.91	8.30
8	38	Mitral Insufficiency	5.97	8.38
9	72	Mitral Insufficiency	3.57	3.29
10	42	Aortic Stenosis	4.89	5.00
11	45	Aortic Stenosis	5.32	5.18
12	38	Aortic Insufficiency and Stenosis	6.30	12.00
13	35	Aortic Insufficiency	4.92	11.35
14	31	Hypertensive Heart Disease	4.26	3.60
15	43	Hypertensive Heart Disease	4.68	3.28
16	33	Hypertensive Heart Disease	4.99	3.72
17	46	Hypertensive Heart Disease	6.06	3.37
18	44	Hypertensive Heart Disease	5.82	7.56
19	54	Chronic Lung Disease	8.28	3.05
20	45	Chronic Lung Disease	4.30	6.07
21	57	Chronic Lung Disease	4.82	2.85
22	40	Idiopathic Atrial Fibrillation	2.89	3.98
23	32	Idiopathic Myocardial Hypertrophy	3.19	3.71
24	54	Ischaemic Heart Disease	6.06	7.60

*Shure Brothers, Inc., Evanston, Illinois.

$$\Delta V = \rho \frac{L^2}{Z_0^2} \Delta Z$$

Where ΔV represents the stroke volume in cm^3 , L the distance between the inner pair of electrodes in cm, Z_0 the value of the baseline impedance between the electrodes in ohms, and ΔZ the measured maximum impedance change. ρ is a constant (150 ohm cm) representing the electrical resistivity of blood at 100 kc. In calculating the impedance cardiac output determinations the average stroke volume was taken as the mean value from 10 consecutive heart beats.

Indicator dilution curves were obtained following injection of indocyanine green with a Colson Gilford Densitometer. In the patients undergoing diagnostic cardiac catheterization the dye was injected into either the right ventricle or the main pulmonary artery and sampled from a brachial artery. In the other subjects the dye was injected into a median cubital vein and arterial blood was sampled from a brachial artery. When simultaneous indicator dilution curves were made, the impedance changes were recorded after the injection of dye but immediately prior to and during inscription of the dye curve. Both were therefore recorded in the same phase of held respiration.

RESULTS

The impedance wave form in normal subjects and in most patients resembled that shown in Figure 1. However, in some patients with valve disease there were considerable variations especially in the size of the

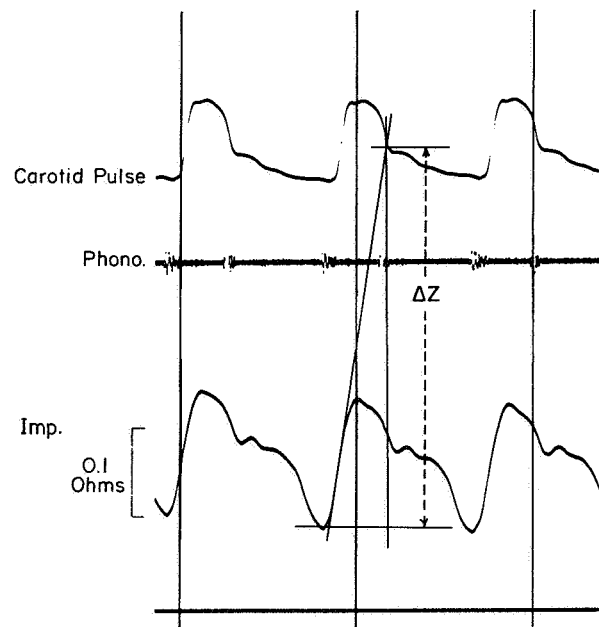


Fig. 1. From the top downwards, the carotid arterial pressure pulse, phonocardiogram and impedance signal (an upward deflection denotes a decrease in thoracic impedance). The initial upward slope is extrapolated as far as the pulmonic component of the second heart sound. The total height of this slope represents the ΔZ used in equation 1 to compute stroke volume.

diastolic waves. Simultaneous measurement of cardiac output by impedance plethysmography and indicator dilution before and after isoproterenol in the 13 normal subjects provided a comparison of the two methods in estimating absolute resting cardiac output and estimating the size of a change in cardiac output. Twenty-six paired values for cardiac output were obtained (Figure 2) and were subjected to regression analysis. The mean indicator dilution control cardiac output was 6.3 L/min rising to 9.5 L/min following the infusion. The ratio of the cardiac output computed from impedance plethysmography to that measured by the indicator dilution technique was 1.34 during the control state and 1.23 following the isoproterenol. This difference was not significant ($P > 0.2$). The regression equation was: Impedance cardiac output = $2.93 + 0.86 \times$ indicator dilution cardiac output L/min (\pm SE 2.33 L/min), with a correlation coefficient of $r = 0.68$.

The results of simultaneous estimation of cardiac output by indicator dilution and impedance plethysmography in the 24 patients with heart disease is illustrated in Figure 3 and listed in Table I. A correlation coefficient of $r = 0.26$ was obtained for these data. In patients 7, 12, and 13 (Table I) the impedance estimate exceeded the dye estimate considerably. Two of these patients had significant aortic regurgitation while one had mitral regurgitation with severe pulmonary hypertension. In patient 12 and in a third patient with aortic regurgitation in whom simultaneous indicator

dilution cardiac output determinations were not made, the impedance measurements were repeated on several separate days. The impedance estimate of cardiac output was always in the same high range. No patient was studied with significant aortic regurgitation who had a normal or low impedance cardiac output value. In patients 10 and 11 who have aortic stenosis the impedance and indicator dilution estimates of cardiac output agreed fairly closely.

In six of the patients with heart disease associated with atrial fibrillation, the impedance stroke volumes for individual beats were compared to the length of the preceding cardiac cycles, Figure 4. Impedance stroke volume was found to vary with preceding cycle length in the expected manner. Although the relationship differed slightly in each patient, the correlations were good in four of the patients but much less so for two of the patients, both of whom had pure mitral stenosis. In two patients (Number 1 and 2, Table I) impedance stroke volume of individual beats was compared to simultaneous direct measurements of the stroke volume of the same beats by the pressure gradient technique.¹ Figure 5 shows the relation of stroke volume estimated by the impedance plethysmographic method and the pressure gradient technique for individual cardiac cycles. The correlation coefficients were $r = 0.93$ for one patient and $r = 0.91$ for the other patient. It should be noted that the absolute values for stroke volume given by each method differ considerably.

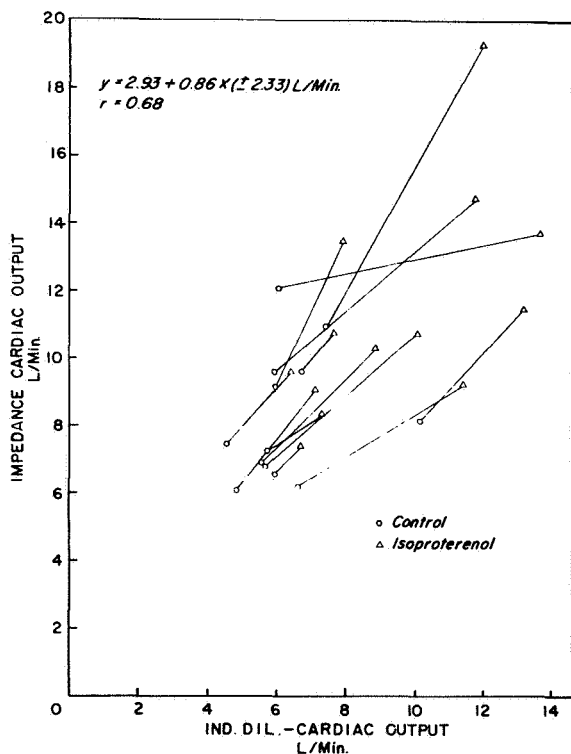


Fig. 2. Comparison of cardiac output values given by impedance plethysmography with those obtained by indicator dilution technique in thirteen healthy subjects before and after infusion of isoproterenol.

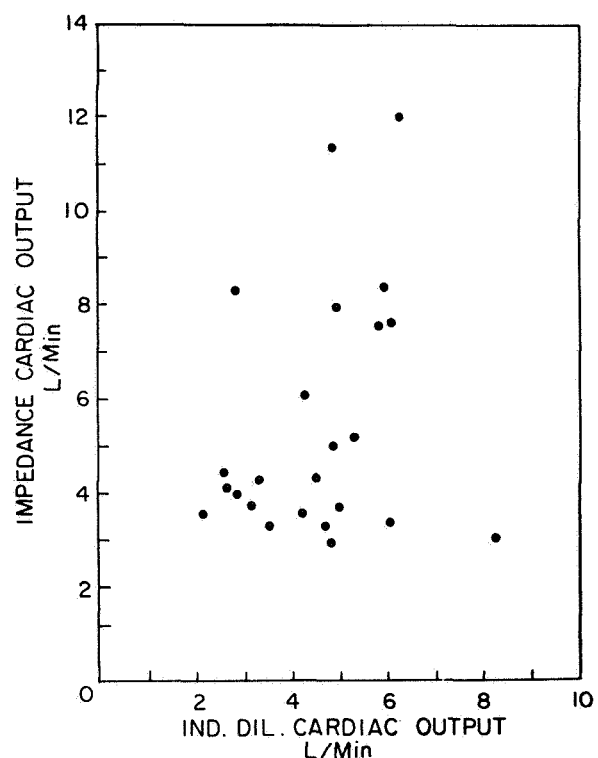


Fig. 3. Comparison of cardiac output computed by impedance plethysmography with that obtained by indicator dilution technique in the twenty-four patients with heart disease listed in Table I.

DISCUSSION

These preliminary findings in a small group of subjects tend to support the concept that there may be a direct relationship between the stroke volume and a change in electrical impedance. However, in spite of careful attention to the details of the technique, the correlation between estimates of cardiac output from the indicator dilution method and impedance plethysmography in normal subjects was poor. In similar studies performed by Kubicek and co-workers⁴ the correlation appears to be much closer, but the form in which their data is published precludes a direct comparison with our results. The widest scatter between indicator dilution and impedance values was found in those patients with heart disease. This finding may be related at least in part to the cardiac abnormality. For example, in the patients with aortic incompetence the impedance cardiac output was unrealistically high. Obvious differences in the shape of the impedance wave form occur between patients, but to date we have been unable to categorize pathological states by the nature of the impedance curve. A better relationship between stroke volume as given by the pressure gradient technique and the impedance stroke volume was noted in two patients with atrial fibrillation. Also

a fairly good correlation was found between filling time and impedance stroke volume determination in six other patients with atrial fibrillation. These findings would suggest that for a short duration in a given patient the present impedance plethysmographic technique may yield a reasonable index of stroke volume.

The reasons for the poor correlation noted in our studies are obscure. Although we have noticed no systematic discrepancies in obese or thin subjects, it is possible that the girth of the lower thorax or the neck affect the impedance change for a given stroke volume. Despite close attention to technique, variations in electrode placement, respiration, and the shape of individual subjects also may be partly responsible. In addition, the formula used to compute the impedance stroke volume is empirically derived and may well be wrong. Clearly a considerable amount of research is necessary before this technique can be considered ready for clinical use. However, an accurate atraumatic method of continuously measuring cardiac output and beat-to-beat changes in stroke volume will be of extreme value to a number of medical applications. This is particularly so in physiological monitoring during real or experimental flight conditions in selected subjects. For this reason the impedance plethysmographic method is felt to deserve further evaluation.

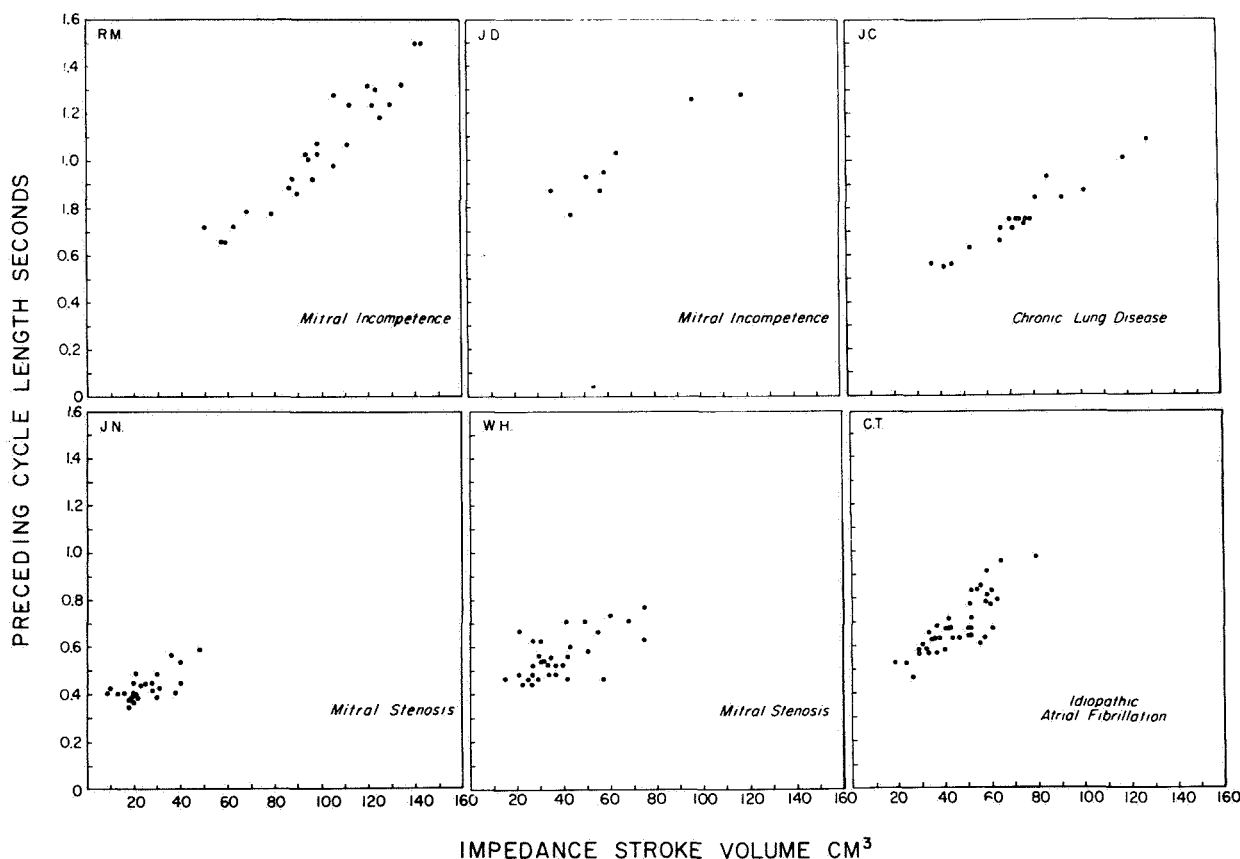


Fig. 4. Correlation of impedance stroke volume with the preceding cycle length for individual beats in six patients with atrial fibrillation.

DETERMINATION OF CARDIAC OUTPUT IN MAN BY IMPEDANCE PLETHYSMOGRAPHY—HARLEY & GREENFIELD

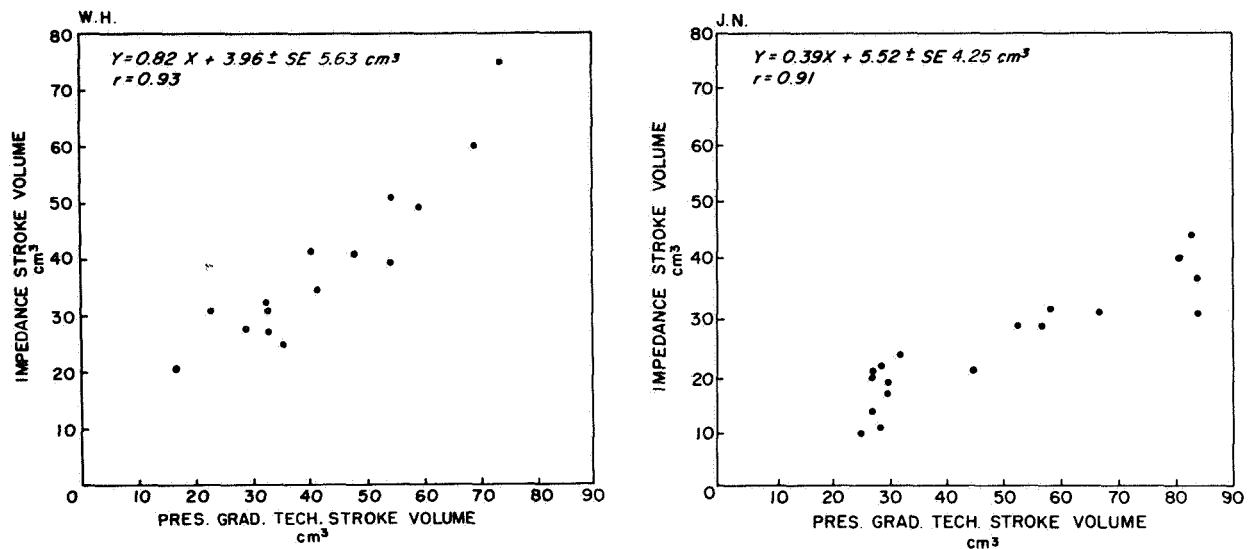


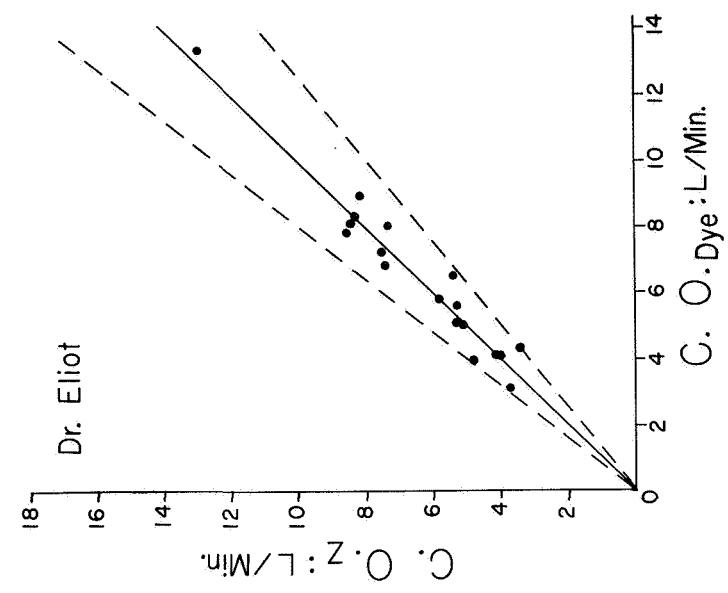
Fig. 5. Comparison of stroke volume for individual beats obtained by impedance plethysmography with those obtained for the same beats by the pressure gradient technique in two patients with pure mitral stenosis and atrial fibrillation.

ACKNOWLEDGEMENT

The authors wish to thank Dr. S. M. Fox of the Heart Disease Control program for his help in initiating these studies.

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(Eliot)

TABLE II-1

Patient #	Diagnosis	Procedure	C.O.Dye	C.O.Z	Z/Dye
1	mild mitral insufficiency	control Isuprel	4.1 5.0	6.2 7.8	1.51 1.56 (1.54)
2	normal heart	control Isuprel	5.8 8.3	6.3 9.0	1.09 1.08 (1.09)
3	normal heart	control Isuprel	8.1 13.3	10.3 15.9	1.27 1.19 (1.23)
4	mild pulmonic stenosis, atrial septal defect	control Isuprel	5.6 7.2	6.5 9.2	1.16 1.28 (1.22)
5	Idiopathic myocardopathy severe failure	control Isuprel	3.1 6.5	4.2 6.2	1.36 0.95 (1.15)
6	post op. coarctation of aorta	control Isuprel	7.8 8.9	8.2 7.9	1.05 0.89 (0.97)
7	normal heart	control Isuprel	4.1 5.1	7.7 9.8	1.80 1.92 (1.86)
8	coronary artery disease	control Isuprel	4.3 3.9	3.5 4.9	0.81 1.25 (1.03)
9	severe coronary artery disease	control Isuprel	6.8 8.0	5.5 5.4	0.81 0.68 (0.74)

C.O.Dye: Cardiac output-Dye dilution method

C.O.Z : Impedance cardiac output

Z/Dye : Ratio of impedance cardiac output to dye cardiac output

Mean Z/Dye in parentheses

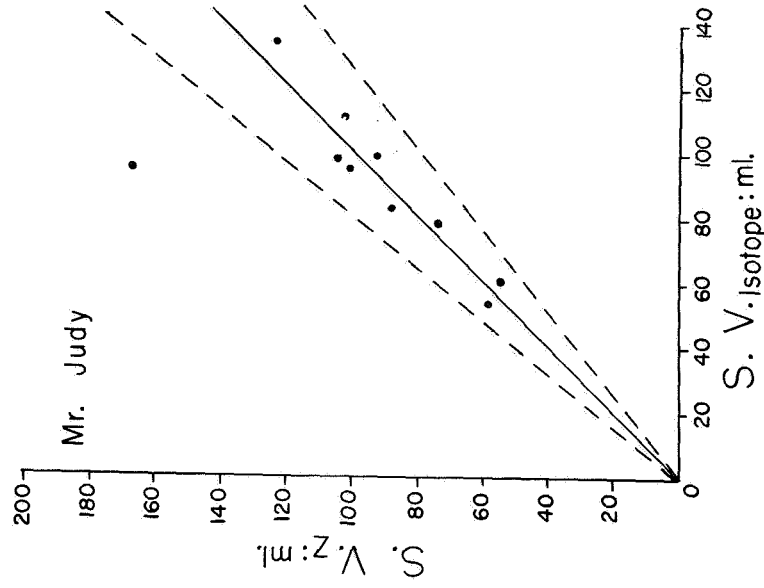


Fig. II-6 Corrected values of stroke volume by the Impedance method plotted against the original values obtained by the Isotope dilution technique

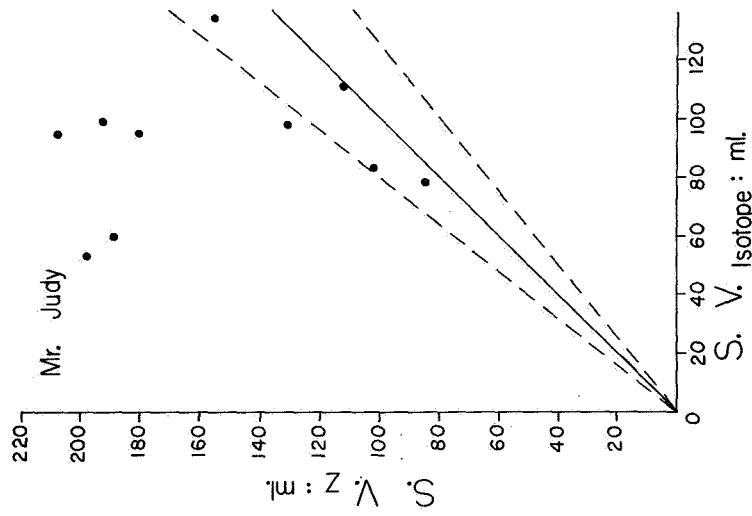


Fig. II-5 Stroke volume values obtained by the Impedance method and the Isotope dilution technique

TABLE II-2

Subj.	Cond.	Isotope Dil. Data	Heart Rt. Beat/Min.	Eject. time.		$Z_{sv}/\text{Isotope}_{sv}$	Eject. time		$Z_{sv}/\text{Isotope}_{sv}$
				1st Deriv.	C.O. cc/beat l/min		ECG	C.O. cc/beat l/min	
1	Passive	97.8	6.950	72	130.9 [±]	9.340 [±]	1.34	97.9 [±]	6.985 [±]
	Active	134.0	10.463	78	27.7	1.880		17.5	1.171
2	Passive	95.1	6.848	72	154.6 [±]	12.013 [±]	1.15 (1.25)	113.5 [±]	8.822 [±]
	Active	110.5	9.287	84	4.1	0.310		3.6	0.225
3	Passive	77.6	5.898	76	180.9 [±]	7.812 [±]	1.15	122.4 [±]	8.782 [±]
	Active	82.9	8.209	99	6.6	0.323		5.3	0.239
4	Passive	59.9	4.132	69	111.7 [±]	9.438 [±]	1.01 (1.08)	129.1 [±]	10.884 [±]
	Active	53.4	4.010	75	4.8	0.877		10.5	1.035
5	Passive	99.2	5.455	56	85.2 [±]	6.474 [±]	1.09	61.2 [±]	4.647 [±]
	Active	95.0	7.128	75	3.5	0.314		1.6	0.133
6	Passive	99.2	5.455	56	101.6 [±]	9.994 [±]	1.22 (1.16)	67.9	6.635 [±]
	Active	95.0	7.128	75	3.7	0.268		3.2	0.300
7	Passive	59.9	4.132	69	189.7 [±]	12.998 [±]	3.16	147.6 [±]	10.110 [±]
	Active	53.4	4.010	75	9.4	0.753		7.5	0.470
8	Passive	99.2	5.455	56	199.2 [±]	14.934 [±]	3.73 (3.45)	153.9 [±]	11.541 [±]
	Active	95.0	7.128	75	16.5	1.358		2.5	0.589
9	Passive	99.2	5.455	56	192.5 [±]	10.816 [±]	1.94	147.0 [±]	8.259 [±]
	Active	95.0	7.128	75	22.3	1.434		14.5	0.990
10	Passive	99.2	5.455	56	207.6 [±]	15.455 [±]	2.18 (2.06)	155.7 [±]	11.594 [±]
	Active	95.0	7.128	75	3.8	0.423		4.2	0.481

Cond.: Activity State

Isotope Dil. Data: Cardiac Output Determined by Isotope Dilution Technic

Eject. time, 1st Deriv.: Impedance Cardiac Output measured using Ejection time determined from dZ/dt

Eject. time, ECG: Impedance Cardiac Output measured using Ejection time determined from ECG.

 $Z_{sv}/\text{Isotope}_{sv}$: Ratio of Impedance Stroke Volume to Isotope Stroke VolumeMean $Z_{sv}/\text{Isotope}_{sv}$ is in parentheses

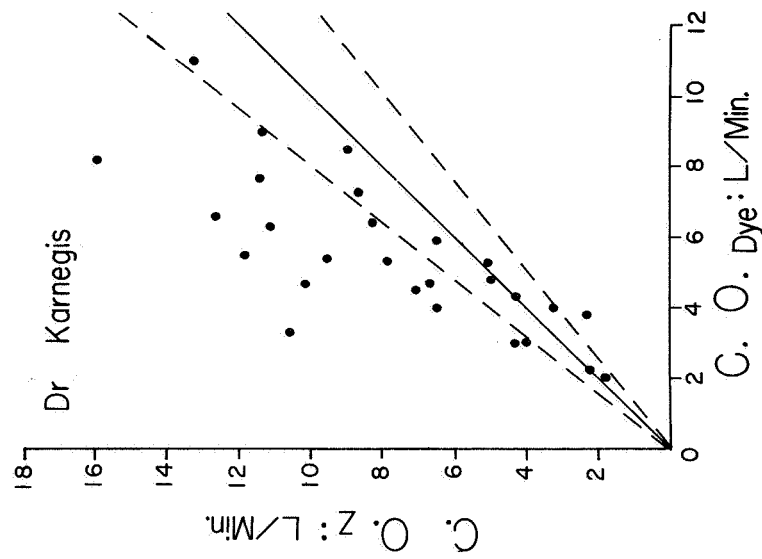


Fig. II-7 A graph of cardiac output values obtained by the Impedance and Dye dilution techniques

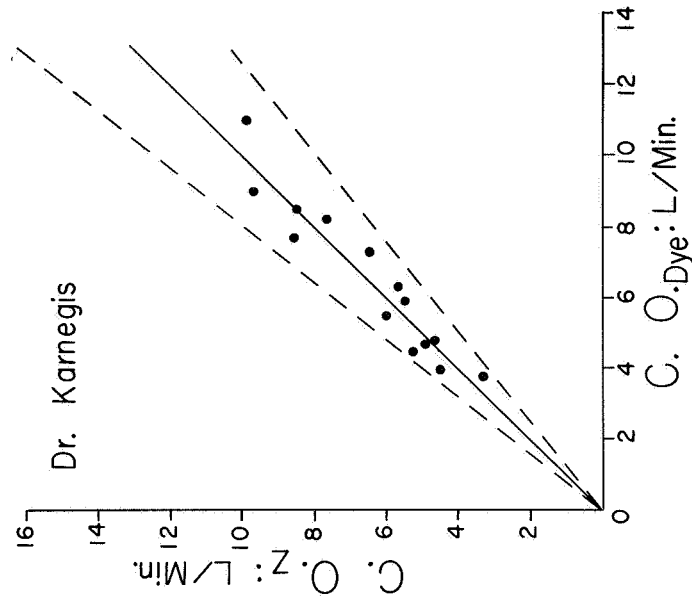


Fig. II-8 A graph of corrected values of cardiac output by the Impedance method plotted against the original values by the Dye method

(Karnegis)

TABLE II-3

PATIENT	DIAGNOSIS	PROCEDURE	C.O.F	C.O.DYE	C.O.Z	Z/DYE
A.N.	mild M.S.	rest exercise	10.0	7.7 11.0	11.5 13.3	1.49 1.20 (1.35)
I.N.	Turner's Syndrome MI	rest	3.3	2.95	4.3	1.41
M.M.	MS, MI, TI	rest	2.7		4.4	
A.E.	MS, MI	rest	2.5	2.15	2.2	1.02
M.K.	AS, AI, MI	rest	5.3	5.33	5.1	0.96
O.M.	AI, MI, Coronary Dis.	rest	4.6	5.26	7.9	1.56
C.D.	mild AI, MI	rest	5.1	3.0	3.98	1.33
L.S.	AI, MI	rest	4.2	5.35	9.6	1.78
L.H.	IDPA	rest exercise	6.8	5.9 9.0	6.5 11.4	1.10 1.26 (1.18)
D.S.	Dis. Aneurism, AI	rest	4.0	4.0	6.5	1.62
P.B.	MS, MI, AS, AI, TS	rest	2.4			
F.W.	AS, AI, MI	rest	4.8		6.2	
W.S.	mild MI	rest	6.7	6.57	12.7	1.93
W.H.	severe AS, mild AI	rest	4.8	3.6		
M.G.	mod.-severe AS, MS mild AI, MI	rest	3.7	4.26	4.3	1.01

(Karnegis)

TABLE II-3 cont'd

PATIENT	DIAGNOSIS	PROCEDURE	C.O.F	C.O.DYE	C.O.Z	Z/DYE
B.K.	AS, AI, MI	rest	3.3		3.5	
J.S.	MI	rest	6.7	6.4	8.3	1.30
T.M.	AS, AI, MI	rest	4.9	4.65	6.7	1.44
A.C.	AS	rest Isuprel	4.8	5.5 6.3	11.9 11.2	2.16 1.79 (1.97)
M.N.	MS, MI	rest	3.2	3.25	10.6	3.26
L.S.	left atrial myxoma	rest	2.6		7.2	
Z.S.	AS, AI	rest exercise	4.3	4.65 8.2	10.2 16.0	2.20 1.95 (2.08)
O.B.	minimal AI mild MI	rest exercise	5.4	4.75 8.45	5.0 9.0	1.05 1.06 (1.06)
M.D.	MS, MI, peculiar wave form	rest exercise	3.7	3.8 4.0	2.3 3.2	0.61 0.80 (0.71)
T.H.	mild MI	rest Isuprel	5.7	4.5 7.3	7.1 8.7	1.58 1.19 (1.39)
L.V.	MS, MI, AI	rest	2.3	1.96	1.75	0.89

C.O.F: Cardiac Output, Fick Method

C.O.DYE: Cardiac Output, Dye Dilution Method

C.O.Z: Impedance Cardiac Output

Z/DYE: Ratio of Impedance Cardiac Output to
Dye Cardiac Output

Mean Z/DYE in parentheses

AI = Aortic Insufficiency
MI = Mitral Insufficiency
TI = Tricuspid Insufficiency
AS = Aortic Stenosis
MS = Mitral Stenosis

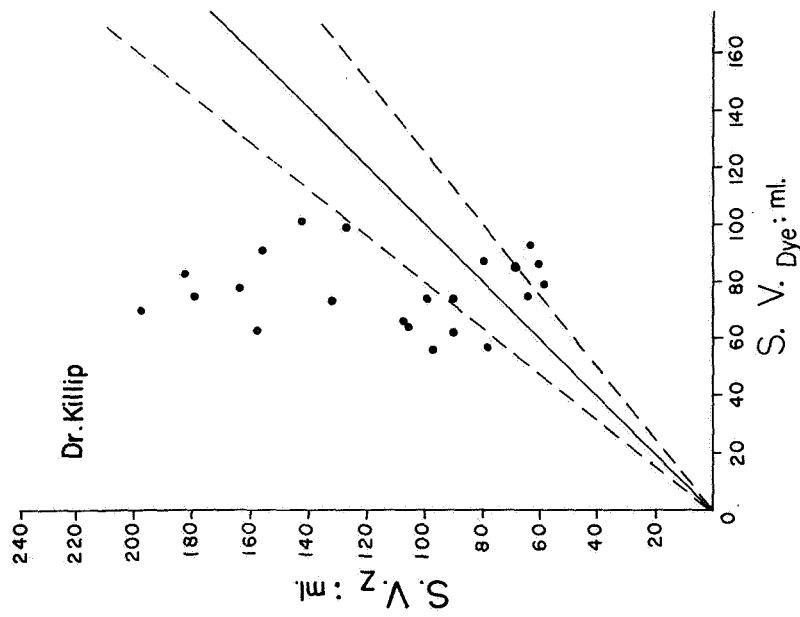


Fig. II-9 A plot of stroke volume values obtained by the Impedance and Dye dilution methods

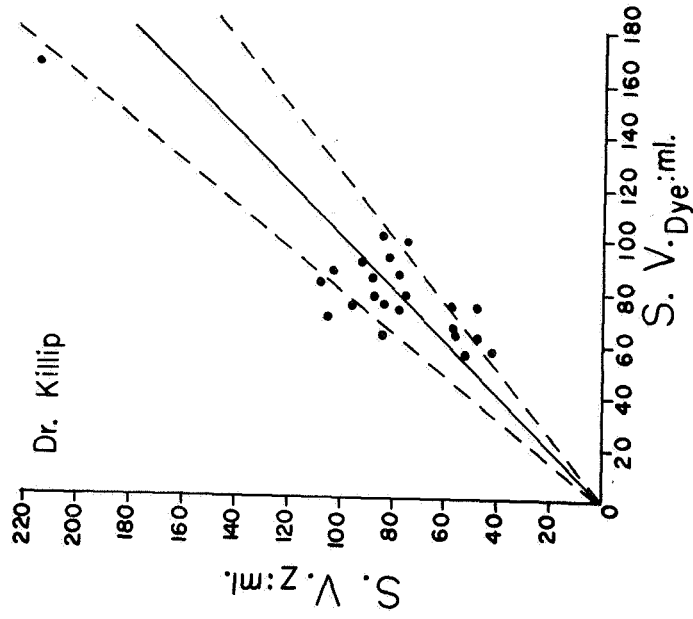


Fig. II-10 A graph of corrected Impedance stroke volume values plotted against the original values obtained by the Dye dilution technique

TABLE II-4

(Killip)

Patient	Diagnosis	HR	C.O. Dye	C.O. Z	Z/Dye
W.W.	Hemangioma		7.46	7.29	0.97
age - 18 yrs.	right cheek		7.17	8.18	1.14
			6.92	6.85	0.99
			7.85	6.75	0.86
			7.06	5.74	0.82
			8.27	6.61	0.79
					Mean (.92)
J.D.	Complete Heart	28	4.67	10.30	2.20
age - 64 yrs.	Block-Artificial	54	4.53	9.89	2.18
	pacemaker	54	3.99	7.13	1.78
		54	4.95	8.46	1.70
		70	7.11	10.00	1.40
		70	6.95	8.95	1.28
		100	7.48	9.93	1.32
					Mean (1.69)
B.S.	Complete Heart	65	4.10	10.30	2.51
age - 76 yrs.	Block-Pacemaker	65	4.86	5.86	1.20
		65	5.07	10.70	2.11
	Rate Adjusted	65	4.93	11.70	2.37
		77	4.85	6.93	1.42
		76	5.07	8.15	1.60
		75	5.32	14.90	2.80
		90	5.80	9.50	1.63
		91	5.18	8.84	1.70
		91	5.20	7.16	1.37
					Mean (1.87)
G.V.	Complete Heart	72	6.20	4.32	0.69
age - 68 yrs.	Block-Pacemaker	72	6.16	4.90	0.79
		72	6.73	4.54	0.67
	Rate Adjusted	79	5.95	5.10	0.91
		79	6.27	4.60	0.73
		79	6.95	6.25	0.89
					Mean (.78)

C.O. Dye: Cardiac Output, Dye Dilution Method L/Min Z/Dye: Ratio of Impedance Cardiac

C.O. Z: Impedance Cardiac Output L/Min Output to Dye Cardiac Output

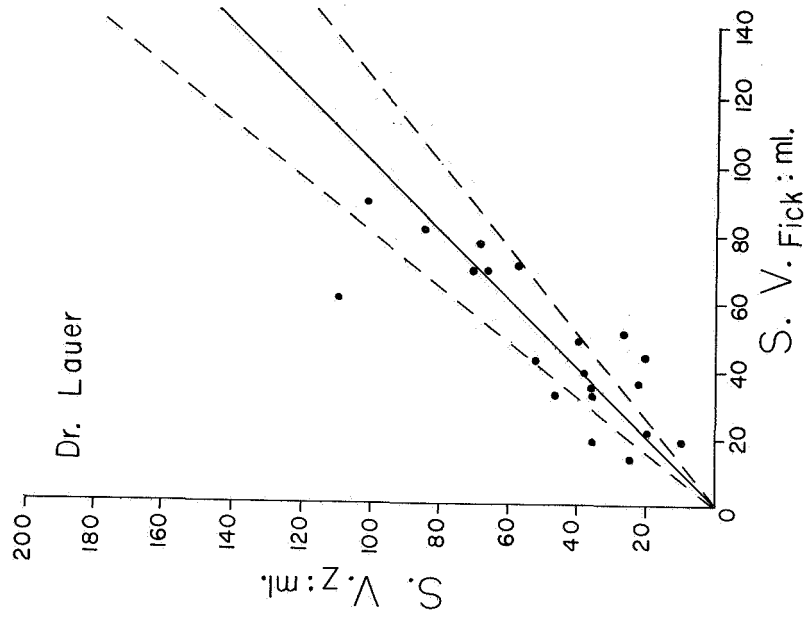


Fig. II-12 A graph of corrected Impedance stroke volume values plotted against the original values obtained by the Fick method

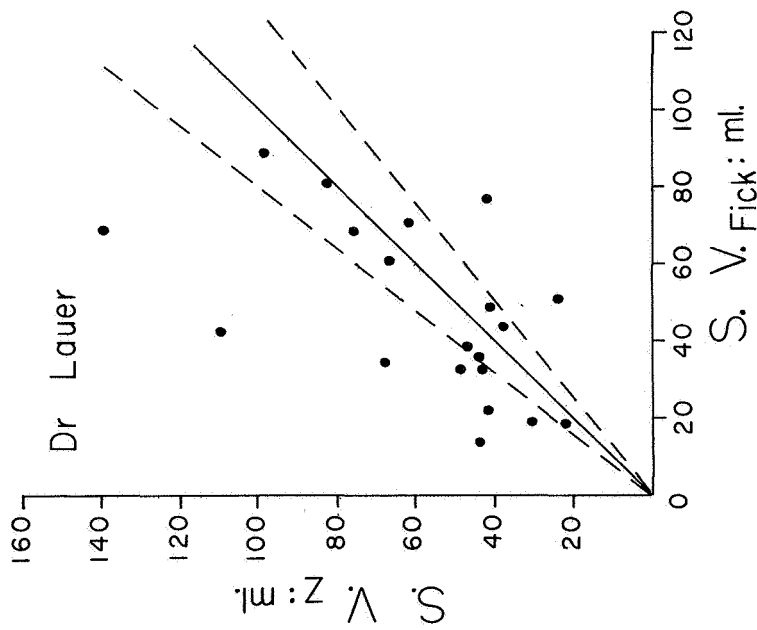


Fig. II-11 A plot of stroke volume values obtained by the Impedance and Fick methods

TABLE II-5 (Lauer)

Patient	Age	Sex	Diagnosis	State	FICK METHOD			IMPEDANCE METHOD			
					Stroke Vol.	C.O.	H.R.	Stroke Vol.	C.O.	H.R.	Z/Fick Ratio
K.N.	13	M	Bicuspid AV	Resting Isup.	43.0 69.3	3.44 8.32	80 120	110.35 139.91	10.79 16.55	98 118	2.56 1.59 (2.07)
E.T.	7	M	Tetralogy of Fallot-postop.	Resting Isup.	21.9 18.6	2.19 2.60	100 140	41.78 21.57	3.97 3.91	96 180	1.90 2.24 (2.08)
S.W.	9	F	Partial AV canal	Resting Isup.	43.7 14.1	5.24 2.26	120 160	37.53 44.40	4.42 4.94	117 111	0.85 2.66 (1.76)
R.L.	6	M	T/F, postop. Brocks	Resting Isup.	33.1 39.1	3.31 5.48	100 140	43.05 46.70	4.21 6.92	97 148	1.30 1.10 (1.20)
M.S.	14	M	Ebstein's Anomaly	Resting Isup.	69.4 70.9	6.94 8.51	100 120	75.63 61.99	6.48 7.28	86 118	1.08 1.06 (1.07)
R.B.	3	M	Tetralogy of Fallot-postop.	Resting Isup.	48.9 33.2	5.87 5.32	120 160	41.08 48.67	6.16 7.75	148 160	0.84 1.23 (1.04)
D.F.	6	F	Mild PS ASD ff mild L/R	Resting Isup.	34.7 36.3	3.12 5.08	90 140	68.48 44.46	6.34 6.06	92 137	1.97 1.88 (1.93)
W.S.	14	M	Normal	Resting Isup.	76.5 60.9	7.65 8.53	100 140	41.95 67.30	5.01 9.14	119 135	0.54 0.68 (0.61)
J.S.	15	M	Bicuspid AV	Resting Isup.	81.1 89.4	6.49 7.15	80 80	82.75 98.50	6.63 7.88	81 80	1.02 0.92 (0.97)
T.A.	6	M	VSD, bidir. shunt, Occ. PVD	Resting Isup.	50.5 18.5	6.50 3.33	130 180	23.75 31.39	3.50 4.14	152 130	0.47 1.28 (0.87)

Z/Fick Ratio: Ratio of Impedance stroke volume to Z/Fick stroke volume.

Mean Z/Fick is in parentheses

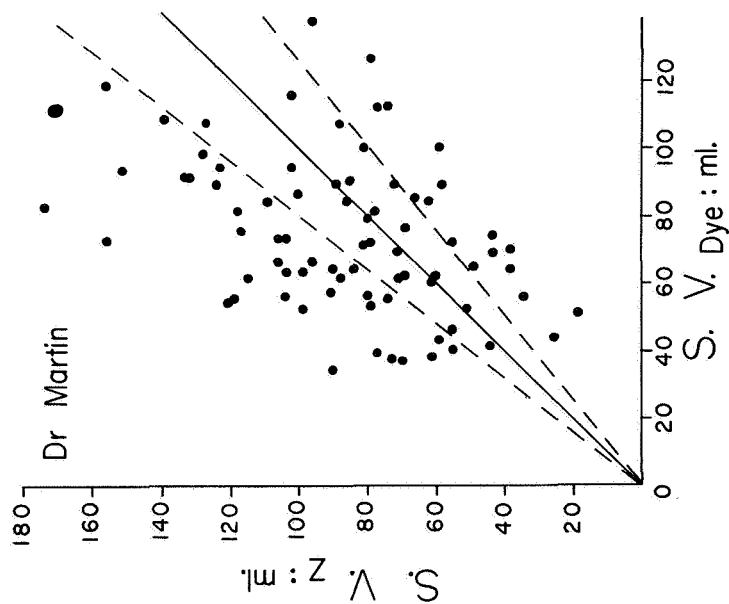


Fig. II-13 A graph of stroke volume values obtained by the Impedance and Dye dilution techniques

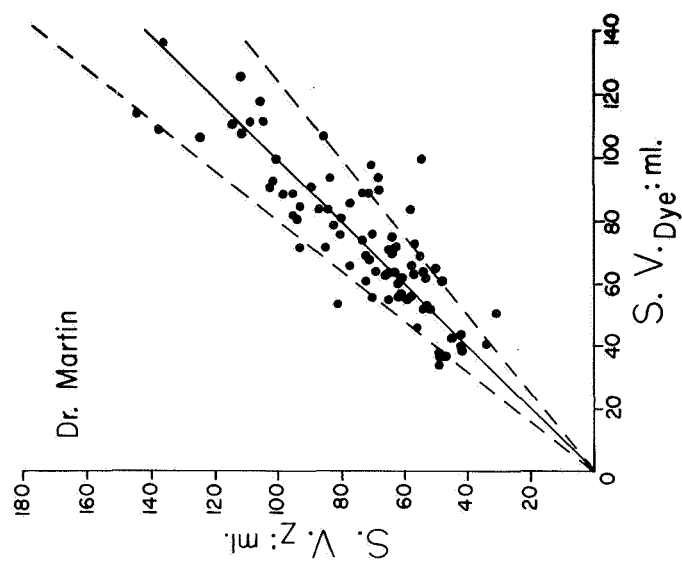


Fig. II-14 A graph of corrected Impedance stroke volume values plotted against the original values obtained by the Dye method

(Martin)

TABLE II-6

Patient #	Sample #	SV _Z	SV _{Dye}	Z/Dye
1	1	128	98	1.31
	2	-	-	-
	3	106	66	1.61
	4	117	75	1.56
	5	104	73	1.42
	6	99	52	1.92
	7	77	39	1.97
	8	90	34	2.64
	11	119	55	2.16
	12	115	61	1.89
	13	174	82	2.12
	14	156	72	2.17
	15	104	63	1.65
	16	88	61	1.44
				(1.83)
2	1	81	100	0.81
	2	70	37	1.89
	3	73	37	1.97
	4	79	53	1.49
	5	99	63	1.57
	6	106	73	1.45
	7	121	54	2.24
	8	104	56	1.86
	9	91	57	1.60
	10	86	84	1.02
	11	170	111	1.53
	12	127	107	1.19
	13	151	93	1.62
	14	123	94	1.31
	15	133	91	1.46
	16	102	94	1.09
	17	156	118	1.32
				(1.49)

(Martin)

TABLE II-6 cont'd

Patient #	Sample #	SV _Z	SV _{Dye}	Z/Dye
3	1	132	91	1.45
	2	71	69	1.03
	3	124	89	1.39
	4	80	56	1.43
	5	55	40	1.38
	6	109	84	1.30
	7	90	64	1.42
	8	69	62	1.11
	9	100	86	1.41
	11	84	64	1.33
	12	59	43	1.37
	13	44	41	1.07
				(1.30)
4	2	62	84	0.74
	3	77	112	0.69
	5	102	115	0.89
	6	88	107	0.64
	8	66	85	0.78
	9	74	112	0.66
	11	96	137	0.70
	12	79	126	0.63
				(0.71)
5	1	85	90	0.94
	2	61	38	1.60
	3	74	55	1.35
	4	118	81	1.46
	5	79	72	1.10
	6	89	89	1.00
	7	139	108	1.29
	8	171	110	1.55
	9	96	66	1.05
	10	81	71	1.14
				(1.25)

(Martin)

TABLE II-6 cont'd

Patient #	Sample #	SV _Z	SV _{Dye}	Z/Dye
6	1	58	89	0.65
	2	18	51	0.35
	3	25	44	0.57
	4	34	56	0.61
	5	55	72	0.76
	6	43	69	0.62
	7	38	64	0.59
	8	38	70	0.54
	9	43	74	0.62
	10	59	100	0.59 (0.59)
7	1	72	89	0.81
	2	80	79	1.01
	3	60	62	0.97
	4	55	46	1.20
	5	51	52	0.98
	6	49	65	0.75
	7	78	81	0.96
	8	69	76	0.91
	9	61	60	1.02
	10	71	61	1.16 (0.98)

SV_Z: Stroke Volume by Impedance MethodSV_{Dye}: Stroke Volume by Cardio Green Dye Method

Z/Dye: Ratio of Impedance Stroke Volume to Dye Stroke Volume - Mean Z/Dye is in parentheses

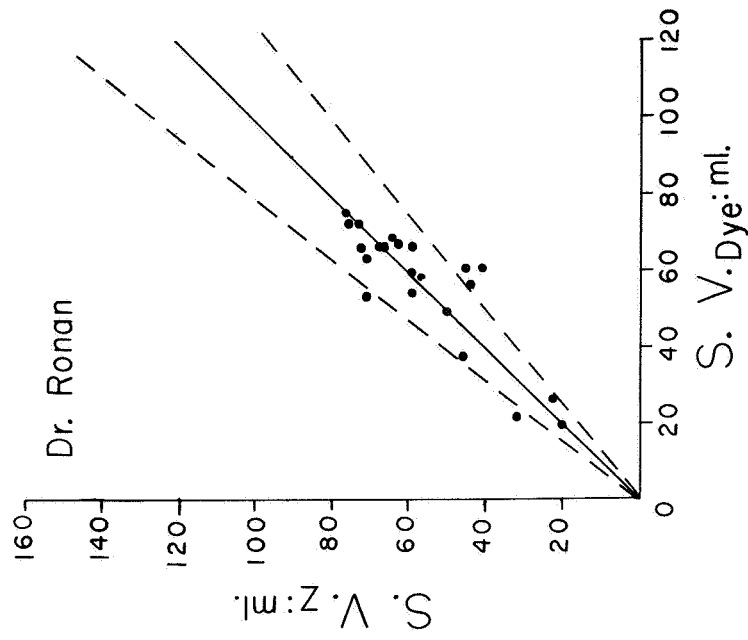


Fig. II-16 A graph of corrected Impedance stroke volume values plotted against the original values by the Dye method

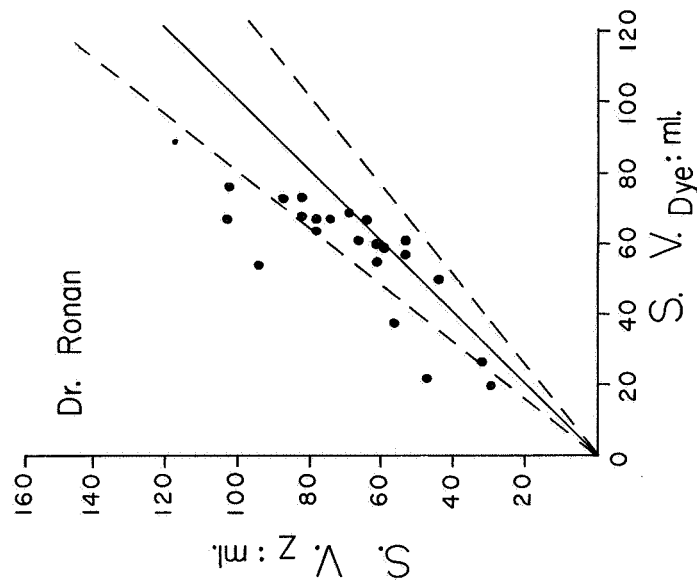


Fig. II-15 A graph of stroke volume values obtained by the Impedance and Dye dilution methods

(Ronan)

TABLE II-7

Patient	Clinical Setting	Impedance			Dye Dilution			C.O.	Z/Dye
		S.V.	H.R.	C.O.	S.V.	H.R.	C.O.		
G.	Intensive care	45	98	4.4	50	96	4.8	0.90	
B.	Intensive care	54	87	4.7	57	90	5.2	0.95	
		57	72	4.1	38	84	3.2	1.50	(1.24)
S.	Coronary Angio.	88	80	7.0	73	80	5.9	1.20	
C.	Coronary Angio.	75	63	4.8	67	66	4.4	1.12	
D.	Coronary Angio.	70	80	5.6	69	78	5.4	1.01	
		79	78	6.1	67	78	5.2	1.17	(1.09)
L.	Coronary Angio.	104	63	6.6	67	72	4.8	1.55	
M.	Coronary Angio.	103	64	6.6	76	70	5.3	1.35	
H.	Coronary Angio.	60	68	4.1	59	72	4.2	1.01	
	Angiotensin	62	77	4.8	55	78	4.3	1.12	
	Angiotensin	62	79	4.9	60	84	5.0	1.03	(1.05)
T.	Coronary Angio.	65	97	6.3	67	90	6.0	0.97	
	Angiotensin	83	81	6.7	73	75	5.5	1.13	
	Angiotensin	79	90	7.1	64	84	5.4	1.23	(1.11)
D.	Coronary Angio.	54	100	5.4	61	102	6.2	0.88	
	Angiotensin	84	83	7.1	68	84	5.2	1.23	
	Angiotensin	95	86	8.2	54	84	4.5	1.75	(1.33)
S.	Coronary Angio.	48	86	4.2	22	84	1.9	2.18	
	Angiotensin	30	98	3.0	20	102	2.1	1.50	
	Control	33	96	3.2	27	96	2.6	1.22	
	Isuprel	67	98	6.6	61	96	5.8	1.09	(1.49)

S.V.: Stroke Volume
H.R.: Heart Rate
C.O.: Cardiac Output

Z/Dye: Ratio of Impedance Stroke Volume to Dye
Stroke Volume -- Mean Z/Dye is in parentheses

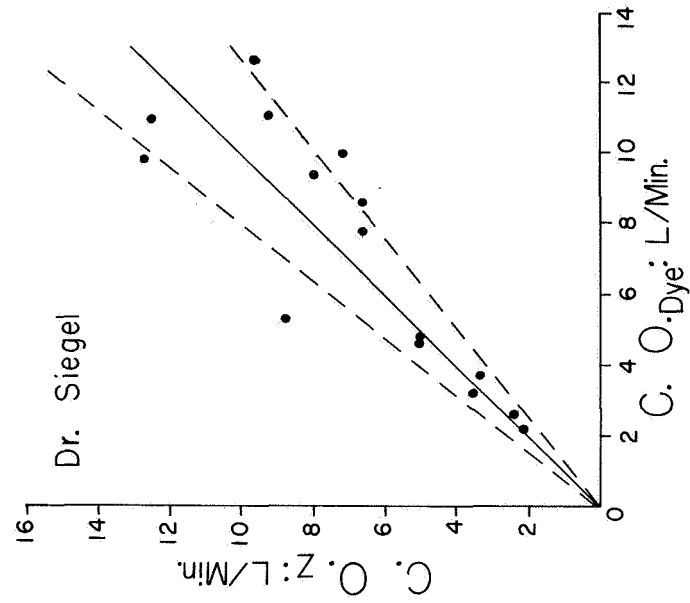


Fig. II-18 A graph of corrected Impedance cardiac output values plotted against the original values by the Dye method

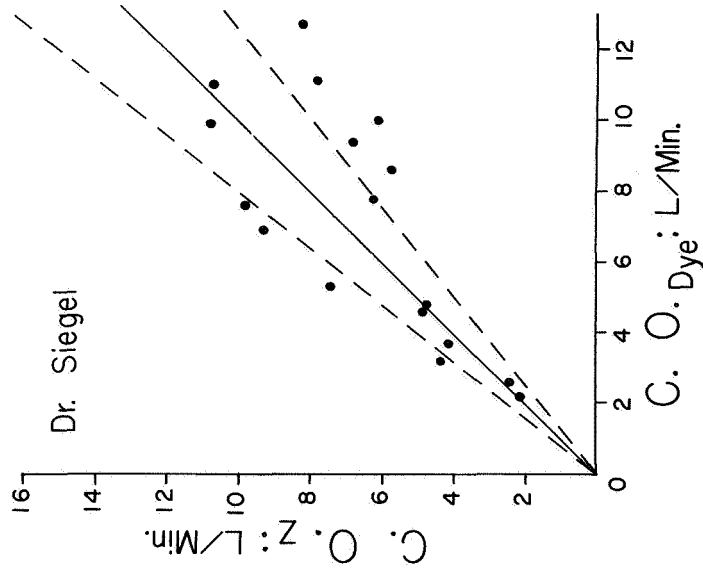


Fig. II-17 A graph of cardiac output values obtained by the Impedance and Dye dilution techniques

TABLE II-8 (Siegel)

Patient	Intervention	CO ₂	CO Computer	SH	Z/Dye	CO Manual	SH	Z/Dye	CO Gamma	Varient	Z/Dye
DM	Control	4.76	3.93		1.21	4.55		1.04	4.20		1.13
	p 500 ml Plasmonate	4.71	4.73		0.99	4.81		0.97	5.25		0.90
	1γ/min Isuprel	6.27	7.83		0.80	7.84		0.79	9.70		0.65
	p Isuprel	5.82	3.12		MEAN 1.00			MEAN 0.93			MEAN 0.89
D	Control Room Air	4.29	3.75		1.37	3.24		1.32	5.60		0.77
	100% O ₂	4.11			1.09	3.73		1.10	4.80		0.86
	p 100% O ₂	5.57			MEAN 1.23			MEAN 1.21			MEAN 0.82
PM	Control Room Air	2.13	2.17		0.98	2.17		0.98	2.60		0.82
	100% O ₂	2.43	4.08		0.59	2.55		0.95	5.20		0.47
					MEAN 0.79			MEAN 0.97			MEAN 0.65
Q	Control Room Air	5.66	10.47		0.54	8.56		0.66	8.60		0.65
	100% O ₂	6.11	10.09		0.60	10.03		0.60	9.20		0.66
	Control Room Air	8.50									
	Control Room Air	7.83	10.65		0.73	11.10		0.70	9.00		0.87
	100% O ₂	8.22	12.40		0.66	12.67		0.64	12.20		0.67
	Control Room Air	10.83	9.64		1.12	9.92		1.09	11.40		0.95
	100% O ₂	10.66	10.58		1.00	10.95		0.97	10.00		1.06
	Control Room Air	7.42	5.34		1.38	5.33		1.39	4.60		1.61
	100% O ₂	6.80	8.57		0.79	9.38		0.72	8.60		0.79
					MEAN 0.86			MEAN 0.85			MEAN 0.91
A	Control Room Air	9.33	5.07		1.84	6.94		1.34	6.10		1.53
	100% O ₂		4.80			6.27			5.05		
MD	Control Room Air	9.76	8.56		1.14	7.56		1.29	10.60		1.08

KEY TO COLUMN HEADINGS - TABLE II-8 (Siegel)

C.O. Z : Impedance Cardiac Output

C.O.Computer S.H.: Dye Cardiac Output automatically computed by Stewart Hamilton Method

C.O.Manual S.H.: Dye Cardiac Output manually computed by Stewart Hamilton Method

C.O.gamma varient: Cardiac Output, Gamma Varient Method

Z/Dye: Ratio of Impedance C.O. to S.H. Dye C.O.

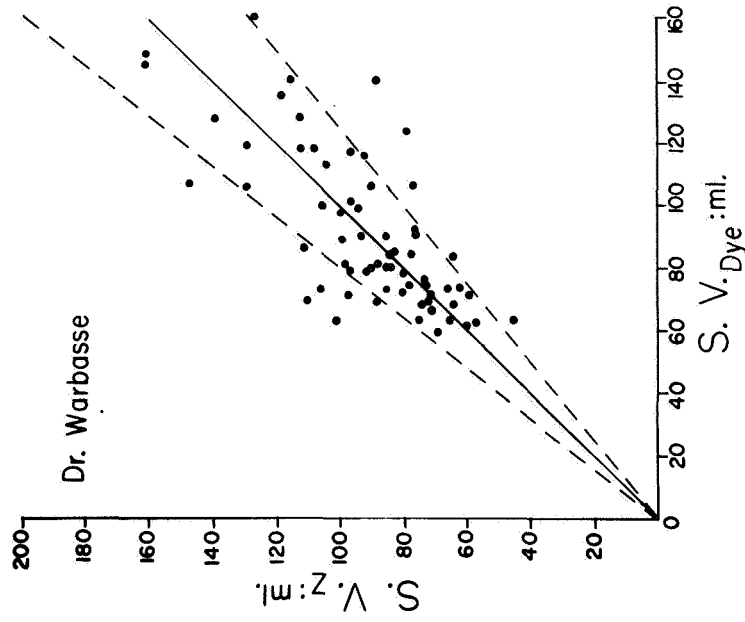


Fig. II-20 A graph of the corrected Impedance stroke volume values plotted against the original values obtained by the Dye dilution method

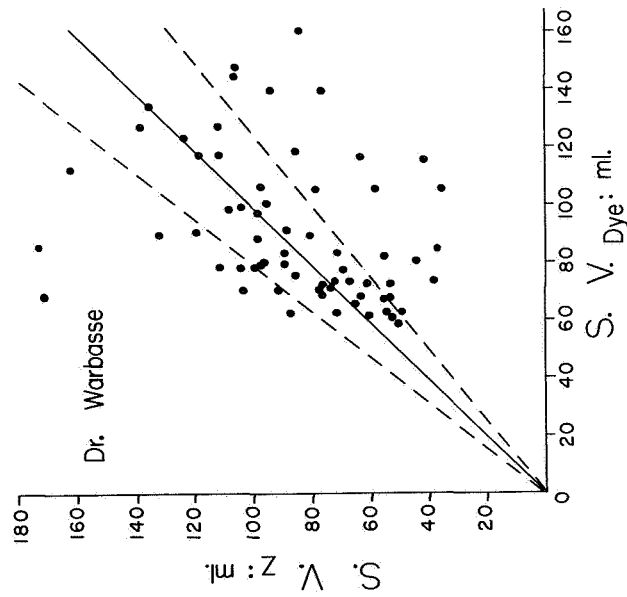


Fig. II-19 A graph of stroke volume values obtained by the Impedance and Dye dilution methods

(Warbasse)

TABLE II-9
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION

Study #	Patient's Initials	Single Typical Beat		Average 4 heart Beats		Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error Vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	
1	C.W.							
1a		82.11	4.93	16	76.98	4.62	+9	4.24
b		71.85	4.31	2			(1.09)	
c		76.98	4.62	9				
d		76.98	4.62	9				
2a		89.56	5.55	42	71.08	4.41	+13	3.90
b		68.24	5.02	8			(1.13)	
c		72.50	5.55	15				
d		72.50	5.29	15				
3a		99.97	6.00	24	96.16	5.77	+19	4.83
b		96.50	5.79	20			(1.19)	
c		91.68	5.50	14				
d		96.5	5.79	20				
4a		48.03	5.91	24	48.91	6.03	-22	7.74
b		48.03	5.91	24			(.78)	
c		49.14	6.04	22				
d		50.44	6.20	20				

TABLE II-9 contd.
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION
(Warbasse)

Study #	Patient's Initials	Single Typical Beat		Average 4 Heart Beats		Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	
1	C.W.							
5a		115.3	7.03	2	117.78	7.18		118.03 61 7.20
b		122.09	7.45	3.4			-0.22	
c		115.3	7.03	2			(1.00)	
d		118.4	7.22	0.3				
6a		96.84	8.72	23	99.10	8.91	+25	79.00 90 7.11
b		99.10	8.92	25				
c		99.10	8.92	25			(1.25)	
d			9.12	28				

(Warbasse)

TABLE II-10
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION

Study #	Patient's Initials	Single Typical Beat		Average 4 Heart Beats		Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	
2	D.B.							
1a		72.11	4.98	4.0	76.35	5.27	+10.2	69 4.78
b		74.60	5.15	7.7			(1.10)	
c		74.60	5.15	7.7				
d		84.10	5.80	21.4				
2a		86.81	5.64	8.1	89.10	5.79	+10.9	80.31 65 5.22
b		89.52	5.82	11.5			(1.11)	
c		86.81	5.64	8.1				
d		93.25	6.06	16.1				
3a		93.22	11.65	33.4	93.22	11.65	-33.4	139.92 17.49
b		93.22	11.65	33.4			(0.67)	
c		95.30	11.91	31.9				
d		91.15	11.39	35.9				
4a		90.67	13.48	7.4	89.47	13.06	+6.0	84.41 12.24
b		85.00	12.33	0.7			(1.06)	
c		89.14	12.92	5.6				
d		93.07	13.50	10.3				

(Warbasse)

TABLE II-10 cont'd
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION

Study #	Patient's Initials	Single Typical Beat			Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye			
2	D.B.									
5a		63.02	6.30	2.3	60.39	6.04	-1.9	61.60	100	6.16
b		60.28	6.03	2.1			(0.98)			
c		60.28	6.03	2.1						
d		57.96	5.80	5.9						
6a		107.49	13.87	34.0	102.7	13.26	+44.6	71.01	129	9.17
b		101.16	13.05	42.3			(1.45)			
c		101.16	13.05	42.3						
d		101.16	13.05	42.3						

TABLE II-11
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION
(Warbasse)

Study #	Patient's Initials	Single Typical Beat		Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye		
3	R.F.								
1a		91.84	5.88	14.4	97.2	6.22	+21.0	64	5.14
b		89.46	5.73	11.4			(1.21)		
c		107.35	6.87	33.6					
d		100.2	6.41	24.8					
2a		109.28	6.49	37.5	111.3	6.61	+40.0	59.4	4.72
b		120.42	7.15	51.5			(1.4)		
c		111.99	6.65	40.9					
d		103.5	6.15	30.3					
3a		101.68	6.20	29.2	104.4	6.28	+32.6	61	4.84
b		101.68	6.20	29.2			(1.33)		
c		104.96	6.40	33.4					
d		107.40	6.55	36.5					
4a		141.61	11.33	4.9	135.18	10.82	+ 0.1	80	10.80
b		146.85	11.75	8.8			(1.00)		
c		110.0	8.8	18.5					
d		142.27	11.38	5.4					

TABLE II-11 cont'd
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION
(Warbasse)

Study #	Patient's Initials	Single Typical Beat			Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye			
3	R.F.									
5a		105.83	10.58	6.9	107.55	10.76	+8.6	99	100	9.90
b		107.95	10.8	9.0			(1.09)			
c		97.37	9.74	1.65						
d		119.06	11.91	20.2						
6a		86.77	7.01	5.54	87.5	7.08	-4.74	91.85	81	7.44
b		86.77	7.01	5.54			(0.95)			
c		86.77	7.01	5.54						
d		89.70	7.27	2.35						
7a		82.21	6.17	7.8	84.5	6.23	+10.8	76.26	75	5.72
b		85.26	6.39	11.8			(1.11)			
c		85.26	6.39	11.8						
d		85.26	6.39	11.8						

TABLE II-12
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION
(Warbasse)

Study #	Patient's Initials	Single Typical Beat		Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye		
4	H.R.								
1a		83.22	5.66	17.63	95.12	7.47	-5.85	68	6.87
b		98.76	6.72	2.25			(0.94)		
c		105.06	7.14	3.99					
d		93.43	6.35	7.52					
2a		90.62	6.80	1.44	97.88	7.34	+9.57	75	6.70
b		99.35	7.45	11.22			(1.10)		
c		98.53	7.39	10.29					
d		103.03	7.73	15.33					
3a		94.12	7.25	4.13	98.18	7.56	0.00	77	7.56
b		99.91	7.69	1.76			(1.00)		
c		103.03	7.93	4.94					
d		95.67	7.37	2.56					
4a		111.45	11.15	5.15	110.66	11.07	-5.82	100	11.75
b		120.23	12.02	2.32			(0.94)		
c		96.21	9.62	18.12					
d		114.76	11.48	2.33					

(Warbasse)

TABLE II-12 cont'd
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION

Study #	Patient's Initials	Single Typical Beat			Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye			
4	H.R.									
5a		140.98	13.25	9.98	138.04	12.97	+7.68	128.19	94	12.05
b		145.14	13.64	13.22						
c		130.68	12.28	1.93			(1.08)			
d		135.38	12.72	5.6						
6a		112.70	10.14	12.03	110.87	9.98	-13.46	128.11	90	11.53
b		118.46	10.66	7.53			(0.87)			
c		105.62	9.51	17.56						
d		106.69	9.60	16.72						
7a		108.71	9.35	8.59	104.29	8.97	+4.17	100.12	86	8.61
b		109.05	9.39	8.93			(1.04)			
c		111.04	9.55	10.91						
d		88.36	7.60	11.74						

(Warbasse)

TABLE II-13
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION

Study #	Patient's Initials	Single Typical Beat		Average 4 Heart Beats		Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	
5	B.G.							
1a		73.628	5.74	0.81	71.74	5.60	-3.35	78 5.79
b		70.12	5.47	5.54			(0.97)	
c		69.74	5.44	6.05				
d		73.46	5.73	1.04				
2a		75.30	5.87	4.32	73.26	5.71	+1.50	78 5.63
b		75.43	5.88	4.50			(1.01)	
c		72.23	5.63	0.059				
d		70.09	5.47	2.9				
3a		62.49	6.24	15.21	67.38	6.73	-8.58	100 7.37
b		70.72	7.07	4.04			(0.91)	
c		62.49	6.24	15.21				
d		73.80	7.38	0.14				
4a		70.09	7.13	16.14	70.86	7.22	-15.22	101.7 8.50
b		65.89	6.70	21.17			(0.85)	
c		75.16	7.64	10.07				
d		72.69	7.39	13.03				

TABLE II-13 cont'd
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION
(Warbasse)

Study #	Patient's Initials	Single Typical Beat		Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye		
5	B.G.								
5a		62.65	5.51	24.86	60.91	5.36	-16.24	88	6.40
b		59.39	5.23	18.34			(0.84)		
c		58.97	5.19	18.92					
d		62.65	5.51	13.86					
6a		65.00	5.30	0.43	65.26	5.39	-0.64	81	5.32
b		67.28	5.45	0.44			(0.99)		
c		66.08	5.35	0.61					
d		67.28	5.45	2.44					

(Warbasse)

TABLE II-14
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION

Study #	Patient's Initials	Single Typical Beat			Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye			
6	L.T.									
1a		160.07	12.65	87.	172.96	12.34		85.57	79	6.76
b		161.27	12.10	78.6			+102.1			
c		170.84	12.22	80.7			(2.02)			
d		199.65	12.38	83.1						
2a		179.87	11.2	161	171.26	10.76		68.89	63	4.34
b		158.95	10.01	130.7			+148.6			
c		177.94	11.21	158.			(2.48)			
d		168.28	10.6	144.						
3a		158.62	18.24	40.3	162.01	18.63		113.04	115	13.0
b		151.40	17.41	30.9			+43.3			
c		161.30	18.55	42.7			(1.43)			
d		176.72	20.32	56.33						
4a		118.72	14.24	4.20	122.68	14.72		123.92	120	14.87
b		119.65	14.36	4.20			-1.0			
c		130.59	15.67	5.38			(0.99)			
d		121.76	14.61	1.75						

TABLE II-14 cont'd
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION
(Warbasse)

Study #	Patient's Initials	Single Typical Beat		Average 4 Heart Beats		Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	
6	L.T.							
5a		120.41	12.28	32.29	119.09	12.14		90.59
b		117.77	12.01	30.0				
c		117.77	12.01	30.0				
d		120.41	12.28	32.29				
6a		121.13	11.5	34.90	132.48	12.58		89.79
b		132.14	12.55	47.18				
c		132.14	12.55	47.18				
d		144.57	13.72	60.94				
7a		91.38	12.15	28.47	91.33	12.14		71.13
b		97.40	12.95	36.69				
c		89.46	11.90	25.58				
d		87.08	11.58	22.42				

(Warbasse)

TABLE II-15
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION

Study #	Patient's Initials	Single Typical Beat		Average 4 Heart Beats		Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	
7	C.J.							
1a		31.29	2.28	63.4	37.25	2.72	-56.4	85.48 73 6.24
b		39.73	2.90	53.5			(0.44)	
c		35.96	2.63	57.9				
d		42.03	3.08	50.8				
2a		38.63	2.76	47.7	38.40	2.74	-48.0	73.80 71.4 5.24
b		38.63	2.76	47.7			(0.52)	
c		40.17	2.87	45.6				
d		36.18	2.58	50.1				
3a		51.95	6.23	51.0	58.18	6.95	-45.1	106.00 120 12.72
b		53.91	6.47	49.1			(0.55)	
c		59.80	7.18	43.6				
d		67.04	8.05	36.8				
4a		39.95	4.79	65.6	41.27	4.95	-64.5	116.25 120 13.95
b		41.15	4.94	64.6			(0.36)	
c		42.40	5.09	63.5				
d		41.58	4.99	64.2				

TABLE II-15 cont'd
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION
(Warbasse)

Study #	Patient's Initials	Single Typical Beat			Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye			
7	C.J.									
5a		46.85	3.98	42.1	44.23	3.76	-45.4	80.94	85	6.88
b		46.54	3.96	42.5			(0.55)			
c		42.78	3.64	47.2						
d		40.74	3.46	49.7						
6a		31.26	3.19	70.6	34.51	3.52	-67.6	106.47	102	10.86
b		37.84	3.86	64.5			(0.32)			
c		34.47	3.52	67.6						
d		34.47	3.52	67.6						

TABLE II-16
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION

[illegible]

TABLE II-16 cont'd
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION
(Warbasse)

Study #	Patient's Initials	Single Typical Beat			Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume	Impedance Cardiac Output L/Min	% of Error vs Dye			
8	J.P.									
5a		75.71	5.68	45.8	76.09	5.25	-45.54	139.70	67	9.36
b		71.50	4.79	48.8			(0.54)			
c		74.56	5.00	46.6						
d		82.59	5.53	40.9						
6a		108.62	9.88	27.1	105.98	9.65		145.27	91	13.22
b		107.52	9.78	26.0			-27.05			
c		103.19	9.39	29.0			(0.73)			
d		104.86	9.54	27.8						
7a		56.12	3.98	51.9	63.49	4.50	-45.63	116.76	71	8.29
b		65.94	4.68	43.5			(0.54)			
c		70.19	4.98	39.9						
d		61.73	4.38	47.1						

(Warbasse)

TABLE II-17
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION

Study #	Patient's Initials	Single Typical Beat			Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye			
9	C.R.									
1a		51.83	3.16	37.77	55.17	3.35	-33.76	83.28	61	5.08
b		61.96	3.78	25.61			(0.66)			
c		53.45	3.26	35.82						
d		53.45	3.26	35.82						
2a		53.35	3.33	26.93	53.15	3.32	-27.21	73.01	62.5	4.60
b							(0.73)			
c		54.26	3.39	25.69						
d		51.83	3.24	29.01						
3a		53.33	3.25	21.43	54.63	3.33	-19.51	67.87	61	4.14
b		46.59	2.84	31.36			(0.80)			
c		62.95	3.84	7.25						
d		55.63	3.39	18.04						
4a		82.51	8.50	8.23	79.94	8.23	-11.08	89.90	103	9.26
b		82.51	8.50	8.23			(0.89)			
c		74.67	7.69	16.95						
d		80.08	8.25	10.93						

TABLE II-17 cont'd
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION
(Warbasse)

Study #	Patient's Initials	Single Typical Beat		Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye		
9	C.R.								
5a		83.59	8.96	20.99	77.73	8.32	-26.53	105.79	11.32
b		76.43	8.18	27.76			(0.73)		
c		77.40	8.28	26.84					
d		73.49	7.86	30.54					
6a		67.3	5.79	13.62	68.71	5.91	-11.81	77.91	6.7
b		67.30	5.79	13.62			(0.88)		
c		66.25	5.70	14.97					
d		74.00	6.36	5.02					
7a		95.60	10.99	54.41	86.63	9.96	+37.22	63.13	7.26
b		78.52	9.03	24.37			(1.37)		
c		78.52	9.03	24.37					
d		93.87	10.80	48.72					
8a		52.86	4.97	14.04	52.01	4.89	-15.42	61.49	5.78
b		49.75	4.68	19.1			(0.85)		
c		51.21	4.81	19.1					
d		54.22	5.10	11.83					

TABLE II-18
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION
(Warbasse)

Study #	Patient's Initials	Single Typical Beat			Average 4 Heart Beats			Dye Stroke Volume cc	Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye			
10	J.B.									
1a		54.66	3.72	19.16	53.44	3.80	-21.35	67.94	68	4.62
b		60.27	4.01	11.29			(0.79)			
c		57.53	3.91	15.33						
d		52.49	3.57	22.75						
2a		62.68	4.32	9.71	63.27	4.37	-8.86	69.42	69	4.79
b		67.47	4.66	2.81			(0.91)			
c		67.32	4.65	3.03						
d		55.62	3.84	19.88						
3a		53.39	6.57	15.49	53.97	6.64	-14.57	63.17	123	7.77
b		50.06	6.16	20.76			(0.85)			
c		53.52	6.58	15.28						
d		58.89	7.24	6.78						
4a		81.57	6.77	11.02	76.31	6.34	+3.83	73.49	83	6.10
b		78.02	6.48	6.16			(1.04)			
c		69.51	5.77	5.42						
d		76.13	6.32	3.59						

TABLE II-18 cont'd
STROKE VOLUMES - ELECTRICAL IMPEDANCE AND INDICATOR DILUTION
(Warbasse)

Study #	Patient's Initials	Single Typical Beat			Average 4 Heart Beats			Heart Rate	Dye Cardiac Output L/Min
		Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye	Impedance Stroke Volume cc	Impedance Cardiac Output L/Min	% of Error vs Dye		
10	J.B.								
5a		49.27	6.0	17.10	49.56	6.04	-16.61	122	7.25
b		49.27	6.0	17.10			(0.03)		
c		48.95	5.97	17.64					
d		50.76	6.19	14.59					

(Kubicek et al. 1966)

Table II-19

SUBJECT	METHOD	SUPINE	SITTING	EXERCISE I 4 min. 6 min.	RECOVERY I	EXERCISE II 4 min. 6 min.	RECOVERY II
1	Dye Z _D	6.1 5.9 10.6 10.7	4.9 4.4 9.0 9.2	9.2 9.4 15.6 16.9	4.2 4.0 8.4 8.2	10.8 11.1 22.3 20.7	6.1 6.1 8.9 9.4
2	Dye Z _D	9.2 6.4 4.7 4.8	5.1 3.8 7.0 6.3	10.0 7.2 9.8 7.1	4.0 3.5 5.4 5.0	11.7 8.9 9.4 9.2	4.7 3.9 6.7 5.6
3	Dye Z _D	7.8 8.0 11.3 11.4	6.7 6.0 9.5 8.9	14.6 11.8 15.8 12.2	6.0 6.9 9.0 9.7	12.9 18.2 16.3 22.5	4.9 6.2 7.3 7.6
4	Dye Z _D	8.2 8.3 10.7 9.5	6.9 6.0 7.3 7.0	10.7 15.5 15.1 15.4	6.8 7.5 8.1 8.7	12.5 16.7 18.7 15.7	8.8 6.5 7.2 7.0
5	Dye Z _D	8.0 7.7 6.6 7.2	5.9 6.7 7.2 7.1	14.0 17.9 12.3 12.4	7.2 7.6 6.8	13.8 12.5	6.5 5.7 6.0 6.0
6	Dye Z _D	8.7 8.5 10.7 10.1	5.2 5.6 7.1 7.3	10.4 11.2 12.7 13.4	5.9 4.3 6.3 6.7	13.1 9.5 16.9 16.2	4.7 4.8 5.4 5.6
7	Dye Z _D	7.6 7.6 7.6 7.0	5.6 5.6 5.1 5.1	9.5 11.7 10.9 9.7	5.2 5.8 4.8 5.2	16.9 13.4 14.4 13.0	5.7 5.1 5.4 4.5
8	Dye Z _D	7.2 7.0 8.6 8.1	4.8 7.0 7.3	10.3 12.6 12.7	5.5 5.8 7.3 6.9	15.7 14.2 17.1 16.2	5.7 5.2 7.4 6.1
9	Dye Z _D	7.1 6.3 7.0 7.2	5.1 5.5 6.5 6.3	9.0 9.2 8.4 9.4	5.9 5.4 7.3 6.7	14.1 15.2 13.8 15.0	5.6 5.6 7.4 7.5
10	Dye Z _D	10.0 8.3 6.7 6.4	7.6 7.6 7.9 7.2	14.6 14.6 10.2 11.0	7.9 6.8 7.0 6.8	16.5 18.1 13.0 10.9	5.7 4.7 7.1 7.8

Cardiac output in L/Min. by the Dye dilution and Impedance (Z_D) methods

Table II-20 Average Ratios of the Impedance Calculated Cardiac Output to Dye Dilution Cardiac Output for each Experimental Condition. Standard Deviations of a Sample are shown for the Various Averages.

Z Cardiac Output									
Dye Cardiac Output									
Subject	Supine	Sitting	Exercise				Recovery		
			I	I	II	II	I	II	Average ±S.D.
1	1.77	1.69	1.75	2.02	2.03	1.50	1.79	±.18	<div> <div>←</div> <div>→</div> <div>s = .24</div> </div>
2	.63	1.51	.99	1.39	.91	1.44	1.14	±.32	
3	1.43	1.38	1.08	1.45	1.25	1.35	1.32	±.13	
4	1.22	1.11	1.20	1.17	1.22	.95	1.15	±.09	
5	.87	1.14	.79	.94		.98	.94	±.12	
6	1.20	1.33	1.21	1.31	1.49	1.16	1.28	±.11	
7	.96	.91	.98	.91	.91	.91	.93	±.03	
8	1.17	1.45	1.00	1.25	1.11	1.23	1.20	±.14	
9	1.06	1.21	.98	1.23	.98	1.33	1.13	±.13	
10	.72	.99	.73	.94	.70	1.45	.92	±.26	
Average	1.10	1.27	1.07	1.26	1.17	1.23	1.18		
<div> <div>←</div> <div>→</div> <div>s = .08</div> </div>									

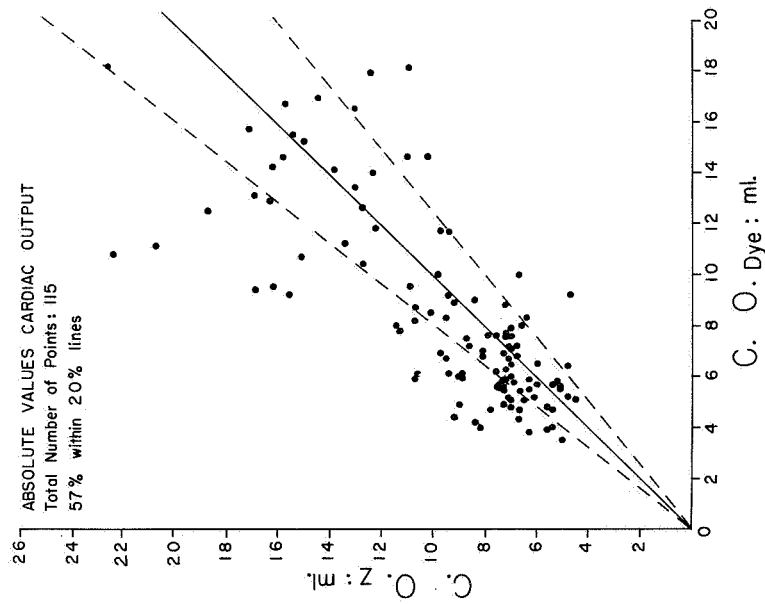


Fig. II-21 Absolute values of cardiac output by the Impedance and Dye dilution methods

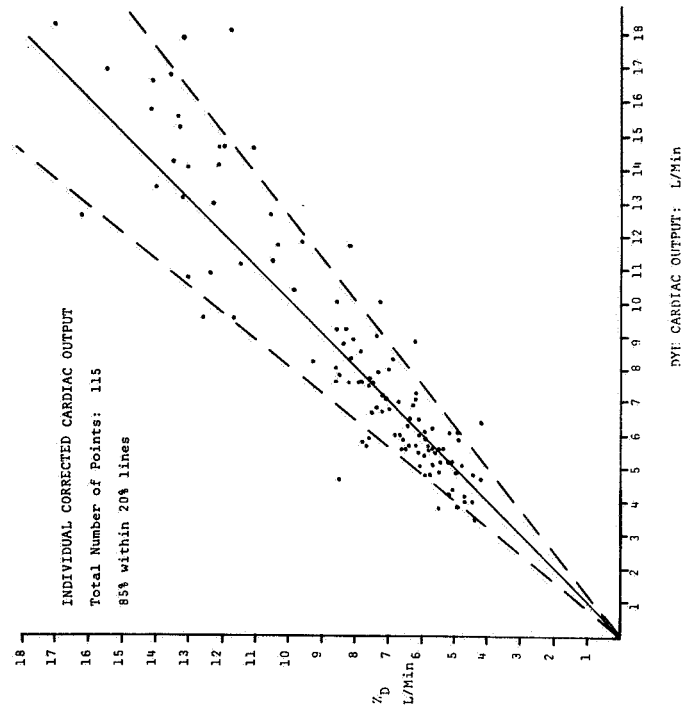


Fig. II-22 Individual corrected Impedance cardiac output values plotted against the original values by the Dye method. Kubicek et al., Aerospace Medicine Vol. 37, No. 12 Dec. 1966.

Part IIIAN INFLIGHT PROTOTYPE AND CLINICAL LABORATORY
IMPEDANCE ELECTRODE - CABLE HARNESS SYSTEM

Previous investigations by this laboratory (Kubicek et al., July 1967 Final Progress Report for Contract NAS 9-4500, Chapter Two) have determined that an adhesive electrode fabricated from metalized Mylar satisfied criteria concerning electrical characteristics and subject comfort and convenience. The purpose of this chapter is to describe an inflight prototype model electrode-cable harness system which implements the Mylar electrodes and is also applicable for the clinical or research laboratory.

The use of a harness with the four-band electrode system is desirable from the standpoint of maintaining the cable and electrode system as near constant as possible during a given experiment. Movement of the body electrodes due to varying cable tension can cause artifacts on the impedance records which are especially troublesome during dynamic experiments. With the harness it is also possible to standardize the electrode placement for a given subject.

The design criteria for the prototype inflight harness model required ease of donning and doffing and use of a lightweight durable material.

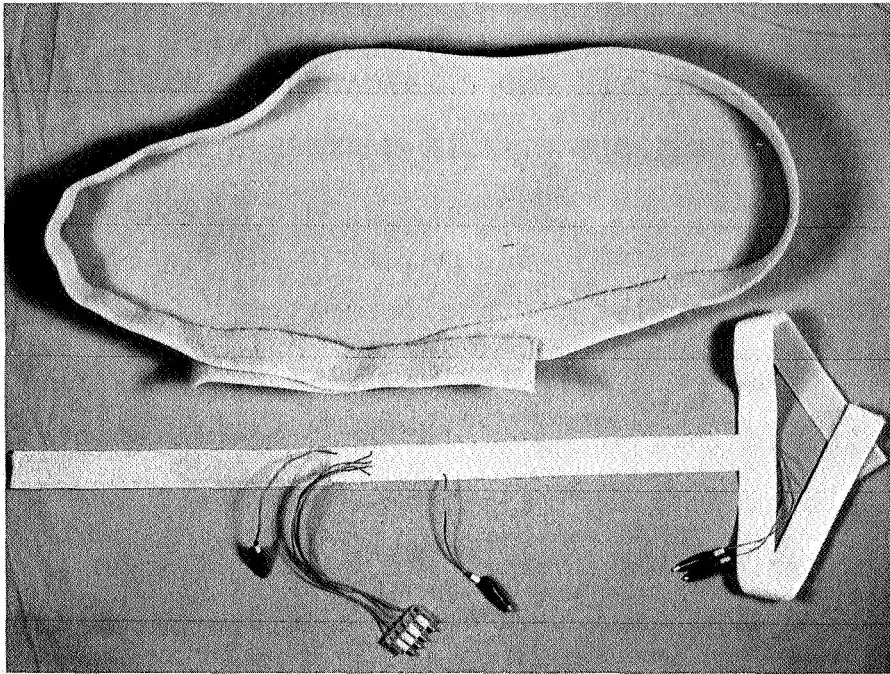


Fig. 1 Wire carrier and belt

I. Design and Fabrication

The cable harness, shown in figure 1, is composed of two parts, a vertical member called the wire carrier, and the horizontal member or the belt.

Wire Carrier - the wire carrier is composed of 1" wide Dacron fabric sewn with vertical and horizontal members. The vertical portion is two thicknesses sewn together, with 4 wires sandwiched in between the Dacron tape. Velcro hook material is placed at the caudal end to secure the end with the belt. The horizontal member of the wire carrier has Velcro pile and hook material to secure itself in a loop loosely about the neck as shown in figure 5.

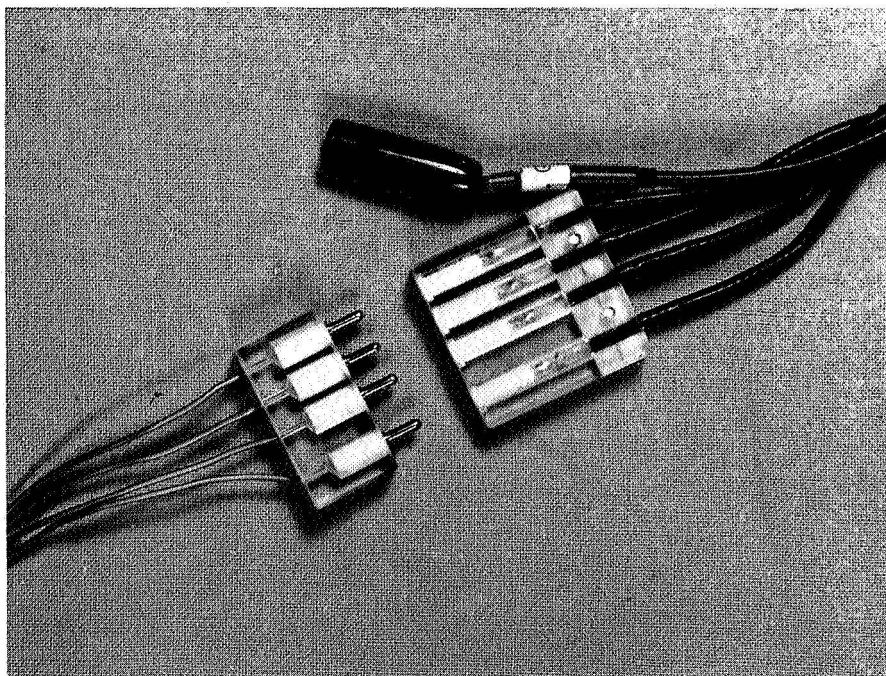


Fig. 2 Cable to harness connector

Conventional miniature alligator clips are used at the electrode end. Due to unavailability and lack of adaptability of commercial connectors, a special connector was developed for use at the cable end. Conventional miniature pin jacks and plugs were imbedded in plexiglass blocks to form a male and female connection as shown in figure 2. Note that this connector is keyed and can only be mated in one position, thus insuring that the four electrodes are correctly attached to the impedance cardiograph (ZCG). A fifth connector, the black pin jack seen in figure 2, is available for use as a separate ground connection on the subject if required by the experimental conditions or protocol.

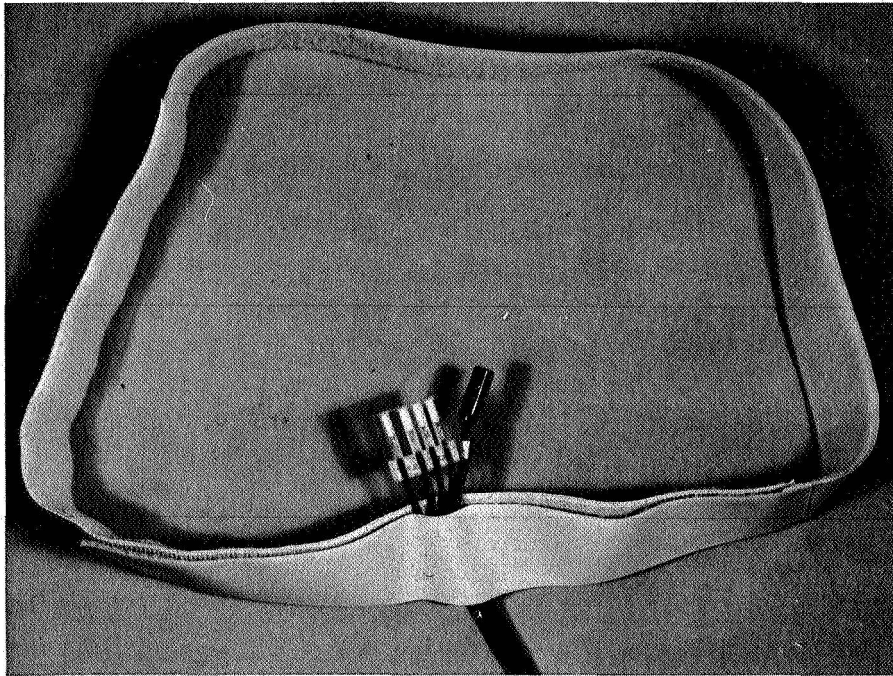


Fig. 3 Strain relief of cable by use of belt

Belt - The belt is made of conventional 2 inch wide Velcro pile with a length of Velcro hook sewn on. It secures around the waist with the hook engaging the belt and sandwiching the cable from the ZCG between the two as shown in figure 3. This results in a strain relief for the connector and cables under movement or exercise conditions.

II. Placement of Tape Electrodes and Harness on Patient

Body Electrodes - Figure 4 shows the tape-on electrodes in place on a subject. The electrodes are numbered 1 through 4 from the neck down. Care must be taken to place electrodes 1 and 2 on the neck at least 3 cm. apart in order to obtain an accurate Z_0 reading. Electrode 3 is at the level of the

xiphisternal junction and band 4 is placed around the torso near the lower abdomen.

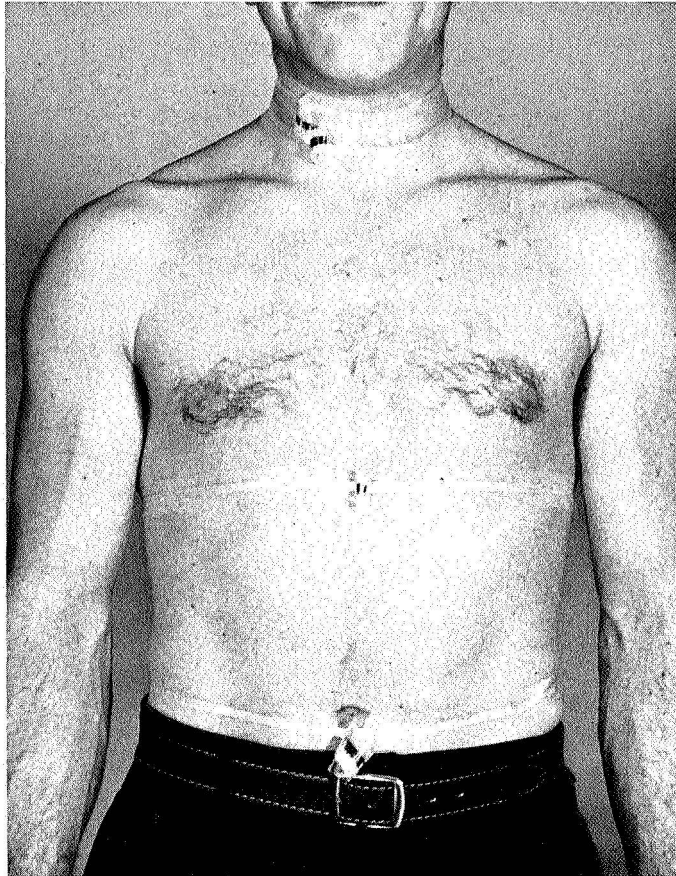


Fig. 4 Disposable electrodes in place

Harness - The electrode harness is shown in place on a subject in figure 5. The horizontal member of the wire carrier is looped loosely about the neck and secured with itself by means of the Velcro pile and hook material.

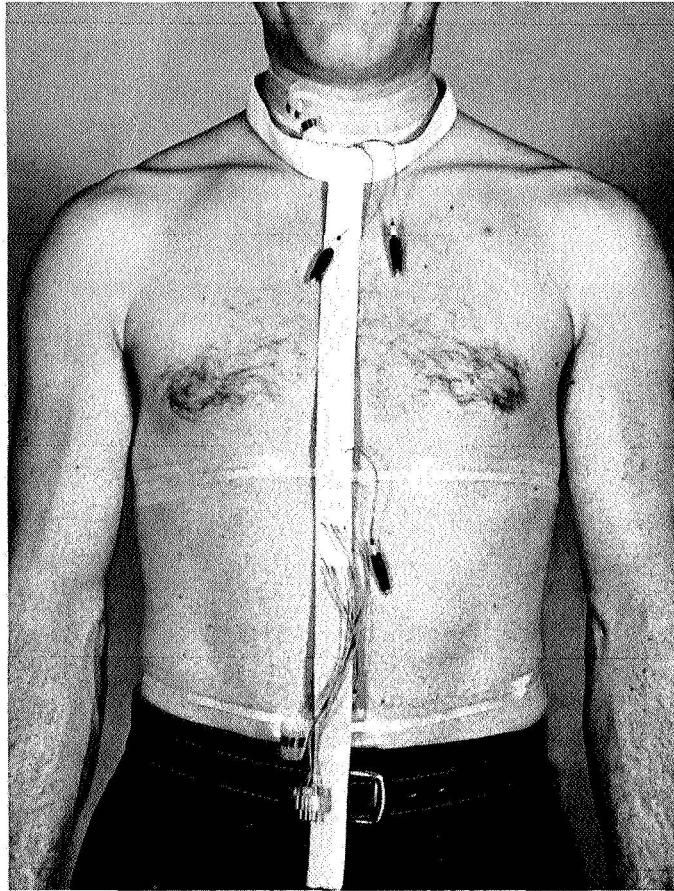


Fig. 5 Wire carrier on subject

The belt is placed around the waist with the pile side turned inward toward the body, as shown in figure 6. This Velcro pile engages the Velcro hook from the wire carrier and secures the caudal end of the wire carrier. An alligator clip is attached to the tape electrode as shown in figure 7. The tape should be bent back upon itself and the alligator clip placed to engage both sets of teeth on the aluminum conductor.

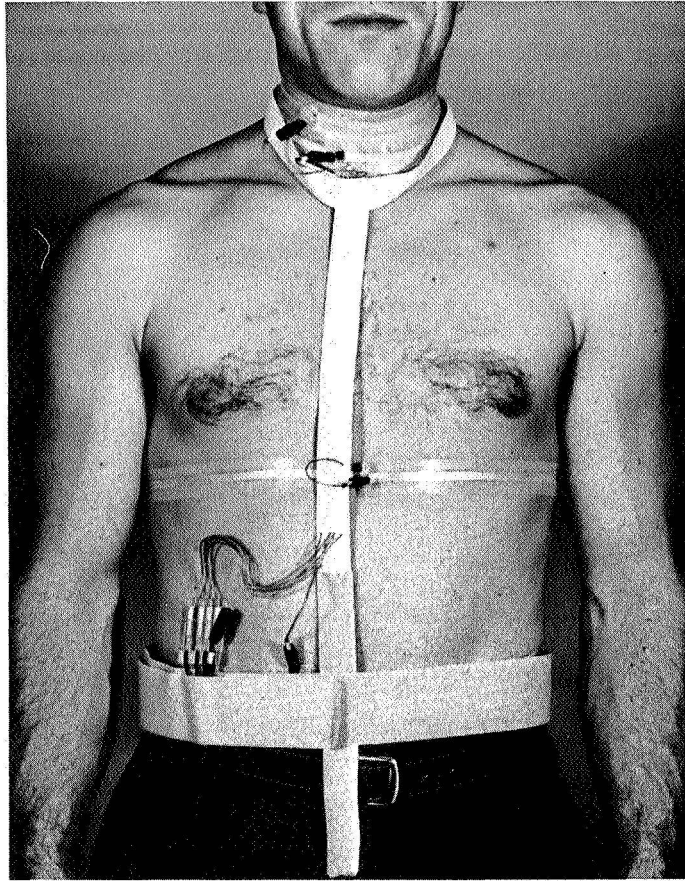


Fig. 6 Complete harness arrangement on subject



Fig. 7 Fastening of clip leads from wire carrier to electrode

III. Evaluation and summary of results obtained from the cable harness:

The harness has been used in our laboratory under various conditions. It has proven very successful in exercise studies to stabilize the electrodes and prevent cable motion from pulling on the electrodes. It is presently being utilized as standard equipment with the ZCG cardiographs by the various research laboratories involved in the evaluation study (chapter one). These laboratories indicate that the harness has worked successfully and an inflight model based on this prototype would appear to be quite functional.

Part IV

DIGITAL COMPUTER PROGRAM FOR COMPUTING STROKE VOLUME AND
CARDIAC OUTPUT FROM THORACIC IMPEDANCE CHANGES
DURING THE CARDIAC CYCLE (ZCG)

A digital computer program was developed that calculates the cardiac stroke volume, cardiac output and heart rate from analog information received from a ZCG instrument. The program is able to calculate the above parameters using only the first derivative of the thorax electrical impedance signal and the mean thoracic impedance. A total of 512 beats can be continuously calculated. The output from the computer is either in printed form showing the beat by beat values, four beat averages and normalized results or in graphic form using a digital plotter. The program was developed for a Spear micro-LINC 300 computer in assembly language.

Figure 1 shows a typical (dZ/dt) waveform recorded from four-band electrodes on the thorax as was previously reported (final report NAS 9-4500, July 1967). Shown in figure 1 are the points on the waveform used in the calculation of stroke volume and cardiac output. The stroke volume and cardiac output were calculated using the formulas shown below

$$\Delta V = \rho \frac{L^2 \tau}{Z_o^2} (dZ/dt)_{\min} \quad \text{eq. 1}$$

$$\text{and C.O.} = \Delta V / T \quad \text{eq. 2}$$

where ΔV = stroke volume (cc)

ρ = resistivity of blood at 100 kHz and
37.5°C (150 ohm-cm)

L = mean distance between pick up electrodes (cm)

Z_0 = impedance between pick up electrodes (ohms)

$(dZ/dt)_{\min}$ = minimum value of the first time derivative of Z (ohms per sec)

$\tau = (T_3 - T_1)$ = ventricular ejection time as determined from the dZ/dt waveform

T = the time interval between heart beats in minutes

C.O. = cardiac output (cc per min)

Figure 1 shows the minimum value of dZ/dt , T_1 , T_3 , and T . The difference between T_1 and T_3 is the ventricular ejection time. T_1 is found by going back in time down the dZ/dt waveform as shown in fig. 1 from $(dZ/dt)_{\min}$ to $.15(dZ/dt)_{\min}$. This is done to eliminate from the ejection time determination the slow decrease in impedance that occurs with some individuals at the start of systole. T_3 , the end of systole, is indicated by the peak positive dZ/dt after $(dZ/dt)_{\min}$. In some subjects T_3 is not clearly defined; therefore the program will not calculate the correct ejection time. Also in some patients with heart valve defects, the waveform will be modified so that the program will not work correctly. The program was developed using only impedance information and does not require the ECG for timing. A simpler program could be developed using the ECG for timing but it could put a restriction on the use of the program in some applications.

Simplified Program Description

A simplified description of the sampling and calculation portion of the program is described below. The program starts

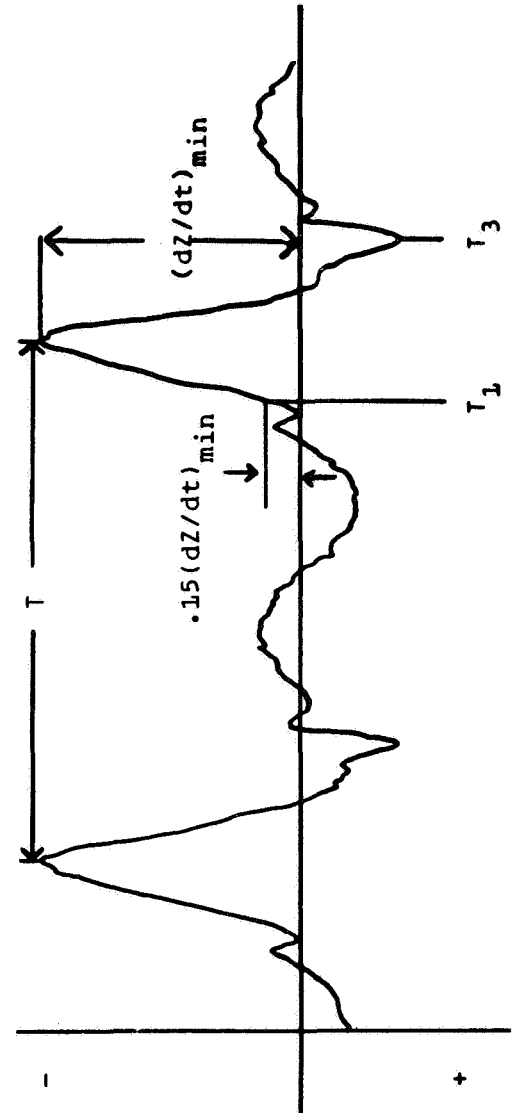
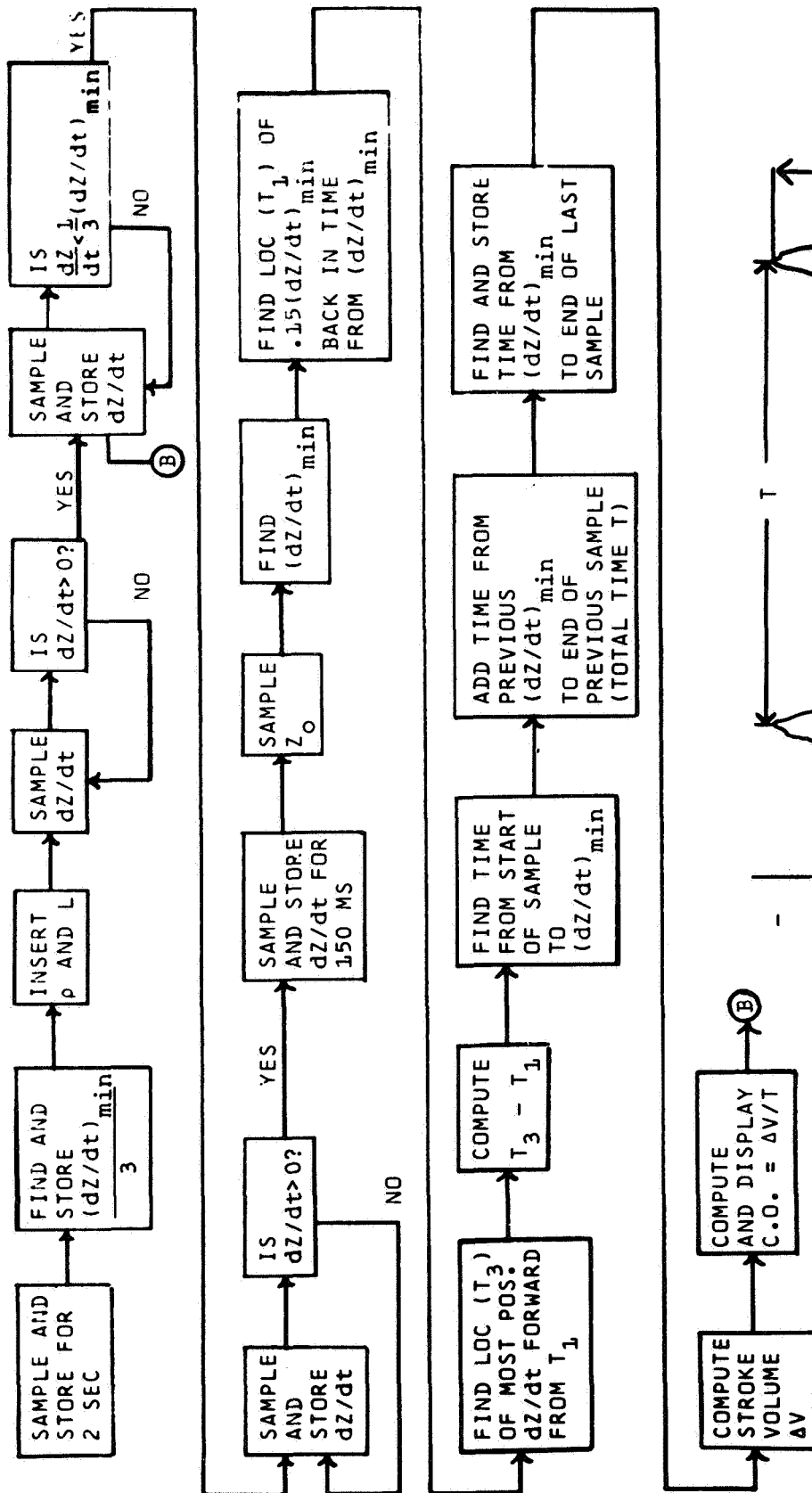


FIG.1 SIMPLIFIED
BLOCK DIAGRAM AND
SAMPLE dz/dt
WAVEFORM

by sampling dZ/dt for two seconds as shown in fig. 1. It then finds $(dZ/dt)_{\min}$ and divides it by three (in fig. 1 negative dZ/dt is above the zero line). The computer then starts sampling dZ/dt and looking for a positive dZ/dt value. When it finds a positive value it starts sampling and storing. The computer is now looking for the start of the next complete systole. Referring to the waveform shown in fig. 1, it can be seen that dZ/dt is positive only in the last part of systole or during diastole. If it is assumed that the computer found the positive value occurring during the latter part of systole, then from fig. 1 it can be seen that the next negative value of dZ/dt will occur during diastole. The normal subjects tested to date have shown negative dZ/dt values during diastole to be greater than $1/3(dZ/dt)_{\min}$. Therefore, since the computer is looking for the start of a systole, it jumps over any dZ/dt until it is less than $1/3(dZ/dt)_{\min}$ of the previous beat. After it finds a dZ/dt less than $1/3(dZ/dt)_{\min}$ it assumes it is in a systolic ejection period and it begins to look for a zero crossing which will occur after $(dZ/dt)_{\min}$. When the computer finds a zero crossing, it samples for 150 ms more which is enough time to cover a complete systolic ejection period. After a 150 ms, it samples the Z line to obtain Z_0 . The computer then finds $(dZ/dt)_{\min}$ and the location in memory of $.15(dZ/dt)_{\min}$ by going back in time down the dZ/dt waveform from $(dZ/dt)_{\min}$ as shown in fig. 1. Because the sampling rate is constant and the samples are stored in consecutive location in the memory, their position in the memory will be an indication of their occurrence in real

time. After T_1 is found, it goes forward in time and finds the location in the memory of the most positive dZ/dt value in the current samples which corresponds to T_3 . The computer then calculates $T_3 - T_1$ to obtain the systole ejection time τ . At this point the computer has all the information necessary to compute stroke volume.

The computer then proceeds to obtain T in order to compute heart rate per minute. It computes the time from the start of the sampling and storing period to $(dZ/dt)_{\min}$ and adds to it the time from the previous $(dZ/dt)_{\min}$ to the end of the previous sample period. The latter time interval will be in error on the first beat because of the delay necessary for the computer to find the start of systole. The computer then stores the time from the $(dZ/dt)_{\min}$ of the present beat to the end of the current sample for use in calculating T for the next beat. The stroke volume and cardiac output is then calculated and the value of cardiac output is displayed on a cathode ray tube as a point on a graph. The computer then jumps to point B in the flow chart to start the next beat.

Operational Description of Program

The program computes, plots and prints stroke volume, pulse rate, and cardiac output. It consists of one master program and five sub-programs. The master program is called COCAL; the sub-programs are called INT-DSP, COMPUTE1, FIN-DSP1, PLOT1 and PRINT1. When the program COCAL is loaded in the computer the first display appears on the cathode ray display tube and the sub-programs are

called in from digital tape as needed.

After the program is loaded and started a series of displays are shown asking questions about the values of the constants and calibrate factors as shown in fig. 2. The first displays gives the value of ρ as 150 ohm-cm. If this value is not desired, the delete key on the keyboard can be struck and the desired value of ρ entered. After the correct value is entered the end of line (EOL) key is struck which stores the value and a new display appears. The next two displays ask for the value of L front and L back. From these two values the computer computes the mean value and stores it as L. The next two displays ask for the values of the calibration factors relating Z_0 and dZ/dt and analog input voltage representations of these parameters. The next display asks the operator to type S if the desired analog signals are entering the computer. After S is typed and the EOL key struck, the computer starts sampling the input signals and computes cardiac output. The computer can be temporarily halted and the sampling stopped at any time by raising sense switch 0. This feature allows the operator to stop the sampling if any artifacts appear or to compute only selected segments of the data from a long run. Also with the use of three other sense switches the digitized input waveforms or the calculated cardiac output results can be viewed on the cathode ray tube as the sampling and calculating is going on. All of the sampling and calculations are done in real time on a beat by beat basis. When the desired number of beats have been sampled and computed, the EOL key is struck to end this portion of the problem and to call in the output routines.

RHO IN OHM-CM. IS
150

L FRONT IN CM =

L BACK IN CM =

Z CAL
1 OHM = --- V.

DZ/DT CAL
1 OHM/SEC = --- V.

TYPE S IF READY TO
SAMPLE

Fig. 2 Constants and Calibration factors as shown in input displays

1-RESTART PROGRAM
2-PLOT
3-PRINT
4-SCOPE

1-HUMAN DATA
2-DOG DATA

1-X AXIS=10 IN.
2-X AXIS=20 IN.

1-C.D.
2-P.R.
3-S.V.
4-C.D. + P.R.
5-C.D. + S.V.
6-P.R. + S.V.
7-ALL THREE

Fig. 3 Plotting option displays

The display that appears after the EOL key is struck is shown in the top display of figure 3 and is called the main selection option display. This is the display that is used to choose if plotting, printing or a cathode ray tube display of the data is desired. The choice is made by striking keyboard keys 2, 3 or 4. After the completion of the execution of any of the output operations this display reappears. The first choice on the display will restart the sampling and cardiac output calculation portion of the program. If key 2 followed by the EOL key are struck, indicating that plotting is desired, the next display will allow a choice between dog data or human data. The purpose of these choices is to adjust the scales to optimize the size of the graphs for the different values of stroke volume and cardiac output that occur in dogs and humans. The next choice is the length of the X axis desired. The last choice made, as indicated in figure 3, is to determine which variables or combination of variables should be plotted. After the execution of the last set of options the plotting operation will start. Two other switch settings on the computer control plotting functions. One is sense switch 1 which determines whether every point is plotted or only four beat average. The second is a register of switches called RSW which controls whether symbols will be plotted on the graph and if so how often. After the completion of the graph the display shown in the top of figure 3 returns.

The next option (number 3) is for printing the results on the digital printer. The values for the cardiac output, stroke volume and pulse rate are automatically printed after selecting this option. The four beat averages, and the four beat averages

normalized to the first average are printed for all the parameters. Striking the EOL key will terminate the printing of any parameter and the completion of printing of the entire computed results will return the program to the main option selection display as shown in the top of figure 3.

The last option (number 4) is the oscilloscope display of the computed results. The selections involved in this option are shown in figure 4. By striking key 1, 2 or 3, either the pulse rate, stroke volume or cardiac output can be displayed on the oscilloscope in graphic form similar to that plotted by the digital plotter. Striking the EOL key returns to the main selection option. From the main selection option the entire cycle can be repeated and the program restarted to sample data and compute cardiac output.

FLOW CHART AND ASSEMBLY LANGUAGE PROGRAM

The digital computer used in developing the computer program was a micro-LINC-300 manufactured by Spear Inc. Its logical structure is basically similar to the original LINC machine designed by Clark and Molnar (1,2). The principal differences between the micro-LINC 300 and the original LINC are in the input and output structure and the speed of operation. The machine used for this program has a real time clock that operates at speeds of 250 Hz, 500 Hz, 1000 Hz, and 4000 Hz. The clock operates through a priority interrupt system and is used in the program to determine the analog sampling rate.

The machine also has a small oscilloscope display that is

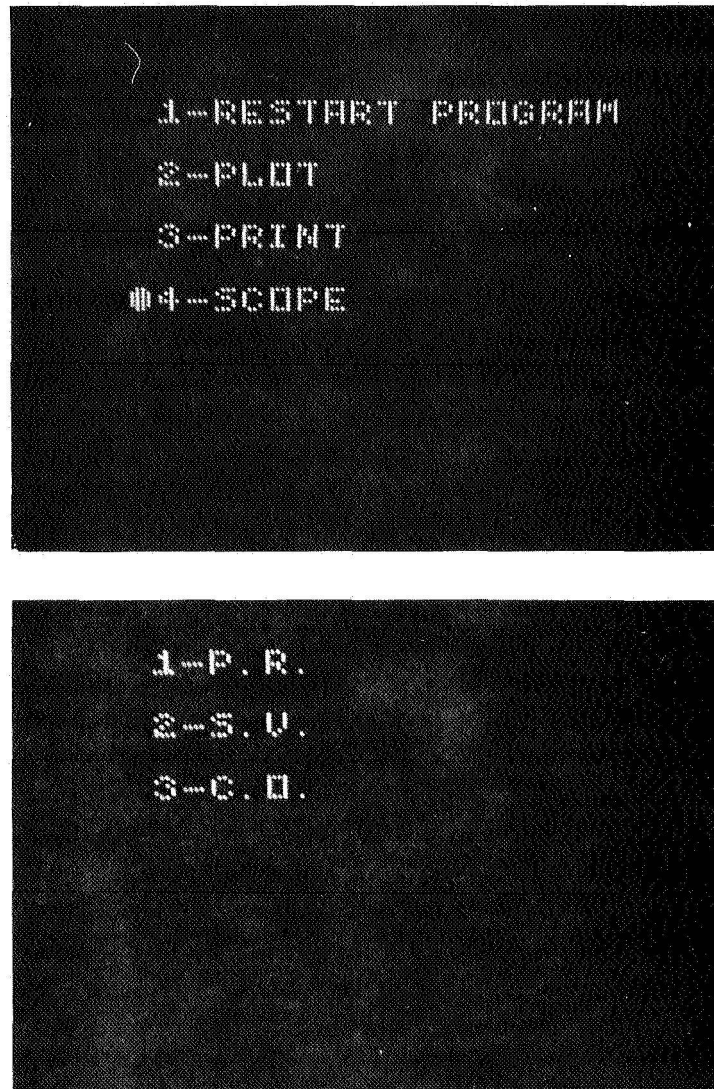


Fig. 4 Oscilloscope display option

controlled directly by the computer, four small digital tape transports with addressable 256 word blocks, a digital plotter, a digital printer and 12 analog to digital conversion channels controlled by the computer. The computer has a 4K memory with 12 bit words and operates with a memory cycle time of 1 microsec.

The computer program is written in an assembly language called LAP6. The assembly program is rather powerful and performs control functions as well as converting programs.

The following is a brief description of the programs used in the total cardiac output computing program.

COCAL - this program is the main control program. The program controls the analog to digital conversion and chooses the proper points from the curve for calculation. The program also locates the position of the other programs on tape and calls in most of the other programs as needed.

INT-DSP - this program generates the initial displays used in reading in the constants and calibration factors.

FIN-DSP1 - this program generates the final display routines that are used to choose the options for printing, plotting or oscilloscope display.

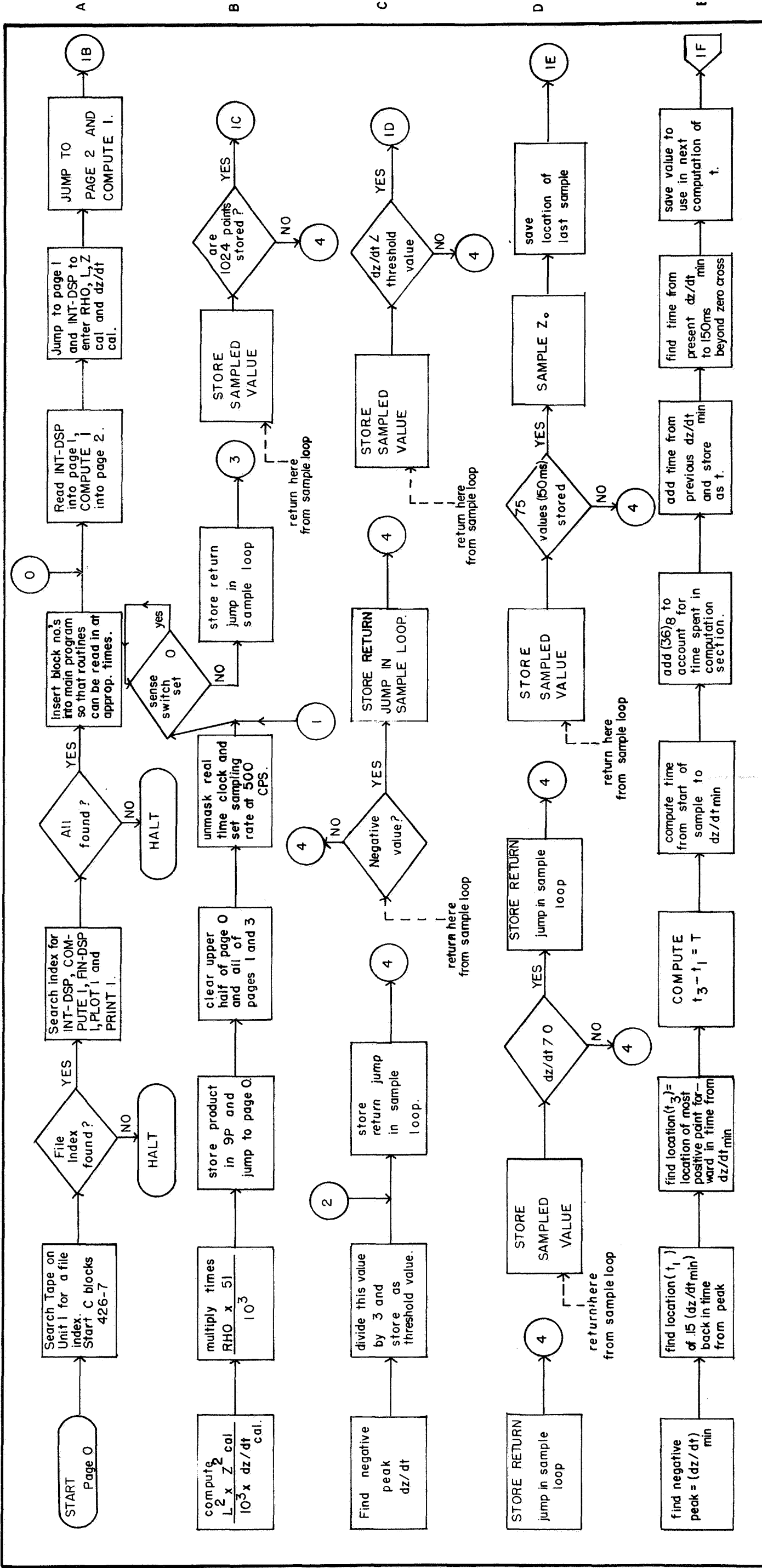
COMPUTE1 - this program performs the calculating operations in double precision floating point arithmetic.

PLOT1 - this program controls the plotting operations.

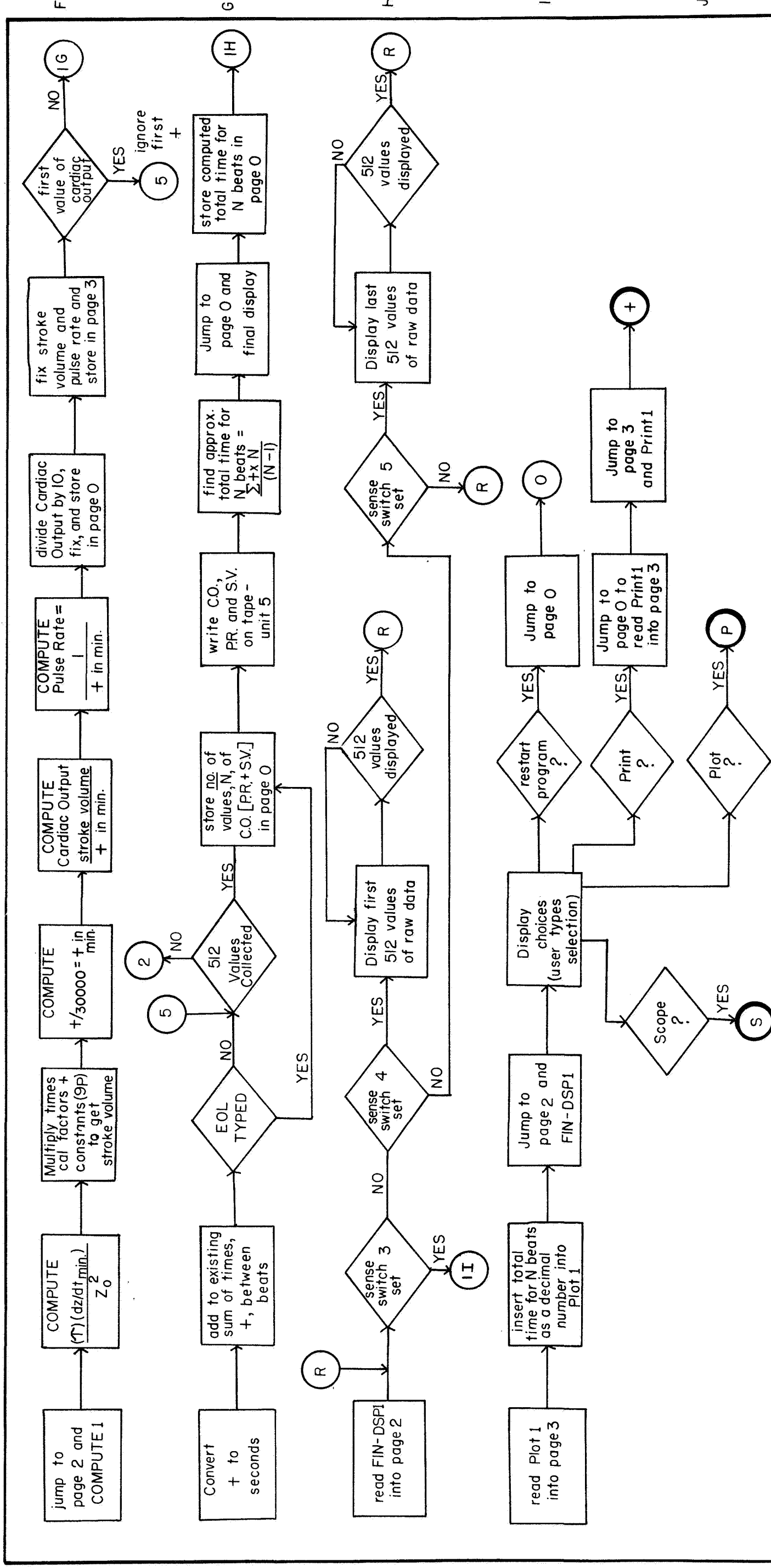
PRINT1 - this program controls the printing operations.

The next six fold-out pages contain detailed flow charts of

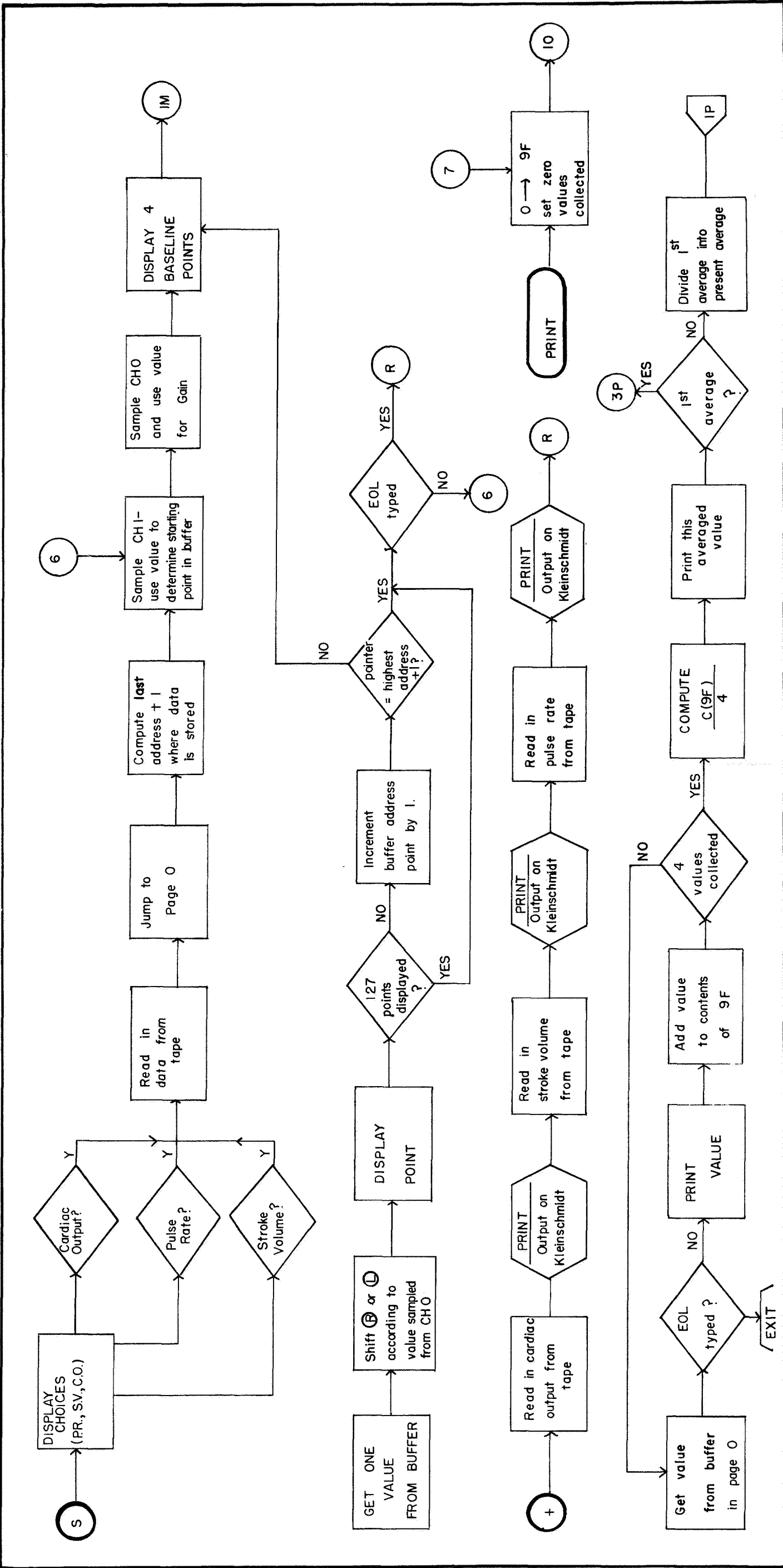
the program. Following the flow charts is a complete manuscript listing of the computer program. Following the manuscript listing is an appendix that contains details on the program operations, a section on the computation of stroke volume, and cardiac output, and samples of the printer and computer outputs.



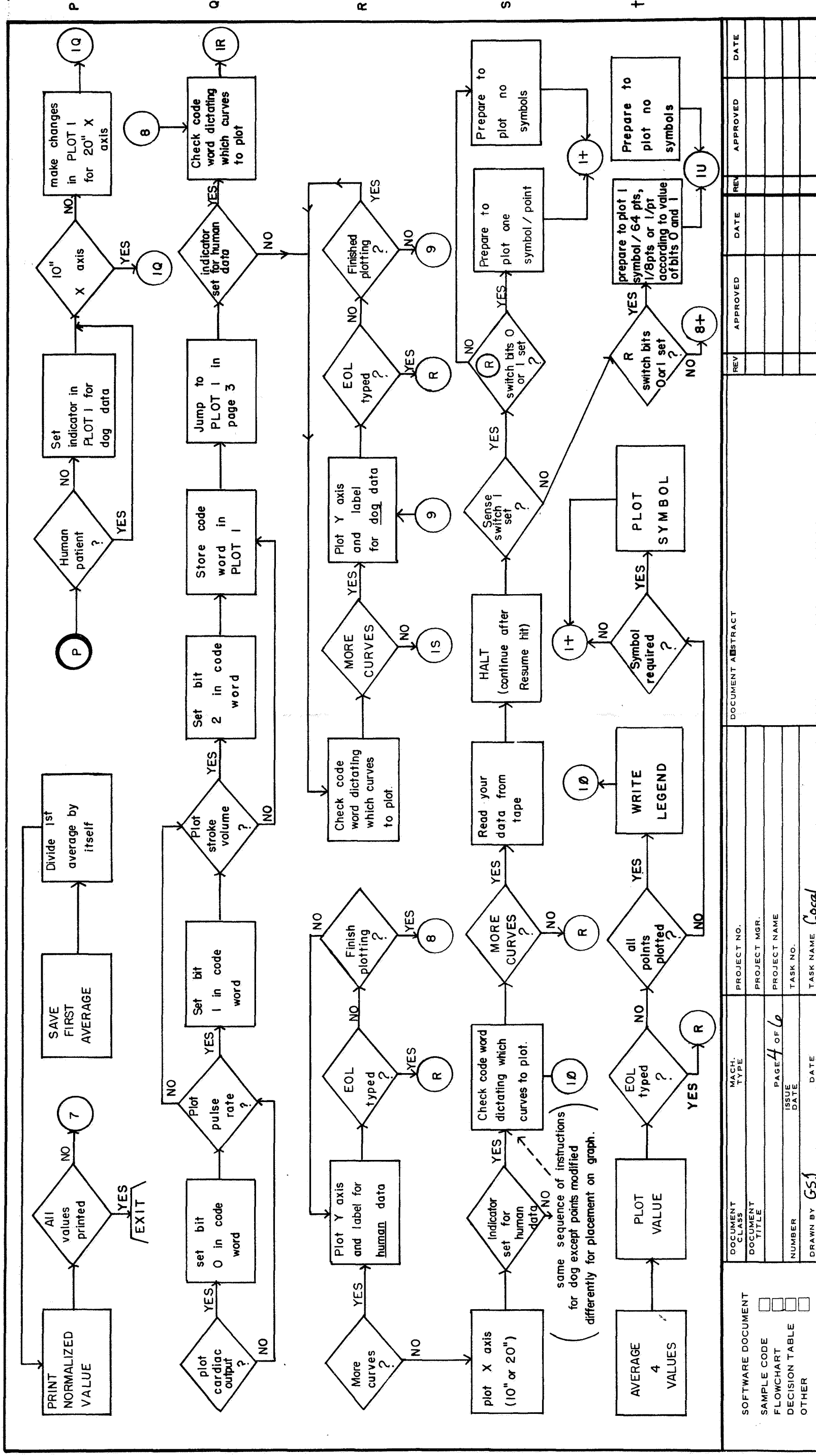
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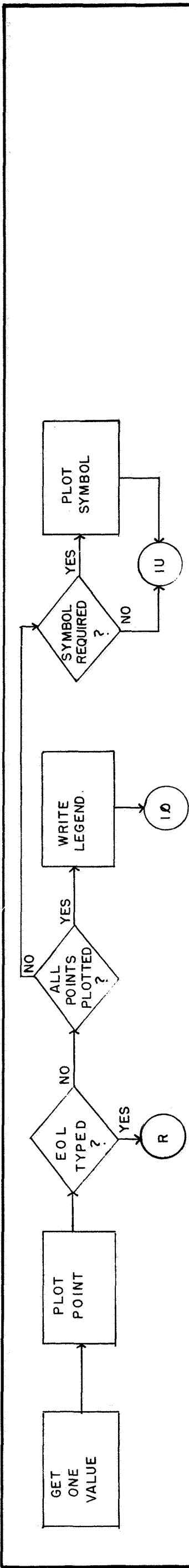


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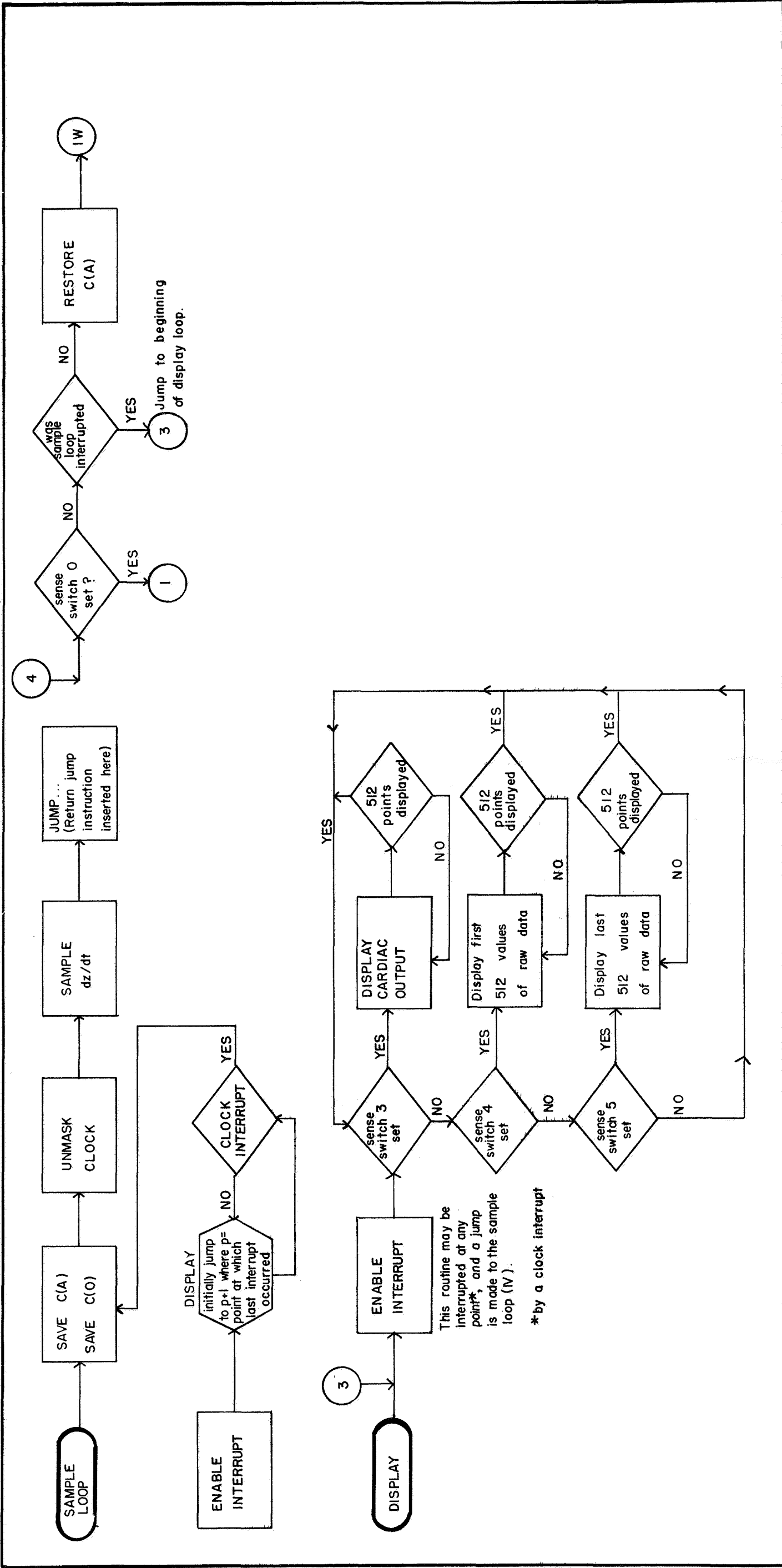


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2G 0325	457	9D 0546	700
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2L 0365	521	9G 0605	737
2M 0372	527		
2S 0044	172		
3C 0773	1124		
3D 0774	1125		
3E 0764	1115		
3F 0765	1116		
3G 0766	1117		
3H 0767	1120		
3S 0047	175		
4S 0046	174		
5B 0454	610		
5C 0463	617		
5D 0664	1015		
5E 0716	1047		
5F 0720	1051		
5G 0735	1066		
5S 0437	573		
6S 0626	756		
6T 0741	1072		
7A 1000	1136		
7B 1143	1301		
7C 1205	1343		
7D 1226	1364		
7E 1213	1351		
7F 1156	1314		
7G 1003	1141		
7H 1175	1333		
7I 1235	1373		
7J 1152	1310		
7K 1202	1340		
7M 1261	1417		
7N 1265	1423		
7O 1271	1427		
7P 1275	1433		
7Q 1301	1437		
7R 0426	562		
7S 0433	567		
8A 0500	631		
8B 0501	632		

CONT

```

[PROGRAM TO COMPUTE CARDIAC OUTPUT
[TRUDI JUNCKER - 1968
[UTILITY ROUTINES = SCOPE=SP
[                               DBLFLT
[                               CALCOMP PLOT
[TO OPERATE =
[USE LAP6-2S TO LOAD COCAL. THIS PROGRAM STARTS
[AUTOMATICALLY AND QUESTIONS AND COMMANDS WILL APPEAR
[ON THE SCOPE.
[   TYPE IN CHARACTERS TO FILL IN THE BLANKS AND
[   TERMINATE WITH AN EOL. THE NEXT DISPLAY WILL
[   THEN APPEAR. IF A MISTAKE IS MADE, THE DEL KEY
[   CAN BE USED TO ERASE THE ENTRIES IN THE CURRENT
[   DISPLAY. USE OF THE CASE KEY WILL RETURN YOU
[   TO THE FIRST DISPLAY.
[AFTER S*EOL IS TYPED, THE COMPUTER WILL START
[ SAMPLING THE ANALOG INPUT AND COMPUTE CARDIAC OUTPUT.
[ USE OF SENSE SWITCHES 3-5 ALLOWS THE USER TO VIEW THE
[ RAW DATA [SWITCHES 4-5] AND THE CARDIAC OUTPUT VALUES
[ [SWITCH 3] AS THE SAMPLING IS TAKING PLACE. USE OF
[ SENSE SWITCH 0 ALLOWS THE USER CONTROL OVER THE DATA
[ SAMPLED. IN THE UP POSITION SENSE SWITCH 0 DIRECTS THE
[ COMPUTER TO IGNORE THE INPUT DATA - WHICH MIGHT BE
[ NOISY, ETC. SAMPLING RESUMES WHEN SENSE SWITCH 0
[ IS IN THE DOWN POSITION. THE EOL KEY CAN BE USED TO
[ DICTATE THE NUMBER OF VALUES OF C.O., P.R. AND S.V.]
[ COLLECTED. IF DEPRESSED, THE SAMPLING STOPS AND THE
[ ACCUMULATED VALUES OF C.O., P.R. AND S.V. ARE WRITTEN
[ ON TAPE. A JUMP IS MADE TO THE FINAL DISPLAY ROUTINE.
[ IF NOT DEPRESSED, 512 VALUES OF EACH ARE COLLECTED
[ AND SAVED ON TAPE AND A JUMP MADE TO THE FINAL
[ DISPLAY.
[
[                               FINAL DISPLAY
[THE SENSE SWITCHES ARE USED TO DICTATE THE FINAL
[ DISPLAY.
[   SS4-5 = RAW DATA AS BEFORE.
[
[   SS3 = SCOPE DISPLAY OF OUTPUT OPTIONS. THE USER
[   MUST CHOOSE HIS COURSE OF ACTION [RESTART
[   PROGRAM, PLOT, PRINT, SCOPE] BY TYPING THE NUMBER
[   OF HIS CHOICE FOLLOWED BY EOL. TYPING EOL WILL
[   RESULT EITHER IN THE APPEARANCE OF THE NEXT
[   DISPLAY OR, AS IN THE CASE OF PRINT, THE
[   OUTPUT OF DATA. DEL ERASES THE ENTRIES IN THE
[   CURRENT DISPLAY. DEPRESSING THE CASE KEY
[   RETURNS YOU TO AN EARLIER DISPLAY. TO EXAMINE
[   THE RAW DATA WHILE IN THE SCOPE DISPLAY
[   ROUTINE, RAISE SS4 OR 5, DEPRESS SS3 AND WHILE
[   VIEWING THE FIRST DISPLAY LIST, HIT THE
[   CASE KEY.
[
[                               PRINT ROUTINE
[CARDIAC OUTPUT IS PRINTED FIRST, THEN STROKE VOLUME
[ AND LASTLY PULSE RATE. THE EOL KEY MAY BE USED TO
[ INTERRUPT THE TYPING OF ONE SET OF VALUES TO GO ON TO
[ THE NEXT. DEPRESSING THE EOL KEY WHEN PULSE RATE IS

```

COCAL,2 LN=72

CONT

[BEING PRINTED WILL RESULT IN A RETURN TO THE
[DISPLAYED LIST OF OUTPUT OPTIONS. THE USER MAY MAKE
[ANOTHER SELECTION.

[
[
[DISPLAY CURVE ROUTINE
[USE POTENTIOMETER KNOB 0 TO VARY GAIN
[AND KNOB 1 TO VIEW DIFFERENT PORTIONS OF THE CURVE.
[USE EOL TO RETURN TO THE DISPLAYED LIST OF OUTPUT
[OPTIONS.

[
[
[PLOT ROUTINES
[THE COMPUTER WILL HALT AFTER DATA IS READ FROM TAPE
[AND BEFORE A GIVEN CURVE IS PLOTTED. THE USER MAY
[CHANGE PENS AND SET SWITCHES AT THIS TIME.

[SENSE SWITCH 1
[UP=AVERAGE EVERY 4 POINTS AND PLOT AVERAGE.
[DOWN=DO NOT AVERAGE THE VALUES AND PLOT EVERY
[POINT.

[RIGHT SWITCH BITS 0 AND 1 DICTATE THE PLOTTING OF
[SYMBOLS.

[X = C.O.
[S = P.R.
[0 = S.V.
[AVERAGED VALUES PLOTTED
[VALUE OF BITS 0 AND 1 NO. OF SYMBOLS
[0 NONE
[1-3 ONE/POINT

[EVERY POINT PLOTTED
[VALUE OF BITS 0 AND 1 NO. OF SYMBOLS
[0 0
[1 1/64 POINTS
[2 1/8 POINTS
[3 ONE/POINT

[WHEN THE NECESSARY SWITCHES ARE SET, LIFT RESUME TO
[PLOT THE CURVE.

[AT THE END OF THE PLOTTING, A RETURN IS MADE TO
[THE DISPLAYED LIST OF OUTPUT OPTIONS. SHOULD THE
[USER WANT TO RETURN TO THE DISPLAYED LIST BEFORE
[THE PLOTTING IS FINISHED, HE MAY TYPE EOL.
[TO RESTART COCAL, CHOOSE THE FIRST SELECTION IN THE
[DISPLAYED LIST [1=RESTART PROGRAM].

```

      $1
1 6020 JMP20
      $20
20 7000 JMP7A
21 6022 JMP22 [JUMP HERE ON CLOCK INTERRUPT
22 0056 SET16
23 0000 0
24 4044 STC2S [SAVE [A]
25 1020 LDA&
26 0004 4
27 0541 OPR41 [UNMASK CLOCK
30 0016 NOP
31 0110 SAM10 [SAMPLE DZ/DT
32 0000 #1S 0 [FILLED IN WITH JUMP INSTRUCTION
33 0460 SNS&0 [IF SENSE SWITCH 0 IS SET,
34 6146 JMP1C [RESTART SAMPLING PROCEDURE

```

```

CONT
35 1000 LDA COTHERWISE GO TO DISPLAY LOOP
36 0016 16
37 1460 SAE&
40 6046 4S+6000
41 6043 JMP'+2
42 6426 JMP7R CIF INTERRUPT ROUTINE INTERRUPTED, JUMP TO B
      BEGINNING OF DISPLAY LOOP
43 1020 LDA&
44 0000 #2S 0 COTHERWISE RESTORE [A]
45 0010 ENI CENABLE INTERRUPT
46 6016 #4S JMP16 C&ND JUMP TO '+1 IN DISPLAY LOOP WHERE '+ PO
      INT AT WHICH LAST INTERRUPT OCCURRED
47 0007 #3S MSC7
50 0730 RDC&X CREAD INITIAL DISPLAY ROUTINE
51 4450 4/450
52 0730 RDC&X
53 5451 5/451
54 0642 UMB2
55 0730 RDC&X CREAD FLOATING POINT ROUTINES
56 4247 4/247
57 0730 RDC&X
60 5250 5/250
61 0730 RDC&X
62 6251 6/251
63 0710 RDC&X
64 7252 7/252
65 0640 UMB0
66 0601 LMB1
67 6020 JMP20 C&NTER RHO*L& AND CAL FACTORS
      CRETURN HERE AFTER ENTERING THE ABOVE CONSTANTS
70 0061 SET&1 CCLEAR UPPER HALF OF PAGE 0 AND
71 1000 1000 C&LL OF PAGE 1
72 0011 CLR
73 1041 STA1
74 0221 XSK&1
75 6073 JMP'+2
76 0061 SET&1
77 2000 2000
100 1041 STA1
101 0221 XSK&1
102 6100 JMP'+2
103 0643 UMB3 CCLEAR PAGE 3
104 0061 SET&1
105 2000 2000
106 1041 STA1
107 0221 XSK&1
110 6106 JMP'+2
111 1020 LDA&
112 7777 7777
113 0540 OPR40 CMASK ALL DEVICES
114 1020 LDA&
115 0004 4
116 0540 OPR40 CUNMASK REAL TIME CLOCK
117 1020 LDA&
120 0002 2
121 0544 OPR44 CSAMPLING RATE = 500 CPS
122 0016 NOP

```

```

      *   CONT
123 0642      UMB2
124 1020      LDA& [LOAD INDEX REGISTERS 6,7, AND 10
125 2777      2777 [TO PREPARE FOR STORING CARDIAC
126 1040      STA [OUTPUT, PULSE RATE AND STROKE
127 2006      2006 [VOLUME
130 1040      STA
131 2007      2007
132 1020      LDA&
133 3777      3777
134 1040      STA
135 2010      2010
136 0011      CLR
137 1040      STA
140 2500      2500
141 1040      STA
142 2501      2501
143 1040      STA
144 2502      2502
145 0641      UMB1
146 0460 #1C SNS&0
147 6146      JMP'+1
150 0063      SET&3 [SAMPLE 1024 POINTS
151 3777      3777
152 1020      LDA&
153 6156      1D+6000
154 4032      STC1S [STORE JUMP IN INTERRUPT HANDLER
155 6426      JMP7R [JUMP TO ENABLE INTERRUPT
156 1063 #1D STA&3
157 0203      XSK3
160 6033      JMP1S+1
161 0063      SET&3 [FIND MAX DZ/DT
162 3777      3777
163 0011      CLR
164 4500      STC8A
165 0223 #1A XSK&3
166 6170      JMP'+2
167 6200      JMP1B
170 1003      LDA3
171 0017      COM
172 2500      ADD8A
173 0471      APO&
174 6165      JMP1A
175 1003      LDA3
176 4500      STC8A
177 6165      JMP1A
200 1000 #1B LDA [FIND 1/3 DZ/DT MAX
201 0500      8A
202 1240      MUL
203 4501      8E+4000
204 4502      STC8C
205 1020 #1E LDA& [WAIT FOR NEGATIVE VALUE
206 6211      1F+6000 [STORE JUMP IN INTERRUPT HANDLER
207 4032      STC1S
210 6033      JMP1S+1
211 0471 #1F APO&
212 6033      JMP1S+1
213 0064 #1G SET&4 [START STORING

```



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CONT
214 3777      3777
215 1020      LDA&
216 6221      1H*6000
217 4032      STC1S [STORE JUMP IN INTERRUPT HANDLER
220 6033      JMP1S+1
221 1064 #1H   STA&4
222 0017      COM
223 2502      ADD&C
224 0471      APO&
225 6033      JMP1S+1
226 1000      LDA
227 0004      4
230 4503      STC8D
231 0065      SET&5
232 7767      =10
233 1020      LDA&
234 6237      1I*6000
235 4032      STC1S [STORE JUMP IN INTERRUPT HANDLER
236 6033      JMP1S+1
237 1064 #1I   STA&4
240 0225      XSK&5
241 6033      JMP1S+1
242 1020      LDA&
243 6246      1J*6000
244 4032      STC1S [STORE JUMP IN INTERRUPT HANDLER
245 6033      JMP1S+1
246 1064 #1J   STA&4
247 0471      APO&
250 6033      JMP1S+1
251 0065      SET&5 [SAMPLE 150 MS AFTER ZERO CROSS
252 7664      =113
253 1020      LDA&
254 6257      1K*6000
255 4032      STC1S
256 6033      JMP1S+1
257 1064 #1K   STA&4
260 0225      XSK&5
261 6033      JMP1S+1
262 0111 #2A   SAM11
263 4504      STC8E
264 2004      ADD4
265 1040      STA
266 0510      8L
267 0017      COM
270 1120      ADA&
271 2000      2000
272 4010      STC10
      [FIND MAX
273 0067 #2B   SET&7
274 3777      3777
275 0011      CLR
276 4500      STC8A
277 0230 #2C   XSK&10
300 6302      JMP'+2
301 6314      JMP2D
302 1027      LDA&7
303 0017      COM

```

```

CONT
304 2500 ADD8A
305 0471 APO&
306 6277 JMP2C
307 1007 LDA7
310 4500 STC8A
311 2007 ADD7
312 4505 STC8F
313 6277 JMP2C
      [DIVIDE BY 3
314 2500 #2D ADD8A
315 1240 MUL
316 4501 8B+4000
317 4502 STC8C
      [FIND T1
320 2502 ADD8C
321 0341 SCR1
322 4506 STC8J
323 0052 SET12
324 0505 8F
325 1020 #2G LDA&
326 7776 =1
327 2012 ADD12
330 4012 STC12
331 1012 LDA12
332 0017 COM
333 2506 ADD8J
334 0451 APO
335 6325 JMP2G
336 1000 LDA
337 0012 12
340 4507 STC8K
      [FIND T3
341 0052 #2H SET12
342 0505 8F
343 2510 ADD8L
344 0017 COM
345 2012 ADD12
346 4014 STC14
347 4511 STC8M
350 0234 #2K XSK&14
351 6353 JMP'+2
352 6365 JMP2L
353 1032 LDA&12
354 0017 COM
355 2511 ADD8M
356 0451 APO
357 6350 JMP2K
360 1012 LDA12
361 4511 STC8M
362 2012 ADD12
363 4512 STC8N
364 6350 JMP2K
      [COMPUTE T3 = T1
365 1000 #2L LDA
366 0507 8K
367 0017 COM
370 2512 ADD8N

```

```

CONT
371 4513      STC8P
      [COMPUTE T
372 2505      #2M ADD8F
373 1120      ADA&
374 6035      =1742 [=2000 + 36 TO ACCOUNT FOR TIME SPENT IN COM
      PUTATION SECTION
375 2514      ADD8R
376 4515      STC8S
377 2505      ADD8F
400 0017      COM
401 2510      ADD8L
402 4514      STC8R
403 0640      UMB0 [JUMP TO ROUTINE TO COMPUTE
404 0602      LMB2 [CARDIAC OUTPUT, STROKE VOLUME
405 6102      JMP102 [AND PULSE RATE
      $410
410 0007      MSC7
411 1020      LDA&
412 6626      6S+6000
413 4437      STC5S
414 0730      RDC&% [READ IN FINAL DISPLAY ROUTINE
415 4221      4/221
416 0730      RDC&%
417 5222      5/222
420 0730      RDC&%
421 6223      6/223
422 0710      RDC%
423 7224      7/224
424 0641      UMB1
425 6433      JMP7S
426 0010      #7R ENI
427 1020      LDA&
430 0016      0016 [NOP
431 1040      STA
432 0437      5S
433 0077      #7S SET&17
434 6777      =1000
435 0443      SNS3
436 6443      JMP'+5
437 0016      #5S NOP
440 0062      SET&2
441 0777      777
442 6463      JMP5C
443 0444      SNS4
444 6450      JMP'+4
445 0062      SET&2
446 3777      3777
447 6454      JMP5B
450 0445      SNS5
451 6433      JMP7S
452 0062      SET&2
453 2777      2777
454 0011      #5B CLR
455 0162      DIS&2
456 1002      LDA2
457 0142      DIS2
460 0237      XSK&17

```

```

CONT
461 6454      JMP5B
462 6433      JMP7S
463 1002      #5C LDA2
464 0343      SCR3
465 1120      ADA&
466 7400      =377
467 0162      DIS&2
470 0237      XSK&17
471 6463      JMP5C
472 6433      JMP7S
              $500
[STORAGE
500 0000      #8A 0 [CURRENT MAX
501 1252      #8B 1252 [1/3
502 0000      #8C 0 [THRESHOLD
503 0000      #8D 0 [T1 LOCATION
504 0000      #8E 0 [ZT
505 0000      #8F 0 [LOCATION OF CURRENT PEAK
506 0000      #8J 0 [0.15 PEAK
507 0000      #8K 0 [T1 LOC
510 0000      #8L 0 [LOC LAST SAMPLE
511 0000      #8M 0 [TEMP MIN
512 0000      #8N 0 [T3 LOC
513 0000      #8P 0 [T3-T1
514 0000      #8R 0 [1ST PART OF T
515 0000      #8S 0 [T
516 0000      #8T 0 [TOTAL NO. OF VALUES FOR CO,PR, AND SV
              [USED IN PLOT,PRINT, AND SCOPE ROUTINES
              $520
520 1000      LDA
521 0516      8T
522 1120      ADA&
523 1000      1000
524 4573      STC9C [SET LAST ADDRESS+1 WHERE DATA IS STORED
525 0062      #9F SET&2
526 0777      777
527 0063      SET&3
530 7600      7600
531 0101      SAM1 [STARTING POINT IN BUFFER
532 1120      ADA&
533 1400      1400
534 4555      STC9B
535 0100      SAM0
536 0451      APO
537 6605      JMP9G
540 1120      ADA&
541 0001      1
542 0346      SCR6
543 1120      ADA&
544 0240      240
545 4556      STC9A
546 1020      #9D LDA&
547 7400      =377
550 0162      DIS&2 [DISPLAY BASELINE
551 0162      DIS&2
552 0162      DIS&2
553 0162      DIS&2

```

```

      CONT
554 1000 LDA CGET VALUE
555 0000 #9B 0
556 0000 #9A 0
557 1120 ADA&
560 7400 =377
561 0142 DIS2 CDISPLAY POINT
562 0223 XSK&3
563 6565 JMP9E
564 6576 JMP9C+3
565 1020 #9E LDA&
566 0001 1
567 1140 ADM
570 0555 9E
571 0017 COM
572 1120 ADA&
573 0000 #9C 0
574 0471 APO&
575 6546 JMP9D
576 0415 KST
577 6525 JMP9F
600 0515 KRD CEOL MEANS RETURN TO MAIN DISPLAY
601 1460 SAE&
602 0012 0012
603 6525 JMP9F
604 6433 JMP7S
605 1120 #9G ADA&
606 7776 =1
607 0017 COM
610 0346 SCR6
611 1120 ADA&
612 0340 340
613 4556 STC9A
614 6546 JMP9D
620 0642 UMB2
621 1000 LDA
622 2502 2502 CAVERAGE TIME BETWEEN BEATS X NO. OF BEATS
623 1040 STA
624 0774 3D
625 6410 JMP410
626 0643 #6S UMB3
627 0730 RDC&%
630 4612 4/612 CREAD IN PLOT ROUTINE
631 0730 RDC&%
632 5613 5/613
633 0730 RDC&%
634 6614 6/614
635 0710 RDC&%
636 7615 7/615
637 1000 LDA
640 0516 8T
641 0017 COM
642 1040 STA
643 3700 3700
644 0017 COM
645 0342 SCR2
646 0017 COM

```

```

CONT
647 1040 STA
650 3701 3701
[ROUTINE TO CONVERT [AVERAGE T X 512] TO A DECIMAL NUM
BER REPRESENTED BY KEYBOARD CODES
651 0070 SET&10
652 0763 3E*1
653 0071 SET&11
654 0766 3H*1
655 1000 LDA
656 0774 3D
657 4773 STC3C
660 0011 CLR
661 4764 STC3E
662 4765 STC3F
663 4766 STC3G
664 0230 #5D XSK&10
665 0231 XSK&11
666 1011 LDA11
667 0450 AZE
670 6716 JMP5E
671 1000 LDA
672 0764 3E
673 0450 AZE
674 6677 JMP'+3
675 1020 LDA&
676 0014 14
677 1140 ADM
700 2373 2373
701 1000 LDA
702 0765 3F
703 0246 ROL6
704 1140 ADM
705 2374 2374
706 1000 LDA
707 0766 3G
710 0246 ROL6
711 1140 ADM
712 2375 2375
713 0640 UMB0
714 0602 LMB2
715 6020 JMP20 [DISPLAY CHOICES=PLOT OR SCOPE
716 1000 #5E LDA
717 0773 3C
720 1111 #5F ADA11
721 0470 AZE&
722 6735 JMP5G
723 0451 APO
724 6664 JMP5D
725 1040 STA
726 0773 3C
727 1020 LDA&
730 0001 1
731 1150 ADM10
732 1000 LDA
733 0773 3C
734 6720 JMP5F
735 1020 #5G LDA&

```

```

CONT
736 0001      1
737 1150      ADM10
740 6671      JMP5D+5
741 0730 #6T  RDC&%  [READ IN PRINT ROUTINE
742 4571      4/571
743 0730      RDC&%
744 5572      5/572
745 0730      RDC&%
746 6573      6/573
747 0710      RDC%
750 7574      7/574
751 1000      LDA
752 0516      8T
753 1120      ADA&
754 7776      7776
755 0342      SCR2
756 0017      COM
757 1040      STA
760 2377      2377
761 0640      UMB0
762 0603      LMB3
763 6020      JMP20 [JUMP TO PRINT VALUES
764 0000 #3E 0
765 0000 #3F 0
766 0000 #3G 0
767 7633 #3H 7633 [=144
770 7765      7765 [=12
771 7776      7776 [=1
772 0000      0
773 0000 #3C 0
774 0000 #3D 0
[CODING TO READ IN AND SEARCH THE FILE INDEX FOR
[INT=DSP,COMPUTE1,FIN=DSP1,PLOT1,AND PRINT1.
[WHEN A ROUTINE IS FOUND, ITS BLOCK NUMBER IS INSERTED
[INTO THE MAIN PROGRAM. IF A ROUTINE IS NOT FOUND,
[THE COMPUTER HALTS. IF THE FILE INDEX IS NOT
[LOCATED IN BLOCKS 426-7, THE TAPE IS SEARCH FOR IT.
[IF NOT FOUND, THE COMPUTER HALTS.
      $1000
1000 0711 #7A RCG%
1001 1426      1/426
1002 7152      JMP7J
1003 0062 #7G SET&2
1004 1260      7M=1 [INT=DSP
1005 7205      JMP7C
1006 1120      ADA&
1007 4000      4000
1010 1040      STA
1011 0051      51
1012 1120      ADA&
1013 1001      1001
1014 1040      STA
1015 0053      53
1016 0001      SET&1
1017 3007      3007
1020 0062      SET&2
1021 1264      7N=1 [COMPUTE1

```

```

CONT
1022 7205    JMP7C
1023 1120    ADA&
1024 4000    4000
1025 1040    STA
1026 0056    56
1027 1120    ADA&
1030 1001    1001
1031 1040    STA
1032 0060    60
1033 1120    ADA&
1034 1001    1001
1035 1040    STA
1036 0062    62
1037 1120    ADA&
1040 1001    1001
1041 1040    STA
1042 0064    64
1043 0061    SET&1
1044 3007    3007
1045 0062    SET&2
1046 1270    70=1 [FIN=DSP1
1047 7205    JMP7C
1050 1120    ADA&
1051 4000    4000
1052 1040    STA
1053 0415    415
1054 1120    ADA&
1055 1001    1001
1056 1040    STA
1057 0417    417
1060 1120    ADA&
1061 1001    1001
1062 1040    STA
1063 0421    421
1064 1120    ADA&
1065 1001    1001
1066 1040    STA
1067 0423    423
1070 0061    SET&1
1071 3007    3007
1072 0062    SET&2
1073 1274    7P=1 [PLOT1
1074 7205    JMP7C
1075 1120    ADA&
1076 4000    4000
1077 1040    STA
1100 0630    630
1101 1120    ADA&
1102 1001    1001
1103 1040    STA
1104 0632    632
1105 1120    ADA&
1106 1001    1001
1107 1040    STA
1110 0634    634
1111 1120    ADA&
1112 1001    1001

```



```

CONT
1113 1040 STA
1114 0636 636
1115 0061 SET&1
1116 3007 3007
1117 0062 SET&2
1120 1300 7Q=1 [PRINT1
1121 7205 JMP7C
1122 1120 ADA&
1123 4000 4000
1124 1040 STA
1125 0742 742
1126 1120 ADA&
1127 1001 1001
1130 1040 STA
1131 0744 744
1132 1120 ADA&
1133 1001 1001
1134 1040 STA
1135 0746 746
1136 1120 ADA&
1137 1001 1001
1140 1040 STA
1141 0750 750
1142 6047 JMP3S
1143 1020 #7B LDA&
1144 0010 10
1145 1140 ADM
1146 1001 7A+1
1147 5151 STC'+2
1150 0711 RCG%
1151 0000 0
1152 0065 #7J SET&5
1153 7767 7767
1154 0061 SET&1
1155 2777 2777
1156 1021 #7F LDA&1
1157 1460 SAE&
1160 5757 5757
1161 7163 JMP'+2
1162 7202 JMP7K
1163 1000 LDA
1164 1001 7A+1
1165 1460 SAE&
1166 1776 1776
1167 7171 JMP'+2
1170 7175 JMP7H
1171 1460 SAE&
1172 1416 1416
1173 7143 JMP7B
1174 0000 HLT
1175 1020 #7H LDA&
1176 1006 1006
1177 1040 STA
1200 1001 7A+1
1201 7147 JMP7B+4
1202 0225 #7K XSK&5
1203 7156 JMP7F

```

```

CONT
1204 7003 JMP7G
1205 0044 #7C SET4
1206 0000 0
1207 1000 LDA
1210 0002 2
1211 5231 STC7D+3
1212 7235 JMP7I
1213 1020 #7E LDA&
1214 0007 7
1215 7226 JMP7D
1216 1020 LDA&
1217 0006 6
1220 7226 JMP7D
1221 1020 LDA&
1222 0005 5
1223 7226 JMP7D
1224 1020 LDA&
1225 0004 4
1226 1140 #7D ADM
1227 0001 1
1230 0062 SET&2
1231 0000 0
1232 0201 XSK1
1233 7235 JMP'+2
1234 0000 HLT
1235 1021 #7I LDA&1
1236 1462 SAE&2
1237 7213 JMP7E
1240 1021 LDA&1
1241 1462 SAE&2
1242 7216 JMP7E+3
1243 1021 LDA&1
1244 1462 SAE&2
1245 7221 JMP7E+6
1246 1021 LDA&1
1247 1462 SAE&2
1250 7224 JMP7D=2
1251 1020 LDA&
1252 0003 3
1253 1140 ADM
1254 0001 1
1255 1001 LDA1
1256 1560 BCL&
1257 7000 7000
1260 6004 JMP4
1261 3441 #7M 3441
1262 4717 4717
1263 2746 2746
1264 4377 4377
1265 2642 #7N 2642
1266 4043 4043
1267 5047 5047
1270 3001 3001
1271 3134 #7O 3134
1272 4117 4117
1273 2746 2746
1274 4301 4301

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	CONT		
1275	4337	#7P	4337
1276	4247		4247
1277	0177		0177
1300	7777		7777
1301	4345	#7Q	4345
1302	3441		3441
1303	4701		4701
1304	7777		7777

INT=DSP,0

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	VALUE	LINE
1N	0164	147
1O	0202	165
1P	0217	202
1Q	0272	255
1R	0234	217
1S	0251	234
2N	0177	162
5A	0031	12
6A	0062	43
7A	0111	73
7B	0121	103
7C	0122	104
7D	0135	117
7E	0143	125
7F	0153	135
7G	0154	136
7H	0155	137
7I	0156	140
7J	0157	141
7K	0160	142
7L	0161	143
8A	0074	55
9A	0400	317
9B	0431	351
9D	0447	367
9E	0457	400
9F	0466	407
9G	0470	411
9H	0473	414
9J	0520	441
9K	0523	444
9M	0530	451
9N	0542	463
9Q	0555	476
9R	0562	503
9S	0573	514
9T	0610	531
9U	0764	710
9V	0617	541
9W	0626	550
9X	0627	552
9Y	0653	576

INT=DSP,1 LN=1

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```
CONT
20 0070 SET&10
21 0153 7F
22 0011 CLR
23 4153 STC7F
24 4154 STC7G
25 4155 STC7H
26 4156 STC7I
27 4157 STC7J
30 4160 STC7K
31 1020 #5A LDA&
32 0001 0001
33 1340 STH
34 4764 9U+4000
35 1020 LDA&
36 0500 0500
37 4765 STC9U+1
40 1040 STA
41 1000 1000
42 1020 LDA&
43 4164 1N+4000 [RHO IN OHM-CM IS 150
44 6400 JMP9A
45 6020 JMP20
46 6111 JMP7A [CONVERT DECIMAL TO BINARY
47 1020 LDA&
50 0202 10 [L FRONT IN CM = ==.
51 6400 JMP9A [JUMP TO SCOPE PKG
52 6020 JMP20
53 6111 JMP7A [DEC TO BINARY-TREAT AS INTEGER
54 1020 LDA&
55 0217 1P [L BACK IN CM = ==.
56 6400 JMP9A [JUMP TO SCOPE PKG
57 6020 JMP20
60 6111 JMP7A [DEC TO BIN-TREAT AS INTEGER
61 6143 JMP7E [FIND L MEAN
62 1020 #6A LDA&
63 0234 1R [Z CAL-1 OHM = -.== V.
64 6400 JMP9A [JUMP TO SCOPE PKG
65 6020 JMP20
66 6111 JMP7A [DEC TO BIN-TREAT AS INTEGER
67 1020 LDA&
70 0251 1S [DZ/DT CAL-1 OHM/SEC = -.== V.
71 6400 JMP9A [JUMP TO SCOPE PKG
72 6020 JMP20
73 6111 JMP7A [DEC TO BIN-TREAT AS INTEGER
74 1020 #8A LDA&
75 0272 1Q [TYPE S IF READY TO SAMPLE
76 6400 JMP9A
77 6020 JMP20
100 1000 LDA
101 0764 9U
102 1420 SHD&
103 4600 4600
104 6106 JMP'+2
105 6074 JMP8A
106 0641 UMB1
107 0602 LMB2
110 6020 JMP20 [JUMP TO FLOATING POINT ROUTINES
```

CONT

[CONVERT NUMBER FROM DECIMAL TO BINARY

```

111 0054 #7A SET14
112 0000 0
113 0067 SET&7
114 0764 9U [LOCATION OF CHARACTERS ENTERED THRU KEYBOARD
115 0071 SET&11
116 7774 7774
117 0073 SET&13
120 0161 7L
121 1327 #7B LDH&7
122 1307 #7C LDH7
123 0246 ROL6
124 0346 SCR6
125 0470 AZE&
126 6135 JMP7D
127 1120 ADA&
130 7776 7776
131 1347 STH7
132 1013 LDA13
133 1150 ADM10
134 6122 JMP7C
135 0231 #7D XSK&11
136 6141 JMP +3
137 1030 LDA&10
140 6014 JMP14
141 1033 LDA&13
142 6121 JMP7B
143 1000 #7E LDA
144 0154 7G
145 1100 ADA
146 0155 7H
147 0341 SCR1
150 1040 STA
151 0160 7K
152 6062 JMP6A
153 0000 #7F 0 [RHO
154 0000 #7G 0 [L FRONT
155 0000 #7H 0 [L BACK
156 0000 #7I 0 [Z CAL IN VOLTS X 100
157 0000 #7J 0 [DZ/DT CAL IN VOLTS X 100
160 0000 #7K 0 [L MEAN
161 0144 #7L 144
162 0012 12
163 0001 1
[DISPLAY TEXT
164 0003 #1N 0003
165 4533 4533 [RHO IN OHM=CM. IS ==
166 4214 4214
167 3441 3441
170 1442 1442
171 3340 3340
172 1726 1726
173 4015 4015
174 1434 1434
175 4614 4614
176 5656 5656
177 1313 #2N 1313

```

CONT		
200	1314	1314
201	5776	5776
202	0003	#10 0003
203	3714	3714 [L FRONT IN CM = --. "
204	3145	3145
205	4241	4241
206	4714	4714
207	3441	3441
210	1426	1426
211	4014	4014
212	2314	2314
213	5656	5656
214	1313	1313
215	1513	1513
216	5777	5777
217	0003	#1P 0003
220	3714	3714 [L BACK IN CM = --. "
221	2524	2524
222	2636	2636
223	1434	1434
224	4114	4114
225	2640	2640
226	1423	1423
227	1456	1456
230	5613	5613
231	1315	1315
232	1314	1314
233	5777	5777
234	0003	#1R 0003 [Z CAL
235	5514	5514 [I OHM = --. V.
236	2624	2624
237	3756	3756
240	5601	5601
241	1442	1442
242	3340	3340
243	1423	1423
244	1413	1413
245	1513	1513
246	1314	1314
247	5115	5115
250	5777	5777
251	0003	#1S 0003 [DZ/DT CAL
252	2755	2755 [I OHM/SEC = --. V.
253	2127	2127
254	4714	4714
255	2624	2624
256	3756	3756
257	5601	5601
260	1442	1442
261	3340	3340
262	2146	2146
263	3026	3026
264	1423	1423
265	1413	1413
266	1513	1513
267	1314	1314
270	5115	5115

271	5777	5777
272	0001	#1Q 0001 [TYPE S IF READY TO SAMPLE
273	4754	4754
274	4330	4330
275	1446	1446
276	1434	1434
277	3114	3114
300	4530	4530
301	2427	2427
302	5414	5414
303	4742	4742
304	5656	5656
305	4624	4624
306	4043	4043
307	3730	3730
310	5656	5656
311	1314	1314
312	5777	5777

```

[SCOPE=SP ,SP=SAME PAGE
[GENERAL PURPOSE ROUTINES FOR ENTERING DATA
[AND SELECTING OPTIONS
[ G.FELLOWS*FEB 67
[CODE 0=ENTER TEXT
[CODE 1=STAR OPTION AND RETURN TO '+2
[CODE 2=STAR OPTION AND RETURN TO '+1+N
[ WERE N IS POSITION OF OPTION IN LIST
[CASE ALWAYS RETURNS TO '+1
[60 AT TEXT END,DISPLAY ONCE AND RETURN '+1
[76 AT END OF TEXT MEANS RETURN TO '+2 ON EOL
[77 AT END OF TEXT MEANS RETURN TO '+2 ON EOL
[ IF CORRECT NO. OF ENTRIES MADE
[LOAD TAG OF TEXT IN ACCUM, THEN JUMP 9A
[9A CAN BE PUT AT START OF ANY QUARTER IN LOWER PAGE
[USES REGS 1,2,3,4,5,6

```

400	0046	#9A SET 6
401	0000	0
402	0062	SET&2
403	1775	1775
404	0471	AP0&
405	0222	XSK&2
406	1560	BCL&
407	4000	4000
410	4001	STC1
411	2006	ADD6
412	1040	STA
413	0523	9K
414	2653	ADD9Y [1
415	4626	STC9W
416	1301	LDH 1
417	0017	COM
420	4555	STC9Q
421	1321	LDH&1
422	0017	COM
423	2655	ADD9Y+2
424	4447	STC9D
425	2001	ADD1


```

      CONT
426 4460      STC9E+1
427 0222      XSK&2
430 6446      JMP9D=1
      [CLEAR WORKING AREA 9U
431 0061 #9E SET&1
432 7747      =30
433 0062      SET&2
434 4763      9U=4000
435 1020      LDA&
436 0017      17
437 0043      SET 3
440 0555      90
441 0203      XSK 3
442 2654      ADD9Y+1
443 1362      STH&2
444 0221      XSK&1
445 6443      JMP'=2
446 0066      SET&6
447 0000 #9D 0
450 0011      CLR
451 4763      STC9U=1
452 1020      LDA&
453 0001      1
454 4613      STC9T+3
455 0065      SET&5
456 0764      9U
      [START OF DISPLAY
457 0062 #9E SET&2
460 0000      0
461 0064      SET&4
462 0764      9U
463 1020      LDA&
464 0336      336
465 4470      STC9G
466 2656 #9F ADD9Y+3
467 1160      ADM&
470 0000 #9G 0
471 0061      SET&1
472 0070      70
473 1322 #9H LDH&2
474 1420      SHD&
475 1300      1300
476 1324      LDH&4
477 1420      SHD&
500 5600      5600
501 6466      JMP9F
502 1420      SHD&
503 5700      5700
504 6520      JMP9J
505 0241      ROL 1
506 1120      ADA&
507 0627      9X
510 4003      STC3
511 2522      ADD9J+2
512 2001      ADD1
513 4001      STC1
514 2470      ADDSG

```

```

CONT
515 1743 DSC 3
516 1763 DSC&3
517 6473 JMP9H
520 1322 #9J LDH&2
521 1420 SHD&
522 6004 6004
523 6000 #9K JMP
524 0415 KST
525 6457 JMP9E
526 0226 XSK&6
527 6542 JMP9N
530 0415 #9M KST
531 6530 JMP'=1
532 0063 SET&3
533 7577 *200
534 0225 XSK&5
535 6534 JMP'=1
536 0223 XSK&3
537 6534 JMP'=3
540 0515 KBD
541 6431 JMP9B
542 0515 #9N KBD
543 1420 SHD&
544 1300 1300
545 6431 JMP9B
546 1420 SHD&
547 2300 2300
550 6523 JMP9K
551 1420 SHD&
552 1200 1200
553 6617 JMP9V
554 0064 SET&4
555 0000 #9Q 0
556 0204 XSK 4
557 6562 JMP9R
560 1365 STH&5
561 6457 JMP9E
562 4573 #9R STC9S
563 0043 SET 3
564 0523 9K
565 0223 XSK&3
566 1322 LDH&2
567 1420 SHD&
570 7700 7700
571 6530 JMP9M
572 1460 SAE&
573 0000 #9S 0
574 6610 JMP9T
575 1020 LDA&
576 0016 16
577 1365 STH&5
600 1000 LDA
601 0613 9T+3
602 2763 ADD9U=1
603 4763 STC9U=1
604 2003 ADD3
605 0224 XSK&4

```

```

      CONT
606 4626      STC9W
607 6452      JMP9E=5
610 0223 #9T XSK&3
611 1325      LDH&5
612 1020      LDA&
613 0000      0
614 0241      ROL 1
615 4613      STC'=2
616 6566      JMP9R+4
      [EOL
617 1302 #9V LDH 2
620 1460      SAE&
621 0077      77
622 6625      JMP9W=1
623 0226      XSK&6
624 6530      JMP9M
625 0011      CLR
626 6000 #9W JMP
      [CODE TABLE
627 4136 #9X 4136
630 3641      3641
631 2101      2101
632 0177      0177
633 4523      4523
634 2151      2151
635 4122      4122
636 2651      2651
637 2414      2414
640 0477      0477
641 5172      5172
642 0651      0651
643 1506      1506
644 4225      4225
645 4443      4443
646 6050      6050
647 5126      5126
650 2651      2651
651 5120      5120
652 3651      3651
653 0001 #9Y 1
654 7774      =3
655 7775      =2
656 7661      =116
657 0000      0000
660 0000      0000
661 0100      0100 [PERIOD
662 0000      0000
663 7736      7736 [STAR
664 3677      3677
665 0404      0404 [DASH
666 0404      0404
667 0404      0404 [PLUS
670 0437      0437
671 0403      0403 [SLASH
672 6010      6010
673 4177      4177 [BRACKET OPEN
674 0000      0000

```

	CONT		
675	1212	1212	[= SIGN
676	1212	1212	
677	4477	4477	[A
700	7744	7744	
701	5177	5177	
702	2651	2651	
703	4136	4136	
704	2241	2241	
705	4177	4177	
706	3641	3641	
707	4577	4577	
710	4145	4145	
711	4477	4477	
712	4044	4044	
713	4136	4136	
714	2645	2645	
715	1077	1077	
716	7710	7710	
717	7741	7741	
720	0041	0041	
721	4142	4142	
722	4076	4076	
723	1077	1077	
724	4324	4324	
725	0177	0177	
726	0301	0301	
727	3077	3077	
730	7730	7730	
731	3077	3077	
732	7706	7706	
733	4177	4177	
734	7741	7741	
735	4477	4477	
736	3044	3044	
737	4276	4276	
740	0376	0376	
741	4477	4477	
742	3146	3146	
743	5121	5121	
744	4651	4651	
745	4040	4040	
746	4077	4077	
747	0177	0177	
750	7701	7701	
751	0176	0176	
752	7402	7402	
753	0677	0677	
754	7701	7701	
755	1463	1463	
756	6314	6314	
757	0770	0770	
760	7007	7007	
761	4543	4543	
762	6151	6151	
		\$763	
763	0000	0	
764	0000	#9U 0	

INT-DSP,11 LN=711

148

CONT

COMPUTE1:0

149

	VALUE	LINE		VALUE	LINE
1F	0432	422	6I	0330	316
1G	0456	446	6J	0350	336
1H	0511	501	6K	0361	347
1I	0537	527	6L	0372	360
1J	1612	2000	6Y	0770	1145
1K	1643	2031	6Z	0771	1146
1L	1551	1736	7C	0400	550
1M	1561	1746	7D	0747	1124
1N	1571	1756	7I	0463	636
1T	1600	1766	7M	0612	766
2A	0404	373	7R	0754	1131
2B	0407	376	7T	0562	735
2C	0412	401	7U	0741	1116
2D	0416	405	7X	0737	1113
2E	0422	411	7Y	0740	1114
2F	0426	415	8A	0571	744
2G	1112	1274	8B	0574	747
2H	1115	1277	8C	1074	1255
2I	1120	1302	8D	1013	1174
2J	1124	1306	8E	1016	1177
2K	1142	1324	8F	1175	1360
2L	1160	1342	8G	1311	1475
2T	1604	1772	8H	1037	1220
3B	0635	1011	8I	1056	1237
3C	0650	1024	8J	1203	1366
3D	0667	1043	8K	1205	1370
3E	0657	1033	8L	1221	1404
3F	0706	1062	9A	1230	1413
3G	0715	1071	9B	1233	1416
3H	0701	1055	9C	1340	1524
3I	0722	1076	9D	1237	1422
3J	0602	755	9E	1355	1541
3K	0437	607	9F	1377	1563
3L	0450	621	9G	1610	1776
3M	0467	642	9H	1611	1777
3N	0600	753	9I	1606	1774
3O	0601	754	9J	1607	1775
3P	0736	1112	9K	1425	1611
3Q	0735	1111	9L	1372	1556
3R	0454	625	9M	1430	1615
3S	0570	743	9N	1453	1640
3T	3000	2055	9O	1457	1644
3U	0411	561	9P	1464	1651
3V	0576	751	9Q	1531	1716
3W	0577	752	9R	1541	1726
3X	0733	1107	9S	1577	1764
3Y	0734	1110	9T	1267	1452
3Z	0416	566	9Y	1700	2053
4A	0235	221	9Z	1701	2054
5A	0254	240			
5B	0262	246			
6A	0213	176			
6B	0216	201			
6C	0222	205			
6D	0226	211			
6E	0232	215			
6F	0271	256			
6G	0305	272			
6H	0313	300			

COMPUTE1:1 LN=1

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CONT
20 1020 LDA&
21 1750 1750 [1000
22 6000 JMP3A [FLOAT = 9E
23 1000 LDA
24 1237 9D [DZ/DT CAL
25 6635 JMP3B
26 7054 JMP1054 [COMPUTE 1000 X DZ/DT CAL
27 1355 9E
30 1377 9F
31 1430 9M [STORE IN 9M
32 1000 LDA
33 1233 9B [L MEAN
34 6635 JMP3B [FLOAT = 9F
35 7054 JMP1054 [COMPUTE L**2
36 1377 9F
37 1377 9F
40 1453 9N [STORE IN 9N
41 1000 LDA
42 1340 9C [Z CAL
43 6635 JMP3B [FLOAT = 9F
44 7054 JMP1054 [COMPUTE Z CAL**2
45 1377 9F
46 6400 =9F
47 7054 JMP1054 [COMPUTE Z CAL**2 X L**2
50 6324 =9N
51 7163 JMP1163 [COMPUTE Z CAL**2 X L**2 / 1000 X DZ/DT CA

L
52 6347 =9M
53 7734 JMP1734
54 6347 =9M [STORE IN 9M
55 1000 LDA
56 1230 9A [RHO
57 6635 JMP3B [FLOAT = 9F
60 7734 JMP1734
61 1377 9F
62 6324 =9N [STORE IN 9N
63 1020 LDA&
64 0063 63 [51
65 6635 JMP3B [FLOAT = 9F
66 7054 JMP1054 [MULTIPLY 51 X RHO
67 1453 9N
70 6400 =9F
71 7163 JMP1163 [DIVIDE BY 1000
72 6422 =9E
73 7054 JMP1054 [MULTIPLY TIMES EXISTING PRODUCT
74 6347 =9M
75 7734 JMP1734 [STORE IN 9F. PRODUCT WILL BE USED
76 6313 =9P [IN NEXT 512 CALCULATIONS OF CARDIAC OUTPU

T
77 0641 UMB1
100 0600 LMB0
101 6070 JMP70 [JUMP BACK TO MAIN PROGRAM
[COME HERE AT END OF SAMPLING TO COMPUTE CARDIAC OUTPU
T, STROKE VOLUME AND PULSE RATE
102 1000 LDA
103 1607 9J [Z
104 6000 JMP3A [FLOAT = 9E

```

```

CONT
105 7054 JMP1054 [COMPUTE Z**2
106 1355 9E
107 1355 9E
110 1453 9N [STORE IN 9N
111 1000 LDA
112 1611 9H [T3-T1
113 6000 JMP3A [FLOAT = 9E
114 1000 LDA
115 1610 9G [DZ/DT MIN
116 6635 JMP3B [FLOAT = 9F
117 7054 JMP1054 [MULTIPLY DZ/DT MIN X [T3-T1]
120 1355 9E
121 6400 *9F
122 7163 JMP1163 [DIVIDE BY Z**2
123 6324 *9N
124 7054 JMP1054 [MULTIPLY TIMES CAL FACTORS AND CONSTANTS
125 6313 *9P [TO GET STROKE VOLUME
126 7734 JMP1734
127 6347 *9M [STORE STROKE VOLUME IN 9M
130 1020 LDA&
131 0144 144
132 6000 JMP3A [FLOAT = 9E
133 1020 LDA&
134 0454 454
135 6635 JMP3B [FLOAT = 9F
136 7054 JMP1054 [FIND PRODUCT
137 1355 9E
140 1377 9F
141 1453 9N [STORE IN 9N
142 1000 LDA
143 1606 9I [T
144 6000 JMP3A [FLOAT = 9E
145 7163 JMP1163 [FIND T/30000
146 1355 9E
147 1453 9N
150 1453 9N [STORE IN 9N
151 7163 JMP1163 [COMPUTE CARDIAC OUTPUT
152 1430 9M
153 1453 9N
154 1377 9F [CARDIAC OUTPUT IN 9F
155 1020 LDA&
156 0001 1
157 6000 JMP3A [FLOAT = 9E
160 7163 JMP1163 [COMPUTE PULSE RATE
161 1355 9E [IN BEATS PER MINUTE
162 1453 9N
163 1453 9N [PULSE RATE IN 9N
164 1020 LDA&
165 0012 12 [10
166 6000 JMP3A [FLOAT = 9E
167 7163 JMP1163 [DIVIDE CARDIAC OUTPUT BY 10
170 1277 9276
171 0642 UMB2
172 1020 LDA&
173 7774 7774
174 4413 STC3U+2
175 4737 STC7X [MAKE PRESENT PEN POSITION

```



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CONT
176 4740      STC7Y [THE ORIGIN
177 1020      LDA&
200 6000      =1777
201 4601      STC30
202 4600      STC3N
203 6741      JMP7U [PEN UP
204 1000      LDA
205 0770      6Y
206 0450      AZE
207 6404      JMP2A
[PLOT LABELS FOR HUMAN DATA
210 1500      SRO [CHECK CODE WORD
211 0771      6Z [PASSED FROM FINAL DISPLAY ROUTINE
212 6222      JMP6C [DRAW AXIS FOR CARDIAC OUTPUT
213 1500      #6A SRO
214 0771      6Z
215 6226      JMP6D [DRAW AXIS FOR PULSE RATE
216 1500      #6B SRO
217 0771      6Z
220 6232      JMP6E [DRAW AXIS FOR STROKE VOLUME
221 6235      JMP4A [DRAW X AXIS
222 0065      #6C SET&5
223 4431      1F=1+4000
224 6271      JMP6F
225 6213      JMP6A
226 0065      #6D SET&5
227 4455      1G=1+4000
230 6271      JMP6F
231 6216      JMP6B
232 0065      #6E SET&5
233 4510      1H=1+4000
234 6271      JMP6F
[ DRAW X AXIS AND LABEL IT
235 6747      #4A JMP7D [PEN DOWN
236 1020      LDA&
237 1776      1776 [FILLED WITH LENGTH OF X AXIS
240 4733      STC3X
241 6612      JMP7M [DRAW X AXIS
242 6741      JMP7U [PEN UP
243 1020      LDA&
244 0062      6Z
245 4734      STC3Y
246 1020      LDA&
247 0454      454
250 4733      STC3X
251 6612      JMP7M [PREPARE TO WRITE LABEL
252 0065      SET&5
253 4536      1I=1+4000
254 1325      #5A LDH&5 [LOAD A WITH CHARACTER
255 1420      SHD&
256 7700      7700 [SEE IF END OF CHARACTER STRING
257 6262      JMP5B [JUMP IF YES
260 6400      JMP7C [OTHERWISE PLOT CHARACTER
261 6254      JMP5A
262 1020      #5B LDA& [SET PEN AT [0,1]
263 0144      144
264 4734      STC3Y

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CONT
265 4733 STC3X
266 6612 JMP7M
267 0640 UMB0
270 7000 JMP1000 [JUMP TO PLOT CURVES
      [DRAW Y AXES AND LABEL THEM]
271 0046 #6F SET6
272 0000 0
273 1020 LDA&
274 0620 620
275 4734 STC3Y
276 1020 LDA&
277 0144 144
300 4733 STC3X
301 6612 JMP7M [MOVE TO [1,4]
302 1020 LDA&
303 0006 6 [CHARACTER ORIENTATION +Y
304 4422 STC3Z+4
305 1325 #6G LDH&5 [LOAD A WITH CHARACTER
306 1420 SHD&
307 7700 7700
310 6313 JMP6H [JUMP IF END OF STRING
311 6400 JMP7C [PLOT CHARACTER
312 6305 JMP6G
313 1020 #6H LDA&
314 0144 144
315 4734 STC3Y
316 1020 LDA&
317 0310 310
320 4733 STC3X
321 6612 JMP7M [MOVE TO [2,1]
322 6747 JMP7D [PEN DOWN
323 1020 LDA&
324 1750 1750
325 4734 STC3Y
326 4422 STC3Z+4 [CHARACTER ORIENTATION +X
327 6612 JMP7M [DRAW LINE TO [2,10]
      [LABEL Y AXIS]
330 1020 #6I LDA&
331 0274 274
332 4733 STC3X
333 6612 JMP7M [DRAW .12 INCH LINE
334 6741 JMP7U [PEN UP
335 1020 LDA&
336 0206 206
337 4733 STC3X
340 6612 JMP7M [LEAVE SPACE FOR NUMBER
341 0415 KST
342 6350 JMP6J
343 0515 KBD
344 1460 SAE&
345 0012 0012
346 6350 JMP6J
347 7034 JMP8H=3
350 1325 #6J LDH&5
351 1420 SHD&
352 1200 1200
353 6372 JMP6L

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CONT
354 1420 SHD&
355 7700 7700
356 6361 JMP6K
357 6400 JMP7C [PLOT NUMBER
360 6350 JMP6J
361 1020 #6K LDA&
362 0310 310
363 4733 STC3X
364 6612 JMP7M
365 1020 LDA& [REDEFINE X AND Y
366 0144 144 [TO BE [0,1]
367 4740 STC7Y
370 4737 STC7X
371 6006 JMP6
372 1020 #6L LDA&
373 0310 310
374 4733 STC3X
375 1020 LDA&
376 7633 7633
377 1140 ADM
400 0734 3Y
401 6612 JMP7M [PREPARE TO PLOT NEXT NUMBER
402 6747 JMP7D [PEN DOWN
403 6330 JMP6I
[PLOT LABELS FOR DOG DATA
404 1500 #2A SRO [CHECK CODE WORD
405 0771 6Z [PASSED FROM FINAL DISPLAY ROUTINE
406 6416 JMP2D [DRAW AXIS FOR CARDIAC OUTPUT
407 1500 #2B SRO
410 0771 6Z
411 6422 JMP2E [DRAW AXIS FOR PULSE RATE
412 1500 #2C SRO
413 0771 6Z
414 6426 JMP2F [DRAW AXIS FOR STROKE VOLUME
415 6235 JMP4A [DRAW X AXIS
416 0065 #2D SET&5
417 5611 1J=1+4000
420 6271 JMP6F
421 6407 JMP2B
422 0065 #2E SET&5
423 4455 1G=1+4000
424 6271 JMP6F
425 6412 JMP2C
426 0065 #2F SET&5
427 5642 1K=1+4000
430 6271 JMP6F
431 6235 JMP4A
[TABLE OF CODES FOR LABELING AXES
432 3714 #1F 3714
433 4330 4330 [L PER MIN
434 4514 4514 [LABEL AXIS 2=20 FOR HUMAN DATA
435 4034 4034
436 4177 4177
437 0200 0200
440 1201 1201
441 1012 1012
442 0106 0106

```

CONT		
443	1201	1201
444	0412	0412
445	0102	0102
446	1201	1201
447	0012	0012
450	1410	1410
451	1214	1214
452	0612	0612
453	1404	1404
454	1214	1214
455	0277	0277
456	2530	#1G 2530
457	2447	2447 [BEATS PER MIN
460	4614	4614 [LABEL AXIS 40-220 FOR HUMAN AND DOG DATA
461	4330	4330
462	4514	4514
463	4034	4034
464	4177	4177
465	0202	0202
466	0012	0012
467	0200	0200
470	0012	0012
471	0110	0110
472	0012	0012
473	0106	0106
474	0012	0012
475	0104	0104
476	0012	0012
477	0102	0102
500	0012	0012
501	0100	0100
502	0012	0012
503	1410	1410
504	0012	0012
505	1406	1406
506	0012	0012
507	1404	1404
510	0077	0077
511	2626	#1H 2626 [CC
512	7702	7702 [LABEL AXIS 20-200 FOR HUMAN DATA
513	0000	0000
514	1201	1201
515	1000	1000
516	1201	1201
517	0600	0600
520	1201	1201
521	0400	0400
522	1201	1201
523	0200	0200
524	1201	1201
525	0000	0000
526	1214	1214
527	1000	1000
530	1214	1214
531	0600	0600
532	1214	1214
533	0400	0400

	CONT	
534	1214	1214
535	0200	0200
536	7777	7777
537	4742	#11 4742 [TOTAL TIME
540	4724	4724
541	3714	3714
542	4734	4734
543	4030	4030
544	1400	1400
545	0061	0061
546	0014	0014
547	4034	4034
550	4177	4177

[CALCOMP PLOT
 [MODIFIED FOR LINC 300
 [F T DAVIDSON 5 OCT 67
 [CHARACTER PLOT
 [PEN MUST BE IN THE
 [UP POSITION

400	1120	#7C	ADA &
401	3000		3T
402	4017		STC 17
403	2000		ADD 0
404	4454		STC 3F
405	1017		LDA 17
406	1120		ADA &
407	2000		2000
410	4017		STC 17
411	1017	#3U	LDA 17
412	0075		SET & 15
413	7776		=1 [MAGNIFICATION
414	0451		APO
415	6754		JMP 7F
416	1317	#3Z	LDH 17
417	1560		BCL &
420	7770		7770
421	1120		ADA &
422	0000		0 [ORIENTATION
423	1560		BCL &
424	7770		7770
425	1120		ADA &
426	0602		3J
427	4016		STC 16
430	1016		LDA 16
431	4442		STC 3K+3
432	1337		LDH & 17
433	0470		AZE &
434	6450		JMP 3I
435	0017		COM
436	4440		STC 3K+1
437	0076	#3K	SET & 16
440	0000		0 [MINUS THE NO. OF INCREMENTS IN THIS DIRECTION
441	1020		LDA &
442	0000		0 [MOTION WORD
443	6463		JMP 7I
444	0236		XSK & 16

```

CONT
445 6441      JMP ' -4
446 0235      XSK & 15
447 6437      JMP 3K
      [TEST FOR END
450 1017 #3L LDA 17
451 1560      BCL &
452 5777      5777
453 0450      AZE
454 0000 #3R RETURN
      [STEP LINE OF CHAR*TABLE=ALLOWS OVERLAP INTO UPPER MEM
      ORY
455 1020      LDA &
456 4000      =3777
457 1140      ADM
460 0017      17
461 1017      LDA 17
462 6411      JMP 3U
      [INCREMENT PLOTTER AND X*Y SR
463 4467 #7I STC 3M
464 2000      ADD 0
465 4570      STC 3S
466 1520      SRO & [TEST FOR =Y
467 0000 #3M [KEY WORD
470 6511      JMP '+21
471 2740      ADD 7Y [TEST FOR POINTS LESS THAN OR EQUAL LOWER B
      OUND
472 2600      ADD 3N
473 0451      APO
474 6505      JMP '+11
475 0011      CLR [TEST FOR POINTS GREATER THAN UPPER BOUND
476 2740      ADD 7Y
477 2601      ADD 3O
500 0471      APO &
501 6505      JMP '+4
502 1020      LDA & [CARRIAGE RIGHT
503 0004      4
504 6571      JMP 8A
505 0011      CLR
506 2740      ADD 7Y [DECREASE POINT INDICATOR IN 7Y
507 2576      ADD 3V
510 4740      STC 7Y
511 1500      SRO [TEST FOR +Y
512 0467      3M
513 6536      JMP '+23
514 2740      ADD 7Y [TEST FOR POINTS GREATER THAN OR EQUAL LOWE
      R BOUND
515 2601      ADD 3O
516 2577      ADD 3W
517 0471      APO &
520 6532      JMP '+12
521 0011      CLR [TEST FOR POINTS LESS THAN LOWER BOUND
522 2740      ADD 7Y
523 2600      ADD 3N
524 2577      ADD 3W
525 0451      APO
526 6532      JMP '+4
527 1020      LDA& [CARRIAGE LEFT

```

```

CONT
530 0010      10
531 6571      JMP 8A
532 0011      CLR
533 2740      ADD 7Y [INCREASE POINT INDICATOR IN 7Y
534 2577      ADD 3W
535 4740      STC 7Y
536 1500      SRO [TEST FOR +X
537 0467      3M
540 6550      JMP '+10
541 1020      LDA & [DRUM DOWN
542 0002      2
543 6571      JMP 8A
544 1000      LDA
545 0737      7X
546 2577      ADD 3W
547 4737      STC 7X
550 1500      SRO [TEST FOR =X
551 0467      3M
552 6562      JMP '+10
553 1020      LDA & [DRUM UP
554 0001      1
555 6571      JMP 8A
556 1000      LDA
557 0737      7X
560 2576      ADD 3V
561 4737      STC 7X
562 1000 #7T LDA
563 0574      8B
564 0546      OPR 46
565 6564      JMP '=1
566 0011      CLR
567 4574      STC 8B
570 1440 #3S S RETURN
571 1600 #8A FSE
572 0574      8B
573 1060      STA &
574 0000 #8B 0
575 6000      JMP 0
576 7776 #3V =1
577 0001 #3W +1
600 1777 #3N 1777 [Y=LOWER BOUND NOTE SIGN
601 6000 #30 =1777 [Y=UPPER BOUND NOTE SIGN
602 7776 #3J =1 [Y
603 7766      =11 [X,=Y
604 7767      =10 [X
605 7765      =12 [X,+Y
606 7775      =2 [+Y
607 7771      =6 [+X,+Y
610 7773      =4 [+X
611 7772      =5 [+X,=Y
    [INTERPOLATED MOTION
612 0076 #7M SET & 16
613 7767      =10
614 0075      SET & 15
615 7776      =1
616 1000      LDA
617 0734      3Y

```

```

CONT
620 2735      ADD 3Q
621 4736      STC 3P
622 2000      ADD 0
623 4454      STC 3R
624 2733      ADD 3X
625 0017      COM
626 2737      ADD 7X
627 0471      APO &
630 6634      JMP '+4
631 0076      SET & 16
632 7773      =4
633 0017      COM
634 1060      STA &
635 0000 #3B  C/DELX/
636 0011      CLR
637 2736      ADD 3P
640 0017      COM
641 2740      ADD 7Y
642 0471      APO &
643 6647      JMP '+4
644 0075      SET & 15
645 7775      =2
646 0017      COM
647 1060      STA &
650 0000 #3C  C/DELY/
651 0077      SET & 17
652 3777      =4000
653 1600      BSE
654 0635      3B
655 0470      AZE &
656 6454      JMP 3R
657 4667 #3E  STC 3D
660 2635      ADD 3B
661 0241      ROL 1
662 4635      STC 3B
663 2650      ADD 3C
664 0241      ROL 1
665 4650      STC 3C
666 1020      LDA &
667 0000 #3D  CRESULT OF BSE
670 0241      ROL 1
671 0451      APO
672 6676      JMP '+4
673 1500      SRO
674 0017      17
675 6657      JMP 3E
676 0011      CLR
677 4706      STC 3F
700 4715      STC 3G
701 0011 #3H  CLR
702 2016      ADD 16
703 4722      STC 3I
704 2635      ADD 3B
705 1220      LAM &
706 0000 #3F  STC 0
707 4000
710 0472      LZE &

```



```

CONT
711 4722      STC 3I
712 0011      CLR
713 2650      ADD 3C
714 1220      LAM &
715 0000 #3G
716 4000      STC 0
717 0452      LZE
720 2015      ADD 15
721 1120      ADA &
722 0000 #3I
723 0450      AZE
724 6463      JMP 7I
725 2577      ADD 3W [+1
726 1140      ADM
727 0017      17
730 0450      AZE
731 6701      JMP 3H
732 6454      JMP 3R
733 0000 #3X 0000 [DESIRED X
734 0000 #3Y 0000 [DESIRED Y
735 0000 #3Q 0000 [Y=SHIFT
736 0000 #3P 0000 [3Y+3Q
737 0000 #7X 0000 [CURRENT X
740 0000 #7Y 0000 [CURRENT Y
      [PEN SUBROUTINES
741 0056 #7U SET 16 [PEN UP
742 0000      0
743 1020      LDA &
744 0040      40
745 4757      STC 7R+3
746 6756      JMP 7R+2
747 0056 #7D SET 16 [PEN DOWN
750 0000      0
751 1020      LDA &
752 0020      20
753 6745      JMP 7D=2
754 0056 #7R SET 16 [PEN REVERSE
755 0000      0
756 1020      LDA &
757 0020      20
760 1660      BCO &
761 0060      60
762 1040      STA
763 0757      7R+3
764 0546      OPR 46
765 6764      JMP '=1
766 6016      JMP 16
      $770
770 0000 #6Y 0 [FLAG = EQUALS 1 IF DOG EXP., 0 IF HUMAN DATA
771 0000 #6Z 0 [CODE INDICATING WHICH CURVE TO PLOT
      [7=ALL THREE
      [6=PR+SV
      [5=CO+SV
      [4=SV
      [3=CO+PR
      [2=PR
      [1=CO

```

```

CONT
[ROUTINE TO PLOT DESIRED CURVES
$1000
1000 1000 LDA
1001 0771 6Z
1002 0243 ROL3
1003 4771 STC6Z
1004 1000 LDA
1005 0770 6Y
1006 0450 AZE
1007 7112 JMP2G
[ PLOT HUMAN DATA
1010 1500 SR0 [CHECK CODE WORD TO SEE
1011 0771 6Z [WHICH CURVE(S) TO PLOT
1012 7037 JMP8H [PLOT CARDIAC OUTPUT
1013 1500 #8D SR0
1014 0771 6Z
1015 7056 JMP8I [PLOT PULSE RATE
1016 1500 #8E SR0
1017 0771 6Z
1020 7074 JMP8C [PLOT STROKE VOLUME
1021 1000 LDA [COME HERE WHEN FINISHED PLOTTING
1022 0237 4A+2
1023 4733 STC3X
1024 4734 STC3Y
1025 6612 JMP7M
1026 0011 CLR
1027 4737 STC7X
1030 1020 LDA&
1031 0454 454
1032 4733 STC3X
1033 6612 JMP7M [POSITION PEN FOR NEXT GRAPH
1034 0641 UMB1
1035 0600 LMB0
1036 6433 JMP433 [JUMP BACK TO PAGE 0 AND DISPLAY ROUTINE
1037 0770 #8H 770 [READ VALUES FOR CARDIAC OUTPUT
1040 6270 6/270
1041 0750 750
1042 7271 7/271
1043 0000 HLT
1044 1020 LDA&
1045 7467 7467
1046 5233 STC9B
1047 1020 LDA&
1050 0053 53 [X
1051 5340 STC9C
1052 1020 LDA&
1053 5607 9J+4000
1054 7175 JMP8F [PLOT CARDIAC OUTPUT
1055 7013 JMP8D [SEE IF MORE CURVES TO PLOT
1056 0751 #8I 751 [READ IN PULSE RATE DATA
1057 1276 1/276
1060 1020 LDA&
1061 7727 7727
1062 5233 STC9B
1063 1020 LDA&
1064 0062 62 [X
1065 5340 STC9C

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CONT
1066 6612      JMP7M [RETURN TO [0,1]
1067 0000      HLT
1070 1020      LDA&
1071 1606      9I
1072 7175      JMP8F [PLOT PULSE RATE
1073 7016      JMP8E [SEE IF ONE MORE CURVE TO PLOT
1074 0770 #8C 770 [READ IN STROKE VOLUME DATA
1075 6274      6/274
1076 0750      750
1077 7275      7/275
1100 1020      LDA&
1101 7753      7753
1102 5233      STC9B
1103 5340      STC9C [0
1104 6612      JMP7M [RETURN TO [0,1]
1105 0000      HLT
1106 1020      LDA&
1107 1606      9I
1110 7175      JMP8F [PLOT STROKE VOLUME
1111 7021      JMP8E+3 [JUMP TO RETURN TO PAGE 0
          [PLOT DOG VALUES
1112 1500 #2G SRO [EXAMINE CODE WORD TO SEE
1113 0771      6Z [WHICH CURVES TO PLOT
1114 7124      JMP2J [PLOT CARDIAC OUTPUT
1115 1500 #2H SRO
1116 0771      6Z
1117 7142      JMP2K [PLOT PULSE RATE
1120 1500 #2I SRO
1121 0771      6Z
1122 7160      JMP2L [PLOT STROKE VOLUME
1123 7021      JMP8E+3
1124 0770 #2J 770 [READ VALUES FOR CARDIAC OUTPUT
1125 6270      6/270
1126 0750      750
1127 7271      7/271
1130 0000      HLT
1131 0011      CLR
1132 5233      STC9B
1133 1020      LDA&
1134 0053      53 [X
1135 5340      STC9C
1136 1020      LDA&
1137 1610      9G
1140 7175      JMP8F [PLOT CARDIAC OUTPUT
1141 7115      JMP2H
1142 0751 #2K 751 [READ IN PULSE RATE DATA
1143 1276      1/276
1144 1020      LDA&
1145 7727      7727
1146 5233      STC9B
1147 1020      LDA&
1150 0062      62 [1
1151 5340      STC9C
1152 6612      JMP7M [RETURN TO [0,1]
1153 0000      HLT
1154 1020      LDA&
1155 1606      9I

```

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CONT
1156 7175 JMP8F [PLOT PULSE RATE
1157 7120 JMP21
1160 0770 #2L 770 [READ IN STROKE VOLUME DATA
1161 6274 6/274
1162 0750 750
1163 7275 7/275
1164 0011 CLR
1165 5233 STC9B
1166 5340 STC9C [0
1167 6612 JMP7M [RETURN TO [0,1]
1170 0000 HLT
1171 1020 LDA&
1172 1611 9H
1173 7175 JMP8F [PLOT STROKE VOLUME
1174 7021 JMP8E+3
[PLOT CURVE
1175 5237 #8F STC9D
1176 5577 STC9S
1177 0044 SET4
1200 0000 0
1201 0061 SET&1
1202 2777 2777
1203 0461 #8J SNS&1 [IF SENSE SWITCH 1 IS SET
1204 7355 JMP9E [JUMP TO AVERAGE 4 POINTS
1205 0043 #8K SET3
1206 1700 9Y [SET NO. OF POINTS TO PLOT
1207 0536 OPR&16 [READ RSW
1210 1560 BCL& [EXAMINE BITS 0 AND 1
1211 7774 7774
1212 1120 ADA& [C[RSW] DESERMINES NO. OF SYMBOLS PLOTTED
1213 1600 1T
1214 1040 STA
1215 1311 8G
1216 5220 STC'+2
1217 0045 SET5
1220 0000 0
1221 1021 #8L LDA&1 [LOAD A WITH Y COORDINATE
1222 7230 JMP9A [PLOT POINT
1223 1020 LDA&
1224 0002 2
1225 1140 ADM
1226 0733 3X
1227 7221 JMP8L
1230 0050 #9A SET10
1231 0000 0
1232 1120 ADA& [MODIFY FOR PLACEMENT ON GRAPH
1233 0000 #9B 0 [VALUE FILLED IN
1234 0470 AZE&
1235 7240 JMP9D+1
1236 1240 MUL
1237 0000 #9D 0 [VALUE FILLED IN
1240 1120 ADA&
1241 0144 144
1242 1040 STA
1243 0734 3Y [STORE Y COORDINATE
1244 1120 ADA&
1245 6000 =1777

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CONT
1246 0451      APO
1247 7253      JMP'+4
1250 1020      LDA&
1251 1777      1777
1252 4734      STC3Y
1253 6612      JMP7M [PLOT POINT
1254 0415      KST
1255 7263      JMP'+6
1256 0515      KBD
1257 1460      SAE&
1260 0012      0012
1261 7263      JMP'+2
1262 7034      JMP8H=3
1263 0223      XSK&3 [SKIP IF ALL VALUES PLOTTED
1264 7274      JMP'+10 [OTHERWISE CHECK IF SYMBOL TO BE PLOTTED
1265 6741      JMP7U
1266 7430      JMP9M
1267 1020      #9T LDA&
1270 0144      144
1271 4734      STC3Y
1272 4733      STC3X
1273 6004      JMP4
1274 1000      LDA
1275 0001      1
1276 1460      SAE&
1277 3000      3000
1300 7302      JMP'+2
1301 6747      JMP7D [PEN DOWN
1302 1460      SAE&
1303 3003      3003
1304 7306      JMP'+2
1305 6747      JMP7D
1306 0225      XSK&5 [SKIP IF SYMBOL REQUIRED
1307 6010      JMP10 [OTHERWISE GET NEXT POINT
[PLOT SYMBOL
1310 0045      SET5
1311 0000      #8G 0
1312 1000      LDA [SAVE PRESENT X AND Y
1313 0737      7X
1314 5604      STC2T
1315 1000      LDA
1316 0740      7Y
1317 5605      STC2T+1
1320 1020      LDA&
1321 7775      7775
1322 4413      STC3U+2
1323 1020      LDA& [ADJUST X AND Y SO THAT SYMBOL
1324 7771      7771 [IS CENTERED
1325 1140      ADM
1326 0734      3Y
1327 1020      LDA&
1330 7773      7773
1331 1040      STA
1332 1577      9S
1333 1140      ADM
1334 0733      3X
1335 6741      JMP7U [PEN UP

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CONT
1336 6612      JMP7M  [PREPARE TO DRAW SYMBOL
1337 1020      LDA&
1340 0000 #9C  0 [SYMBOL CODE FILLED IN
1341 0642      UMB2
1342 6400      JMP7C [PLOT SYMBOL
1343 0640      UMB0
1344 1000      LDA [RESTORE COORDINATES
1345 1604      2T
1346 4733      STC3X
1347 1000      LDA
1350 1605      2T+1
1351 4734      STC3Y
1352 6612      JMP7M
1353 6747      JMP7D [PEN DOWN
1354 6010      JMP10 [JUMP TO PLOT NEXT POINT
1355 1000 #9E  LDA
1356 1701      9Z
1357 0470      AZE& [IF LESS THAN 4 VALUES, PLOT EVERY
1360 7205      JMP8K [POINT
1361 0043      SET3 [SET NO. OF POINTS TO PLOT=NO. OF VALUES
1362 1701      9Z [DIVIDED BY 4
1363 0536      OPR&16 [READ RSW
1364 1560      BCL& [CHECK TO SEE IF EITHER BIS 0 OR 1 SET
1365 7774      7774
1366 0470      AZE& [SKIP IF SES
1367 7425      JMP9K [IF NOT SET, NO SYMBOLS PLOTTED
1370 1020      LDA& [PREPARE TO PLOT ONE SYMBOL
1371 1603      1T+3 [FOR EVERY POINT
1372 1040 #9L  STA
1373 1311      8G
1374 5376      STC'+2
1375 0045      SET5
1376 0000      0
1377 1021 #9F  LDA&1
1400 1121      ADA&1 [AVERAGE 4 POINTS
1401 0341      SCR1
1402 1560      BCL&
1403 4000      4000
1404 5413      STC'+7
1405 1021      LDA&1
1406 1121      ADA&1
1407 0341      SCR1
1410 1560      BCL&
1411 4000      4000
1412 1120      ADA&
1413 0000      0
1414 0341      SCR1
1415 1560      BCL&
1416 4000      4000
1417 7230      JMP9A [PLOT POINT
1420 1020      LDA&
1421 0010      10
1422 1140      ADM
1423 0733      3X
1424 7377      JMP9F
1425 1020 #9K  LDA&
1426 1600      1T

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CONT
1427 7372 JMP9L
      [WRITE LEGEND
1430 1020 #9M LDA&
1431 1440 1440
1432 4733 STC3X
1433 1020 LDA&
1434 7775 7775
1435 4413 STC3U+2
1436 1000 LDA
1437 1340 9C
1440 0470 AZE&
1441 7453 JMP9N [COME HERE IF STROKE VOLUME
1442 1460 SAE&
1443 0053 0053
1444 7457 JMP9O [COME HERE IF PULSE RATE
1445 1020 LDA& [COME HERE IF CARDIAC OUTPUT
1446 0050 50
1447 4734 STC3Y
1450 0065 SET&5
1451 5550 1L=1+4000
1452 7464 JMP9P
1453 4734 #9N STC3Y
1454 0065 SET&5
1455 5560 1M=1+4000
1456 7464 JMP9P
1457 1020 #9O LDA&
1460 0120 120
1461 4734 STC3Y
1462 0065 SET&5
1463 5570 1N=1+4000
1464 6612 #9P JMP7M
1465 1000 LDA
1466 1577 9S
1467 0470 AZE&
1470 7531 JMP9Q
1471 6741 JMP7U
1472 1000 LDA
1473 1340 9C
1474 0642 UMB2
1475 6400 JMP7C
1476 0640 UMB0
1477 1020 LDA&
1500 0006 6
1501 1140 ADM
1502 0734 3Y
1503 1020 LDA&
1504 0012 12
1505 1140 ADM
1506 0733 3X
1507 6612 JMP7M
1510 6747 JMP7D
1511 1020 LDA&
1512 0032 32
1513 1140 ADM
1514 0733 3X
1515 6612 JMP7M
1516 6741 JMP7U

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CONT
1517 1020 LDA&
1520 7771 7771
1521 1140 ADM
1522 0734 3Y
1523 6612 JMP7M
1524 1000 LDA
1525 1340 9C
1526 0642 UMB2
1527 6400 JMP7C
1530 7541 JMP9R
1531 6747 #9Q JMP7D
1532 1020 LDA&
1533 0062 62
1534 1140 ADM
1535 0733 3X
1536 6612 JMP7M
1537 6741 JMP7U
1540 0642 UMB2
1541 1325 #9R LDH&5
1542 1420 SHD&
1543 7700 7700
1544 7547 JMP'+3
1545 6400 JMP7C
1546 7541 JMP9R
1547 0640 UMB0
1550 7267 JMP9T
1551 1426 #1L 1426
1552 2445 2445
1553 2734 2734
1554 2426 2426
1555 1442 1442
1556 5047 5047
1557 4350 4350
1560 4777 4777
1561 1446 #1M 1446
1562 4745 4745
1563 4236 4236
1564 3014 3014
1565 5142 5142
1566 3750 3750
1567 4030 4030
1570 7777 7777
1571 1443 #1N 1443
1572 5037 5037
1573 4630 4630
1574 1445 1445
1575 2447 2447
1576 3077 3077
1577 0000 #9S 0
      CUSE RSW TO SELECT NO. OF SYMBOLS / CURVE PLOTTED
1600 6777 #1T 6777 CIF 0=NONE
1601 7677 7677 CIF 1= 8
1602 7767 7767 CIF 2= 64
1603 7776 7776 CIF 3= EVERY POINT
1604 0000 #2T 0
1605 0000 0
1606 0005 #9I 5

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      CONT
1607 2000 #9J 2000 [1/2
1610 0002 #9G 2
1611 0024 #9H 24
1612 3714 #1J 3714 [L PER MIN
1613 4330 4330 [LABEL AXIS 0=4.5 FOR DOG VALUES
1614 4514 4514
1615 4034 4034
1616 4177 4177
1617 0461 0461
1620 0512 0512
1621 0461 0461
1622 0012 0012
1623 0361 0361
1624 0512 0512
1625 0361 0361
1626 0012 0012
1627 0261 0261
1630 0512 0512
1631 0261 0261
1632 0012 0012
1633 0161 0161
1634 0512 0512
1635 0161 0161
1636 0012 0012
1637 0061 0061
1640 0512 0512
1641 0061 0061
1642 0077 0077
1643 2626 #1K 2626 [CC
1644 7704 7704 [LABEL AXIS 0=45 FOR DOG VALUES
1645 0512 0512
1646 0400 0400
1647 1203 1203
1650 0512 0512
1651 0300 0300
1652 1202 1202
1653 0512 0512
1654 0200 0200
1655 1201 1201
1656 0512 0512
1657 0100 0100
1660 1214 1214
1661 0512 0512
1662 1400 1400
1663 7777 7777
      $1700
1700 0000 #9Y 0 [TOTAL NO. OF VALUES
1701 0000 #9Z 0 [1/4 TOTAL NO. OF VALUES
      3T=3000

```

VALUE	LINE	VALUE	LINE
1A 1245	1263	4H 1744	2043
1B 1255	1274	4I 1745	2044
1C 1271	1311	4J 1746	2045
1D 1304	1325	4K 1747	2046
1E 1313	1335	4L 1750	2047
1F 1323	1346	5T 0162	144
1G 1331	1355	5U 0217	201
1H 1346	1373	5V 0241	223
1I 1356	1404	5W 0324	306
1J 1366	1415	5X 0346	330
1K 1377	1427	8A 0041	22
1L 1405	1436	8B 0044	25
1M 1411	1443	8C 0047	30
1N 1416	1451	8D 0054	35
1O 1427	1463	8E 0124	105
1P 1434	1471	8F 0127	110
1Q 1444	1502	8G 0132	113
1R 1460	1517	8H 0135	116
1S 1471	1531	8I 0140	121
1T 1507	1550	8J 0143	124
1U 1515	1557	8K 0145	126
1V 1523	1566	8L 0151	132
1W 1532	1576	8M 0154	135
1X 1541	1606	8N 0157	140
1Y 1552	1620	8O 0066	47
1Z 1563	1632	8P 0107	70
2A 1100	1103	9A 0400	376
2B 1112	1116	9B 0431	430
2C 1120	1125	9D 0447	446
2D 1130	1136	9E 0457	457
2E 1145	1154	9F 0466	466
2F 1153	1163	9G 0470	470
2G 1167	1200	9H 0473	473
2H 1203	1215	9J 0520	520
2I 1212	1225	9K 0523	523
2J 1234	1250	9M 0530	530
2K 1572	1643	9N 0542	542
2L 1573	1645	9Q 0555	555
2M 1574	1647	9R 0562	562
2N 1575	1651	9S 0573	573
2O 1610	1665	9T 0610	610
2P 1625	1703	9U 0764	767
2Q 1631	1710	9V 0617	620
2R 1637	1717	9W 0626	627
2S 1641	1722	9X 0627	631
2T 1652	1734	9Y 0653	655
2U 1653	1737		
2V 1660	1745		
2W 1671	1757		
2X 1677	1766		
2Y 1705	1775		
2Z 1720	2011		
3A 1726	2020		
4B 1727	2022		
4C 1732	2026		
4D 1740	2035		
4E 1741	2037		
4F 1742	2041		
4G 1743	2042		

```

CONT
20 1020 LDA&
21 0162 ST [CHOOSE SCOPE OR PLOT
22 6400 JMP9A [JUMP TO SCOPE PKG
23 6151 JMP8L [JUMP BACK TO DISPLAY
24 6154 JMP8M [JUMP TO RESTART PROGRAM
25 6054 JMP8D [JUMP IF PLOT
26 6157 JMP8N [JUMP TO PRINT
27 1020 LDA& [IF SCOPE=SELECT TO DISPLAY PULSE
30 0217 SW [RATE, STROKE VOLUME OR CARDIAC OUTPUT
31 6400 JMP9A [JUMP TO SCOPE PKG
32 6020 JMP20
33 6044 JMP8B [RETURN HERE IF PULSE RATE
34 6047 JMP8C [RETURN HERE IF STROKE VOLUME
35 0770 770 [RETURN HERE IF CARDIAC OUTPUT
36 6270 6/270 [ENTER CO DATA FROM TAPE
37 0750 750
40 7271 7/271
41 0641 #8A UMB1
42 0600 LMB0
43 6520 JMP520 [JUMP TO SCOPE DISPLAY ROUTINE
44 0751 #8B 751 [ENTER PR DATA FROM TAPE
45 1276 1/276
46 6041 JMP8A
47 0770 #8C 770 [ENTER SV DATA FROM TAPE
50 6274 6/274
51 0750 750
52 7275 7/275
53 6041 JMP8A
54 0643 #8D UMB3 [JUMP HERE IF PLOT
55 1020 LDA&
56 0324 SW
57 6400 JMP9A [JUMP TO SCOPE PKG
60 6020 JMP20
61 6066 JMP80 [JUMP IF HUMAN PATIENT
62 1020 LDA&
63 0001 J
64 1040 STA
65 2770 2770
66 1020 #80 LDA&
67 0346 SX [CHOOSE LENGTH OF X AXIS
70 6400 JMP9A [JUMP TO SCOPE PKG
71 6054 JMP8D
72 6107 JMP8P
73 1020 LDA&
74 0004 4 [SET HORIZONTAL INCREMENT IN PLOT ROUTINE
75 1040 STA
76 3224 3224
77 1020 LDA&
100 0020 20
101 1040 STA
102 3421 3421
103 1020 LDA&
104 3774 3774 [SET LENGTH OF X AXIS
105 1040 STA
106 2066 2066
107 1020 #8P LDA&
110 0241 5V [SELECT TO PLOT 1*3 CURVES

```

```

CONT
111 6400      JMP9A [JUMP TO SCOPE PKG
112 6054      JMP8D
113 6124      JMP8E
114 6127      JMP8F
115 6132      JMP8G
116 6135      JMP8H
117 6140      JMP8I
120 6143      JMP8J
121 1020      LDA&
122 0007      7
123 6145      JMP8K
124 1020 #8E  LDA&
125 0001      1
126 6145      JMP8K
127 1020 #8F  LDA&
130 0002      2
131 6145      JMP8K
132 1020 #8G  LDA&
133 0004      4
134 6145      JMP8K
135 1020 #8H  LDA&
136 0003      3
137 6145      JMP8K
140 1020 #8I  LDA&
141 0005      5
142 6145      JMP8K
143 1020 #8J  LDA&
144 0006      6
145 1040 #8K  STA
146 2771      2771 [PLACE CODE IN PAGE 3 - LOC 771
147 0603      LMB3
150 6020      JMP20 [JUMP TO PLOTTING ROUTINES
151 0641 #8L  UMB1 [JUMP BACK TO DISPLAY
152 0600      LMB0
153 6433      JMP433
154 0641 #8M  UMB1 [RESTART PROGRAM
155 0600      LMB0
156 6047      JMP47
157 0643 #8N  UMB3
160 0600      LMB0
161 6741      JMP741 [JUMP TO READ IN PRINT ROUTINE
[DISPLAY TEXT
162 0201 #5T  0201 [1=RESTART PROGRAM
163 1301      1301 [2=PLOT
164 1745      1745 [3=PRINT
165 3046      3046 [4=SCOPE
166 4724      4724
167 4547      4547
170 1443      1443
171 4542      4542
172 3245      3245
173 2440      2440
174 5656      5656
175 1302      1302
176 1743      1743
177 3742      3742
200 4714      4714

```

CONT		
201	5656	5656
202	1303	1303
203	1743	1743
204	4534	4534
205	4147	4147
206	5656	5656
207	1304	1304
210	1746	1746
211	2642	2642
212	4330	4330
213	5777	5777
214	0102	0102
215	0304	0304
216	7777	7777
217	0201	#5U 0201 [1=P.R.
220	1301	1301 [2=S.V.
221	1743	1743 [3=C.O.
222	1545	1545
223	1514	1514
224	5656	5656
225	1302	1302
226	1746	1746
227	1551	1551
230	1514	1514
231	5656	5656
232	1303	1303
233	1726	1726
234	1542	1542
235	1514	1514
236	5777	5777
237	0102	0102
240	0377	0377
241	0201	#5V 0201 [1=C.O.
242	1301	1301 [2=P.R.
243	1726	1726 [3=S.V.
244	1542	1542 [4=C.O. + P.R.
245	1514	1514 [5=C.O. + S.V.
246	5656	5656 [6=P.R. + S.V.
247	1302	1302 [7=ALL THREE
250	1743	1743
251	1545	1545
252	1514	1514
253	5656	5656
254	1303	1303
255	1746	1746
256	1551	1551
257	1514	1514
260	5656	5656
261	1304	1304
262	1726	1726
263	1542	1542
264	1514	1514
265	2014	2014
266	4315	4315
267	4515	4515
270	5656	5656
271	1305	1305

CONT		
272	1726	1726
273	1542	1542
274	1514	1514
275	2014	2014
276	4615	4615
277	5115	5115
300	5656	5656
301	1306	1306
302	1743	1743
303	1545	1545
304	1514	1514
305	2014	2014
306	4615	4615
307	5115	5115
310	5656	5656
311	1307	1307
312	1724	1724
313	3737	3737
314	1447	1447
315	3345	3345
316	3030	3030
317	5777	5777
320	0102	0102
321	0304	0304
322	0506	0506
323	0777	0777
324	0201	0201
325	1301	1301
326	1733	1733
327	5040	5040
330	2441	2441
331	1427	1427
332	2447	2447
333	2414	2414
334	5656	5656
335	1302	1302
336	1727	1727
337	4232	4232
340	1427	1427
341	2447	2447
342	2414	2414
343	5777	5777
344	0102	0102
345	7777	7777
346	0201	0201
347	1301	1301
350	1753	1753
351	1424	1424
352	5334	5334
353	4661	4661
354	0100	0100
355	1434	1434
356	4115	4115
357	5656	5656
360	1302	1302
361	1753	1753
362	1424	1424

#5W

[1=HUMAN DATA
[2=DOG DATA

#5X

[1=X AXIS=10 IN.
[2=X AXIS=20 IN.

	CONT	
363	5334	5334
364	4661	4661
365	0200	0200
366	1434	1434
367	4115	4115
370	5777	5777
371	0102	0102
372	7777	7777

```

[SCOPE=SP ,SP=SAME PAGE
[GENERAL PURPOSE ROUTINES FOR ENTERING DATA
[AND SELECTING OPTIONS
[CG.FELLOWS=FEB 67
[CODE 0=ENTER TEXT
[CODE 1=STAR OPTION AND RETURN TO '+2
[CODE 2=STAR OPTION AND RETURN TO '+1+N
[   WERE N IS POSITION OF OPTION IN LIST
[CASE ALWAYS RETURNS TO '+1
[60 AT TEXT END,DISPLAY ONCE AND RETURN '+1
[76 AT END OF TEXT MEANS RETURN TO '+2 ON EOL
[77 AT END OF TEXT MEANS RETURN TO '+2 ON EOL
[   IF CORRECT NO. OF ENTRIES MADE
[LOAD TAG OF TEXT IN ACCUM, THEN JUMP 9A
[9A CAN BE PUT AT START OF ANY QUARTER IN LOWER PAGE
[USES REGS 1,2,3,4,5,6

```

```

$400
400 0046 #9A SET 6
401 0000 0
402 0062 SET&2
403 1775 1775
404 0471 APO&
405 0222 XSK&2
406 1560 BCL&
407 4000 4000
410 4001 STC1
411 2006 ADD6
412 1040 STA
413 0523 9K
414 2653 ADD9Y [1
415 4626 STC9W
416 1301 LDH 1
417 0017 COM
420 4555 STC9Q
421 1321 LDH&1
422 0017 COM
423 2655 ADD9Y+2
424 4447 STC9D
425 2001 ADD1
426 4460 STC9E+1
427 0222 XSK&2
430 6446 JMP9D=1
[CLEAR WORKING AREA 9U
431 0061 #9B SET&1
432 7747 =30
433 0062 SET&2
434 4763 9U=4000
435 1020 LDA&
436 0017 17

```

```

CONT
437 0043 SET 3
440 0555 9Q
441 0203 XSK 3
442 2654 ADD9Y+1
443 1362 STH&2
444 0221 XSK&1
445 6443 JMP'=2
446 0066 SET&6
447 0000 #9D 0
450 0011 CLR
451 4763 STC9U=1
452 1020 LDA&
453 0001 1
454 4613 STC9T+3
455 0065 SET&5
456 0764 9U
[START OF DISPLAY
457 0062 #9E SET&2
460 0000 0
461 0064 SET&4
462 0764 9U
463 1020 LDA&
464 0336 336
465 4470 STC9G
466 2656 #9F ADD9Y+3
467 1160 ADM&
470 0000 #9G 0
471 0061 SET&1
472 0070 70
473 1322 #9H LDH&2
474 1420 SHD&
475 1300 1300
476 1324 LDH&4
477 1420 SHD&
500 5600 5600
501 6466 JMP9F
502 1420 SHD&
503 5700 5700
504 6520 JMP9J
505 0241 ROL 1
506 1120 ADA&
507 0627 9X
510 4003 STC3
511 2522 ADD9J+2
512 2001 ADD1
513 4001 STC1
514 2470 ADD9G
515 1743 DSC 3
516 1763 DSC&3
517 6473 JMP9H
520 1322 #9J LDH&2
521 1420 SHD&
522 6004 6004
523 6000 #9K JMP
524 0415 KST
525 6457 JMP9E
526 0226 XSK&6

```



```

527 CONT
530 6542 JMP9N
531 0415 #9M KST
531 6530 JMP' =1
532 0063 SET&3
533 7577 =200
534 0225 XSK&5
535 6534 JMP' =1
536 0223 XSK&3
537 6534 JMP' =3
540 0515 KBD
541 6431 JMP9B
542 0515 #9N KBD
543 1420 SHD&
544 1300 1300
545 6431 JMP9B
546 1420 SHD&
547 2300 2300
550 6523 JMP9K
551 1420 SHD&
552 1200 1200
553 6617 JMP9V
554 0064 SFT&4
555 0200 #9Q 0
556 0204 XSK 4
557 6562 JMP9R
560 1365 STH&5
561 6457 JMP9E
562 4573 #9R STC9S
563 0043 SET 3
564 0523 9K
565 0223 XSK&3
566 1322 LDH&2
567 1420 SHD&
570 7700 7700
571 6530 JMP9M
572 1460 SAE&
573 0000 #9S 0
574 6610 JMP9T
575 1020 LDA&
576 0016 16
577 1365 STH&5
600 1000 LDA
601 0613 9T+3
602 2763 ADD9U=1
603 4763 STC9U=1
604 2003 ADD3
605 0224 XSK&4
606 4626 STC9W
607 6452 JMP9E=5
610 0223 #9T XSK&3
611 1325 LDH&5
612 1020 LDA&
613 0000 0
614 0241 ROL 1
615 4613 STC' =2
616 6566 JMP9R+4

```

CEOL

```

      CONT
617 1302 #9V LDH 2
620 1460 SAE&
621 0077 77
622 6625 JMP9W=1
623 0226 XSK&6
624 6530 JMP9M
625 0011 CLR
626 6000 #9W JMP
      [CODE TABLE
627 4136 #9X 4136
630 3641 3641
631 2101 2101
632 0177 0177
633 4523 4523
634 2151 2151
635 4122 4122
636 2651 2651
637 2414 2414
640 0477 0477
641 5172 5172
642 0651 0651
643 1506 1506
644 4225 4225
645 4443 4443
646 6050 6050
647 5126 5126
650 2651 2651
651 5120 5120
652 3651 3651
653 0001 #9Y 1
654 7774 *3
655 7775 *2
656 7661 =116
657 0000 0000
660 0000 0000
661 0100 0100 [PERIOD
662 0000 0000
663 7736 7736 [STAR
664 3677 3677
665 0404 0404 [DASH
666 0404 0404
667 0404 0404 [PLUS
670 0437 0437
671 0403 0403 [SLASH
672 6010 6010
673 4177 4177 [BRACKET OPEN
674 0000 0000
675 1212 1212 [= SIGN
676 1212 1212
677 4477 4477 [A
700 7744 7744
701 5177 5177
702 2651 2651
703 4136 4136
704 2241 2241
705 4177 4177
706 3641 3641

```

CONT		
707	4577	4577
710	4145	4145
711	4477	4477
712	4044	4044
713	4136	4136
714	2645	2645
715	1077	1077
716	7710	7710
717	7741	7741
720	0041	0041
721	4142	4142
722	4076	4076
723	1077	1077
724	4324	4324
725	0177	0177
726	0301	0301
727	3077	3077
730	7730	7730
731	3077	3077
732	7706	7706
733	4177	4177
734	7741	7741
735	4477	4477
736	3044	3044
737	4276	4276
740	0376	0376
741	4477	4477
742	3146	3146
743	5121	5121
744	4651	4651
745	4040	4040
746	4077	4077
747	0177	0177
750	7701	7701
751	0176	0176
752	7402	7402
753	0677	0677
754	7701	7701
755	1463	1463
756	6314	6314
757	0770	0770
760	7007	7007
761	4543	4543
762	6151	6151
		\$763
763	0000	0
764	0000	#9U 0
		[CHARTBL
		[LINC SET
		[FOR CALCHAR
		[CODE LOOKUP NUMBERS
		\$1000
1000	1100	2A
1001	1112	2B
1002	1120	2C
1003	1130	2D
1004	1145	2E

CONT		
1005	1153	2F
1006	1167	2G
1007	1203	2H
1010	1212	2I
1011	1234	2J
[SPECIAL		
1012	1572	2K
1013	1573	2L
1014	1574	2M
1015	1575	2N
1016	1610	2O
1017	1625	2P
1020	1631	2Q
1021	1637	2R
1022	1641	2S
1023	1652	2T
[ALPHABET		
1024	1245	1A
1025	1255	1B
1026	1271	1C
1027	1304	1D
1030	1313	1E
1031	1323	1F
1032	1331	1G
1033	1346	1H
1034	1356	1I
1035	1366	1J
1036	1377	1K
1037	1405	1L
1040	1411	1M
1041	1416	1N
1042	1427	1O
1043	1434	1P
1044	1444	1Q
1045	1460	1R
1046	1471	1S
1047	1507	1T
1050	1515	1U
1051	1523	1V
1052	1532	1W
1053	1541	1X
1054	1552	1Y
1055	1563	1Z
[CASE SPECIAL		
1056	1653	2U
1057	1660	2V
1060	1671	2W
1061	1677	2X
1062	1705	2Y
1063	1720	2Z
1064	1726	3A
1065	1727	4B
1066	1732	4C
1067	1740	4D
1070	1741	4E
1071	1742	4F
1072	1743	4G

	CONT	
1073	1744	4H
1074	1745	4I
1075	1746	4J
1076	1747	4K
1077	1750	4L

EMOTION CODES
[NUMBERS

	[0	
1100	0601	#2A 0601
1101	4301	4301
1102	0404	0404
1103	0501	0501
1104	0602	0602
1105	0701	0701
1106	0004	0004
1107	0101	0101
1110	0202	0202
1111	6605	6605

	[1	
1112	0601	#2B 0601
1113	4602	4602
1114	0201	0201
1115	0406	0406
1116	0101	0101
1117	6705	6705

	[2	
1120	0405	#2C 0405
1121	4501	4501
1122	0602	0602
1123	0701	0701
1124	0001	0001
1125	0104	0104
1126	0604	0604
1127	6602	6602

	[3	
1130	0405	#2D 0405
1131	4501	4501
1132	0602	0602
1133	0701	0701
1134	0001	0001
1135	0101	0101
1136	0701	0701
1137	0001	0001
1140	0101	0101
1141	0202	0202
1142	0301	0301
1143	4701	4701
1144	2605	2605

	[4	
1145	0503	#2E 0503
1146	0601	0601
1147	4204	4204
1150	0503	0503
1151	0006	0006
1152	6603	6603

	[5	
1153	0401	#2F 0401

	CONT	
1154	4701	4701
1155	0602	0602
1156	0501	0501
1157	0402	0402
1160	0301	0301
1161	0202	0202
1162	0101	0101
1163	0403	0403
1164	0604	0604
1165	4702	4702
1166	2004	2004

	[6 #2G	
1167	0501	0501
1170	0402	0402
1171	4602	4602
1172	0701	0701
1173	0001	0001
1174	0101	0101
1175	0202	0202
1176	0301	0301
1177	0401	0401
1200	0504	0504
1201	4702	4702
1202	2004	2004

	[7 #2H	
1203	0601	0601
1204	4402	4402
1205	0501	0501
1206	0401	0401
1207	0502	0502
1210	0204	0204
1211	6706	6706

	[8 #2I	
1212	0503	0503
1213	4701	4701
1214	0001	0001
1215	0101	0101
1216	0202	0202
1217	0301	0301
1220	0401	0401
1221	0501	0501
1222	0602	0602
1223	0501	0501
1224	0401	0401
1225	0301	0301
1226	0202	0202
1227	0101	0101
1230	0001	0001
1231	0701	0701
1232	4703	4703
1233	2602	2602

	[9 #2J	
1234	4504	4504
1235	0401	0401
1236	0301	0301
1237	0202	0202
1240	0101	0101

	CONT	
1241	0001	0001
1242	0701	0701
1243	0602	0602
1244	6703	6703
	[ALPHABET	
	[A	
1245	4404	#1A 4404
1246	0502	0502
1247	0702	0702
1250	0004	0004
1251	4302	4302
1252	0202	0202
1253	4604	4604
1254	6702	6702
	[B	
1255	0403	#1B 0403
1256	4603	4603
1257	0701	0701
1260	0001	0001
1261	0101	0101
1262	0203	0203
1263	0406	0406
1264	0603	0603
1265	0701	0701
1266	0001	0001
1267	0101	0101
1270	6703	6703
	[C	
1271	0603	#1C 0603
1272	0501	0501
1273	4101	4101
1274	0202	0202
1275	0301	0301
1276	0404	0404
1277	0501	0501
1300	0602	0602
1301	0701	0701
1302	4702	4702
1303	2003	2003
	[D	
1304	4406	#1D 4406
1305	0603	0603
1306	0701	0701
1307	0004	0004
1310	0101	0101
1311	0203	0203
1312	6606	6606
	[E	
1313	4406	#1E 4406
1314	0604	0604
1315	4103	4103
1316	0201	0201
1317	4603	4603
1320	4103	4103
1321	4604	4604
1322	6602	6602
	[F	

CONT			
1323	4406	#1F	4406
1324	0604		0604
1325	4103		4103
1326	0201		0201
1327	4603		4603
1330	6703		6703
[G			
1331	0501	#1G	0501
1332	0402		0402
1333	4603		4603
1334	0002		0002
1335	0101		0101
1336	0202		0202
1337	0301		0301
1340	0404		0404
1341	0501		0501
1342	0602		0602
1343	0701		0701
1344	4702		4702
1345	2003		2003
[H			
1346	4406	#1H	4406
1347	4604		4604
1350	4006		4006
1351	4303		4303
1352	0201		0201
1353	4604		4604
1354	4702		4702
1355	2001		2001
[I			
1356	0601	#1I	0601
1357	4602		4602
1360	4201		4201
1361	4406		4406
1362	4201		4201
1363	4602		4602
1364	4703		4703
1365	2003		2003
[J			
1366	0401	#1J	0401
1367	4701		4701
1370	0601		0601
1371	0501		0501
1372	0405		0405
1373	4201		4201
1374	4602		4602
1375	4702		4702
1376	2004		2004
[K			
1377	4406	#1K	4406
1400	4604		4604
1401	4104		4104
1402	4501		4501
1403	4703		4703
1404	6602		6602
[L			
1405	0406	#1L	0406

	CONT	
1406	4006	4006
1407	0604	0604
1410	6602	6602
	[M	
1411	4406 #1M	4406
1412	0702	0702
1413	0502	0502
1414	0006	0006
1415	6602	6602
	[N	
1416	4406 #1N	4406
1417	0701	0701
1420	0001	0001
1421	0702	0702
1422	0001	0001
1423	0701	0701
1424	0406	0406
1425	4702	4702
1426	2004	2004
	[O	
1427	4406 #1O	4406
1430	0604	0604
1431	0006	0006
1432	0204	0204
1433	6606	6606
	[P	
1434	4406 #1P	4406
1435	0603	0603
1436	0701	0701
1437	0001	0001
1440	0101	0101
1441	0203	0203
1442	4703	4703
1443	2603	2603
	[Q	
1444	0401 #1Q	0401
1445	4701	4701
1446	0602	0602
1447	0501	0501
1450	0404	0404
1451	0301	0301
1452	0202	0202
1453	0101	0101
1454	0004	0004
1455	4603	4603
1456	4701	4701
1457	6602	6602
	[R	
1460	4406 #1R	4406
1461	0603	0603
1462	0701	0701
1463	0002	0002
1464	0101	0101
1465	0203	0203
1466	4602	4602
1467	4702	4702
1470	6602	6602

CONT

		CS	
1471	0401	#1S	0401
1472	4701		4701
1473	0602		0602
1474	0501		0501
1475	0401		0401
1476	0301		0301
1477	0202		0202
1500	0301		0301
1501	0401		0401
1502	0501		0501
1503	0602		0602
1504	0701		0701
1505	4702		4702
1506	2003		2003
		CT	
1507	0602	#1T	0602
1510	4406		4406
1511	4202		4202
1512	4604		4604
1513	4702		4702
1514	2004		2004
		CU	
1515	0504	#1U	0504
1516	0402		0402
1517	4006		4006
1520	0204		0204
1521	0406		0406
1522	6706		6706
		CV	
1523	0504	#1V	0504
1524	0402		0402
1525	4004		4004
1526	0102		0102
1527	0302		0302
1530	0404		0404
1531	6706		6706
		CW	
1532	0504	#1W	0504
1533	0402		0402
1534	4006		4006
1535	0302		0302
1536	0102		0102
1537	0406		0406
1540	6706		6706
		CX	
1541	0604	#1X	0604
1542	4401		4401
1543	0304		0304
1544	0401		0401
1545	4604		4604
1546	4001		4001
1547	0104		0104
1550	0001		0001
1551	6606		6606
		CY	
1552	0406	#1Y	0406

CONT		
1553	4001	4001
1554	0702	0702
1555	0502	0502
1556	0401	0401
1557	4102	4102
1560	0001	0001
1561	4003	4003
1562	6604	6604
[Z		
1563	0406	#1Z 0406
1564	4604	4604
1565	0001	0001
1566	0104	0104
1567	0001	0001
1570	0604	0604
1571	6602	6602
[SPECIAL		
[EOL		
1572	2000	#2K 2000
[DELETE=BACKSPACE		
1573	2206	#2L 2206
[SPACE		
1574	2606	#2M 2606
[&		
1575	0602	#2N 0602
1576	0501	0501
1577	4101	4101
1600	0301	0301
1601	0402	0402
1602	4501	4501
1603	4201	4201
1604	0401	0401
1605	0601	0601
1606	0001	0001
1607	6704	6704
['		
1610	0604	#2O 0604
1611	4201	4201
1612	0301	0301
1613	0401	0401
1614	0501	0501
1615	0601	0601
1616	0701	0701
1617	0001	0001
1620	0101	0101
1621	4102	4102
1622	4405	4405
1623	4602	4602
1624	2703	2703
[-		
1625	0403	#2P 0403
1626	4604	4604
1627	4702	4702
1630	2001	2001
[+		
1631	0403	#2Q 0403
1632	4604	4604

CONT		
1633	4302	4302
1634	4004	4004
1635	4701	4701
1636	2603	2603
[/		
1637	4406	#2R 4406
1640	6706	6706
[#		
1641	0404	#2S 0404
1642	4604	4604
1643	4002	4002
1644	4204	4204
1645	4503	4503
1646	4004	4004
1647	4202	4202
1650	4404	4404
1651	6705	6705
[CASE		
1652	2000	#2T 2000
[CASE SPECIAL		
[=		
1653	0504	#2U 0504
1654	4204	4204
1655	4002	4002
1656	4604	4604
1657	6702	6702
[%		
1660	0403	#2V 0403
1661	4002	4002
1662	0701	0701
1663	0601	0601
1664	0501	0501
1665	0402	0402
1666	4002	4002
1667	4701	4701
1670	6602	6602
[,		
1671	0701	#2W 0701
1672	4502	4502
1673	0301	0301
1674	0101	0101
1675	0701	0701
1676	6604	6604
[.		
1677	0602	#2X 0602
1700	4501	4501
1701	0301	0301
1702	0101	0101
1703	0701	0701
1704	6604	6604
[\$		
1705	0403	#2Y 0403
1706	4401	4401
1707	0502	0502
1710	0702	0702
1711	0002	0002
1712	0102	0102

	CONT	
1713	0302	0302
1714	0401	0401
1715	0604	0604
1716	4702	4702
1717	2001	2001
	[
1720	0503	#2Z 0503
1721	0403	0403
1722	4202	4202
1723	0006	0006
1724	0602	0602
1725	4603	4603
	[CASE=CASE	
1726	2000	#3A 2000
	[UNDERLINE	
1727	0101	#4B 0101
1730	4606	4606
1731	6501	6501
	[RIGHT BRACKET	
1732	0601	#4C 0601
1733	4602	4602
1734	0406	0406
1735	0202	0202
1736	4705	4705
1737	2001	2001
	[UP HALF	
1740	2403	#4D 2403
	[DOWN HALF	
1741	2003	#4E 2003
	[NOT USED	
1742	2000	#4F 2000
1743	2000	#4G 2000
1744	2000	#4H 2000
1745	2000	#4I 2000
1746	2000	#4J 2000
1747	2000	#4K 2000
1750	2000	#4L 2000
	[COPY #3	

	VALUE	LINE		VALUE	LINE
1F	0261	250	6I	0157	144
1G	0305	274	6J	0177	164
1H	0340	327	6K	0210	175
1I	0366	355	6L	0221	206
1J	1612	1626	6Y	0770	773
1K	1643	1657	6Z	0771	774
1L	1551	1564	7C	0400	376
1M	1561	1574	7D	0747	752
1N	1571	1604	7I	0463	464
1T	1600	1614	7M	0612	614
2A	0233	221	7R	0754	757
2B	0236	224	7T	0562	563
2C	0241	227	7U	0741	744
2D	0245	233	7X	0737	741
2E	0251	237	7Y	0740	742
2F	0255	243	8A	0571	572
2G	1112	1122	8B	0574	575
2H	1115	1125	8C	1074	1103
2I	1120	1130	8D	1013	1022
2J	1124	1134	8E	1016	1025
2K	1142	1152	8F	1175	1206
2L	1160	1170	8G	1311	1323
2T	1604	1620	8H	1037	1046
3B	0635	637	8I	1056	1065
3C	0650	652	8J	1203	1214
3D	0667	671	8K	1205	1216
3E	0657	661	8L	1221	1232
3F	0706	710	9A	1230	1241
3G	0715	717	9B	1233	1244
3H	0701	703	9C	1340	1352
3I	0722	724	9D	1237	1250
3J	0602	603	9E	1355	1367
3K	0437	435	9F	1377	1411
3L	0450	447	9G	1610	1624
3M	0467	470	9H	1611	1625
3N	0600	601	9I	1606	1622
3O	0601	602	9J	1607	1623
3P	0736	740	9K	1425	1437
3Q	0735	737	9L	1372	1404
3R	0454	453	9M	1430	1443
3S	0570	571	9N	1453	1466
3T	3000	1703	9O	1457	1472
3U	0411	407	9P	1464	1477
3V	0576	577	9Q	1531	1544
3W	0577	600	9R	1541	1554
3X	0733	735	9S	1577	1612
3Y	0734	736	9T	1267	1300
3Z	0416	414	9Y	1700	1701
4A	0064	47	9Z	1701	1702
5A	0103	66			
5B	0111	74			
6A	0042	24			
6E	0045	27			
6C	0051	33			
6D	0055	37			
6E	0061	43			
6F	0120	104			
6G	0134	120			
6H	0142	126			

```

CONT
20 0642    UMB2
21 1020    LDA&
22 7774    7774
23 4413    STC3U+2
24 4737    STC7X [MAKE PRESENT PEN POSITION
25 4740    STC7Y [THE ORIGIN
26 1020    LDA&
27 6000    *1777
30 4601    STC30
31 4600    STC3N
32 6741    JMP7U [PEN UP
33 1000    LDA
34 0770    6Y
35 0450    AZE
36 6233    JMP2A
      [PLOT LABELS FOR HUMAN DATA
37 1500    SRO [CHECK CODE WORD
40 0771    6Z [PASSED FROM FINAL DISPLAY ROUTINE
41 6051    JMP6C [DRAW AXIS FOR CARDIAC OUTPUT
42 1500    #6A SRO
43 0771    6Z
44 6055    JMP6D [DRAW AXIS FOR PULSE RATE
45 1500    #6B SRO
46 0771    6Z
47 6061    JMP6E [DRAW AXIS FOR STROKE VOLUME
50 6064    JMP4A [DRAW X AXIS
51 0065    #6C SET&5
52 4260    1F=1+4000
53 6120    JMP6F
54 6042    JMP6A
55 0065    #6D SET&5
56 4304    1G=1+4000
57 6120    JMP6F
60 6045    JMP6B
61 0065    #6E SET&5
62 4337    1H=1+4000
63 6120    JMP6F
      [DRAW X AXIS AND LABEL IT
64 6747    #4A JMP7D [PEN DOWN
65 1020    LDA&
66 1776    1776 [FILLED WITH LENGTH OF X AXIS
67 4733    STC3X
70 6612    JMP7M [DRAW X AXIS
71 6741    JMP7U [PEN UP
72 1020    LDA&
73 0062    6Z
74 4734    STC3Y
75 1020    LDA&
76 0454    454
77 4733    STC3X
100 6612    JMP7M [PREPARE TO WRITE LABEL
101 0065    SET&5
102 4365    1I=1+4000
103 1325    #5A LDH&5 [LOAD A WITH CHARACTER
104 1420    SHD&
105 7700    7700 [SEE IF END OF CHARACTER STRING
106 6111    JMP5B [JUMP IF YES

```

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CONT
107 6400      JMP7C [OTHERWISE PLOT CHARACTER
110 6103      JMP5A
111 1020 #5B LDA& [SET PEN AT [0,1]
112 0144      144
113 4734      STC3Y
114 4733      STC3X
115 6612      JMP7M
116 0640      UMB0
117 7000      JMP1000 [JUMP TO PLOT CURVES
          CDRAW Y AXES AND LABEL THEM
120 0046 #6F SET6
121 0000      0
122 1020      LDA&
123 0620      620
124 4734      STC3Y
125 1020      LDA&
126 0144      144
127 4733      STC3X
130 6612      JMP7M [MOVE TO [1,4]
131 1020      LDA&
132 0006      6 [CHARACTER ORIENTATION +Y
133 4422      STC3Z+4
134 1325 #6G LDH&5 [LOAD A WITH CHARACTER
135 1420      SHD&
136 7700      7700
137 6142      JMP6H [JUMP IF END OF STRING
140 6400      JMP7C [PLOT CHARACTER
141 6134      JMP6G
142 1020 #6H LDA&
143 0144      144
144 4734      STC3Y
145 1020      LDA&
146 0310      310
147 4733      STC3X
150 6612      JMP7M [MOVE TO [2,1]
151 6747      JMP7D [PEN DOWN
152 1020      LDA&
153 1750      1750
154 4734      STC3Y
155 4422      STC3Z+4 [CHARACTER ORIENTATION +X
156 6612      JMP7M [DRAW LINE TO [2,10]
          CLABEL Y AXIS
157 1020 #6I LDA&
160 0274      274
161 4733      STC3X
162 6612      JMP7M [DRAW .12 INCH LINE
163 6741      JMP7U [PEN UP
164 1020      LDA&
165 0206      206
166 4733      STC3X
167 6612      JMP7M [LEAVE SPACE FOR NUMBER
170 0415      KST
171 6177      JMP6J
172 0515      KBD
173 1460      SAE&
174 0012      0012
175 6177      JMP6J

```



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CONT
176 7034 JMP8H=3
177 1325 #6J LDH&5
200 1420 SHD&
201 1200 1200
202 6221 JMP6L
203 1420 SHD&
204 7700 7700
205 6210 JMP6K
206 6400 JMP7C [PLOT NUMBER
207 6177 JMP6J
210 1020 #6K LDA&
211 0310 310
212 4733 STC3X
213 6612 JMP7M
214 1020 LDA& [REDEFINE X AND Y
215 0144 144 [TO BE [0,1]
216 4740 STC7Y
217 4737 STC7X
220 6006 JMP6
221 1020 #6L LDA&
222 0310 310
223 4733 STC3X
224 1020 LDA&
225 7633 7633
226 1140 ADM
227 0734 3Y
230 6612 JMP7M [PREPARE TO PLOT NEXT NUMBER
231 6747 JMP7D [PEN DOWN
232 6157 JMP6I
[PLOT LABELS FOR DOG DATA
233 1500 #2A SRO [CHECK CODE WORD
234 0771 6Z [PASSED FROM FINAL DISPLAY ROUTINE
235 6245 JMP2D [DRAW AXIS FOR CARDIAC OUTPUT
236 1500 #2B SRO
237 0771 6Z
240 6251 JMP2E [DRAW AXIS FOR PULSE RATE
241 1500 #2C SRO
242 0771 6Z
243 6255 JMP2F [DRAW AXIS FOR STROKE VOLUME
244 6064 JMP4A [DRAW X AXIS
245 0065 #2D SET&5
246 5611 1J=1+4000
247 6120 JMP6F
250 6236 JMP2B
251 0065 #2E SET&5
252 4304 1G=1+4000
253 6120 JMP6F
254 6241 JMP2C
255 0065 #2F SET&5
256 5642 1K=1+4000
257 6120 JMP6F
260 6064 JMP4A
[TABLE OF CODES FOR LABELING AXES
261 3714 #1F 3714
262 4330 4330 [L PER MIN
263 4514 4514 [LABEL AXIS 2-20 FOR HUMAN DATA
264 4034 4034

```

CONT		
265	4177	4177
266	0200	0200
267	1201	1201
270	1012	1012
271	0106	0106
272	1201	1201
273	0412	0412
274	0102	0102
275	1201	1201
276	0012	0012
277	1410	1410
300	1214	1214
301	0612	0612
302	1404	1404
303	1214	1214
304	0277	0277
305	2530	2530
306	2447	2447
307	4614	4614
310	4330	4330
311	4514	4514
312	4034	4034
313	4177	4177
314	0202	0202
315	0012	0012
316	0200	0200
317	0012	0012
320	0110	0110
321	0012	0012
322	0106	0106
323	0012	0012
324	0104	0104
325	0012	0012
326	0102	0102
327	0012	0012
330	0100	0100
331	0012	0012
332	1410	1410
333	0012	0012
334	1406	1406
335	0012	0012
336	1404	1404
337	0077	0077
340	2626	2626
341	7702	7702
342	0000	0000
343	1201	1201
344	1000	1000
345	1201	1201
346	0600	0600
347	1201	1201
350	0400	0400
351	1201	1201
352	0200	0200
353	1201	1201
354	0000	0000
355	1214	1214

#1G [BEATS PER MIN
[LABEL AXIS 40=220 FOR HUMAN AND DOG DATA

#1H [CC
[LABEL AXIS 20=200 FOR HUMAN DATA

```

CONT
356 1000      1000
357 1214      1214
360 0600      0600
361 1214      1214
362 0400      0400
363 1214      1214
364 0200      0200
365 7777      7777
366 4742 #1I 4742 [TOTAL TIME
367 4724      4724
370 3714      3714
371 4734      4734
372 4030      4030
373 1400      1400
374 0061      0061
375 0014      0014
376 4034      4034
377 4177      4177

[LOCAL COMP PLOT
[MODIFIED FOR LINC 300
[F T DAVIDSON 5 OCT 67
[CHARACTER PLOT
[OPEN MUST BE IN THE
[CUP POSITION
$400
400 1120 #7C ADA &
401 3000      3T
402 4017      STC 17
403 2000      ADD 0
404 4454      STC 3R
405 1017      LDA 17
406 1120      ADA&
407 2000      2000
410 4017      STC 17
411 1017 #3U LDA 17
412 0075      SET & 15
413 7776      =1 [MAGNIFICATION
414 0451      APO
415 6754      JMP 7R
416 1317 #3Z LDH 17
417 1560      BCL &
420 7770      7770
421 1120      ADA &
422 0000      0 [ORIENTATION
423 1560      BCL &
424 7770      7770
425 1120      ADA &
426 0602      3J
427 4016      STC 16
430 1016      LDA 16
431 4442      STC 3K+3
432 1337      LDH & 17
433 0470      AZE &
434 6450      JMP 3L
435 0017      COM
436 4440      STC 3K+1
437 0076 #3K SET & 16

```

```

CONT
440 0000      0 MINUS THE NO. OF INCREMENTS IN THIS DIRECTION
441 1020      LDA &
442 0000      0 EMOTION WORD
443 6463      JMP 7I
444 0236      XSK & 16
445 6441      JMP *-4
446 0235      XSK & 15
447 6437      JMP 3K
      CTEST FOR END
450 1017      #3L LDA 17
451 1560      BCL &
452 5777      5777
453 0450      AZE
454 0000      #3R RETURN
      CSTEP LINE OF CHAR=TABLE=ALLOWS OVERLAP INTO UPPER MEM
      ORY
455 1020      LDA &
456 4000      =3777
457 1140      ADM
460 0017      17
461 1017      LDA 17
462 6411      JMP 3U
      CINCREMENT PLOTTER AND X*Y SR
463 4467      #7I STC 3M
464 2000      ADD 0
465 4570      STC 3S
466 1520      SRO & CTEST FOR =Y
467 0000      #3M CKEY WORD
470 6511      JMP *-21
471 2740      ADD 7Y CTEST FOR POINTS LESS THAN OR EQUAL LOWER B
      OUND
472 2600      ADD 3N
473 0451      APO
474 6505      JMP *-11
475 0011      CLR CTEST FOR POINTS GREATER THAN UPPER BOUND
476 2740      ADD 7Y
477 2601      ADD 3O
500 0471      APO &
501 6505      JMP *-4
502 1020      LDA & CARRIAGE RIGHT
503 0004      4
504 6571      JMP 8A
505 0011      CLR
506 2740      ADD 7Y CDECREASE POINT INDICATOR IN 7Y
507 2576      ADD 3V
510 4740      STC 7Y
511 1500      SRO CTEST FOR +Y
512 0467      3M
513 6536      JMP *-23
514 2740      ADD 7Y CTEST FOR POINTS GREATER THAN OR EQUAL LOWE
      R BOUND
515 2601      ADD 3O
516 2577      ADD 3W
517 0471      APO &
520 6532      JMP *-12
521 0011      CLR CTEST FOR POINTS LESS THAN LOWER BOUND
522 2740      ADD 7Y

```

```

CONT
523 2600 ADD 3N
524 2577 ADD 3W
525 0451 APO
526 6532 JMP '+4
527 1020 LDA & [CARRIAGE LEFT
530 0010 10
531 6571 JMP 8A
532 0011 CLR
533 2740 ADD 7Y [INCREASE POINT INDICATOR IN 7Y
534 2577 ADD 3W
535 4740 STC 7Y
536 1500 SRO [TEST FOR +X
537 0467 3M
540 6550 JMP '+10
541 1020 LDA & [DRUM DOWN
542 0002 2
543 6571 JMP 8A
544 1000 LDA
545 0737 7X
546 2577 ADD 3W
547 4737 STC 7X
550 1500 SRO [TEST FOR =X
551 0467 3M
552 6562 JMP '+10
553 1020 LDA & [DRUM UP
554 0001 1
555 6571 JMP 8A
556 1000 LDA
557 0737 7X
560 2576 ADD 3V
561 4737 STC 7X
562 1000 #7T LDA
563 0574 8B
564 0546 OPR 46
565 6564 JMP '=1
566 0011 CLR
567 4574 STC 8B
570 1440 #3S S RETURN
571 1600 #8A BSE
572 0574 8B
573 1060 STA &
574 0000 #8B 0
575 6000 JMP 0
576 7776 #3V =1
577 0001 #3W +1
600 1777 #3N 1777 [Y=LOWER BOUND NOTE SIGN
601 6000 #30 =1777 [Y=UPPER BOUND NOTE SIGN
602 7776 #3J =1 [=Y
603 7766 =11 [=X,-Y
604 7767 =10 [=X
605 7765 =12 [=X,+Y
606 7775 =2 [+Y
607 7771 =6 [+X,+Y
610 7773 =4 [+X
611 7772 =5 [+X,-Y
    [INTERPOLATED MOTION
612 0076 #7M SET & 16

```

```

CONT
613 7767      =10
614 0075      SET & 15
615 7776      =1
616 1000      LDA
617 0734      3Y
620 2735      ADD 3Q
621 4736      STC 3P
622 2000      ADD 0
623 4454      STC 3R
624 2733      ADD 3X
625 0017      COM
626 2737      ADD 7X
627 0471      APO &
630 6634      JMP '+4
631 0076      SET & 16
632 7773      =4
633 0017      COM
634 1060      STA &
635 0000 #3B C/DELX/
636 0011      CLR
637 2736      ADD 3P
640 0017      COM
641 2740      ADD 7Y
642 0471      APO &
643 6647      JMP '+4
644 0075      SET & 15
645 7775      =2
646 0017      COM
647 1060      STA &
650 0000 #3C C/DELY/
651 0077      SET & 17
652 3777      =4000
653 1600      BSE
654 0635      3B
655 0470      AZE &
656 6454      JMP 3R
657 4667 #3E STC 3D
660 2635      ADD 3B
661 0241      ROL 1
662 4635      STC 3B
663 2650      ADD 3C
664 0241      ROL 1
665 4650      STC 3C
666 1020      LDA &
667 0000 #3D CRESULT OF BSE
670 0241      ROL 1
671 0451      APO
672 6676      JMP '+4
673 1500      SRO
674 0017      17
675 6657      JMP 3E
676 0011      CLR
677 4706      STC 3F
700 4715      STC 3G
701 0011 #3H CLR
702 2016      ADD 16
703 4722      STC 3I

```

```

CONT
704 2635      ADD 3B
705 1220      LAM &
706 0000 #3F   STC 0
707 4000      LZE &
710 0472      STC 3I
711 4722      CLR
712 0011      ADD 3C
713 2650      LAM &
714 1220      #3G
715 0000      STC 0
716 4000      LZE
717 0452      ADD 15
720 2015      ADA &
721 1120      #3I
722 0000      AZE
723 0450      JMP 7I
724 6463      ADD 3W [+1
725 2577      ADM
726 1140      17
727 0017      AZE
730 0450      JMP 3H
731 6701      JMP 3R
732 6454      #3X 0000 [DESIRED X
733 0000 #3Y 0000 [DESIRED Y
734 0000 #3Q 0000 [Y=SHIFT
735 0000 #3P 0000 [3Y+3Q
736 0000 #7X 0000 [CURRENT X
737 0000 #7Y 0000 [CURRENT Y
740 0000      CPEN SUBROUTINES
741 0056 #7U SET 16 CPEN UP
742 0000      0
743 1020      LDA &
744 0040      40
745 4757      STC 7R+3
746 6756      JMP 7R+2
747 0056 #7D SET 16 CPEN DOWN
750 0000      0
751 1020      LDA &
752 0020      20
753 6745      JMP 7D=2
754 0056 #7R SET 16 CPEN REVERSE
755 0000      0
756 1020      LDA &
757 0020      20
760 1660      BCO &
761 0060      60
762 1040      STA
763 0757      7R+3
764 0546      OPR 46
765 6764      JMP *-1
766 6016      JMP 16
770 0000 #6Y 0 [FLAG = EQUALS 1 IF DOG EXP., 0 IF HUMAN DATA
771 0000 #6Z 0 [CODE INDICATING WHICH CURVE TO PLOT
      [7=ALL THREE
      [6=PR+SV

```

CONT

```

[5=CO+SV
[4=SV
[3=CO+PR
[2=PR
[1=CO
[ROUTINE TO PLOT DESIRED CURVES
    $1000
1000 1000    LDA
1001 0771    6Z
1002 0243    ROL3
1003 4771    STC6Z
1004 1000    LDA
1005 0770    6Y
1006 0450    AZE
1007 7112    JMP2G
[PLOT HUMAN DATA
1010 1500    SRO [CHECK CODE WORD TO SEE
1011 0771    6Z [WHICH CURVES] TO PLOT
1012 7037    JMP8H [PLOT CARDIAC OUTPUT
1013 1500    #8D SRO
1014 0771    6Z
1015 7056    JMP8I [PLOT PULSE RATE
1016 1500    #8E SRO
1017 0771    6Z
1020 7074    JMP8C [PLOT STROKE VOLUME
1021 1000    LDA [COME HERE WHEN FINISHED PLOTTING
1022 0066    4A+2
1023 4733    STC3X
1024 4734    STC3Y
1025 6612    JMP7M
1026 0011    CLR
1027 4737    STC7X
1030 1020    LDA&
1031 0454    454
1032 4733    STC3X
1033 6612    JMP7M [POSITION PEN FOR NEXT GRAPH
1034 0641    UMB1
1035 0600    LMB0
1036 6433    JMP433 [JUMP BACK TO PAGE 0 AND DISPLAY ROUTINE
1037 0770    #8H 770 [READ VALUES FOR CARDIAC OUTPUT
1040 6270    6/270
1041 0750    750
1042 7271    7/271
1043 0000    HLT
1044 1020    LDA&
1045 7467    7467
1046 5233    STC9B
1047 1020    LDA&
1050 0053    53 [X
1051 5340    STC9C
1052 1020    LDA&
1053 5607    9J+4000
1054 7175    JMP8F [PLOT CARDIAC OUTPUT
1055 7013    JMP8D [SEE IF MORE CURVES TO PLOT
1056 0751    #8I 751 [READ IN PULSE RATE DATA
1057 1276    1/276
1060 1020    LDA&

```



```

CONT
1061 7727      7727
1062 5233      STC9B
1063 1020      LDA&
1064 0062      62 [X
1065 5340      STC9C
1066 6612      JMP7M [RETURN TO [0,1]
1067 0000      HLT
1070 1020      LDA&
1071 1606      9I
1072 7175      JMP8F [PLOT PULSE RATE
1073 7016      JMP8E [SEE IF ONE MORE CURVE TO PLOT
1074 0770 #8C 770 [READ IN STROKE VOLUME DATA
1075 6274      6/274
1076 0750      750
1077 7275      7/275
1100 1020      LDA&
1101 7753      7753
1102 5233      STC9B
1103 5340      STC9C [0
1104 6612      JMP7M [RETURN TO [0,1]
1105 0000      HLT
1106 1020      LDA&
1107 1606      9I
1110 7175      JMP8F [PLOT STROKE VOLUME
1111 7021      JMP8E+3 [JUMP TO RETURN TO PAGE 0
[PLOT DOG VALUES
1112 1500 #2G SR0 [EXAMINE CODE WORD TO SEE
1113 0771      6Z [WHICH CURVES TO PLOT
1114 7124      JMP2J [PLOT CARDIAC OUTPUT
1115 1500 #2H SR0
1116 0771      6Z
1117 7142      JMP2K [PLOT PULSE RATE
1120 1500 #2I SR0
1121 0771      6Z
1122 7160      JMP2L [PLOT STROKE VOLUME
1123 7021      JMP8E+3
1124 0770 #2J 770 [READ VALUES FOR CARDIAC OUTPUT
1125 6270      6/270
1126 0750      750
1127 7271      7/271
1130 0000      HLT
1131 0011      CLR
1132 5233      STC9B
1133 1020      LDA&
1134 0053      53 [X
1135 5340      STC9C
1136 1020      LDA&
1137 1610      9G
1140 7175      JMP8F [PLOT CARDIAC OUTPUT
1141 7115      JMP2H
1142 0751 #2K 751 [READ IN PULSE RATE DATA
1143 1276      1/276
1144 1020      LDA&
1145 7727      7727
1146 5233      STC9B
1147 1020      LDA&
1150 0062      62 [X

```

```

CONT
1151 5340 STC9C
1152 6612 JMP7M [RETURN TO [0,1]
1153 0000 HLT
1154 1020 LDA&
1155 1606 9I
1156 7175 JMP8F [PLOT PULSE RATE
1157 7120 JMP2I
1160 0770 #2L 770 [READ IN STROKE VOLUME DATA
1161 6274 6/274
1162 0750 750
1163 7275 7/275
1164 0011 CLR
1165 5233 STC9B
1166 5340 STC9C [0
1167 6612 JMP7M [RETURN TO [0,1]
1170 0000 HLT
1171 1020 LDA&
1172 1611 9H
1173 7175 JMP8F [PLOT STROKE VOLUME
1174 7021 JMP8E+3
[PLOT CURVE
1175 5237 #8F STC9D
1176 5577 STC9S
1177 0044 SET4
1200 0000 0
1201 0061 SET&1
1202 2777 2777
1203 0461 #8J SNS&1 [IF SENSE SWITCH 1 IS SET
1204 7355 JMP9E [JUMP TO AVERAGE 4 POINTS
1205 0043 #8K SET3
1206 1700 9Y [SET NO. OF POINTS TO PLOT
1207 0536 OPR&16 [READ RSW
1210 1560 BCL& [EXAMINE BITS 0 AND 1
1211 7774 7774
1212 1120 ADA& [CCRSW] DESERMIN E NO. OF SYMBOLS PLOTTED
1213 1600 1T
1214 1040 STA
1215 1311 8G
1216 5220 STC'+2
1217 0045 SET5
1220 0000 0
1221 1021 #8L LDA&1 [LOAD A WITH Y COORDINATE
1222 7230 JMP9A [PLOT POINT
1223 1020 LDA&
1224 0002 2
1225 1140 ADM
1226 0733 3X
1227 7221 JMP8L
1230 0050 #9A SET10
1231 0000 0
1232 1120 ADA& [MODIFY FOR PLACEMENT ON GRAPH
1233 0000 #9B 0 [VALUE FILLED IN
1234 0470 AZE&
1235 7240 JMP9D+1
1236 1240 MUL
1237 0000 #9D 0 [VALUE FILLED IN
1240 1120 ADA&

```

```

CONT
1241 0144      144
1242 1040      STA
1243 0734      3Y [STORE Y COORDINATE
1244 1120      ADA&
1245 6000      =1777
1246 0451      APO
1247 7253      JMP'+4
1250 1020      LDA&
1251 1777      1777
1252 4734      STC3Y
1253 6612      JMP7M [PLOT POINT
1254 0415      KST
1255 7263      JMP'+6
1256 0515      KBD
1257 1460      SAE&
1260 0012      0012
1261 7263      JMP'+2
1262 7034      JMP8H=3
1263 0223      XSK&3 [SKIP IF ALL VALUES PLOTTED
1264 7274      JMP'+10 [OTHERWISE CHECK IF SYMBOL TO BE PLOTTED
1265 6741      JMP7U
1266 7430      JMP9M
1267 1020      #9T LDA&
1270 0144      144
1271 4734      STC3Y
1272 4733      STC3X
1273 6004      JMP4
1274 1000      LDA
1275 0001      1
1276 1460      SAE&
1277 3000      3000
1300 7302      JMP'+2
1301 6747      JMP7D [PEN DOWN
1302 1460      SAE&
1303 3003      3003
1304 7306      JMP'+2
1305 6747      JMP7D
1306 0225      XSK&5 [SKIP IF SYMBOL REQUIRED
1307 6010      JMP10 [OTHERWISE GET NEXT POINT
      [PLOT SYMBOL
1310 0045      SET5
1311 0000      #8G 0
1312 1000      LDA [SAVE PRESENT X AND Y
1313 0737      7X
1314 5604      STC2T
1315 1000      LDA
1316 0740      7Y
1317 5605      STC2T+1
1320 1020      LDA&
1321 7775      7775
1322 4413      STC3U+2
1323 1020      LDA& [ADJUST X AND Y SO THAT SYMBOL
1324 7771      7771 [IS CENTERED
1325 1140      ADM
1326 0734      3Y
1327 1020      LDA&
1330 7773      7773

```

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CONT
1331 1040 STA
1332 1577 9S
1333 1140 ADM
1334 0733 3X
1335 6741 JMP7U [PEN UP
1336 6612 JMP7M [PREPARE TO DRAW SYMBOL
1337 1020 LDA&
1340 0000 #9C 0 [SYMBOL CODE FILLED IN
1341 0642 UMB2
1342 6400 JMP7C [PLOT SYMBOL
1343 0640 UMB0
1344 1000 LDA [RESTORE COORDINATES
1345 1604 2T
1346 4733 STC3X
1347 1000 LDA
1350 1605 2T+1
1351 4734 STC3Y
1352 6612 JMP7M
1353 6747 JMP7D [PEN DOWN
1354 6010 JMP10 [JUMP TO PLOT NEXT POINT
1355 1000 #9E LDA
1356 1701 9Z
1357 0470 AZE& [IF LESS THAN 4 VALUES, PLOT EVERY
1360 7205 JMP8K [POINT
1361 0043 SET3 [SET NO. OF POINTS TO PLOT=NO. OF VALUES
1362 1701 9Z [DIVIDED BY 4
1363 0536 OPR&16 [READ RSW
1364 1560 BCL& [CHECK TO SEE IF EITHER BIS 0 OR 1 SET
1365 7774
1366 0470 AZE& [SKIP IF SES
1367 7425 JMP9K [IF NOT SET, NO SYMBOLS PLOTTED
1370 1020 LDA& [PREPARE TO PLOT ONE SYMBOL
1371 1603 1T+3 [FOR EVERY POINT
1372 1040 #9L STA
1373 1311 8G
1374 5376 STC'+2
1375 0045 SET5
1376 0000 0
1377 1021 #9F LDA&1
1400 1121 ADA&1 [AVERAGE 4 POINTS
1401 0341 SCR1
1402 1560 BCL&
1403 4000 4000
1404 5413 STC'+7
1405 1021 LDA&1
1406 1121 ADA&1
1407 0341 SCR1
1410 1560 BCL&
1411 4000 4000
1412 1120 ADA&
1413 0000 0
1414 0341 SCR1
1415 1560 BCL&
1416 4000 4000
1417 7230 JMP9A [PLOT POINT
1420 1020 LDA&
1421 0010 10

```

```

CONT
1422 1140 ADM
1423 0733 3X
1424 7377 JMP9F
1425 1020 #9K LDA&
1426 1600 IT
1427 7372 JMP9L
      CWRITE LFGEND
1430 1020 #9M LDA&
1431 1440 1440
1432 4733 STC3X
1433 1020 LDA&
1434 7775 7775
1435 4413 STC3U+2
1436 1000 LDA
1437 1340 9C
1440 0470 AZE&
1441 7453 JMP9N [COME HERE IF STROKE VOLUME
1442 1460 SAE&
1443 0053 0053
1444 7457 JMP9O [COME HERE IF PULSE RATE
1445 1020 LDA& [COME HERE IF CARDIAC OUTPUT
1446 0050 50
1447 4734 STC3Y
1450 0065 SET&5
1451 5550 1L=1+4000
1452 7464 JMP9P
1453 4734 #9N STC3Y
1454 0065 SET&5
1455 5560 1M=1+4000
1456 7464 JMP9P
1457 1020 #9O LDA&
1460 0120 120
1461 4734 STC3Y
1462 0065 SET&5
1463 5570 1N=1+4000
1464 6612 #9P JMP7M
1465 1000 LDA
1466 1577 9S
1467 0470 AZE&
1470 7531 JMP9Q
1471 6741 JMP7U
1472 1000 LDA
1473 1340 9C
1474 0642 UMB2
1475 6400 JMP7C
1476 0640 UMB0
1477 1020 LDA&
1500 0006 6
1501 1140 ADM
1502 0734 3Y
1503 1020 LDA&
1504 0012 12
1505 1140 ADM
1506 0733 3X
1507 6612 JMP7M
1510 6747 JMP7D
1511 1020 LDA&

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CONT
1512 0032      32
1513 1140      ADM
1514 0733      3X
1515 6612      JMP7M
1516 6741      JMP7U
1517 1020      LDA&
1520 7771      7771
1521 1140      ADM
1522 0734      3Y
1523 6612      JMP7M
1524 1000      LDA
1525 1340      9C
1526 0642      UMB2
1527 6400      JMP7C
1530 7541      JMP9R
1531 6747 #9Q JMP7D
1532 1020      LDA&
1533 0062      62
1534 1140      ADM
1535 0733      3X
1536 6612      JMP7M
1537 6741      JMP7U
1540 0642      UMB2
1541 1325 #9R LDH&5
1542 1420      SHD&
1543 7700      7700
1544 7547      JMP'+3
1545 6400      JMP7C
1546 7541      JMP9R
1547 0640      UMB0
1550 7267      JMP9T
1551 1426 #1L 1426
1552 2445      2445
1553 2734      2734
1554 2426      2426
1555 1442      1442
1556 5047      5047
1557 4350      4350
1560 4777      4777
1561 1446 #1M 1446
1562 4745      4745
1563 4236      4236
1564 3014      3014
1565 5142      5142
1566 3750      3750
1567 4030      4030
1570 7777      7777
1571 1443 #1N 1443
1572 5037      5037
1573 4630      4630
1574 1445      1445
1575 2447      2447
1576 3077      3077
1577 0000 #9S 0
      CUSE RSW TO SELECT NO. OF SYMBOLS / CURVE PLOTTED
1600 6777 #1T 6777 CIF 0=NONE
1601 7677      7677 CIF 1= 8

```

```

1602 CONT
1603 7767 7767 [IF 2= 64
1604 7776 7776 [IF 3= EVERY POINT
1605 0000 #2T 0
1606 0000 #9I 5
1607 2000 #9J 2000 [1/2
1610 0002 #9G 2
1611 0024 #9H 24
1612 3714 #1J 3714 [L PER MIN
1613 4330 4330 [LABEL AXIS 0=4.5 FOR DOG VALUES
1614 4514 4514
1615 4034 4034
1616 4177 4177
1617 0461 0461
1620 0512 0512
1621 0461 0461
1622 0012 0012
1623 0361 0361
1624 0512 0512
1625 0361 0361
1626 0012 0012
1627 0261 0261
1630 0512 0512
1631 0261 0261
1632 0012 0012
1633 0161 0161
1634 0512 0512
1635 0161 0161
1636 0012 0012
1637 0061 0061
1640 0512 0512
1641 0061 0061
1642 0077 0077
1643 2626 #1K 2626 [CC
1644 7704 7704 [LABEL AXIS 0=45 FOR DOG VALUES
1645 0512 0512
1646 0400 0400
1647 1203 1203
1650 0512 0512
1651 0300 0300
1652 1202 1202
1653 0512 0512
1654 0200 0200
1655 1201 1201
1656 0512 0512
1657 0100 0100
1660 1214 1214
1661 0512 0512
1662 1400 1400
1663 7777 7777
      $1700
1700 0000 #9Y 0 [TOTAL NO. OF VALUES
1701 0000 #9Z 0 [1/4 TOTAL NO. OF VALUES
      3T=3000

```

PRINT1:0

207

	VALUE	LINE		VALUE	LINE
1T	0272	257	7I	1525	1546
1U	0307	274	7J	1531	1552
1V	0321	306	7K	1545	1566
1W	0335	322	7L	1550	1571
1X	0341	326	7M	1565	1607
2A	0642	630	7O	1576	1620
2B	0646	635	7P	1622	1644
2C	0671	661	7Q	1623	1647
2D	0712	703	7R	1646	1672
3L	0400	350	7S	1670	1714
3M	0435	405	7T	1672	1716
3N	0461	431	7U	1704	1730
3O	0502	452	7V	1706	1732
3P	0522	472	7W	1722	1746
3Q	0552	522	7X	1723	1750
4A	0557	533	7Y	1726	1754
4B	0562	537	7Z	1731	1760
4D	0565	543	8A	0052	34
4E	0570	547	8B	0060	42
4F	0573	553	8C	0066	51
4G	0576	557	9A	0125	110
4H	0601	566	9B	0115	100
4I	0611	576	9C	0264	250
4J	0624	611	9D	0267	253
4L	0637	624	9E	0076	61
4M	0627	614	9F	0256	242
5A	1000	1000	9G	0162	145
5B	1045	1046	9H	0170	153
5C	1054	1056	9I	0222	205
5D	1113	1115	9J	0230	213
5E	1142	1144	9K	0246	231
5F	1145	1147	9M	0255	240
5G	1163	1166	9N	0261	245
5H	1224	1227	9Z	0377	340
5I	1226	1231			
5J	1230	1233			
5K	1247	1252			
5L	1256	1261			
5M	1265	1270			
5N	1734	1764			
5O	1743	1774			
5P	1755	2007			
6A	1303	1307			
6B	1313	1320			
6C	1320	1326			
6D	1334	1343			
6E	1351	1361			
6F	1361	1372			
6G	1371	1403			
6H	1374	1407			
6I	1401	1415			
7A	1406	1423			
7B	1427	1444			
7C	1431	1446			
7D	1435	1452			
7E	1446	1463			
7F	1452	1467			
7G	1457	1475			
7H	1501	1520			


```

CONT
20 0770      770 READ IN CARDIAC OUTPUT DATA
21 6270      6/270
22 0750      750
23 7271      7/271
24 0067      SET&7
25 4271      1T*1+4000
26 6052      JMP&A [PRINT TITLE AND VALUES
27 0770      770 READ IN STROKE VOLUME DATA
30 6274      6/274
31 0750      750
32 7275      7/275
33 1020      LDA&
34 0001      1
35 4125      STC9A
36 0067      SET&7
37 4306      1U*1+4000
40 6052      JMP&A [PRINT TITLE AND VALUES
41 0751      751 READ IN PULSE RATE DATA
42 1276      1/276
43 0067      SET&7
44 4320      1V*1+4000
45 6052      JMP&A [PRINT TITLE AND VALUES
46 6671      JMP671
47 0641      UMB1
50 0600      LMB0
51 6433      JMP433 [JUMP TO MAIN DISPLAY
[PRINT TITLE
52 0046      #8A SET6
53 0000      0
54 0011      CLR
55 4255      STC9M
56 6671      JMP671 [PRINT CR+LF
57 6671      JMP671
60 1327      #8B LDH&7 [LOAD ONE CHARACTER
61 1420      SHD& [SEE IF END OF CHARACTER STRING
62 7700      7700
63 6066      JMP&C [COME HERE IF END
64 6642      JMP642 [OTHERWISE PRINT CHARACTER
65 6060      JMP&B [GET NEXT CHARACTER
[PRINT VALUES
66 0052      #8C SET12
67 0377      9Z
70 0071      SET&11 [SKIP FIRST VALUE IN EACH
71 3000      3000 [GROUP AS IT IS INCORRECT
72 0011      CLR
73 4261      STC9N [CLEAR LOCATIONS TO BE OCCUPIED
74 4262      STC9N+1 [BY THE FIRST AVERAGE VALUE
75 4263      STC9N+2
76 0070      #9E SET&10 [SET 4 VALUES/LINE
77 7773      7773
100 6671      JMP671
101 6671      JMP671
102 0011      CLR [CLEAR LOCATIONS TO BE OCCUPIED
103 4256      STC9F [BY THE NEXT AVERAGE VALUE
104 4257      STC9F+1
105 4260      STC9F+2
106 0415      KST [IF EOL KEY STRUCK, GET NEXT SET

```

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CONT
107 6115      JMP9B [OF VALUES, OR IF THE LAST SET
110 0515      KED   [IS PRINTED, GO TO THE MAIN DISPLAY
111 1460      SAE&  [ROUTINE IN PAGE 0
112 0012      0012
113 6115      JMP9B [IF NOT EOL, CONTINUE SAMPLING
114 6006      JMP6
115 1031      #9B LDA&11 [LOAD A WITH VALUE
116 1040      STA
117 0266      9C+2
120 0353      SCR13
121 4265      STC9C+1
122 7743      JMP1743 [FLOAT
123 7513      *9C
124 1020      LDA&
125 0012      #9A 12
126 1040      STA
127 0271      9D+2
130 0353      SCR13
131 4270      STC9D+1
132 7743      JMP1743 [FLOAT
133 7510      *9D
134 7054      JMP1054
135 0264      9C
136 0267      9D
137 0267      9D
140 7000      JMP1000 [ADD VALUE TO CONTENTS OF 9F
141 0267      9D
142 0256      9F
143 0256      9F
144 7734      JMP1734
145 0267      9D
146 6046      *7Z
147 6400      JMP400 [PRINT VALUE
150 6640      JMP640 [PRINT 5 SPACES
151 6640      JMP640
152 6640      JMP640
153 6640      JMP640
154 6640      JMP640
155 0230      XSK&10 [SKIP IF 4 VALUES PRINTED
156 6115      JMP9B [OTHERWISE GET NEXT VALUE
157 6671      JMP671
160 0067      SET&7
161 4334      1W=1+4000
162 1327      #9G LDH&7 [AVERAGE
163 1420      SHD&
164 7700      7700
165 6170      JMP9H [JUMP IF END OF CHARACTER STRING
166 6642      JMP642 [PRINT CHARACTER
167 6162      JMP9G [GET NEXT CHARACTER
170 6640      #9H JMP640
171 6640      JMP640
172 6640      JMP640
173 1020      LDA&
174 0004      4
175 1040      STA
176 0266      9C+2
177 0353      SCR13

```

```

CONT
200 4265 STC9C+1
201 7743 JMP1743
202 7513 *9C
203 7163 JMP1163 [FIND AVERAGE
204 0256 9F
205 0264 9C
206 0256 9F
207 7734 JMP1734
210 0256 9F
211 6046 =7Z
212 6400 JMP400 [PRINT IT
213 6640 JMP640 [PRINT 5 SPACES
214 6640 JMP640
215 6640 JMP640
216 6640 JMP640
217 6640 JMP640
220 0067 SFT&7
221 4340 1X=1+4000
222 1327 #9I LDH&7 [NORMALIZED VALUE
223 1420 SHD&
224 7700 7700
225 6230 JMP9J [JUMP IF END OF CHARACTER STRING
226 6642 JMP642 [PRINT CHARACTER
227 6222 JMP9I [GET NEXT CHARACTER
230 6640 #9J JMP640
231 6640 JMP640
232 6640 JMP640
233 1000 LDA [SEE IF AVERAGE OF FIRST 4 VALUES
234 0255 9M
235 0470 AZE& [SKIP IF NOT THE FIRST
236 6246 JMP9K
237 7163 JMP1163 [DIVIDE PRESENT AVERAGE
240 0256 9F [BY FIRST AVERAGE
241 7516 *9N
242 6400 JMP400 [PRINT NORMALIZED VALUE
243 0232 XSK&12 [SKIP IF REQUIRED NO. OF VALUES PRINTED
244 6076 JMP9E [OTHERWISE GET NEXT 4 VALUES
245 6006 JMP6 [EXIT
246 1020 #9K LDA&
247 0001 1
250 4255 STC9M
251 7734 JMP1734 [PUT AVERAGE UALUE IN
252 0256 9F [9N SO THAT NORMALIZED
253 7516 =9N [VALUE WILL BE 1
254 6237 JMP9J+7
255 0000 #9M 0 [FLAG = SET AFTER FIRST AVERAGE IN EACH
    [GROUP OF VALUES IS COMPUTED
256 0000 #9F 0 [HOLDS PRESENT AVERAGE
257 0000 0
260 0000 0
261 0000 #9N 0 [HOLDS FIRST AVERAGE
262 0000 0
263 0000 0
264 0000 #9C 0
265 0000 0
266 0000 0
267 0000 #9D 0

```

```

      CONT
270 0000      0
271 0000      0
      [TEXT
272 2624 #1T 2624 [CARDIAC OUTPUT IN CC/MIN
273 4527      4527
274 3424      3424
275 2614      2614
276 4250      4250
277 4743      4743
300 5047      5047
301 1434      1434
302 4114      4114
303 2626      2626
304 6421      6421
305 4034      4034
306 4177      4177
307 4647 #1U 4647 [STROKE VOLUME IN CC
310 4542      4542
311 3630      3630
312 1451      1451
313 4237      4237
314 5040      5040
315 3014      3014
316 3441      3441
317 1426      1426
320 2677      2677
321 4350 #1V 4350 [PULSE RATE IN BEATS/MIN
322 3746      3746
323 3014      3014
324 4524      4524
325 4730      4730
326 1434      1434
327 4114      4114
330 2530      2530
331 2447      2447
332 4621      4621
333 4034      4034
334 4177      4177
335 2451 #1W 2451 [AVERAGE
336 3045      3045
337 2432      2432
340 3077      3077
341 4142 #1X 4142 [NORMALIZED VALUE
342 4540      4540
343 2437      2437
344 3455      3455
345 3027      3027
346 1451      1451
347 2437      2437
350 5030      5030
351 7777      7777
      $377
377 0000 #9Z 0 [NO. OF VALUES COLLECTED/4
      [0, VERSION 02
      [OUTPUT
      [CONVERSION
      [MODIFIED FOR KLEINSCHMIDT FTD 12-14=67

```

CONT

```

          $400
          [OUTPUT
          [CONVERSION
400 0055 #3L SET15
401 0000 0
402 7734 JMP5N
403 7204 =4F
404 1020 LDA&
405 7764 =13
406 5764 STC5P+7
407 0074 SET&14
410 7770 =7
411 0073 SET&13
412 7777 =0
413 0011 CLR
414 2574 ADD4F+1
415 0470 AZE&
416 4573 STC4F
417 0011 CLR
420 2573 ADD4F
421 1040 STA
422 1733 7Z+2
423 0353 SCR13
424 5732 STC7Z+1
425 7743 JMP50
426 6046 =7Z
427 7054 JMP5C
430 7220 =4A
431 7755 JMP5P
432 6046 =7Z
433 3732 ADD7Z+1
434 1060 STA&
435 0000 #3M 0
436 4637 STC4L
437 2574 ADD4F+1
440 0261 ROL&1
441 1020 LDA&
442 0017 17
443 0472 LZE&
444 3545 ADD7K
445 6642 JMP2A
446 2435 ADD3M
447 0451 APO
450 0017 COM
451 4570 STC4E
452 6601 JMP4H
453 7374 JMP6H
454 0061 SET&1
455 0573 4F
456 7334 JMP6D
457 0076 SET&16
460 0000 0
461 7045 #3N JMP5B
462 0573 4F
463 0565 4D
464 0570 4E
465 2571 ADD4E+1

```

	CONT	
466	0451	AP0
467	6502	JMP30
470	0011	CLR
471	2016	ADD16
472	1420	SHD&
473	1100	1100
474	6502	JMP30
475	0236	XSK&16
476	7734	JMP5N
477	0570	4E
500	7204	=4F
501	6461	JMP3N
502	0011	#30 CLR
503	2016	ADD16
504	0450	AZE
505	6513	JMP'+6
506	0213	XSK13
507	6513	JMP'+4
510	2574	ADD4F+1
511	0450	AZE
512	6546	JMP3Q=4
513	6642	JMP2A
514	0213	XSK13
515	6522	JMP3P
516	1020	LDA&
517	0061	61
520	6642	JMP2A
521	0233	XSK&13
522	0234	#3P XSK&14
523	6552	JMP3Q
524	1520	SRO&
525	5252	5252
526	6015	JMP15
527	1120	ADA&
530	0030	30
531	6642	JMP2A
532	0074	SET&14
533	7774	=3
534	2435	ADD3M
535	1040	STA
536	0575	4F+2
537	0353	SCR13
540	4574	STC4F+1
541	7743	JMP50
542	7204	=4F
543	1020	LDA&
544	0002	2
545	6434	JMP3M=1
546	0011	CLR
547	2435	ADD3M
550	3550	ADD7L
551	4435	STC3M
552	7163	#3Q JMP5G
553	0565	4D
554	0562	4B
555	0565	4D
556	6457	JMP3N=2

```

CONT
[CONSTANTS +
[SUBROUTINES
[LOG 2
[0.30103
557 7776 #4A 7776
560 2321 2321
561 0116 0116
[10.0
562 0004 #4B 0004
563 2400 2400
564 0000 0000
[TEM1
565 0000 #4D 0
566 0000 0
567 0000 0
[TEM2
570 0000 #4E 0
571 0000 0
572 0000 0
[TEM3
573 0000 #4F 0
574 0000 0
575 0000 0
[1.0
576 0001 #4G 0001
577 2000 2000
600 0000 0000
[10.0 TO
[THE /N/
[/N/ IN 4E
[RESULT IN 4D
601 0057 #4H SET17
602 0000 0
603 7734 JMP5N
604 0562 4F
605 6046 =7Z
606 7734 JMP5N
607 0576 4G
610 7212 =4D
611 2570 #4I ADD4E
612 0470 AZE&
613 6627 JMP4M
614 0361 SCR&1
615 4570 STC4E
616 0472 LZE&
617 6624 JMP4J
620 7054 JMP5C
621 0565 4D
622 1731 7Z
623 0565 4D
624 7054 #4J JMP5C
625 6046 =7Z
626 6611 JMP4I
627 2637 #4M ADD4L
630 0471 AP0&
631 6017 JMP17
632 7163 JMP5G

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```

CONT
633 0576      4G
634 0565      4D
635 0565      4D
636 6017      JMP17
637 0000 #4L 0
640 1020      LDA&
641 0014      14
      [6=BIT CODE
642 1120 #2A ADA&
643 0712      2D
644 4017      STC17
645 1017      LDA17
      [TTYSUB
646 4662 #2B STC2C=7
647 2000      ADD0
650 4656      STC'+6
651 2662      ADD2C=7
652 0341      SCR1
653 0545      OPR45
654 6653      JMP'=1
655 0011      CLR
656 0000      RTN
657 0000      0
660 0000      0
661 0000      0
662 0000      0
663 0000      0
664 0000      0
665 0000      0
666 0000      0
667 0000      0
670 0000      0
      [EOL
671 0011 #2C CLR
672 2000      ADD0
673 4702      STC'+7
674 1020      LDA&
675 0012      12
676 6642      JMP2A
677 1020      LDA&
700 0013      13
701 6642      JMP2A
702 0000      RTN
703 0000      0
704 0000      0
705 0000      0
706 0000      0
707 0000      0
710 0000      0
711 0000      0
      [CODES
712 7540 #2D 7540
713 7542      7542
714 7544      7544
715 7546      7546
716 7550      7550
717 7552      7552

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CONT		
720	7554	7554
721	7556	7556
722	7560	7560
723	7562	7562
724	7432	7432
725	7424	7424
726	7500	7500
727	7514	7514
730	7516	7516
731	7532	7532
732	7526	7526
733	7536	7536
734	7506	7506
735	7416	7416
736	7602	7602
737	7604	7604
740	7606	7606
741	7610	7610
742	7612	7612
743	7614	7614
744	7616	7616
745	7620	7620
746	7622	7622
747	7624	7624
750	7626	7626
751	7630	7630
752	7632	7632
753	7634	7634
754	7636	7636
755	7640	7640
756	7642	7642
757	7644	7644
760	7646	7646
761	7650	7650
762	7652	7652
763	7654	7654
764	7656	7656
765	7660	7660
766	7662	7662
767	7664	7664
770	7572	7572
771	7612	7612
772	7530	7530
773	7534	7534
774	7510	7510
775	7666	7666

[DBLFLT
 [ASSEMBLED
 [FOR Q2,3
 [DOUBLE
 [PRECISION
 [FLTG. PT.
 [SUBROUTINES
 \$1000
 [ADD
 1000 0011 #5A CLR
 1001 2000 ADD0

```

CONT
1002 7406 JMP7A
1003 1001 LDA1
1004 0017 COM
1005 1102 ADA2
1006 0454 OVF
1007 7013 JMP'+4
1010 0354 SCR14
1011 1660 BCO&
1012 7737 7737
1013 0361 SCR&1
1014 0261 ROL&1
1015 0472 LAE&
1016 0017 COM
1017 5566 STC7M+1
1020 7401 JMP6I
1021 0452 LZE
1022 7374 JMP6H
1023 1001 LDA1
1024 1043 STA3
1025 1022 LDA&2
1026 1063 STA&3
1027 1022 LDA&2
1030 1063 STA&3
1031 7565 JMP7M
1032 7501 JMP7H
1033 7523 JMP7I+2
1034 7371 JMP6G
1035 1023 LDA&3
1036 7322 JMP6C+2
1037 0041 SET1
1040 1372 6G+1
1041 0062 SET&2
1042 0000 0
1043 7334 JMP6D
1044 7623 JMP7Q
[SUBTRACT
1045 0011 #5B CLR
1046 2000 ADD0
1047 7406 JMP7A
1050 7401 JMP6I
1051 7332 JMP6D+2
1052 7374 JMP6H
1053 7003 JMP5A+3
[MULTIPLY
1054 0011 #5C CLR
1055 2000 ADD0
1056 7406 JMP7A
1057 1001 LDA1
1060 1102 ADA2
1061 7352 JMP6E+1
1062 5142 STC5E
1063 7320 JMP6C
1064 7401 JMP6I
1065 7334 JMP6D
1066 7374 JMP6H
1067 7334 JMP6D
1070 1022 LDA&2

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	CONT	
1071	1022	LDA&2
1072	0301	ROR1
1073	1042	STA2
1074	7374	JMP6H
1075	1021	LDA&1
1076	1262	MUL&2
1077	1043	STA3
1100	0005	ZTA
1101	1063	STA&3
1102	1021	LDA&1
1103	0301	ROR1
1104	1262	MUL&2
1105	0241	ROL1
1106	1063	STA&3
1107	7376	JMP6H+2
1110	1021	LDA&1
1111	1242	MUL2
1112	7145	JMP5F
1113	7374	#5D JMP6H
1114	1021	LDA&1
1115	1021	LDA&1
1116	0301	ROR1
1117	1262	MUL&2
1120	7145	JMP5F
1121	7371	JMP6G
1122	1023	LDA&3
1123	1023	LDA&3
1124	0261	ROL&1
1125	0241	ROL1
1126	1560	BCL&
1127	7776	7776
1130	5622	STC7P
1131	7371	JMP6G
1132	1023	LDA&3
1133	0261	ROL&1
1134	1063	STA&3
1135	7371	JMP6G
1136	1003	LDA3
1137	1063	STA&3
1140	7371	JMP6G
1141	1020	LDA&
1142	0000	#5E 0
1143	1043	STA3
1144	7623	JMP70
1145	5723	#5F STC7X
1146	7313	JMP6B
1147	5724	STC7X+1
1150	0061	SET&1
1151	1722	7X=1
1152	7371	JMP6G
1153	7501	JMP7H
1154	0062	SET&2
1155	7777	=0
1156	7525	JMP7I
1157	1520	SRO&
1160	2525	2525
1161	7113	JMP5D

PRINT1.14 LN=1164

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	CONT	
1162	7121	JMP5D+6
		CDIVIDE
1163	0011	#5G CLR
1164	2000	ADD0
1165	7406	JMP7A
1166	3545	ADD7K
1167	5231	STC5J+1
1170	1022	LDA&2
1171	0470	AZE&
1172	0000	HLT
1173	7374	JMP6H
1174	1002	LDA2
1175	0017	COM
1176	1101	ADA1
1177	7352	JMP6E+1
1200	7320	JMP6C
1201	7374	JMP6H
1202	7334	JMP6D
1203	7401	JMP6I
1204	7334	JMP6D
1205	7374	JMP6H
1206	1021	LDA&1
1207	1063	STA&3
1210	1021	LDA&1
1211	1063	STA&3
1212	1022	LDA&2
1213	0017	COM
1214	5724	STC7X+1
1215	1022	LDA&2
1216	0017	COM
1217	5725	STC7X+2
1220	5723	STC7X
1221	5726	STC7Y
1222	0062	SET&2
1223	1720	7X=3
1224	7376	#5H JMP6H+2
1225	7227	JMP'+2
1226	7403	#5I JMP6I+2
1227	7501	JMP7H
1230	1520	#5J SRO&
1231	0001	0001
1232	7265	JMP5M
1233	0065	SET&5
1234	7777	=0
1235	7371	JMP6G
1236	1023	LDA&3
1237	0450	AZE
1240	7244	JMP5K=3
1241	1023	LDA&3
1242	0470	AZE&
1243	7251	JMP5K+2
1244	0011	CLR
1245	7371	JMP6G
1246	1023	LDA&3
1247	0451	#5K APO
1250	7256	JMP5L
1251	1002	LDA2

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CONT
1252 1600 BSE
1253 1231 5J+1
1254 1042 STA2
1255 0225 XSK&5
1256 0041 #5L SET1
1257 1372 6G+1
1260 7371 JMP6G
1261 7501 JMP7H
1262 0205 XSK5
1263 7224 JMP5H
1264 7226 JMP5I
1265 0222 #5M XSK&2
1266 0222 XSK&2
1267 0222 XSK&2
1270 1520 SRO&
1271 3333 3333
1272 7233 JMP5J+3
1273 7371 JMP6G
1274 0011 CLR
1275 3723 ADD7X
1276 1063 STA&3
1277 0011 CLR
1300 3726 ADD7Y
1301 1063 STA&3
1302 7623 JMP7Q
      [MOVE 1 TO 2
1303 1001 #6A LDA1
1304 1042 STA2
1305 1021 LDA&1
1306 1062 STA&2
1307 1021 LDA&1
1310 1062 STA&2
1311 0011 CLR
1312 6000 JMP0
      [Z TO A
1313 0005 #6B ZTA
1314 0241 ROL1
1315 0455 ZZZ
1316 3545 ADD7K
1317 6000 JMP0
      [COM SETUP
1320 1021 #6C LDA&1
1321 1662 BCO&2
1322 0261 ROL&1
1323 1020 LDA&
1324 0016 NOP
1325 0452 LZE
1326 3331 ADD'+3
1327 5670 STC7S
1330 6000 JMP0
1331 7314 JMP6D=20
1332 0062 SET&2
1333 7777 =0
      [COM/ABS 1
1334 1021 #6D LDA&1
1335 0361 SCR&1
1336 0261 ROL&1

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CONT
1337 0202 XSK2
1340 0452 LZE
1341 0017 COM
1342 1041 STA1
1343 1021 LDA&1
1344 0202 XSK2
1345 0452 LZE
1346 0017 COM
1347 1041 STA1
1350 6000 JMP0
COVF CHECK
1351 1103 #6E ADA3
1352 0470 AZE&
1353 0011 CLR
1354 1043 STA3
1355 0454 OVF
1356 6000 JMP0
1357 0451 APO
1360 0000 HLT
[RESULT=0
1361 7371 #6F JMP6G
1362 1020 LDA&
1363 4000 =3777
1364 1043 STA3
1365 0011 CLR
1366 1063 STA&3
1367 1063 STA&3
1370 7672 JMP7T
[SET3
1371 0063 #6G SET&3
1372 0000 0
1373 6000 JMP0
[SET NORMAL
1374 0062 #6H SET&2
1375 5726 7Y+4000
1376 0061 SET&1
1377 1723 7X
1400 6000 JMP0
[SET REVERSE
1401 0062 #6I SET&2
1402 1723 7X
1403 0061 SET&1
1404 1726 7Y
1405 6000 JMP0
[SETUP
1406 1560 #7A BCL&
1407 6000 6000
1410 4004 STC4
1411 2000 ADD0
1412 5446 STC7E
1413 1004 LDA4
1414 7457 JMP7G
1415 7452 JMP7F
1416 5431 STC7C
1417 1024 LDA&4
1420 7457 JMP7G
1421 7447 JMP7E+1

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CONT
1422 5435      STC7D
1423 1024      LDA&4
1424 7457      JMP7G
1425 0016      NOP
1426 5372      STC6G+1
1427 7401 #7B  JMP6I
1430 0061      SET&1
1431 0000 #7C  0
1432 7303      JMP6A
1433 0222      XSK&2
1434 0061      SET&1
1435 0000 #7D  0
1436 7303      JMP6A
1437 0224      XSK&4
1440 2004      ADD4
1441 3407      ADD7A+1
1442 5672      STC7T
1443 5622      STC7P
1444 7371      JMP6G
1445 7374      JMP6H
1446 0000 #7E  CRETURN
1447 5435      STC7D
1450 3454      ADD7F+2
1451 7426      JMP7B=1
1452 5435 #7F  STC7D
1453 1020      LDA&
1454 1731      7Z
1455 5431      STC7C
1456 7450      JMP7E+2
      CIR+SIGN TEST
1457 0471 #7G  APO&
1460 0220      XSK&0
1461 0451      APO
1462 0017      COM
1463 1120      ADA&
1464 7760      =17
1465 0361      SCR&1
1466 0261      ROL&1
1467 3462      ADD7G+3
1470 0472      LZE&
1471 6000      JMP0
1472 4001      STC1
1473 1001      LDA1
1474 3667      ADD7S=1
1475 1041      STA1
1476 1120      ADA&
1477 7774      =3
1500 6000      JMP0
      CADD 1 TO 3
1501 0044 #7H  SET4
1502 0000      0
1503 0011      CLR
1504 7371      JMP6G
1505 1021      LDA&1
1506 5531      STC7J
1507 1023      LDA&3
1510 5533      STC7J+2

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PRINT1.20 LN=1530

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CONT
1511 1001 LDA1
1512 1203 LAM3
1513 1021 LDA&1
1514 1223 LAM&3
1515 7371 JMP6G
1516 4000 STC0
1517 1223 LAM&3
1520 4000 STC0
1521 1223 LAM&3
1522 6004 JMP4
1523 0062 SET&2
1524 0000 0
      [CHECK FOR
      [ADD OVERFLOW
1525 0041 #7I SET1
1526 0000 0
1527 7371 JMP6G
1530 1020 LDA&
1531 0000 #7J 0
1532 1660 BCO&
1533 0000 0
1534 0451 APO
1535 6001 JMP1
1536 1023 LDA&3
1537 1640 BCO
1540 1531 7J
1541 0471 APO&
1542 6001 JMP1
1543 7371 JMP6G
1544 1020 LDA&
1545 0001 #7K 1
1546 7351 JMP6E
1547 1020 LDA&
1550 7776 #7L =1
1551 0202 XSK2
1552 7567 JMP7M+2
1553 3622 ADD7P
1554 0202 XSK2
1555 0017 COM
1556 5622 STC7P
1557 7371 JMP6G
1560 1023 LDA&3
1561 1660 BCO&
1562 4000 4000
1563 1043 STA3
1564 6001 JMP1
      [SCR N 3
1565 1020 #7M LDA&
1566 0000 0
1567 0042 SET2
1570 0000 0
1571 0470 AZE&
1572 6002 JMP2
1573 4005 STC5
1574 0064 SET&4
1575 7747 =30
1576 0011 #70 CLR
```


PRINT1,21 LN=1621

224

	CONT	
1577	7371	JMP6G
1600	1023	LDA&3
1601	0361	SCR&1
1602	1043	STA3
1603	1023	LDA&3
1604	0321	ROR&1
1605	1043	STA3
1606	0224	XSK&4
1607	7611	JMP'+2
1610	7613	JMP'+3
1611	0225	XSK&5
1612	7576	JMP70
1613	7371	JMP6G
1614	1023	LDA&3
1615	0261	ROL&1
1616	0452	LZE
1617	0017	COM
1620	5622	STC7P
1621	6002	JMP2
1622	0000	#7P 0
		[NORMALIZE,
		[ROUND,XIT
1623	0011	#7Q CLR
1624	4001	STC1
1625	3622	ADD7P
1626	0321	ROR&1
1627	7371	JMP6G
1630	1023	LDA&3
1631	1463	SAE&3
1632	7637	JMP'+5
1633	0450	AZE
1634	7637	JMP'+3
1635	0472	LZE&
1636	7361	JMP6F
1637	7371	JMP6G
1640	1023	LDA&3
1641	0451	AP0
1642	7704	JMP7U
1643	0241	ROL1
1644	0471	AP0&
1645	7673	JMP7T+1
1646	7371	#7R JMP6G
1647	1023	LDA&3
1650	1023	LDA&3
1651	0321	ROR&1
1652	4000	STC0
1653	1203	LAM3
1654	7371	JMP6G
1655	4000	STC0
1656	1223	LAM&3
1657	0451	AP0
1660	7706	JMP7V
1661	7371	JMP6G
1662	0011	CLR
1663	2001	ADD1
1664	0017	COM
1665	7351	JMP6E

PRINT1.22 LN=1712

225

	CONT	
1666	0041	SET1
1667	0003	3
1670	0016	#7S NOP
1671	0011	CLR
1672	0000	#7T EXIT
1673	1023	LDA&3
1674	0261	ROL&1
1675	1043	STA3
1676	7371	JMP6G
1677	1023	LDA&3
1700	0261	ROL&1
1701	1043	STA3
1702	0221	XSK&1
1703	7643	JMP7R=3
1704	7706	#7U JMP7V
1705	7646	JMP7R
1706	0011	#7V CLR
1707	2000	ADD0
1710	5722	STC7W
1711	3550	ADD7L
1712	7567	JMP7M+2
1713	3550	ADD7L
1714	2001	ADD1
1715	4001	STC1
1716	1003	LDA3
1717	1560	BCL&
1720	4000	4000
1721	1043	STA3
1722	0000	#7W ERTN
		[ARG 1
1723	0000	#7X 0
1724	0000	0
1725	0000	0
		[ARG 2
1726	0000	#7Y 0
1727	0000	0
1730	0000	0
		[FAC
1731	0000	#7Z 0
1732	0000	0
1733	0000	0
		[TRANSFER
1734	0011	#5N CLR
1735	2000	ADD0
1736	7406	JMP7A
1737	0042	SET2
1740	1435	7D
1741	7303	JMP6A
1742	7671	JMP7T=1
		[FLOAT
1743	0011	#50 CLR
1744	2000	ADD0
1745	7406	JMP7A
1746	3435	ADD7D
1747	5372	STC6G+1
1750	7371	JMP6G
1751	1020	LDA&

PRINT1.23 LN=2003

226

	CONT	
1752	0027	27
1753	1043	STA3
1754	7035	JMP5B=10
	CFIX	
1755	0011	#5P CLR
1756	2000	ADD0
1757	7406	JMP7A
1760	3435	ADD7D
1761	5372	STC6G+1
1762	7371	JMP6G
1763	1020	LDA&
1764	7750	=27
1765	7351	JMP6E
1766	0471	APO&
1767	7672	JMP7T
1770	7567	JMP7M+2
1771	7671	JMP7T=1

APPENDIX

OPERATIONAL DETAILS

TAPES

Mount LAP6 - 2S on unit 0, LAP6 - 2S file with programs on unit 1, and a scratch tape on unit 5.

SCOPE DISPLAY OF TEST - initial (INT - DSP) and
final (FIN - DSP1)

Both utilize SCOPE - SP.

In all cases where blanks are to be filled, the number of typed entries must equal the number of blanks.

One constant, rho, is initially set equal to 150 ohm cm. If this value is correct, type EOL and the next display will appear. If incorrect, type DEL to erase the 150, and then enter the correct value followed by EOL.

If the keyboard should lock down while selections are being made or blanks being filled, type the character (s) again and the display will reappear.

Needless to say - make sure there is an analog input signal before typing S-EOL. Likewise, make sure the printer and plotter are on before selecting them for output. Before plotting, position the pen at the right hand margin (small holes). After the first graph, the pen will be positioned under program control.

COPYING PROGRAMS FROM MASTER TAPE TO USER TAPE

To copy COCAL, INT-DSP, COMPUTE1, FIN-DSP1, PLOT1, and PRINT1 from the Master tape on which they now reside (JUNCKER LAP6 - 2S FILE) onto another tape, use LAP6 - 2S and the copy file command (→CF UNIT EOL). These six routines are the only entries in the Master tape file index, so that copying all the entries will not result in unwanted programs being transferred to the user's tape.

EXAMINATION OF THE FILE INDEX BY COCAL

All six routines must exist on the same tape and be listed in that tape's file index. As mentioned previously, this tape is mounted on unit 1. Once in execution, COCAL searches the tape for the file index, examining first blocks 426-7. When found, the index is searched for INT-DSP, COMPUTE1, FIN-DSP1, PLOT1 and PRINT1. The block numbers of these routines are inserted into appropriate locations in COCAL*. If a routine is not found, the computer halts at location (1234)₈.

DATA STORAGE

Cardiac output values are at present stored in blocks 270 and 271, stroke volume in blocks 274 and 275, and pulse rate in blocks 276 and 277 of the scratch tape mounted on unit 5. Should the user wish to store the data elsewhere, he must modify the read/write instructions in COMPUTE1, FIN-DSP1, PLOT1 and PRINT1.

*The block numbers shown in the listing of COCAL are not necessarily correct.

USE OF PAGES BY THE PROGRAM

	<u>Before Sampling</u>	<u>During Sampling</u>	<u>Final Display</u>
Page 0	COCAL 0 - 1304 includes the routine to examine the file index	COCAL 0 - 774 C.O. values 1000 - 1777	COCAL 0 - 774 C.O. or S.V. or P.R. 1000 - 1777
Page 1	INT-DSP	raw data	raw data
Page 2	COMPUTEL	COMPUTEL	FIN-DSP1
Page 3	- - - -	S.V. and P.R. values	PLOT1 or PRINT1

RESTARTING COCAL FROM THE CONSOLE

To restart COCAL at the beginning:*

- 1) Redefine the lower memory bank to be 0
Set left switches: LMB0 (code 600)
Raise D0 lever
- 2) Redefine the upper memory bank to be 1
Set left switches: UMB1 (code 641)
Raise D0 lever
- 3) Start at location (47)₈
Set the right switches: (47)₈
Press the START RSW button

To restart the final display routine in COCAL in the event, for example, the computer tries to plot data but the plotter has not been turned on, repeat steps #1 and #2 but start the program at location (433)₈.

ERROR IN T

There is a small amount of error in the computation of time T between beats. A time gap exists between the sampling of successive beats which needs to be considered for accurate measurement of pulse rate. This gap equals the time spent in calculating stroke volume, cardiac output, and pulse rate. The estimated value of this gap is 62 ms. (18 ms. in COCAL, 44 ms. in COMPUTEL). Converting this value to locations gives 31 locations or, when rounded off, 30 locations. I added the octal equivalent of 30, 36, to the time T as calculated by COCAL in locations 372 - 376.

The user may wish to add a number other than 36. If so, he should change the contents of location 374.

*LAP6-2S and → LOCOCAL,1_{EOL} may also be used.

Computation of Stroke Volume

$$\rho = \rho\text{-ohm cm} \quad (\text{rho})$$

$$L^2 = (L\text{cm}/10)^2 \quad L \text{ is multiplied by 10 when entered}$$

$$\tau = (t \text{ addresses})(2\text{ms/address})(1\text{sec}/10^3\text{ms}) = 2t \text{ sec}/10^3$$

$$\tau = (T_3 - T_1) \quad (\text{See Fig. 1})$$

$$\begin{aligned} (dZ/dt)_{\min} &= DZ \cdot 1\text{volt}/(377)_8 \cdot 100 \text{ ohms}/K \text{ volt sec} = \\ &\quad \frac{100 DZ \text{ ohms}}{(377)_8 K \text{ sec}} \end{aligned}$$

$$DZ = \text{sampld value of } (dZ/dt)_{\min}$$

$$(dZ/dt)_{\text{cal}} = 100 \text{ ohms/sec} = K \text{ volts} [(dZ/dt)_{\text{cal}} \text{ is multiplied by 100 when entered}]$$

$$\begin{aligned} Z_o &= Z \cdot 1 \text{ volt}/(377)_8 \cdot 100 \text{ ohms}/J \text{ volts} = \\ &\quad \frac{100 Z \text{ ohms}}{(377)_8 J} \end{aligned}$$

$$Z_o = \text{sampld value of } Z_o$$

$$Z_{\text{cal}} = 100 \text{ ohms} = J \text{ volts} [Z_{\text{cal}} \text{ is multiplied by 100 when entered}]$$

Insert into formula:

$$\Delta V = \rho L^2 \tau / Z_o \quad (dZ/dt)_{\min}$$

$$\text{to get:} \quad \Delta V = \frac{(\rho \text{ ohm cm})(L^2 \text{ cm}^2)(2t \text{ sec})(10^2 DZ \text{ ohms})(377)_8 J^2}{(10^2)(10^3)(377)_8 (K \text{ sec})(10^4 Z^2 \text{ ohms}^2)}$$

which reduces to:

$$\text{Stroke volume} = \Delta V = \frac{\rho L^2 t (DZ)(Z^2)}{K Z^2} \cdot \frac{51}{10^6} \text{ cm}^3$$

Computation of Pulse Rate

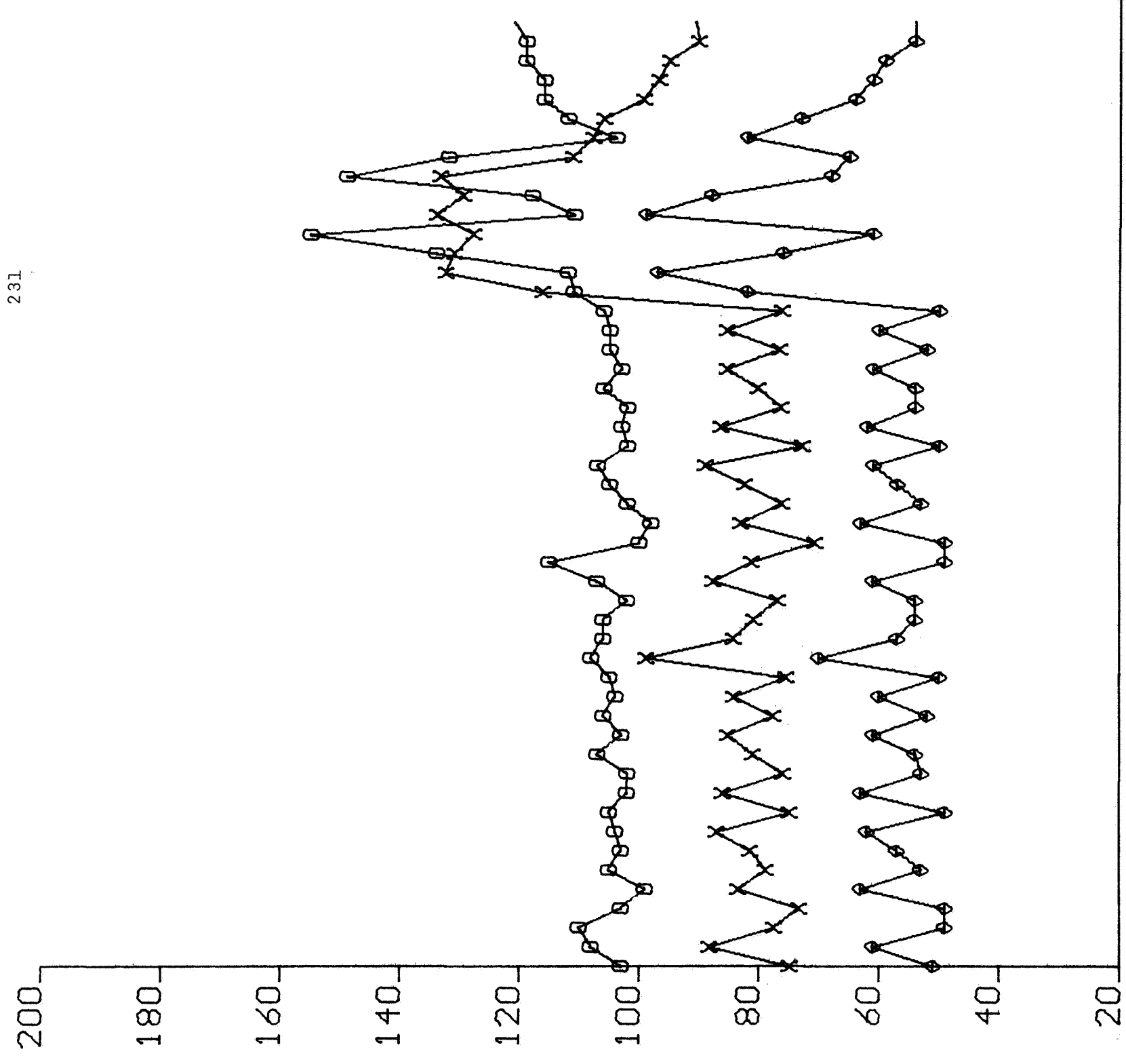
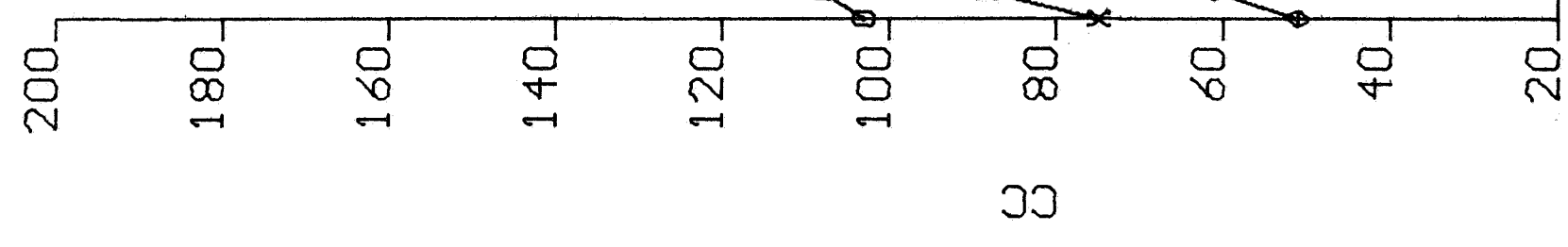
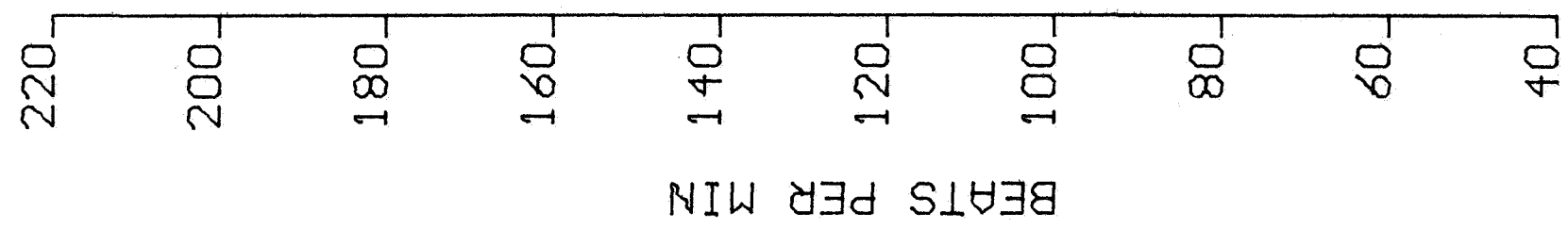
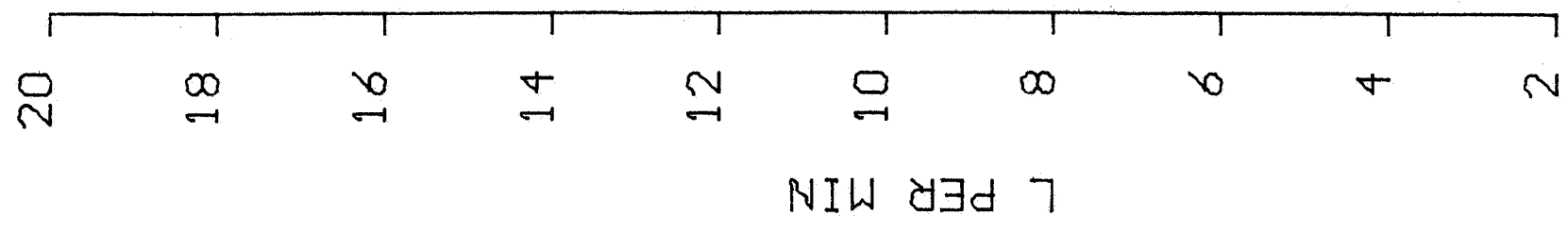
$$T = t' \text{ addresses} \cdot 2\text{ms/address} \cdot 1 \text{ sec}/10^3\text{ms} \cdot 1 \text{ min}/60 \text{ sec} = t' \text{ min}/3 \times 10^4$$

t' = time in addresses between beats (plus 36₈ to allow for computation (of c.o., etc.)

Pulse Rate = $1/T$ beats per min.

Computation of Cardiac Output

Cardiac output = $\Delta V/T$ cc/min



○—○ PULSE RATE
x—x CARDIAC OUTPUT
□—□ STROKE VOLUME

TOTAL TIME 2.4 MIN

CARDIAC OUTPUT IN CC /MIN

+7.870000E+003	+7.570000E+003	+8.210000E+003	+8.130000E+003
AVERAGE +7.945000E+003	NORMALIZED VALUE		+1.000000E+000
+8.660000E+003	+9.160000E+003	+9.390000E+003	+8.680000E+003
AVERAGE +8.972500E+003	NORMALIZED VALUE		+1.129326E+000
+7.520000E+003	+7.490000E+003	+7.320000E+003	+7.190000E+003
AVERAGE +7.380000E+003	NORMALIZED VALUE		+9.288870E=001
+7.300000E+003	+6.970000E+003	+7.860000E+003	+8.110000E+003
AVERAGE +7.560000E+003	NORMALIZED VALUE		+9.515428E=001
+8.770000E+003	+8.620000E+003	+7.930000E+003	+8.280000E+003
AVERAGE +8.400000E+003	NORMALIZED VALUE		+1.057268E+000
+7.140000E+003	+8.220000E+003	+7.940000E+003	+7.700000E+003
AVERAGE +7.750000E+003	NORMALIZED VALUE		+9.754571E=001

STROKE VOLUME IN CC

+1.060000E+002	+9.900000E+001	+1.060000E+002	+1.020000E+002
AVERAGE +1.032500E+002	NORMALIZED VALUE		+1.000000E+000
+1.060000E+002	+1.100000E+002	+1.150000E+002	+1.130000E+002
AVERAGE +1.110000E+002	NORMALIZED VALUE		+1.075060E+000
+1.070000E+002	+1.110000E+002	+1.110000E+002	+1.090000E+002
AVERAGE +1.095000E+002	NORMALIZED VALUE		+1.060532E+000
+1.060000E+002	+9.600000E+001	+1.050000E+002	+1.000000E+002
AVERAGE +1.017500E+002	NORMALIZED VALUE		+9.854731E=001
+1.040000E+002	+9.900000E+001	+9.300000E+001	+1.050000E+002
AVERAGE +1.002500E+002	NORMALIZED VALUE		+9.709453E=001
+9.600000E+001	+1.120000E+002	+1.100000E+002	+1.050000E+002
AVERAGE +1.057500E+002	NORMALIZED VALUE		+1.024212E+000

PULSE RATE IN BEATS/MIN

+7.400000E+001	+7.600000E+001	+7.700000E+001	+7.900000E+001
AVERAGE +7.650000E+001	NORMALIZED VALUE		+1.000000E+000
+8.100000E+001	+8.300000E+001	+8.100000E+001	+7.600000E+001
AVERAGE +8.025000E+001	NORMALIZED VALUE		+1.049019E+000
+7.000000E+001	+6.700000E+001	+6.500000E+001	+6.500000E+001
AVERAGE +6.675000E+001	NORMALIZED VALUE		+8.725499E=001
+6.800000E+001	+7.100000E+001	+7.400000E+001	+8.000000E+001
AVERAGE +7.325000E+001	NORMALIZED VALUE		+9.575173E=001
+8.400000E+001	+8.600000E+001	+8.400000E+001	+7.800000E+001
AVERAGE +8.300000E+001	NORMALIZED VALUE		+1.084967E+000
+7.400000E+001	+7.200000E+001	+7.100000E+001	+7.200000E+001
AVERAGE +7.225000E+001	NORMALIZED VALUE		+9.444452E=001

References

1. Clark, W. A., C. E. Molnar, The LINC: A description of the laboratory instrument computer. Annals of the New York Academy of Science, Vol. 115, pages 653-668, July 1964.
2. Clark, W. A., and C. E. Molnar. A description of the LINC in computers in biomedical research. Ed. by Ralph W. Stacy and Bruce Waxman Academic Press, New York 1965.